AbstractID: 5117 Title: Estimating conversion coefficient of KERMA free in air to glandular dose in mammography: a comparison between BR12 model and a realistic voxel model
Purpose: To compare conversion coefficient of KERMA free in air to glandular dose, in mammography, simulated to BR12 model and a realistic breast voxel model.

Method and Materials: We simulate the glandular dose $\left(\mathrm{D}_{\mathrm{g}}\right)$ and KERMA free in air $\left(\mathrm{K}_{\mathrm{a}}\right)$, using the Monte Carlo program MCNP (version 4B) to estimate the conversion coefficient ( $\mathrm{c}_{\mathrm{g}}$ ) of KERMA free in air at entrance skin in glandular dose. The computational universe generated to simulate a mammographic procedure mimics LORAD III mammographic equipment. The focal spot of molybdenum irradiates photons isotropically in a solid angle of $16.8^{\circ}$. The bucky is 0.6190 m far from de focal spot. Above the model there is a PMMA compress paddle 0.002 m thicker. The add filtration ( $30 \mu \mathrm{~m}$ Mo thicker and $25 \mu \mathrm{~m}$ Rh thicker) was located at 0.050 m far from the focal spot. Tow spectra were used in voxel model simulations: 28 kVp with Mo add filtration and 30 kVp with Rh add filtration.

Results The $\mathrm{c}_{\mathrm{g}}$ presented on $\mathrm{Mo} / \mathrm{Rh}$ simulation was 1.5 times larger than the presented on $\mathrm{Mo} / \mathrm{Mo}$ simulation. Comparing the voxel model to the BR12 model we have actually a super estimation on both simulated $\mathrm{c}_{\mathrm{g}}$ values: 3.4 times considering the simulation with $\mathrm{Mo} / \mathrm{Mo}$ target/filter combination, and 2.4 times considering the simulation with $\mathrm{Mo} / \mathrm{Rh}$ target/filter combination.

Conclusion: The $\mathrm{c}_{\mathrm{g}}$ values show a decrease of $58.7 \%$ considering the $\mathrm{Mo} / \mathrm{Rh}$ target/filter combination and a decrease of $70.2 \%$ considering the $\mathrm{Mo} / \mathrm{Mo}$ target/filter combination, to the realistic breast model as comparative pattern. These variation on $\mathrm{c}_{\mathrm{g}}$ are probably caused by the definition of a non-anthropomorphic model composed by an homogeneous distribution of tissues as pattern, that makes unviable the observation of the absorbed energy by each tissue; and because this model do not consider the position of glandular tissue in the real breast geometry.

