Purpose:

When apat ientb odypar tis outsid eof the CTs canfieldofview, truncationar tifacts generallyocc urintheimagesleadi ng toinacc uracyi nthe CT number(HU) in the se affected images. I nprotont herapytreatmentpl anning, CT numbersare converted to stoppingpowersto calculatedos e, bea mrangeand range compensatorsfort he treatmentfieldstocover the targetvolum es. We have evaluated the effects of the sear tifacts on protondos ecalculation accura cyandon range uncertainty fors pinal fields used for cranial spinali rradiation.

Methodand Material:

A thoracic phantom wasima gedonaGE16 slice CT scanneru singastandardb odypr otocol.T wo RMIbonetissue b locks simulatingpati ent arm/orshou lderwaspl acedoutsid eof the scanf ieldofvi ew.Twoset sof scanswer eobt ainedwi thandwithoutthe bonet issueblock s. Protontrea tmentplans were g enerated using Eclipsetreat mentplanningsyst em.Then, treatmentpl answer e comparedtoeachoth ertodeter minet hedos eandrangediffe rences.

Result:

There is a vora lof 20-30 HUdi fference in the target are adueto the imaget runcationarti facts. This creates a 2-3 mm difference in the range of the proton and 50 % do sel ine between the plans with and withou truncation artifacts.

Conclusion:

Theim age artifacts causeu ncertainty indoseestim ations in the distale dgeof the treatmenttar get. The differencebetween theorr ectedplan andt hetrun catedpl an ison theorder of 2 -3mm, which is comparable to the distalmargin normally used to account for therange uncertainty for the spinefield proton therapy treatment planning.