

Robust Optimization

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Philips Medical Systems

Learning objectives

- Describe the basics ideas and methods of robust optimization
- Describe examples in which robust optimization leads to a new quality of the treatment plans (better than margins)

Uncertainties in Radiation Therapy

- Geometric, physical, technical
 - Patient setup
 - Location of tumor & inner organs (“motion”)
 - Dose calculation
 - Beam delivery system
- Biologic, clinical
 - Volume definition (targets and OARs)
 - Dose prescription (uniform or dose painting)
 - Tolerance dose
 - EUD, NTCP, TCP models (if used)

Uncertainty and Motion

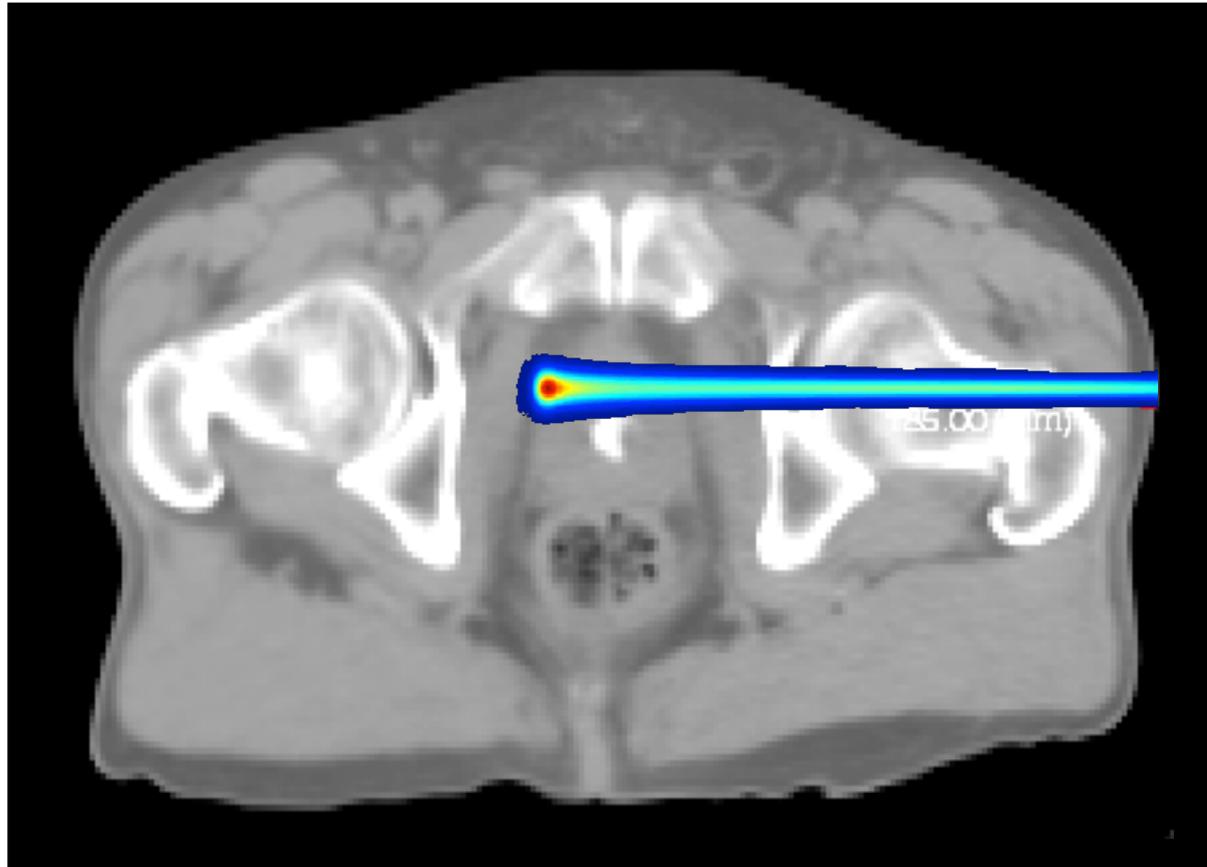
- Motion does not necessarily imply uncertainty
 - If motion is perfectly known, then there is no uncertainty. This case is “easy” to deal with.
- But, when there is motion (e.g., breathing), there are typically more potential sources of uncertainty:
 - Uncertainties in the motion characteristics such as frequency, amplitude, shape of trajectory, irregularity of the motion.

Additional uncertainties in **proton** therapy:

Range uncertainties

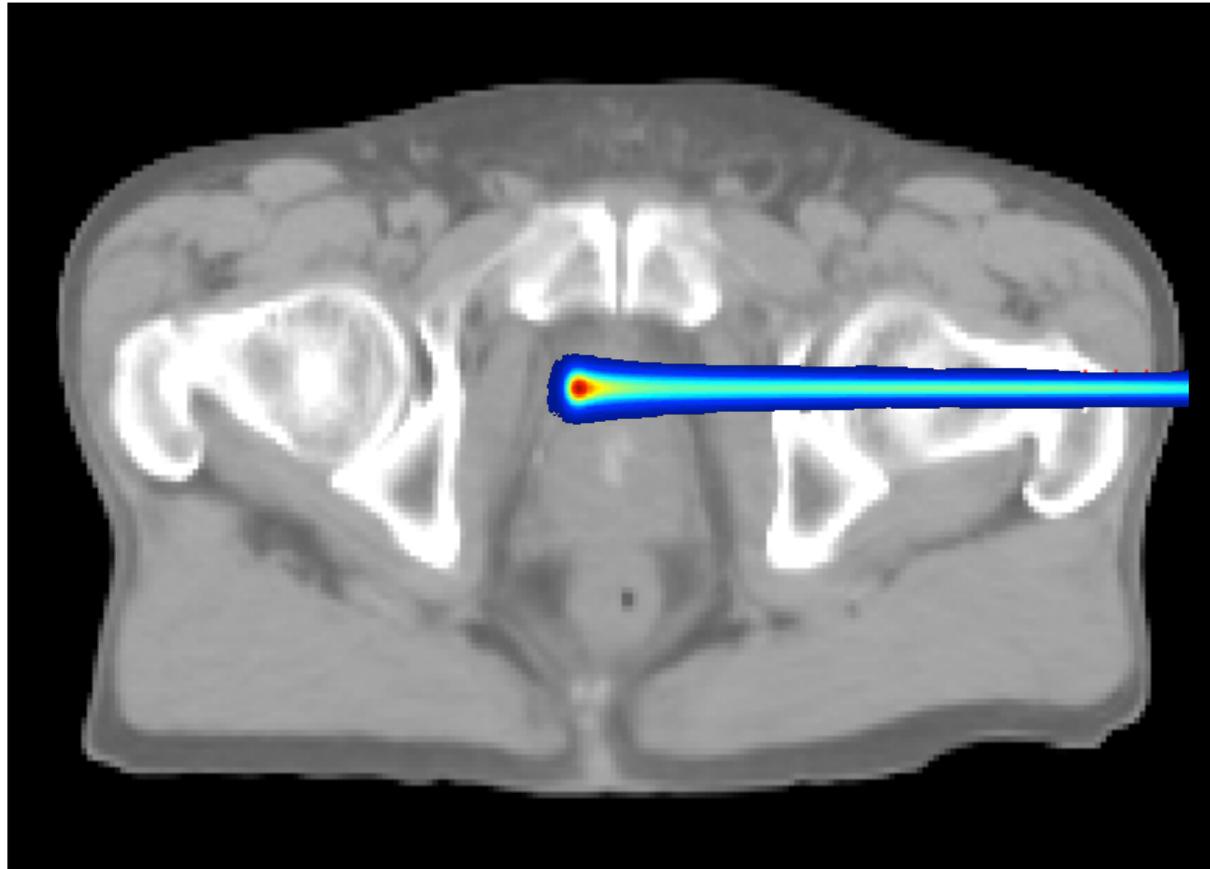
- Differences between treatment preparation and treatment delivery (~ 1 cm)
 - Daily setup variations
 - Internal organ motion
 - Anatomical/ physiological changes during treatment
- Dose calculation errors (~ 3 -5 mm)
 - Conversion of CT number to stopping power
 - Inhomogeneities, metallic implants
 - CT artifacts
- Biological effect uncertainties

Proton range uncertainties: Range uncertainties due to setup



Jan 08

Proton range uncertainties: Range uncertainties due to setup

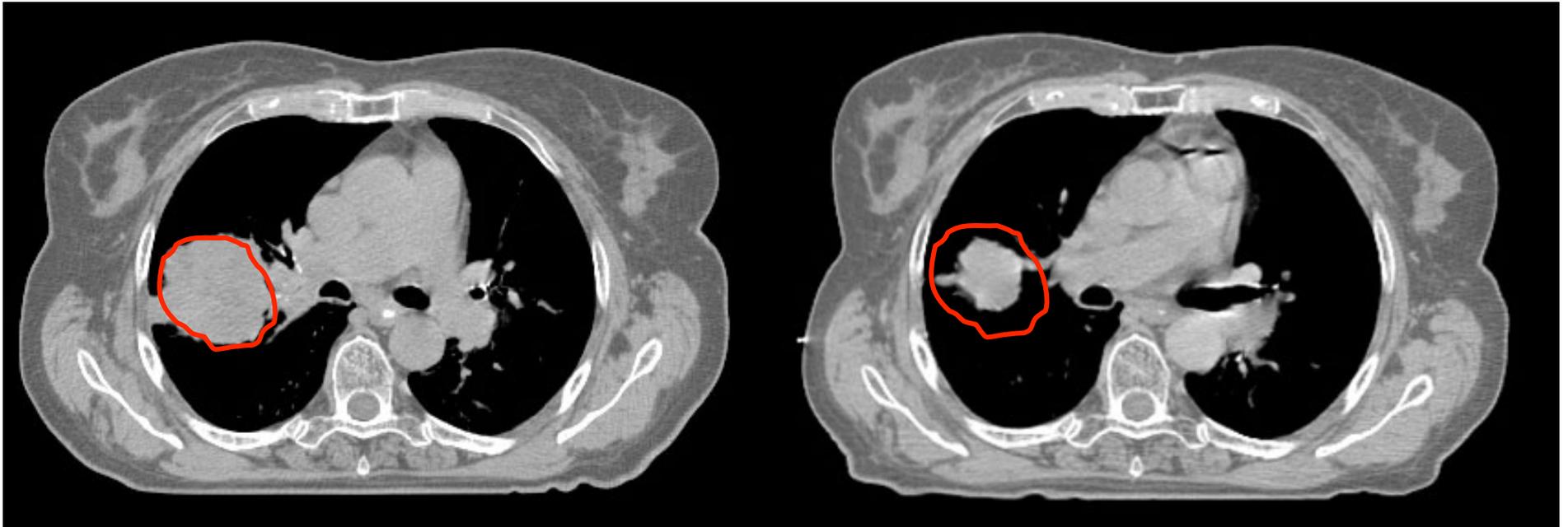


Jan 11

Proton range uncertainties: Tumor motion and shrinkage

Initial Planning CT
GTV 115 cc

5 weeks later
GTV 39 cc

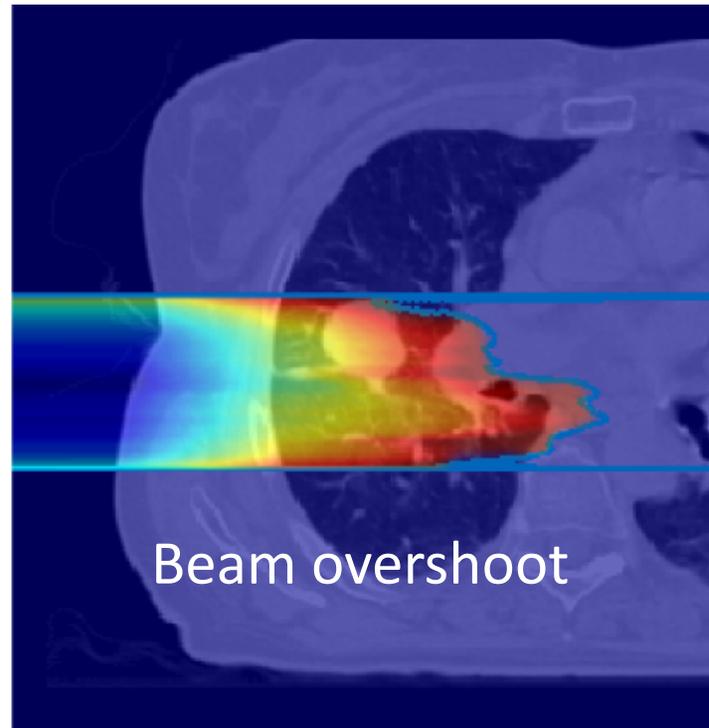
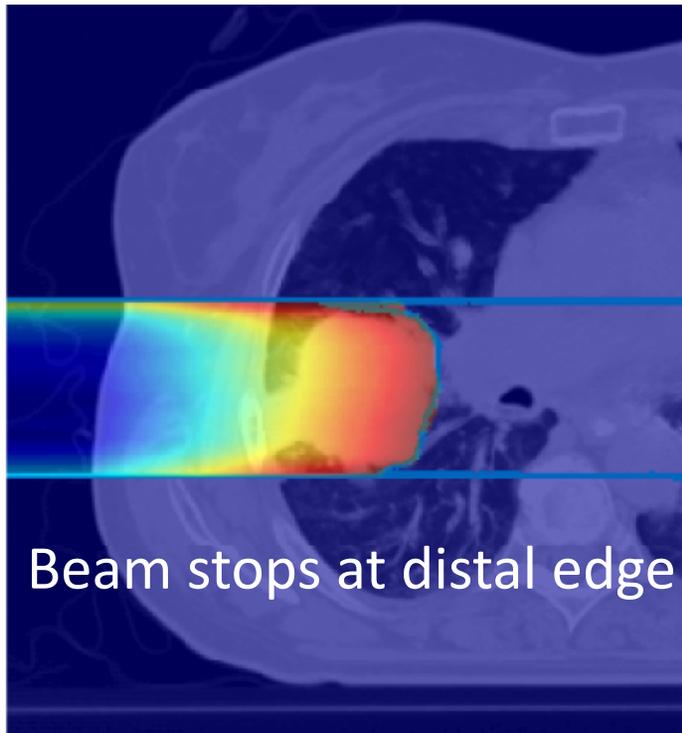


S. Mori, G. Chen

Proton range uncertainties: Tumor motion and shrinkage

What you see in the plan...

is not always what you get.



S. Mori, G. Chen



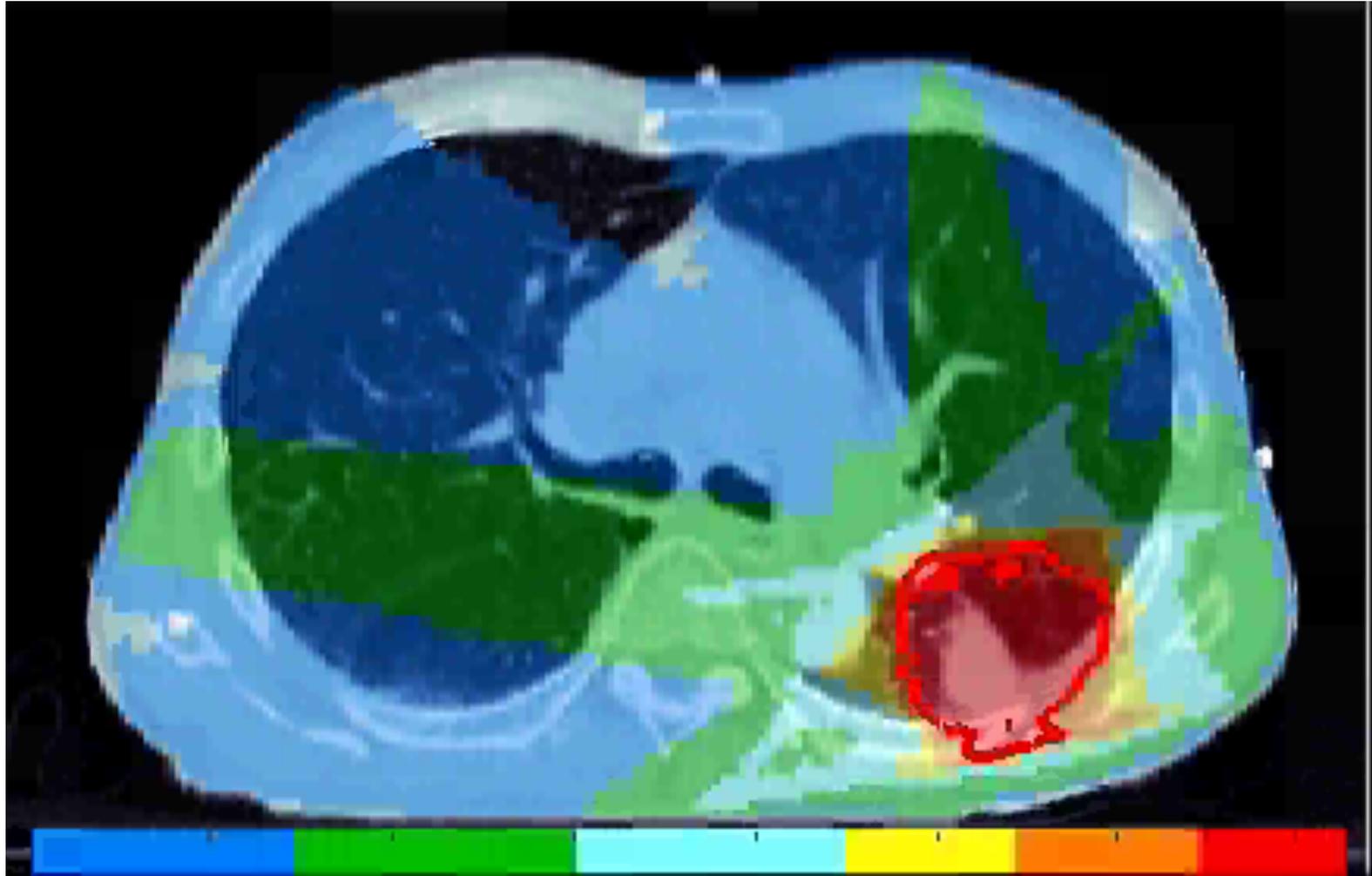
MASSACHUSETTS
GENERAL HOSPITAL

RADIATION ONCOLOGY

Margins to counteract uncertainties

- Margins around target volumes lead to higher dose to normal tissue
- PTV margins rely on “static dose cloud” assumption – not always justified
- Margins can overlap (PTV, PRV), what then?

The “static dose cloud” assumption
– ok for photons, not for protons –



- A potentially better way to deal with uncertainties:
 - Robust Optimization.

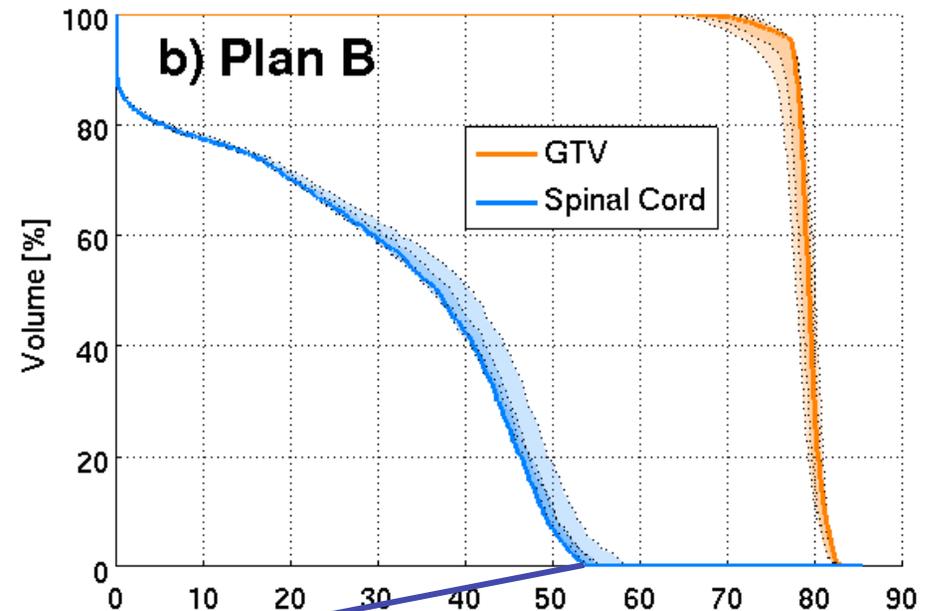
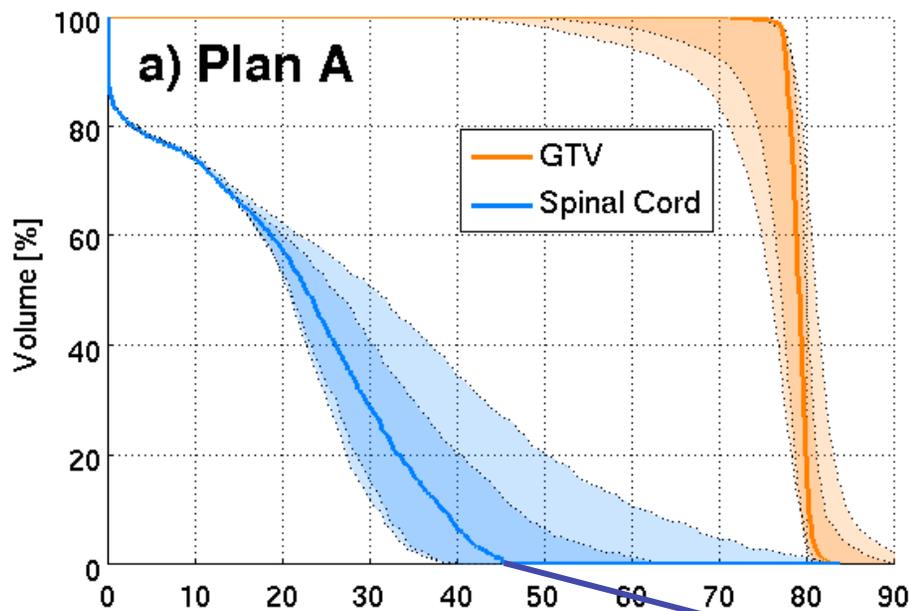
Robust Optimization – Outline

1. Uncertainties, motion, and margins ✓
2. Robust optimization principles
3. Examples of application

Robustness definition

- Robustness = immunity to uncertainty

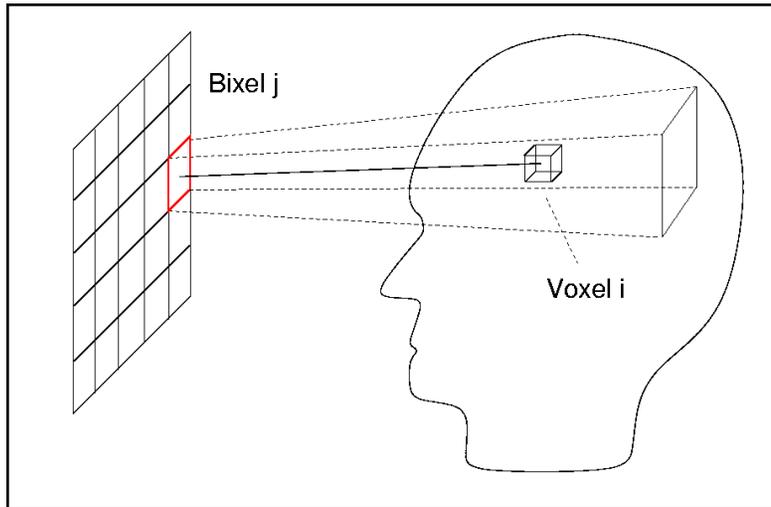
Examples: non-robust (Plan A) and robust (Plan B)



Price of robustness!

Visualize uncertainties: DVH bands, Trofimov 2011

The “standard model” of IMRT optimization



Dose is a linear function of
Bixel weights

$$d_i(x) = \sum_j D_{ij} x_j$$

Objective function

$$\underset{x}{\text{minimize}} \quad f(d(x))$$

subject to

Dosimetric constraints:

$$l_m \leq c_m(d(x)) \leq u_m \quad \forall m$$

Physical constraints:

$$x_j \geq 0 \quad \forall j$$

Robust optimization = robustness + optimization

- We want to make a treatment plan as good as possible and at the same time protect it against uncertainties
 - One thing is clear: there is always a **price of robustness**
- How can we do that?

Robust plan optimization, 2 ways:

- Consider different scenarios of treatment delivery (instances of geometry of patient positions, motion trajectories)
 1. **“Stochastic programming”**: describe uncertainties with random variables, assume probability density functions (pdf), and optimize expected value of the objective function
 2. **The worst case approach** (mathematics, Ben-Tal, Nemirovski) : make sure that constraints are fulfilled in all scenarios, and that we obtain the best plan in the worst case

1. Stochastic programming – the probabilistic approach

For different scenarios s :

$$d_i^s(x) = \sum_j D_{ij}^s x_j$$

probability of scenario s

minimize
 x

$$\langle f \rangle = \sum_s p_s f(d^s(x))$$

subject to

$$x_j \geq 0 \quad \forall j$$



1. Stochastic programming

- example: quadratic objective function

Objective function:

$$f(d) = \sum_i (d_i - d_i^{pres})^2$$

Expected dose:

$$\langle d_i \rangle = \sum_s p_s d_i^s$$

Expected objective function (to be minimized):

$$\langle f \rangle = \sum_i \left[\underbrace{(\langle d_i \rangle - d_i^{pres})^2}_{\text{average deviation}} + \underbrace{\sum_s p_s (d_i^s - \langle d_i \rangle)^2}_{\text{Variance}} \right]$$

Accuracy, bias **Variance**
Precision

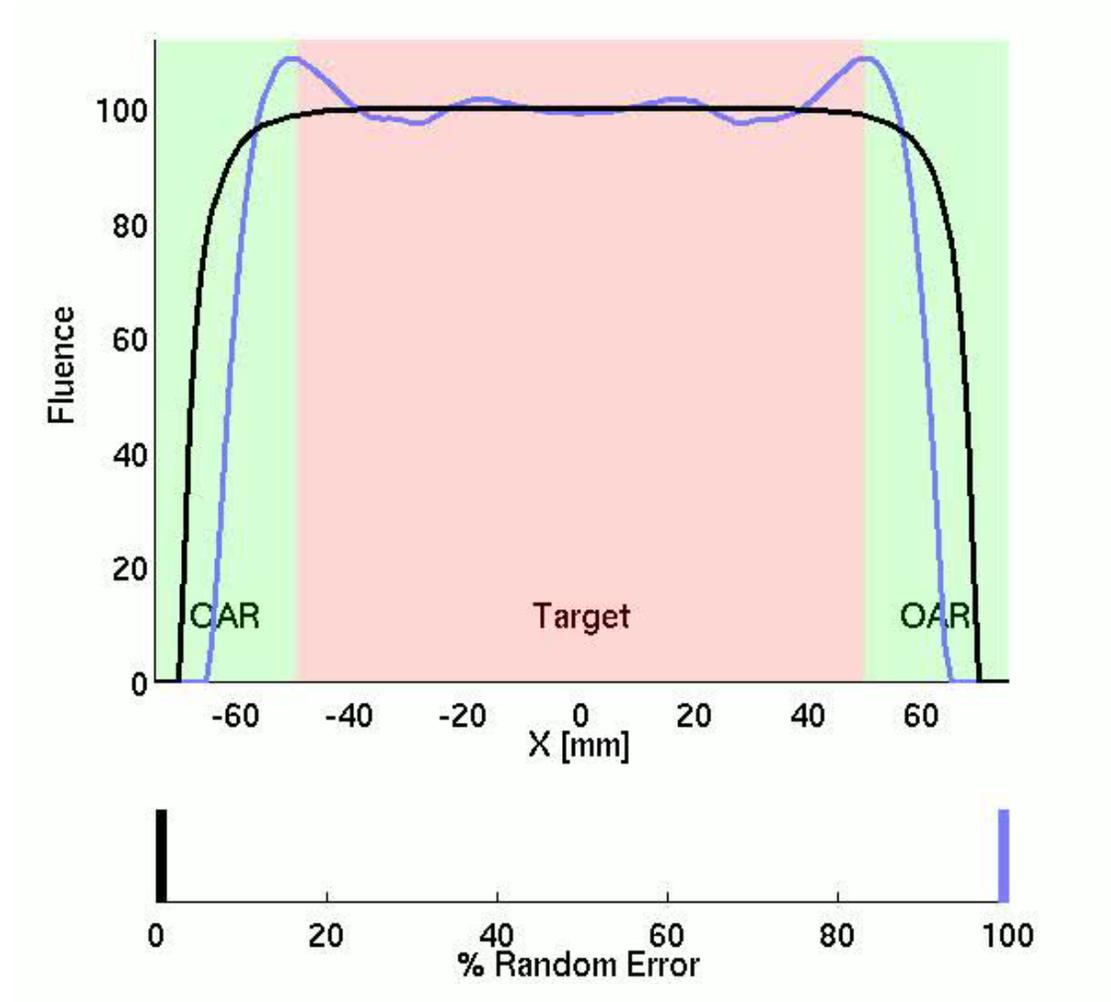
Example: setup error (1D)

- Error scenarios defined by shifting to the left or right in steps of 1mm.
- **Random error:** 32 random shifts (for 32 fractions) sampled from a Gaussian with a mean of zero and a set standard deviation σ_{Rand}
- **Systematic error:** single shift with standard deviation σ_{Sys} added to the random shift above
- Objective function:

$$f(d) = w_T \sum_{i \in T} (d_i - D^{\text{pres}})^2 + w_{HT} \sum_{i \in HT} (d_i)^2$$

Example: setup error (1D)

$$(10 \text{ mm})^2$$
$$\sigma_{Tot}^2 = \sigma_{Rand}^2 + \sigma_{Sys}^2$$



Observations:

- Random errors require smaller margins than systematic errors -> van Herk margin recipe.
- A new type of dose distribution emerges from the probabilistic approach: beam “horns” instead of margins.

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2. Worst case approach

For different scenarios s :
$$d_i^s(x) = \sum_j D_{ij}^s x_j$$

minimize $\left[\max_s f(d^s) \right]$

subject to

$$l_m \leq c_m(d^s(x)) \leq u_m \quad \forall m, \quad \forall s$$

$$x_j \geq 0 \quad \forall j$$

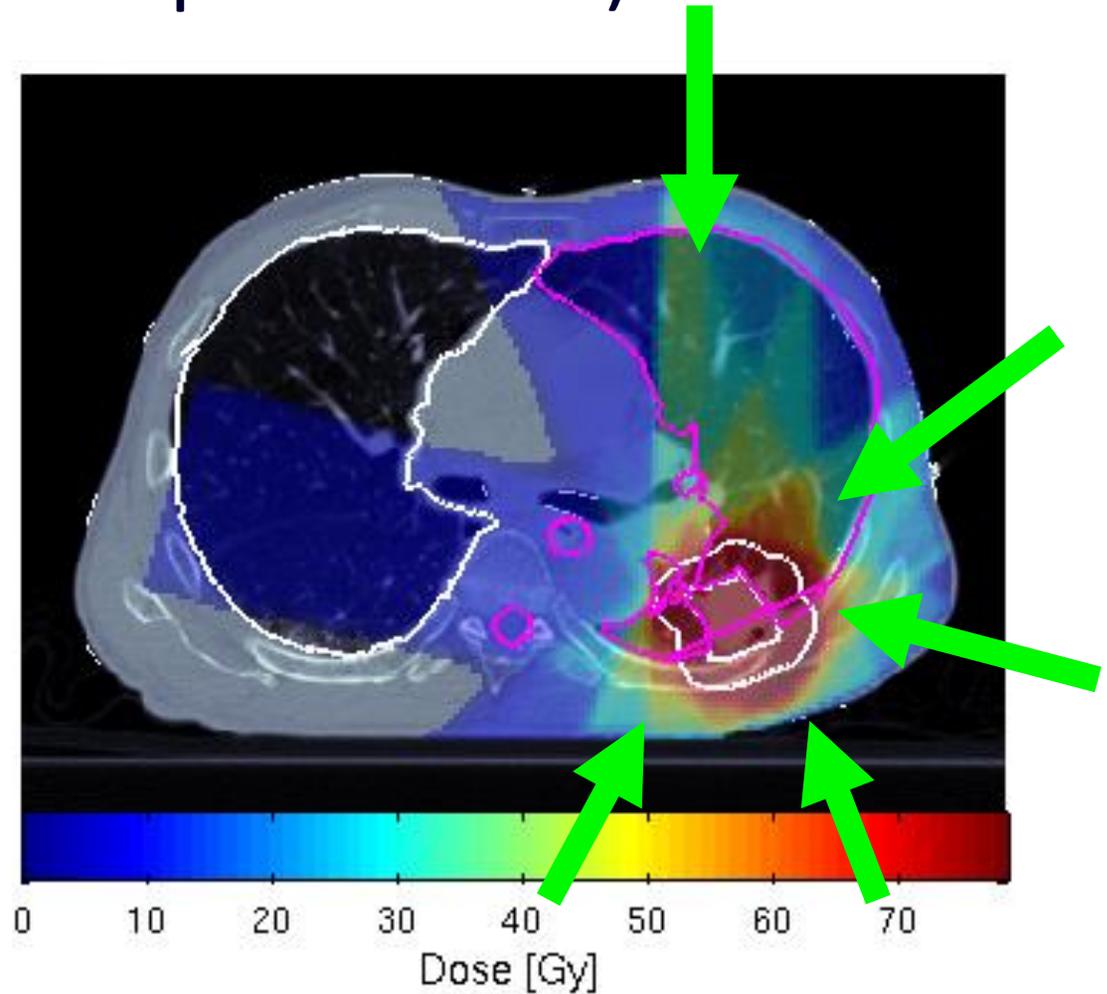
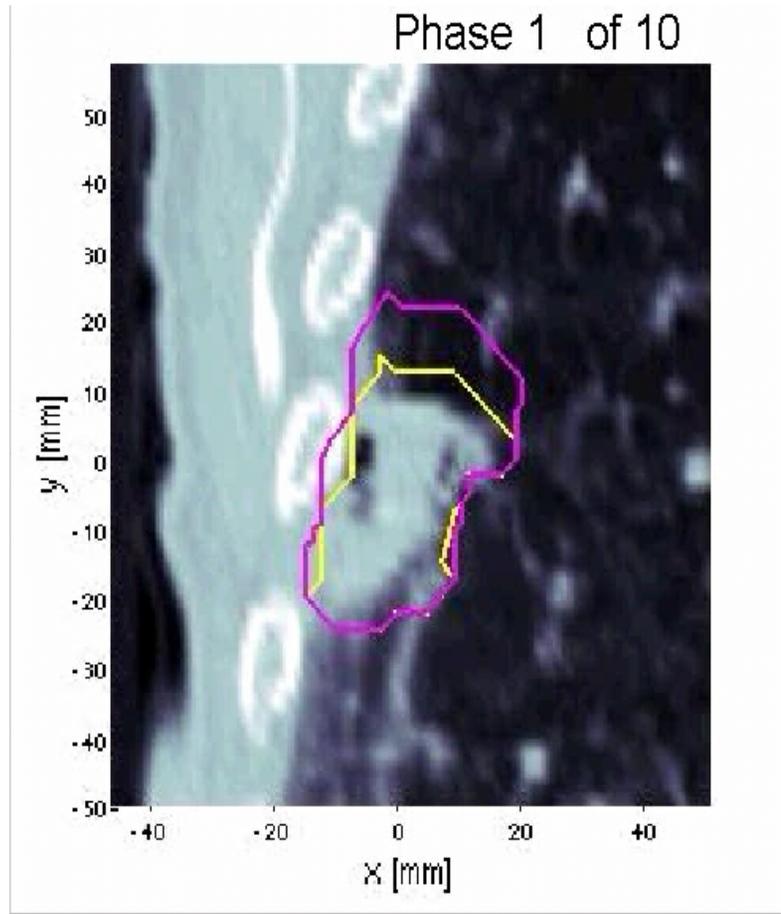


Robust Optimization – Outline

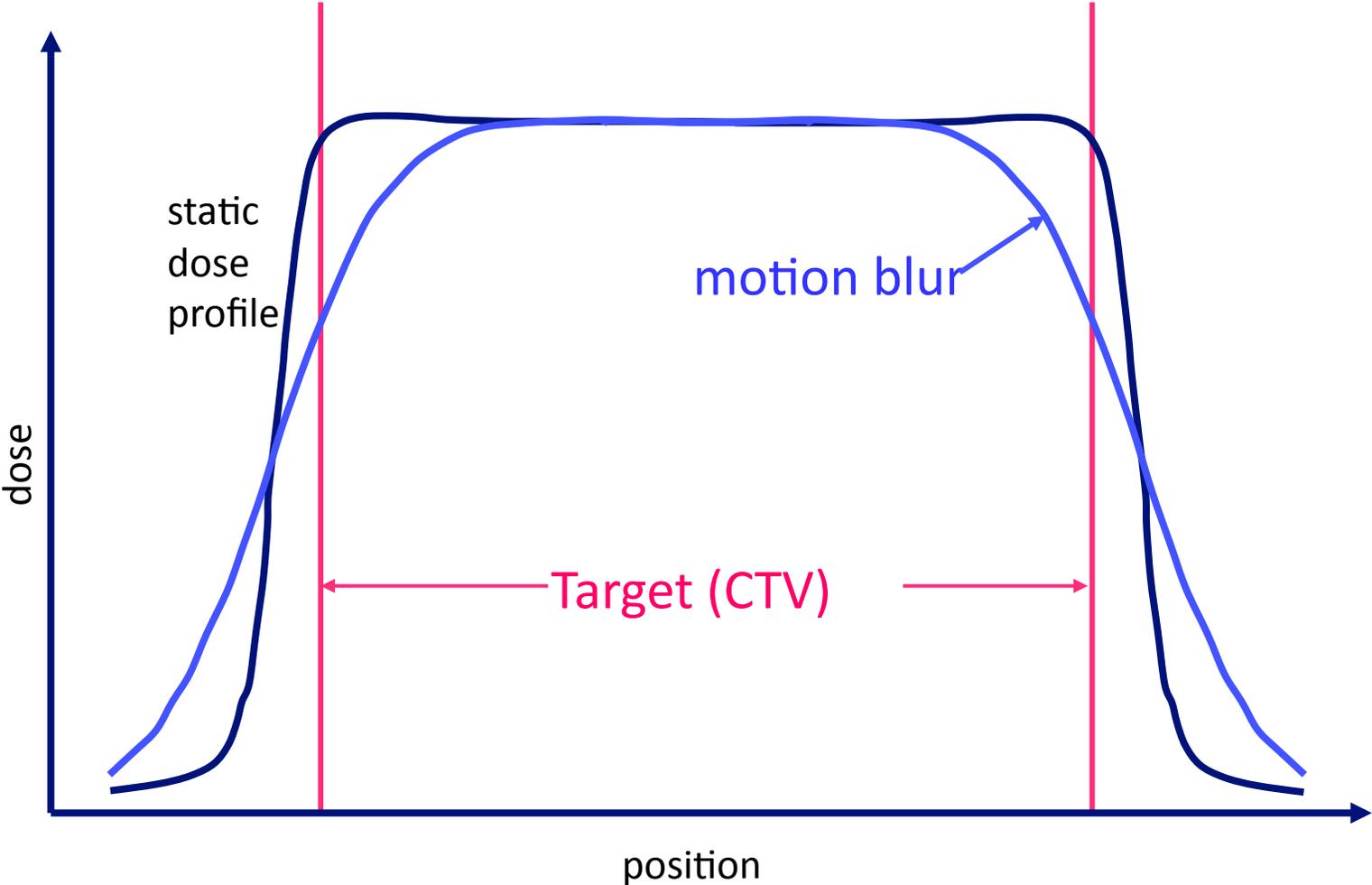
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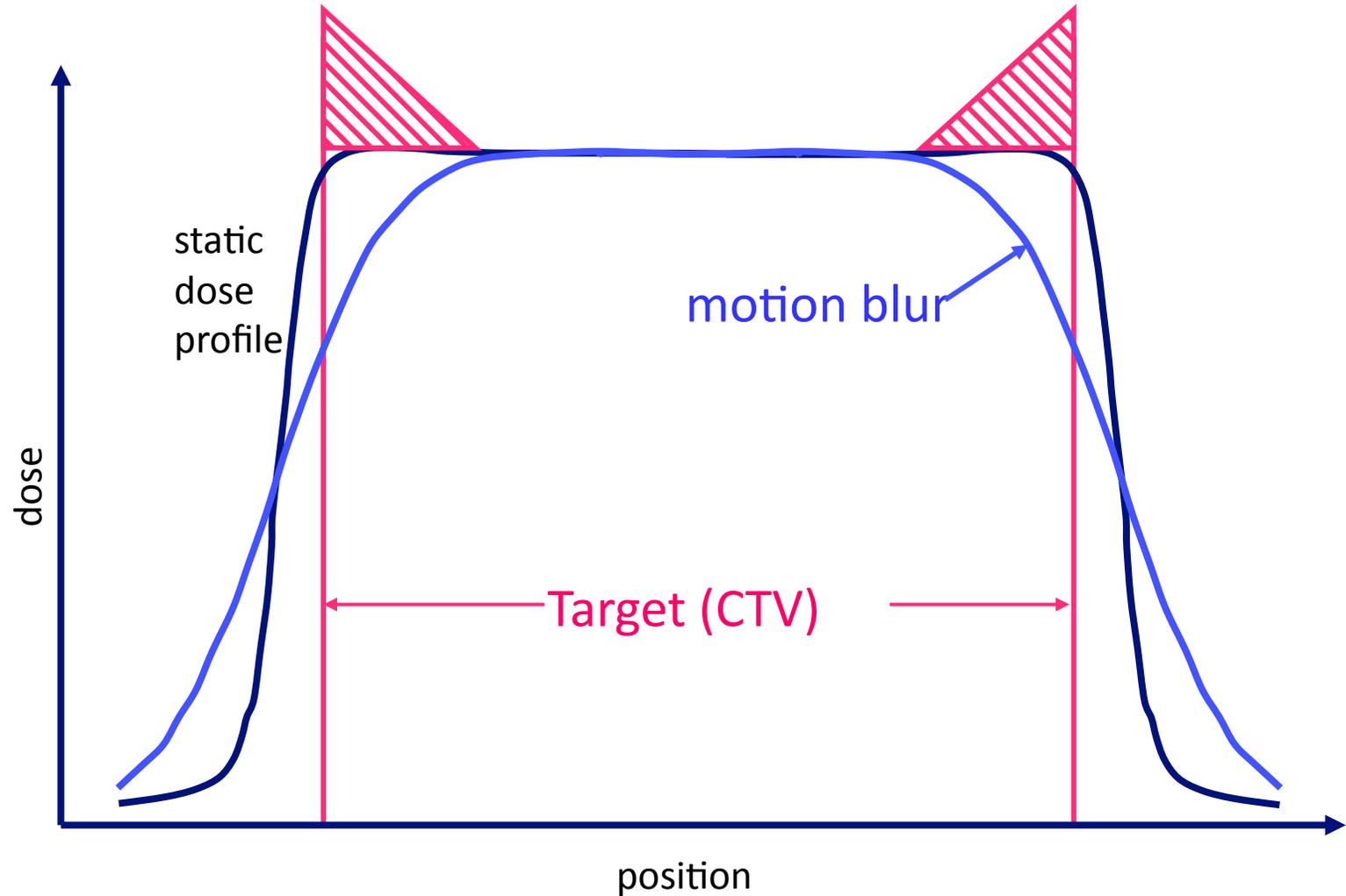
Example 1: Lung, breathing motion Robust (worst case optimization)



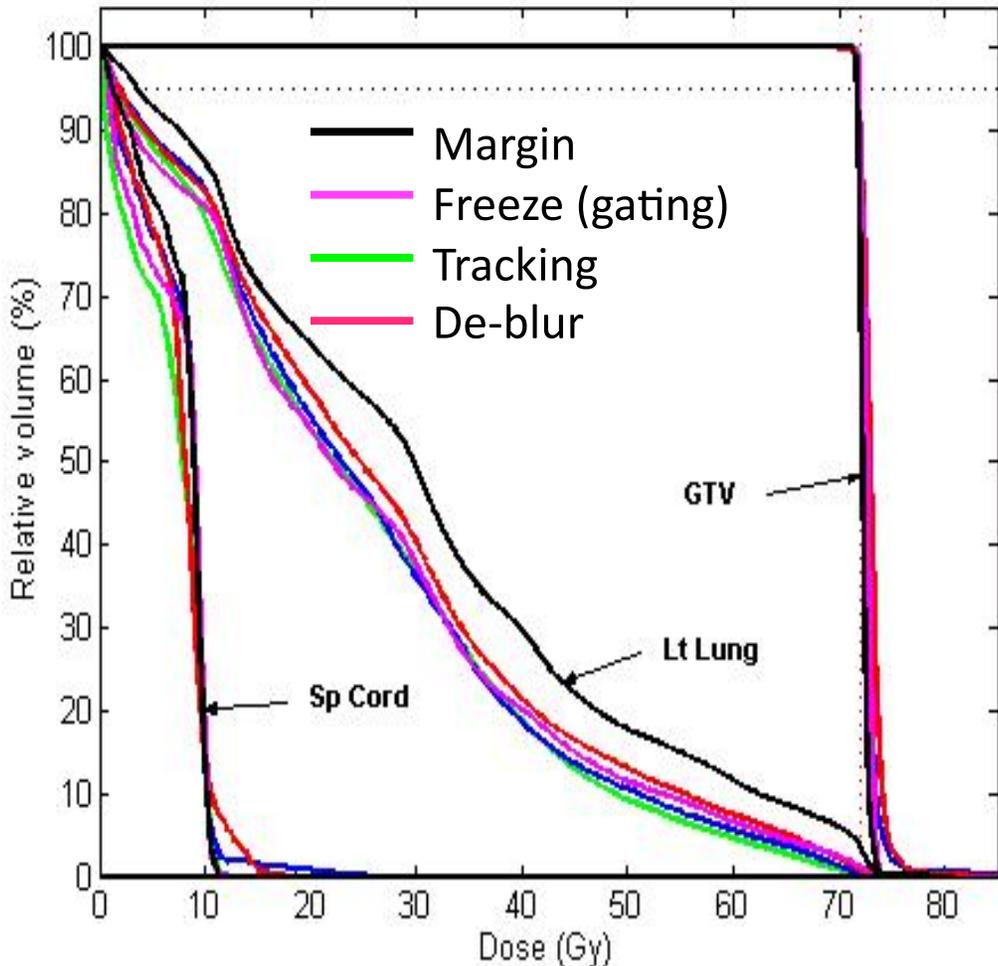
Dose blurring



De-blurring with IMRT -> "horns"



DVH for 4 different techniques



20% reduction of mean dose to left lung compared to margin

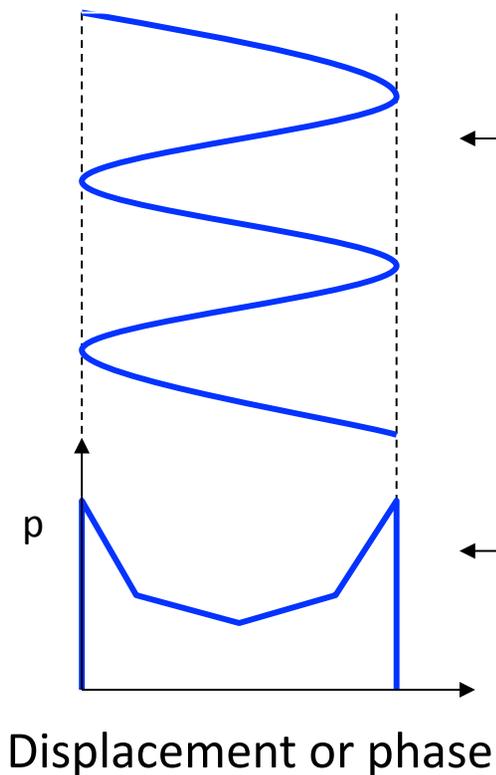
Trofimov et al., Phys Med Biol. 50:2779-98, 2005

- Dose conformality of edge-enhanced IMRT with “horns” is almost as good as gating or tracking
- Is this too good to be true?



Uncertainty model for de-blurring method

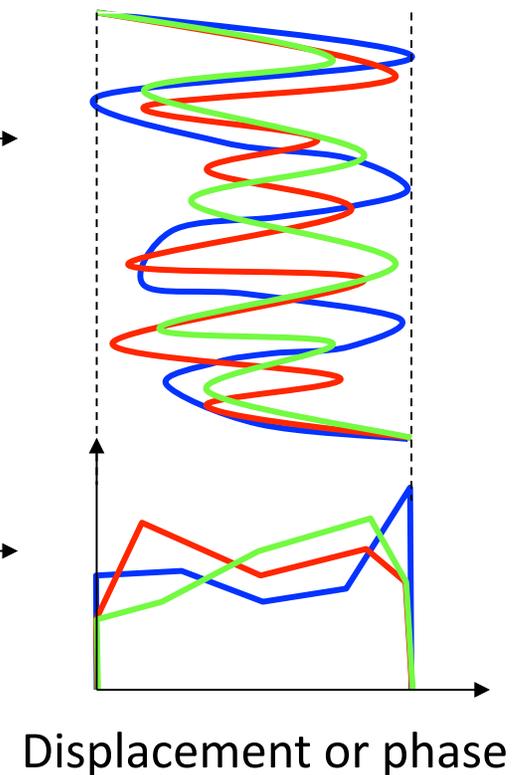
- PDF for regular motion



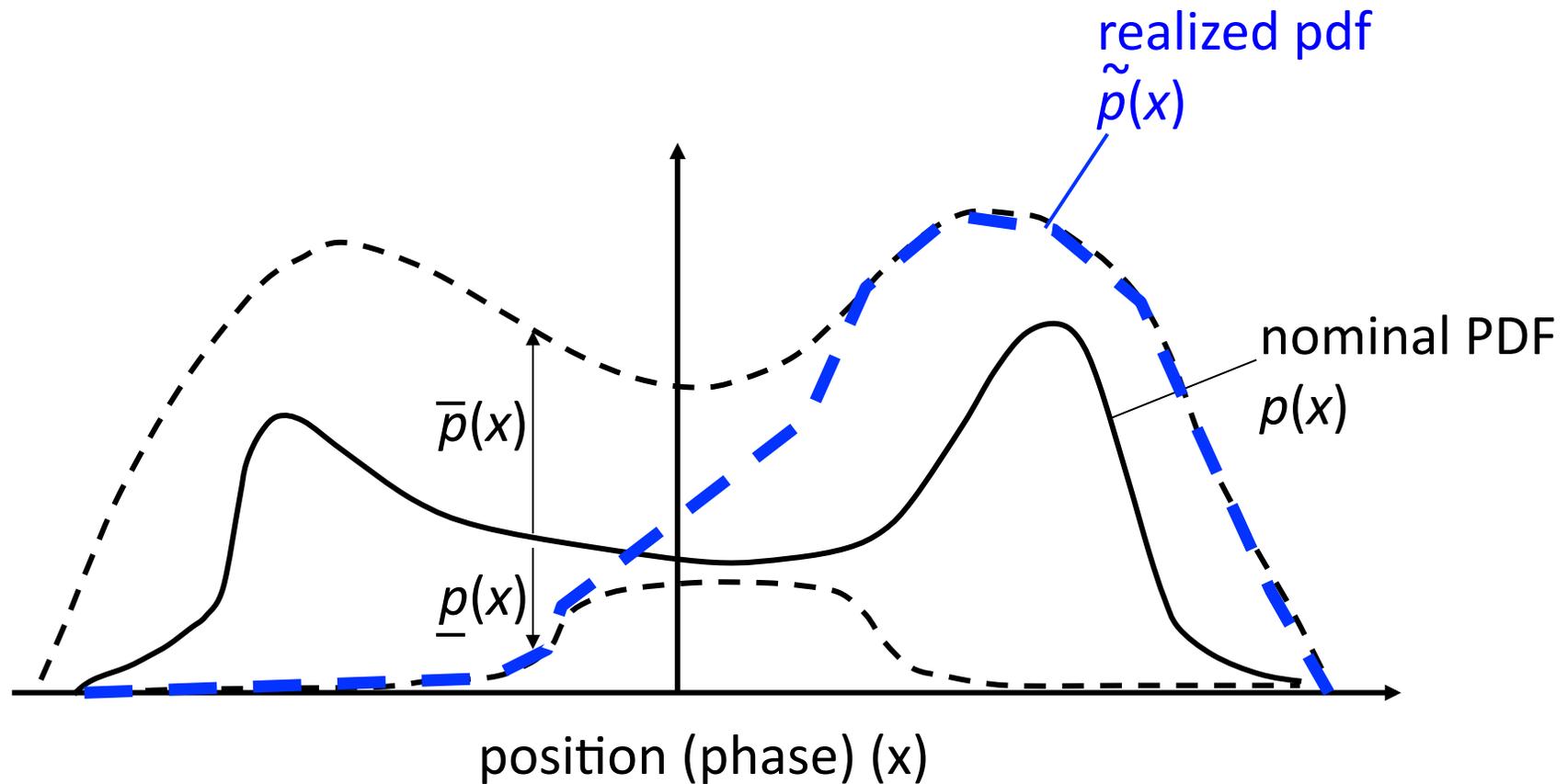
- Uncertain motion may lead to many PDFs

← Motion →

← PDF →



Uncertainty set – PDF and “error bars”



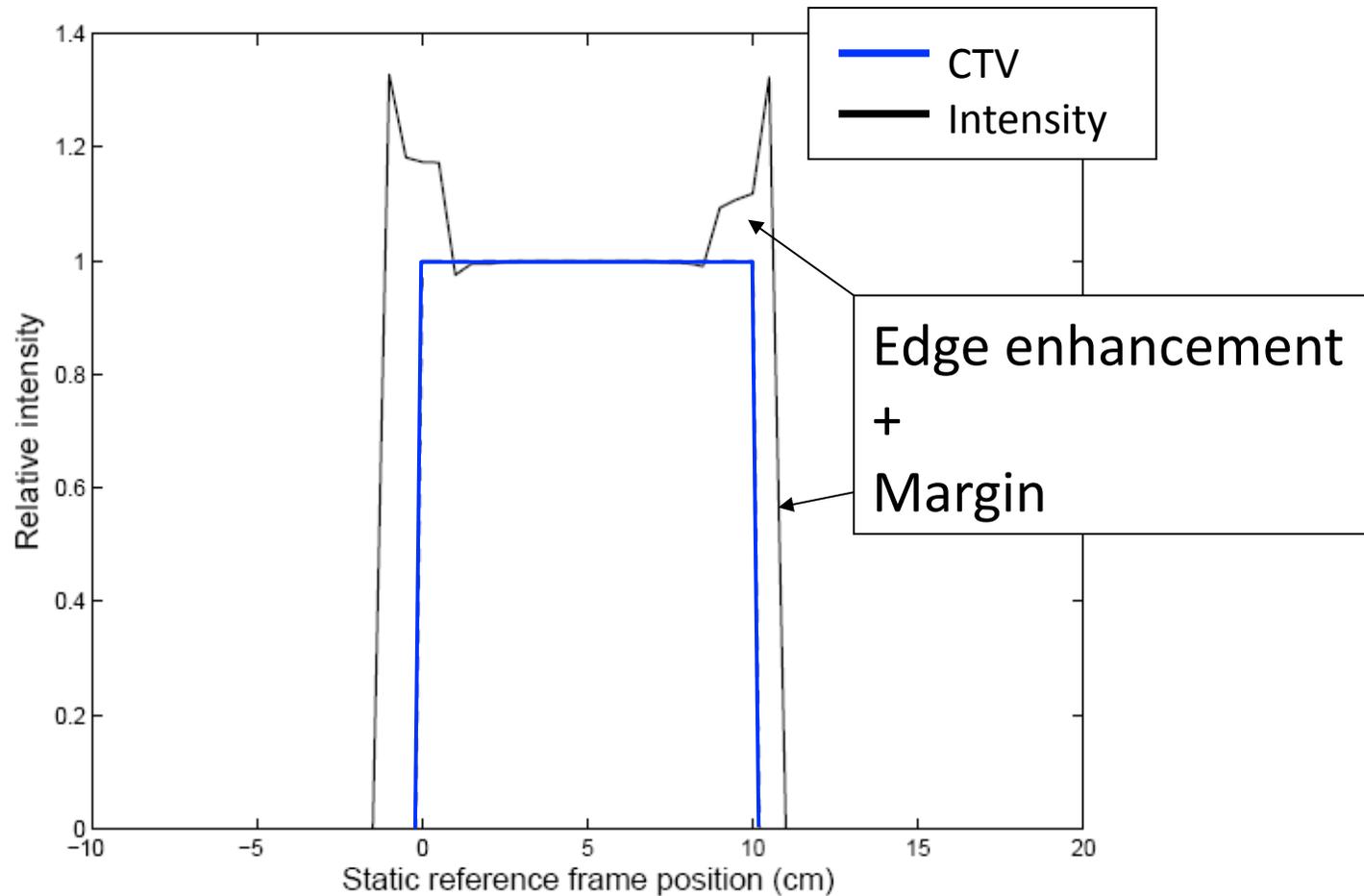
Tim Chan et al: Phys Med Biol 51:2567 (2006)

What is the worst case?

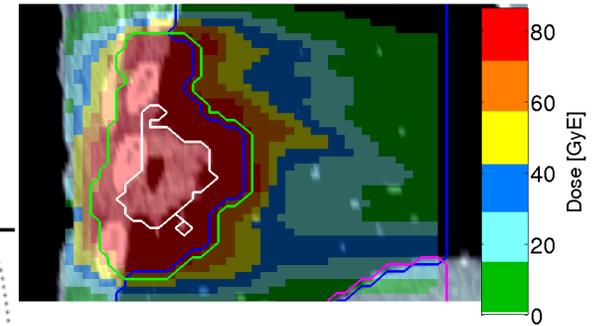
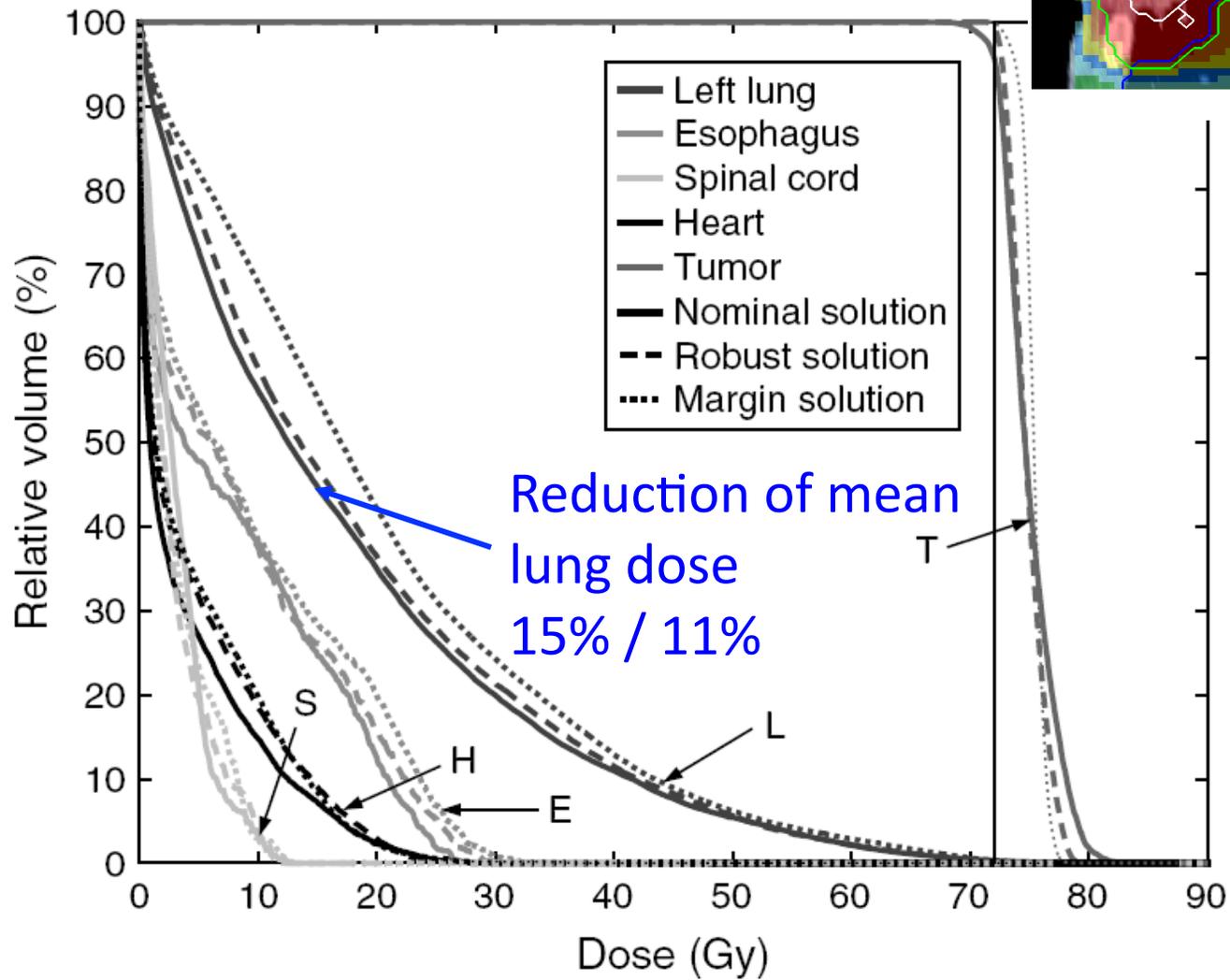
- A given **target** voxel gets different dose values for different breathing phases x .
- Worst case is when low dose values are more likely (\bar{p}) and high dose values are less likely (\underline{p}).

- As a consequence, robustification will limit spikes in intensity maps
- improved deliverability.

Robust edge enhanced intensity profile

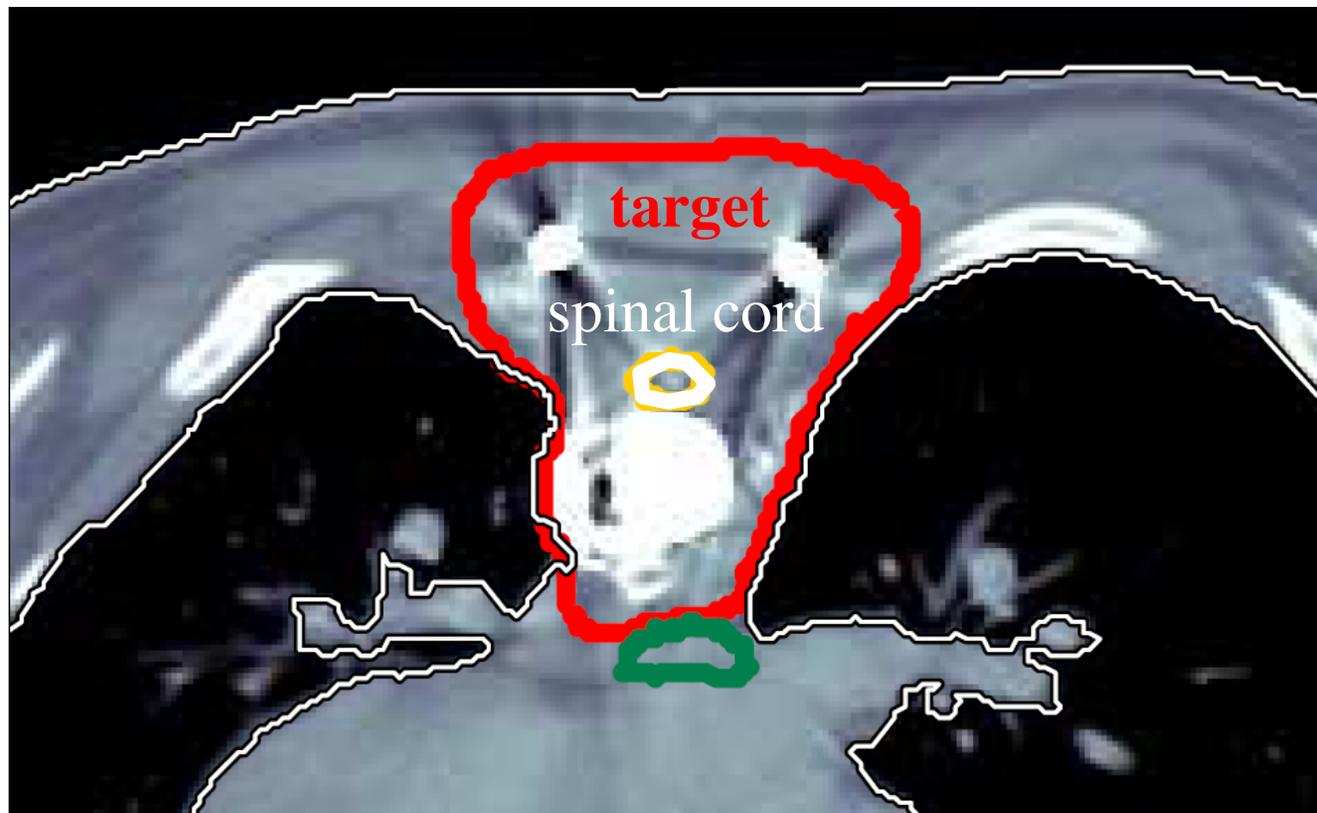


Clinical lung case



Example 2: Protons, range uncertainties

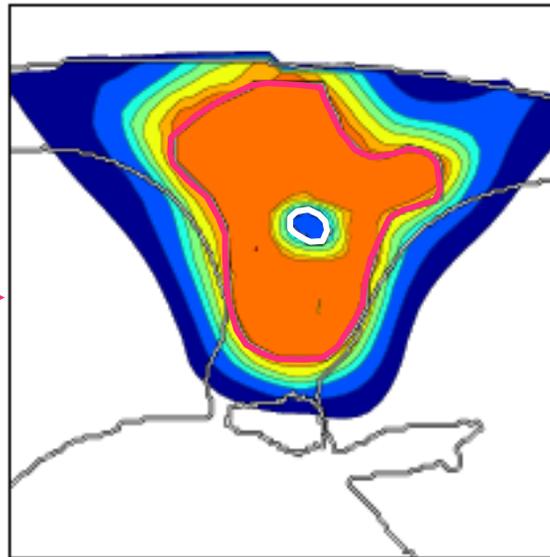
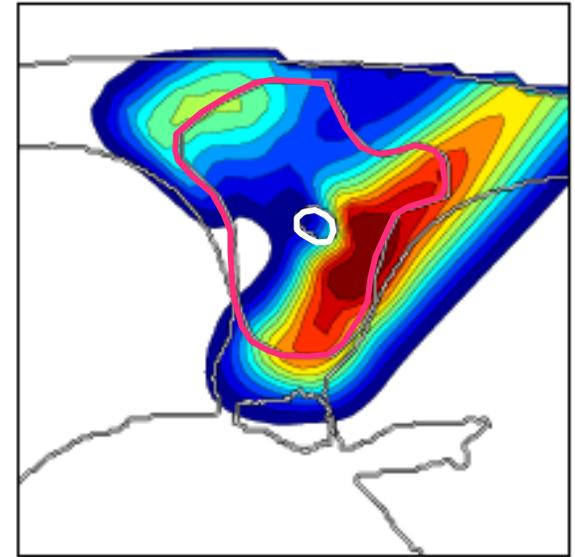
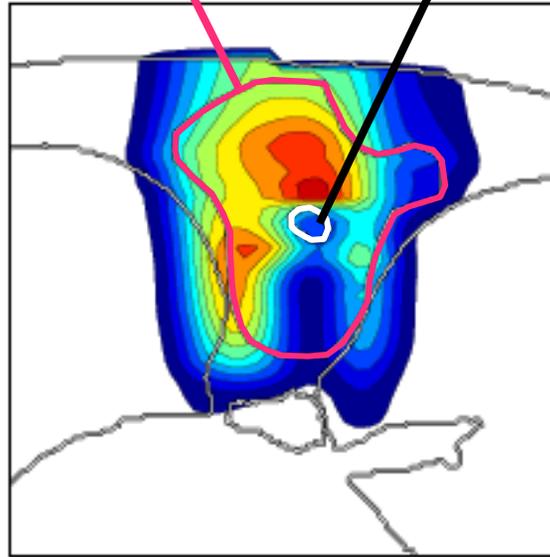
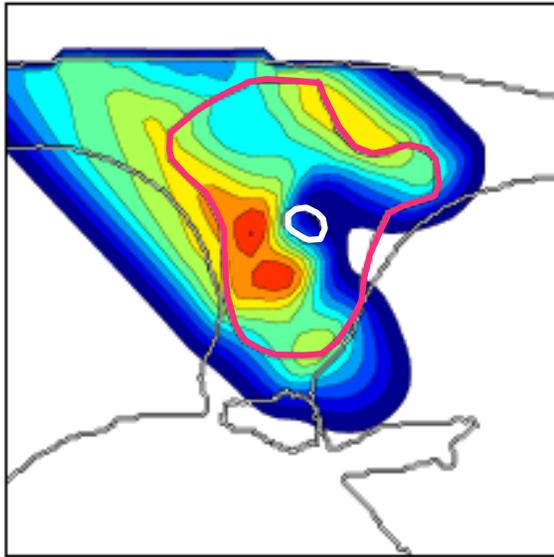
Stochastic programming



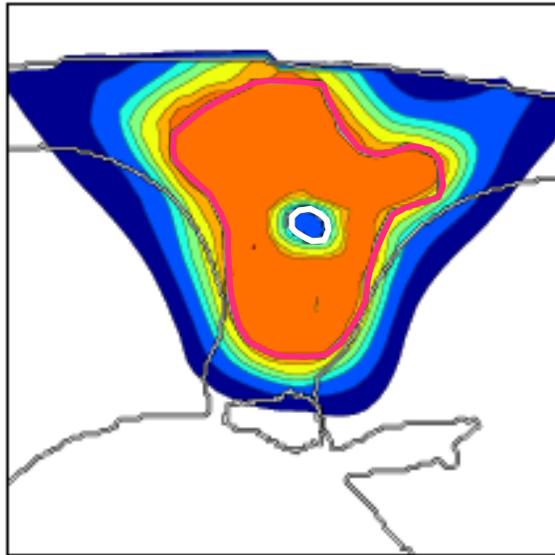
IMPT plan, 3 fields

target

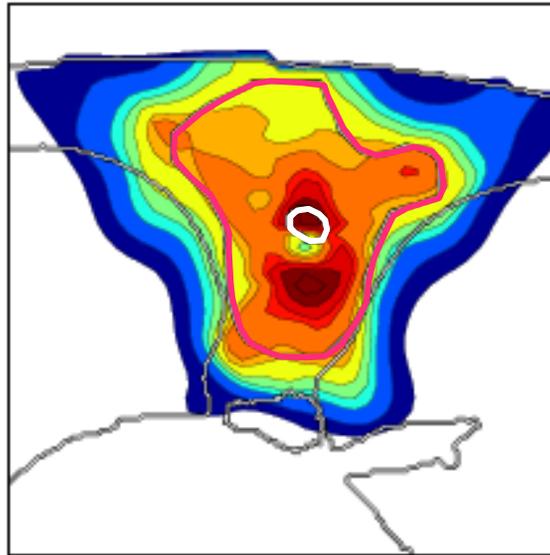
spinal cord



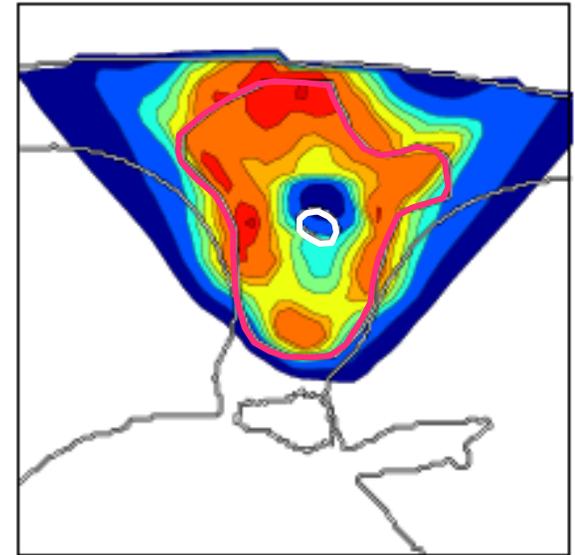
Sensitivity analysis



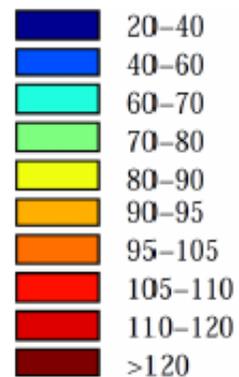
(a) Nominal dose



(b) 5mm overshoot



(c) 5mm undershoot



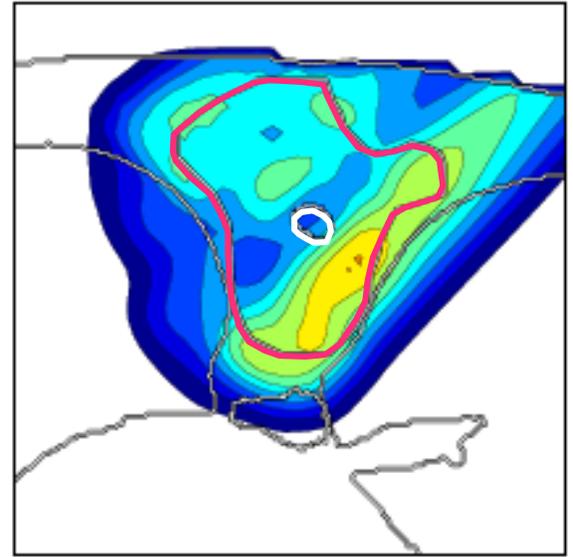
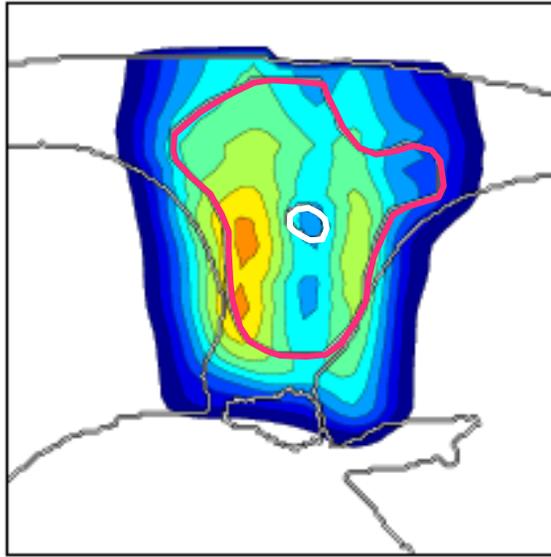
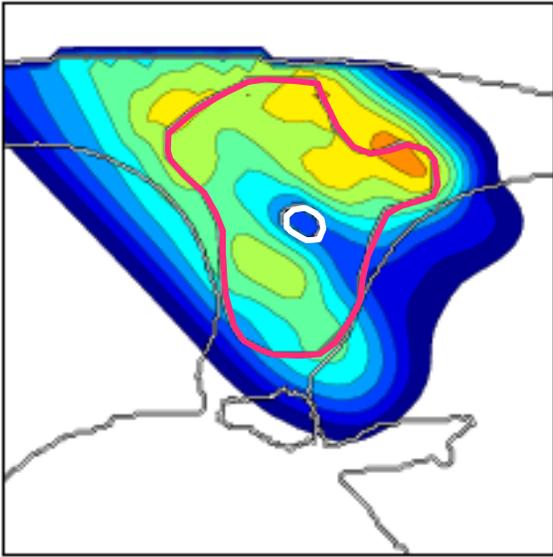
Stochastic programming

$$\underset{x}{\text{minimize}} \quad \sum_s p_s \left[\underbrace{w_T \sum_{i \in T} (d_i^s - D^{pres})^2}_{\text{Target dose deviation}} + \underbrace{w_{SC} \sum_{i \in SC} (d_i^s)^2}_{\text{Spinal cord dose}} \right] + \underbrace{f_{HT}(d^1)}_{\text{healthy tissue dose}}$$

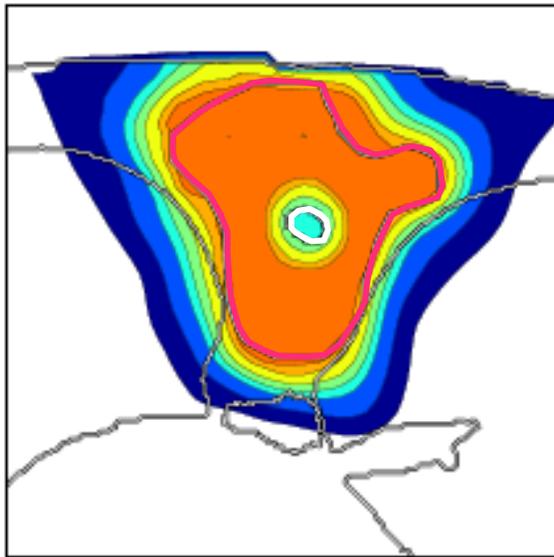
3 scenarios:

- *Scenario 1*: Nominal scenario, $p_1 = 0.5$
- *Scenario 2*: 5 mm range overshoot, $p_2 = 0.25$
- *Scenario 3*: 5 mm range undershoot, $p_3 = 0.25$

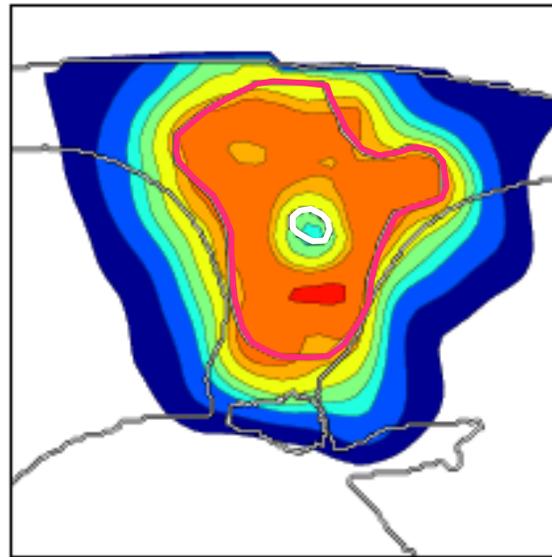
Robust IMPT plan



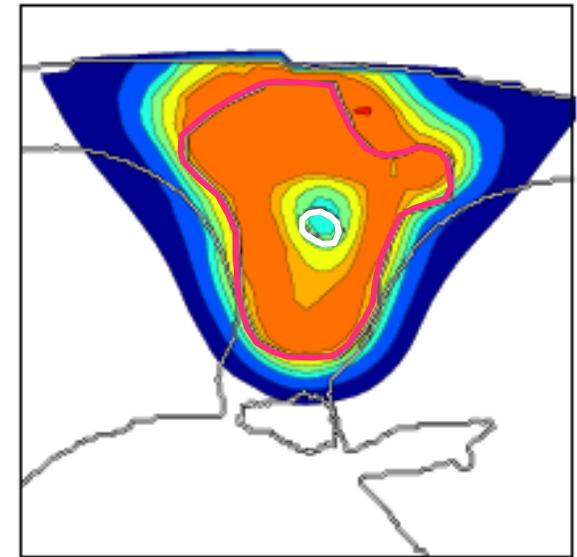
Sensitivity analysis II (robust plan)



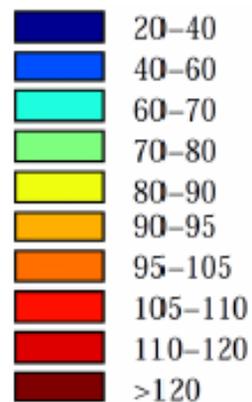
(a) Nominal dose



(b) 5mm overshoot



(c) 5mm undershoot



Vision for the future

- No (PTV) margins in treatment planning
- Instead, quantify motion and uncertainties, and let the planning system find a robust solution. This may be a margin-like solution but could also be an advanced intensity-modulated solution (e.g., “horns”).

Main take-home-messages:

- Two ways to include uncertainties in treatment planning:
 1. stochastic programming (optimization of *expected* outcome)
 2. optimize worst case
- Robust optimization can lead to new types of fault-tolerant dose distributions, e.g. beam “horns” for motion, and robust proton dose distributions.
- There is always a price of robustness.