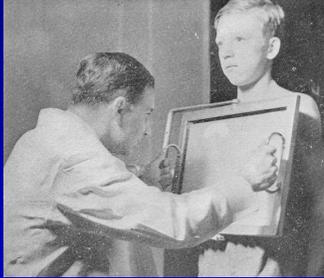


# Fluoroscopic Imaging Equipment Considerations for Optimization of Performance and Dose



Phil Rauch  
Henry Ford Health Systems  
Detroit, MI



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## Fluoroscopic Technology (*Real-time* image production & display)

X-ray Intensity Distribution



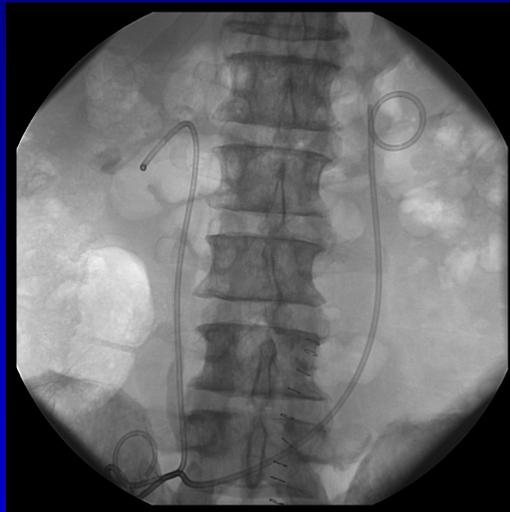
Radiation Capture  
(Detector)



Output Light Intensity  
Distribution



Visible Image  
(Film, Display Monitor)



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## Dose Reduction vs Image Quality

### ◆ Dose reduction depends on...

- ....technology
- ....proper equipment design
- ....proper set up of equipment parameters
- ....proper utilization of the equipment
- ....**knowledge and skill of the radiologist**



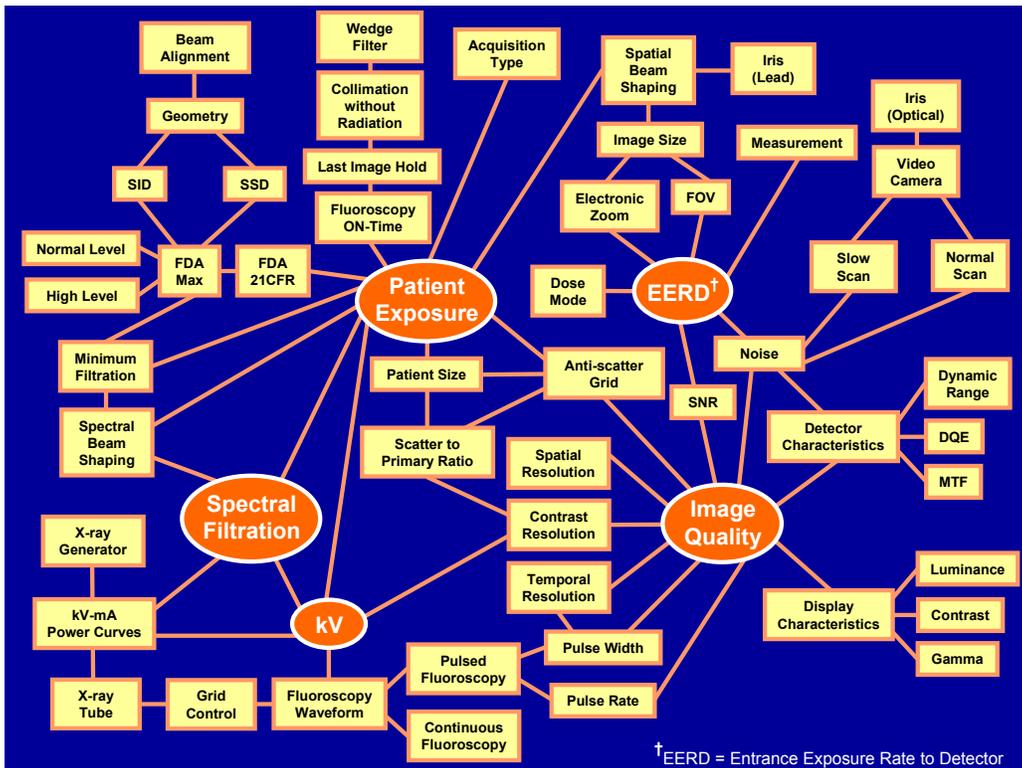
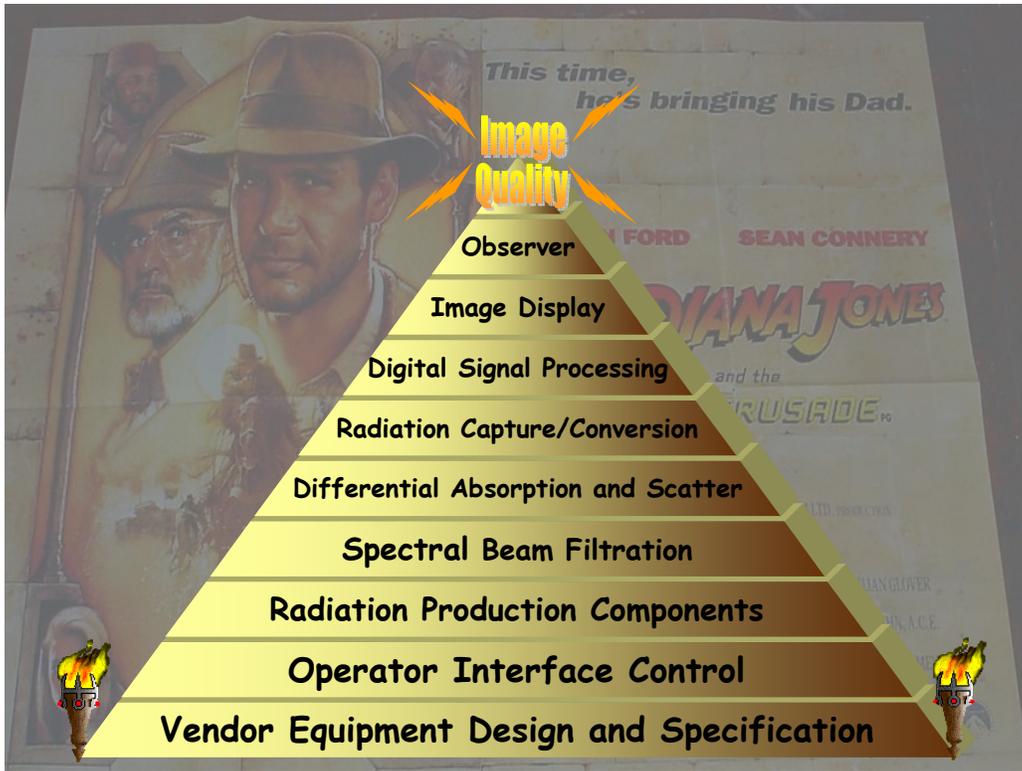
## Dose Reduction vs Image Quality

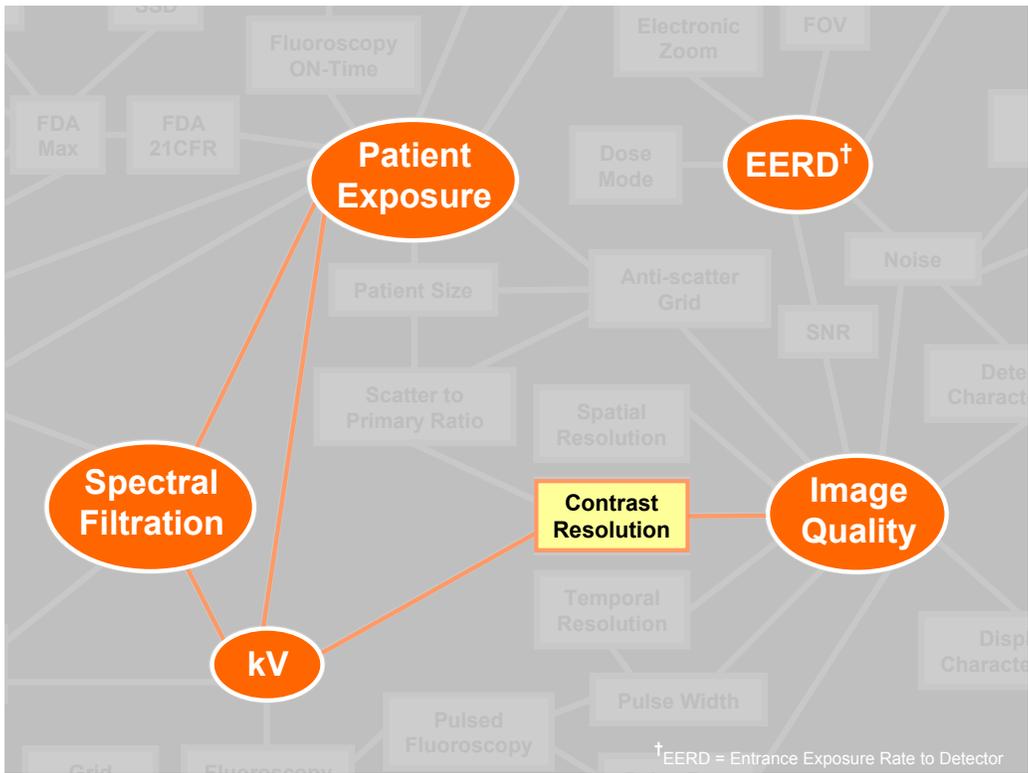
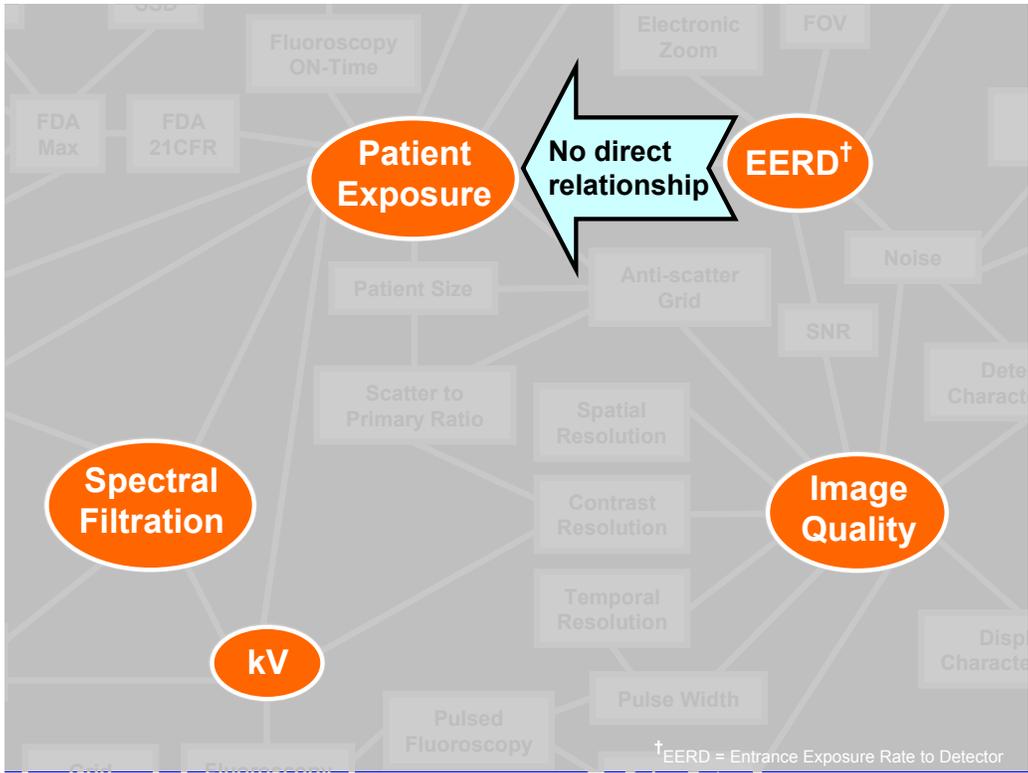
### ◆ Image quality depends on...

- ....technology
- ....proper equipment design
- ....proper set up of equipment parameters
- ....proper utilization of the equipment
- ....**knowledge and skill of the radiologist**

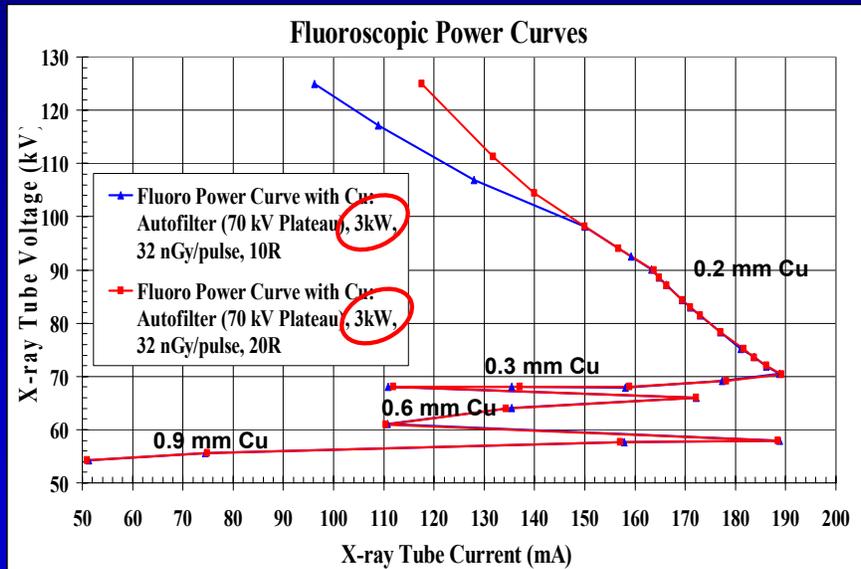
*but the pursuit of dose reduction and image quality is like.....*







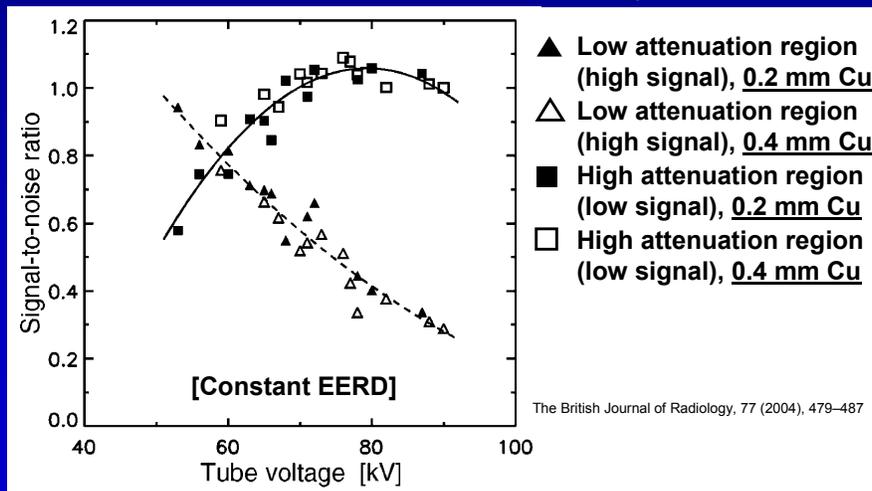
# Fluoroscopy (New Paradigm)



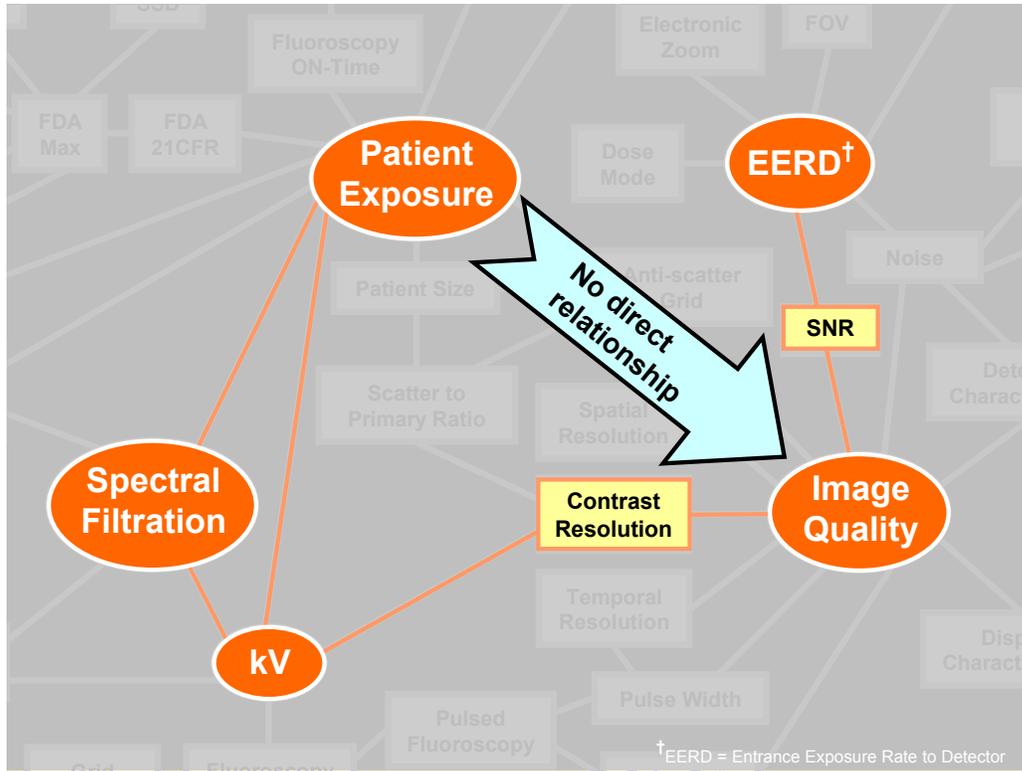
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# Fluoroscopy (New Paradigm)

## ◆ Contrast to Noise Ratio vs KVp



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## Image Quality: What is it?

- ◆ “Image quality depends only on intrinsic, objective physical characteristics of an imaging system, and can be measured independently of an observer”

*Definitions courtesy Ralph Schaetzing, Agfa Corp.*

# Detector Input Dose Rates (FP)

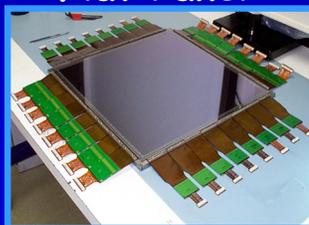
## Detector Metrics



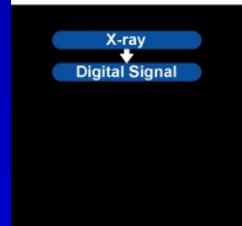
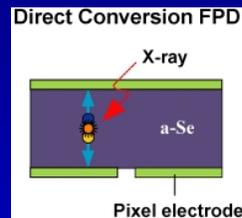
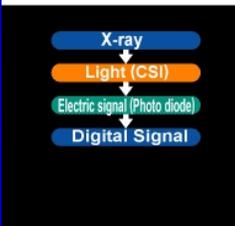
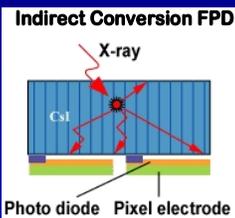
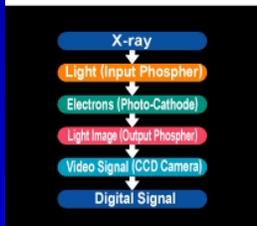
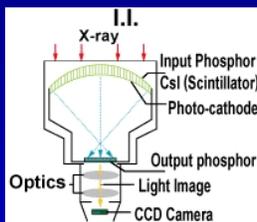
## Image Intensifier



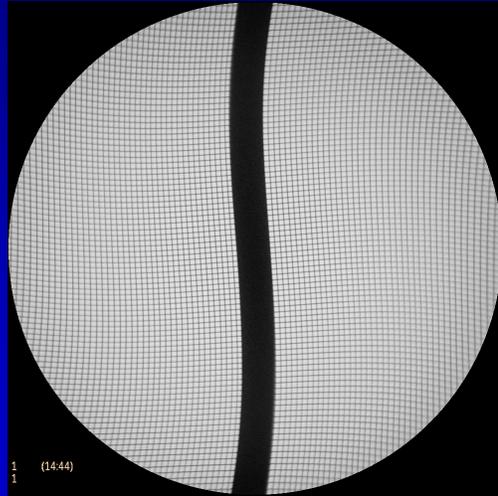
## Flat Panel



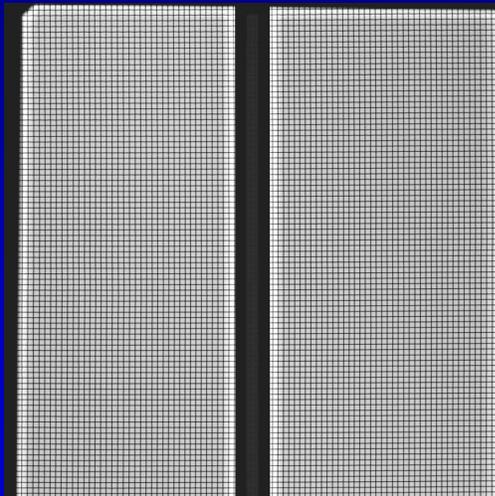
# Image Detector



# Distortion



**XRII**

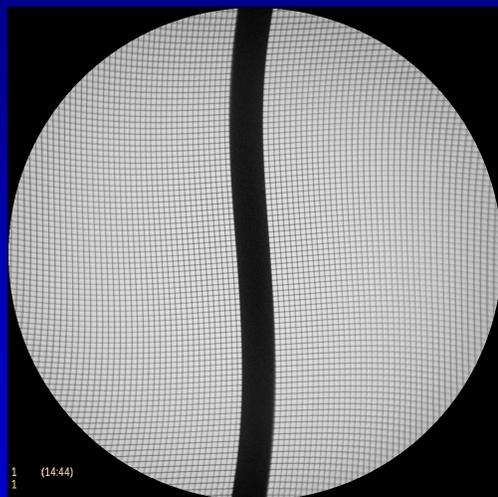


**Flat Panel**

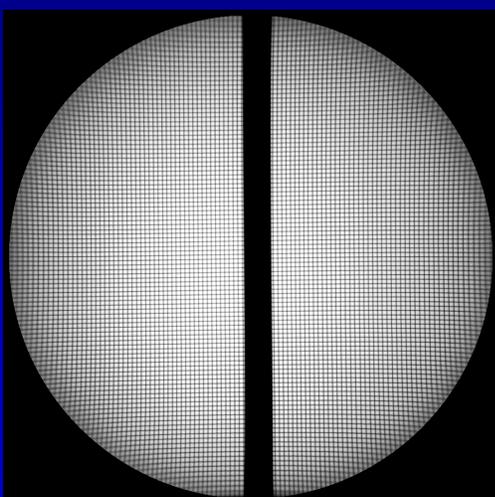


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# Distortion



**XRII**

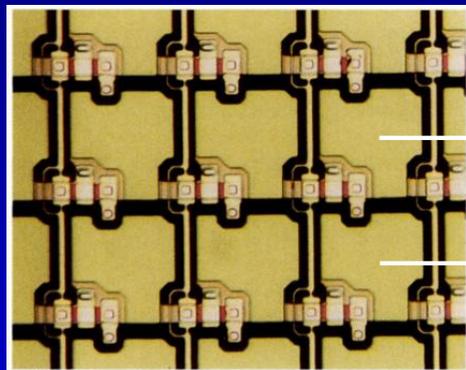


**XRII**



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# Pixel Pitch – Estimated Resolution



Pixel Pitch

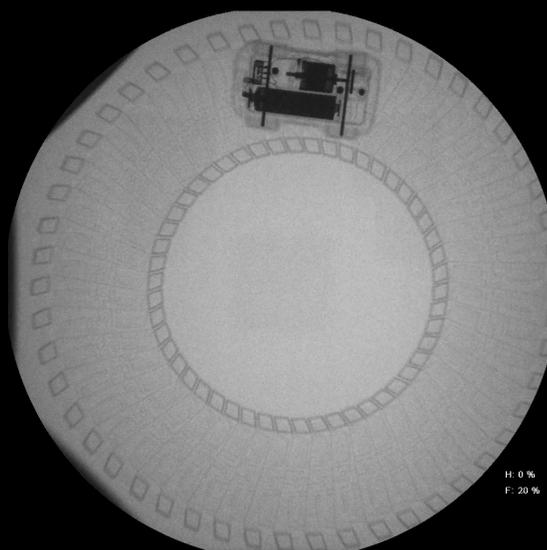
Detector	Mfg.	Pixel Pitch	Nyquist (lp/mm)	Nyquist x 2 <sup>^(.5)</sup> (lp/mm)	Mesh Lines per Inch at 45-degrees
Safire (a-Se, a-Si TFT)	Shimadzu	0.150	3.33	4.71	120
Philips, Siemens (CsI(Tl), a-Si TFT) - Angio	Trixell	0.154	3.25	4.59	117
Philips, Siemens (CsI(Tl), a-Si TFT) - Cardiac	Trixell	0.184	2.72	3.84	98
GE, Revolution (CsI(Tl), a-Si TFT)	GE	0.200	2.50	3.54	90



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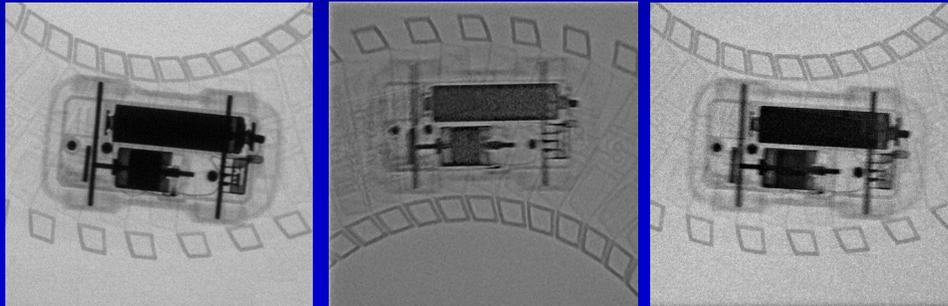


(I'm from the motor city - Detroit)

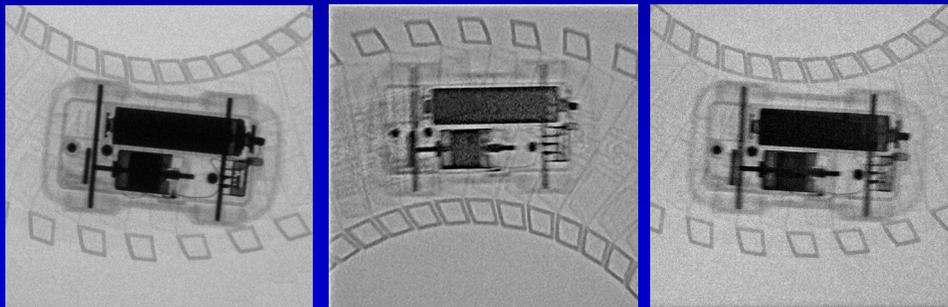
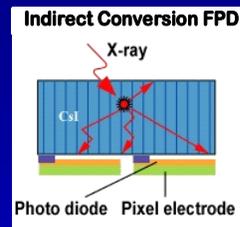
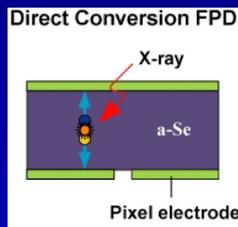
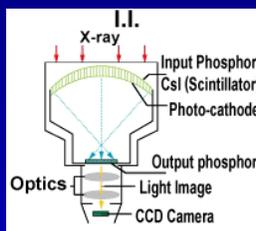


# Image Detector (Fluoro LIH)

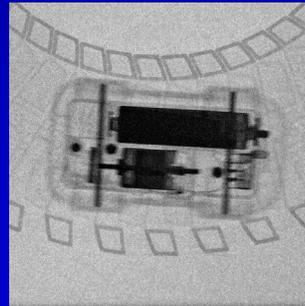
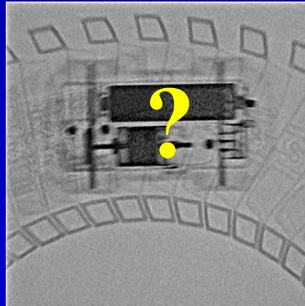
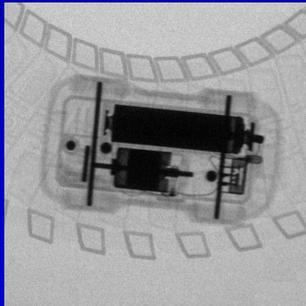
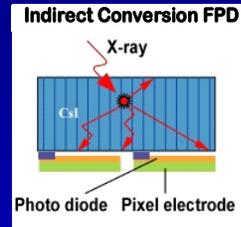
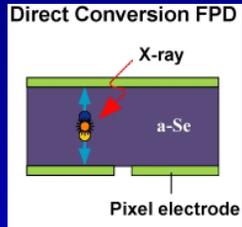
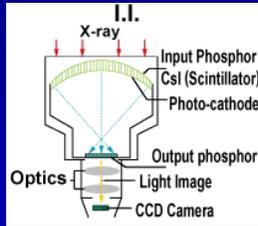
- ◆ Can you match the fluoroscopy LIH image to the detector?
  - A. Image Intensifier
  - B. Indirect Flat Panel
  - C. Direct Flat Panel



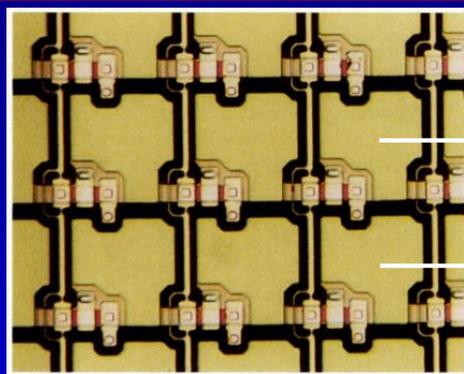
# Image Detector (Fluoro LIH)



# Image Detector (Fluoro LIH)



# Pixel Pitch – Direct Capture



Pixel Pitch

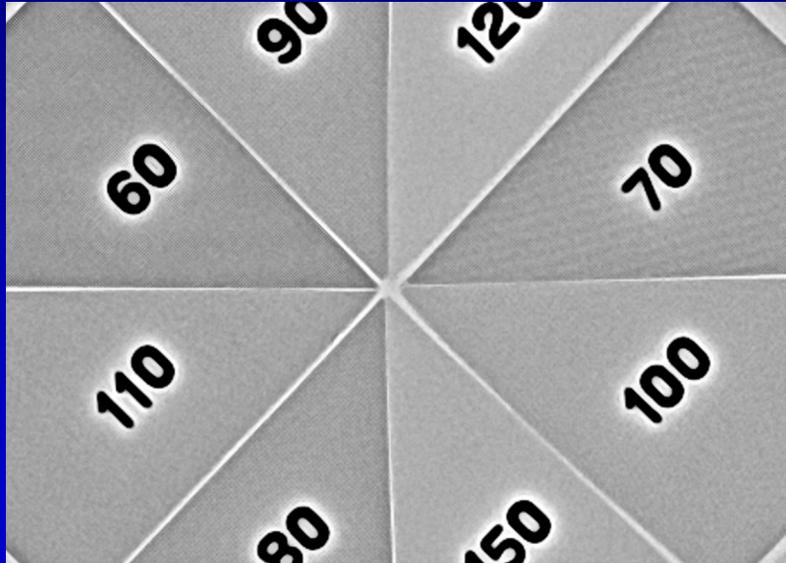
Detector  
Safire (a-Se, a-Si TFT)

Mfg.  
Shimadzu

Pixel Pitch (lp/mm)	Nyquist (lp/mm)	Nyquist x 2 <sup>^(.5)</sup> (lp/mm)
0.150	3.33	4.71

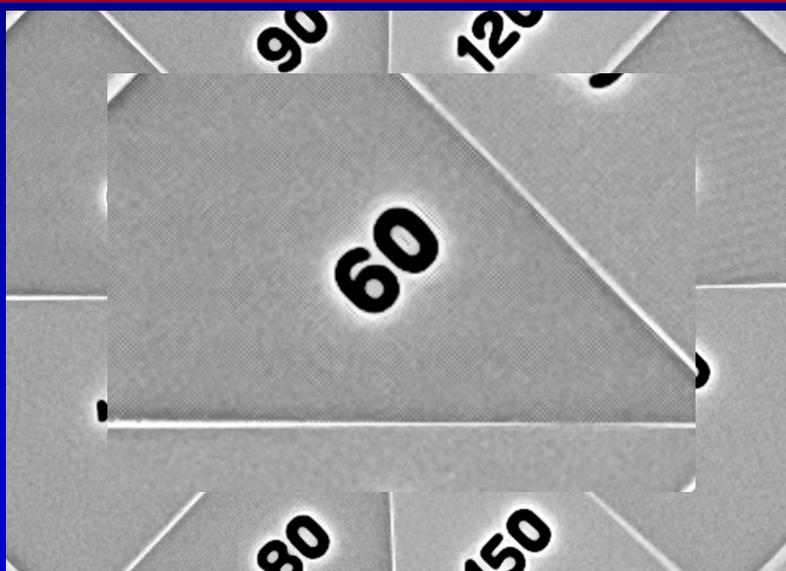
Mesh Lines per Inch at 45-degrees  
120

## a-Se Detector, Pixel Pitch 0.15 mm



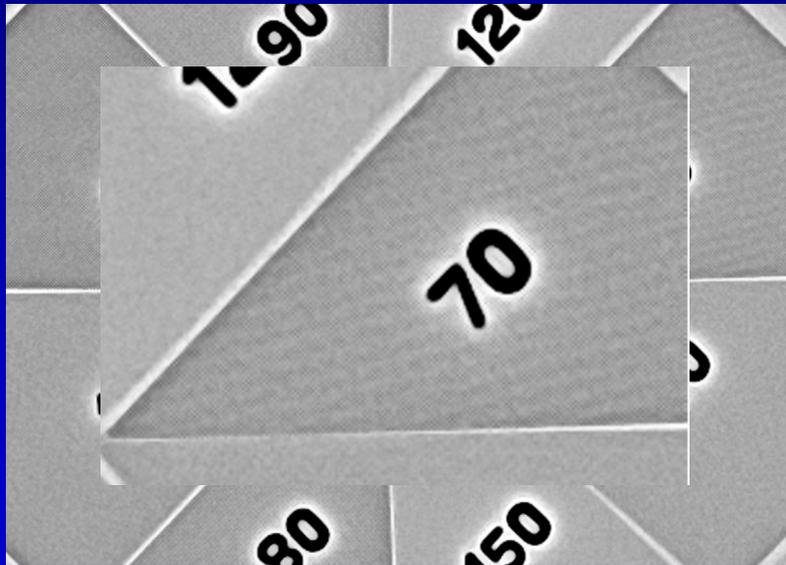
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## a-Se Detector, Pixel Pitch 0.15 mm



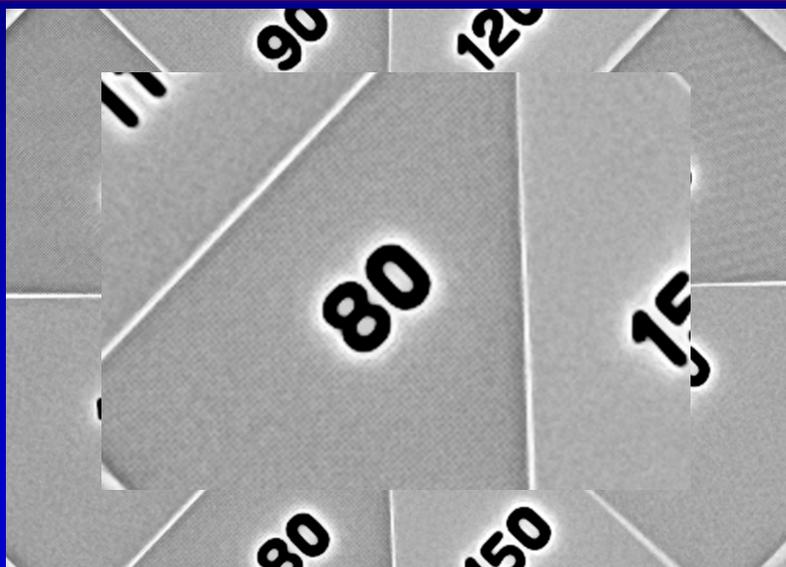
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## a-Se Detector, Pixel Pitch 0.15 mm



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## a-Se Detector, Pixel Pitch 0.15 mm

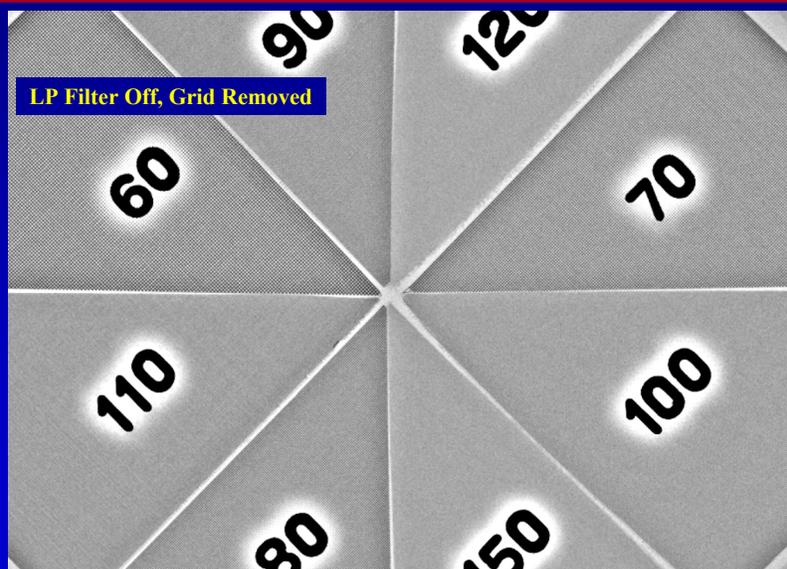


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## a-Se Detector, Pixel Pitch 0.15 mm

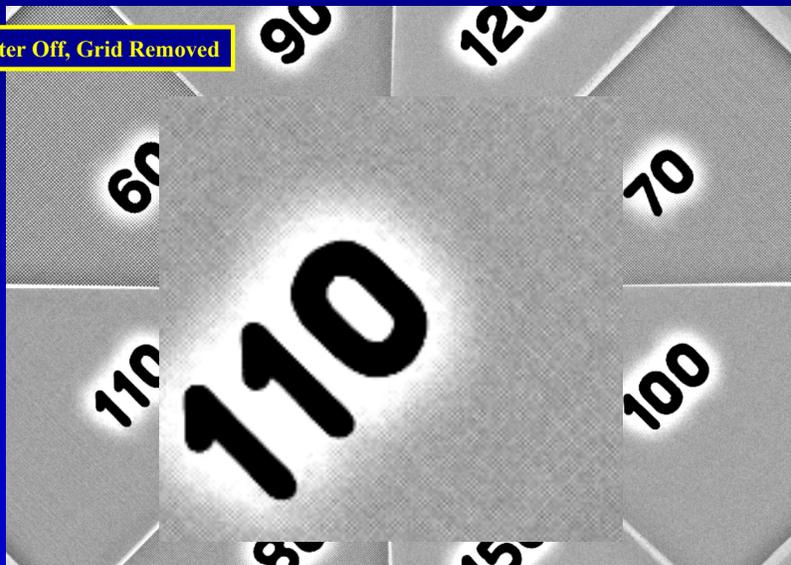
- ◆ Stationary anti-scatter grid (44 l/cm)
- ◆ Low pass filter was utilized to remove grid lines from the image
- ◆ This severely compromised the potential high spatial resolution of this detector
- ◆ Verification by temporarily turning off the lp filter and removing the grid

## a-Se Detector, Pixel Pitch 0.15 mm



## a-Se Detector, Pixel Pitch 0.15 mm

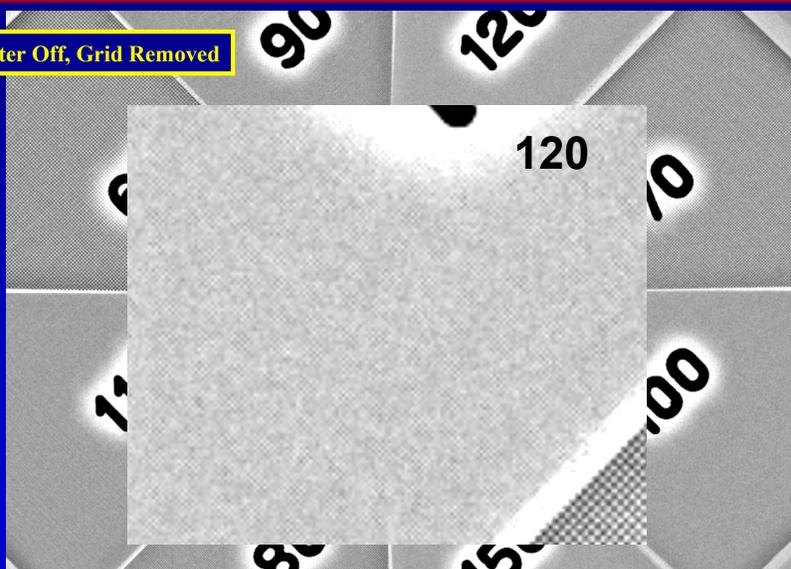
LP Filter Off, Grid Removed



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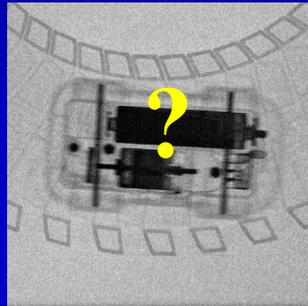
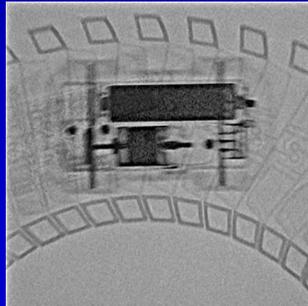
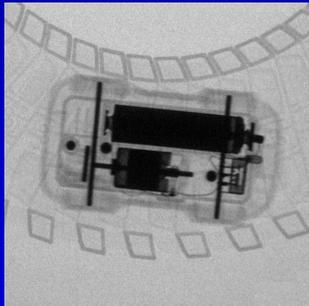
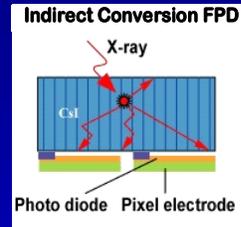
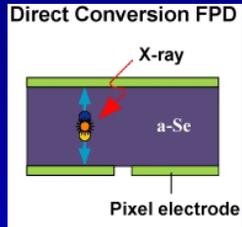
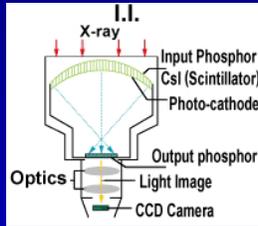
## a-Se Detector, Pixel Pitch 0.15 mm

LP Filter Off, Grid Removed



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# Image Detector (Fluoro LIH)



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## Indirect conversion

- ◆ Pixel binning was used for the chosen field of view resulting in a reduction in detail resolution
- ◆ Recursive filtering was utilized, and this resulted in edge blurring (more on this later)



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# Resolution

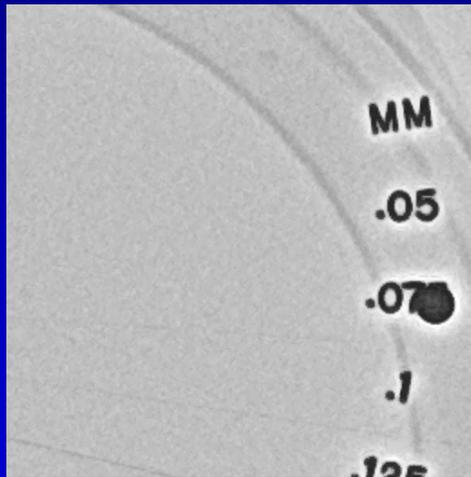
Can you see a  $50\mu$  wire using a flat panel detector with a pixel pitch of  $150\mu$ ? With a pixel pitch of  $200\mu$ ?



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# Resolution

Direct Capture,  $150\mu$  pixel pitch

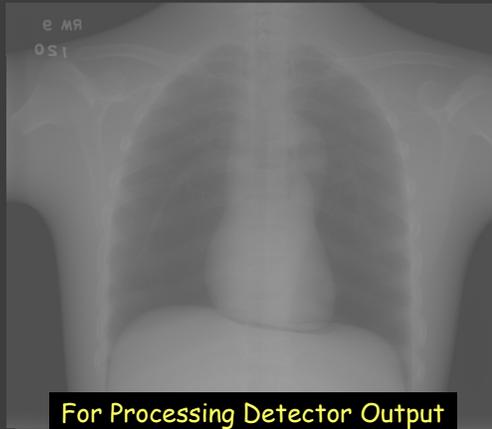


Indirect Capture,  $200\mu$  pixel pitch



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# Radiation Capture/Conversion



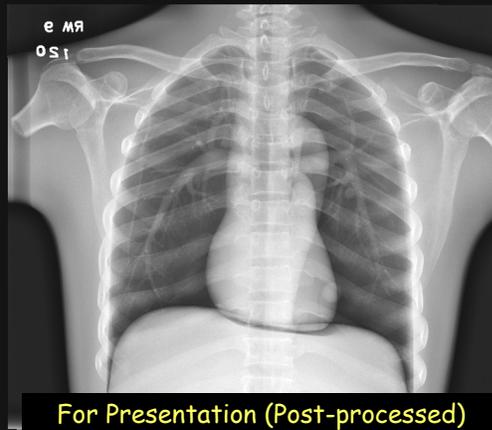
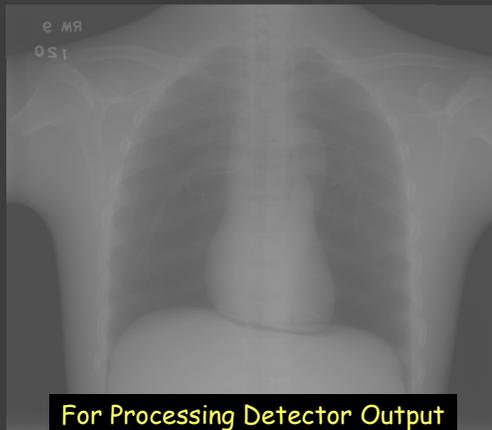
## Digital Signal Processing

- Exposure scaling
- Segmentation
- Histogram analysis
- Multi-scale frequency enhance
- Noise reduction
- Edge restoration
- Dynamic range rendering
- Grayscale presentation



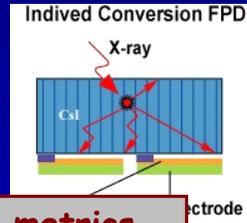
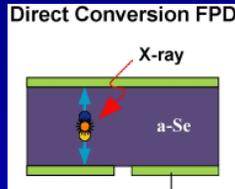
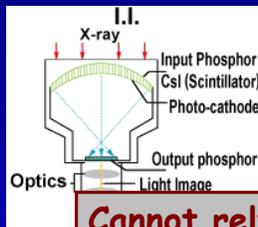
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# Radiation Capture/Conversion

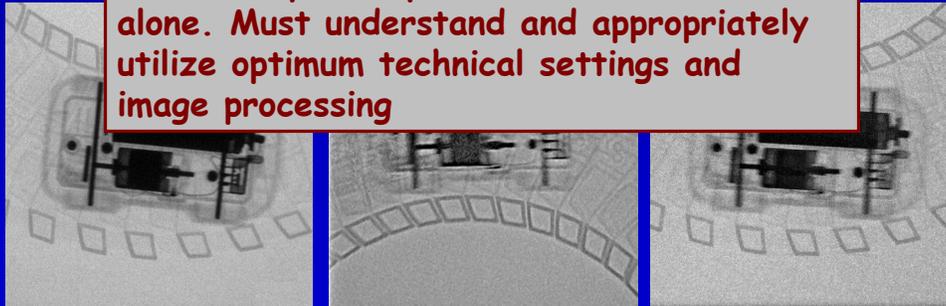


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# Image Detector (Fluoro LIH)



Cannot rely on reported detector metrics alone. Must understand and appropriately utilize optimum technical settings and image processing



# Detector Input Dose Rates (XRII)

Dose Rate Selection

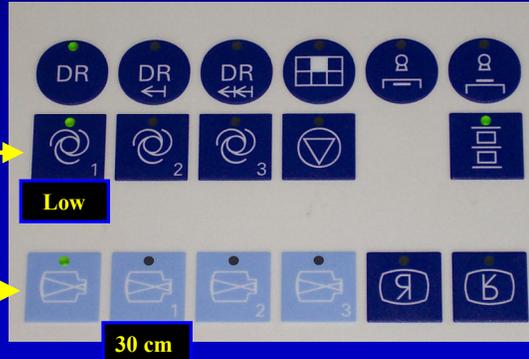
Field of View Selection

DR DR DR DR DR DR  
DR ← DR ←← DR  
1 2 3  
Low Norm High  
40 cm 30 cm 22 cm 17 cm

# Detector Input Dose Rates (XRII)

Dose Rate Selection

Field of View Selection



Continuous Fluoroscopy: Input dose per frame of fluoroscopy?

# Detector Input Dose Rates (XRII)

- Low Dose Mode
- Cont. Fluoroscopy
- 30 cm FOV

Detector Input Dose/Fr?

- A. 0.37  $\mu\text{R}$  (3.2 nGy)
- B. 0.75  $\mu\text{R}$  (6.6 nGy)
- C. 1.5  $\mu\text{R}$  (13.1 nGy)
- D. 3.0  $\mu\text{R}$  (26.3 nGy)
- E. 6.0  $\mu\text{R}$  (52.6 nGy)
- F. No Clue



.....values assume FDA minimum beam filtration

# Detector Input Dose Rates (XRII)

- Low Dose Mode
- Cont. Fluoroscopy
- 30 cm FOV

Detector Input Dose/Fr?

- A. 0.37  $\mu\text{R}$  (3.2 nGy)
- B. 0.75  $\mu\text{R}$  (6.6 nGy)**
- C. 1.5  $\mu\text{R}$  (13.1 nGy)
- D. 3.0  $\mu\text{R}$  (26.3 nGy)
- E. 6.0  $\mu\text{R}$  (52.6 nGy)
- F. No Clue



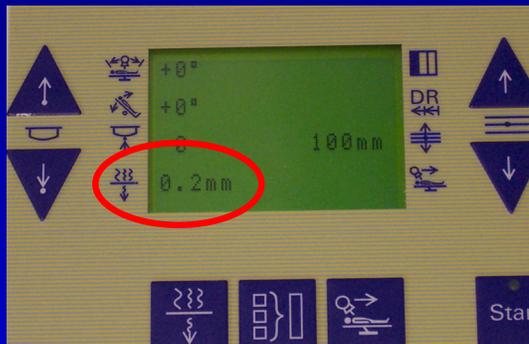
.....values assume FDA minimum beam filtration

# Detector Input Dose Rates (XRII)

- Low Dose Mode
- Cont. Fluoroscopy
- 30 cm FOV

Detector Input Dose/Fr?

- A. 0.37  $\mu\text{R}$  (3.2 nGy)
- B. 0.75  $\mu\text{R}$  (6.6 nGy)**
- C. 1.5  $\mu\text{R}$  (13.1 nGy)
- D. 3.0  $\mu\text{R}$  (26.3 nGy)
- E. 6.0  $\mu\text{R}$  (52.6 nGy)
- F. No Clue



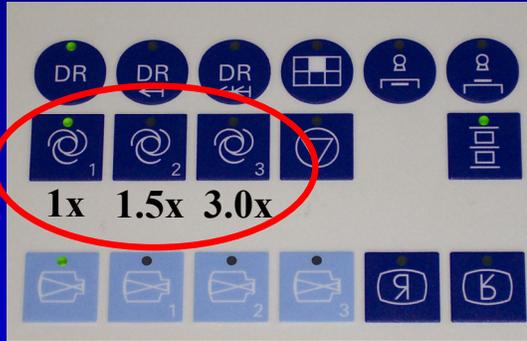
.....values assume FDA minimum beam filtration

.....can use 2x these values if minimum 0.2 mm Cu beam filtration is utilized

# Detector Input Dose Rates (XRII)

- Low Dose Mode
- Cont. Fluoroscopy
- 30 cm FOV

Detector Input Dose/Fr?



# Detector Input Dose Rates (XRII)

- Low Dose Mode
- Cont. Fluoroscopy
- 30 cm FOV

Detector Input Dose/Fr?



Detector dose scales inversely as either the ratio of the FOV, or as the ratio squared

## Video Frame Rate

What is the video frame rate in the U.S.A.?

Ans: 30 video frames per second



## Detector Input Dose Rates (XRII)

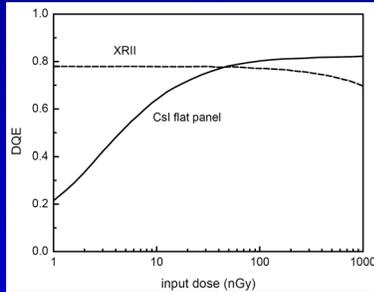
- ◆ Rauch's 30-30-30 Rule:
  - For a nominal 30 cm image intensifier field of view (FOV),  
Pulse rate of 30 pps,  
Set the EERD to 30  $\mu\text{R}/\text{sec}$
  - For other FOV's, scale by either the ratio of the FOV (auto optical lens aperture) or the square of the ratio
  - Double the values if spectral beam filtration (e.g. minimum 0.2 mm Cu) is utilized

**For flat panel, special consideration is required!!**



# Detector Input Dose Rates (FP)

## Detector Metrics (Fluoroscopy Doses)

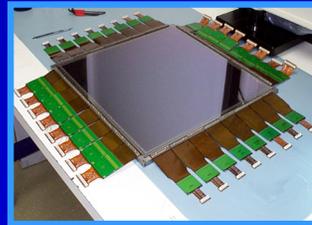


Adapted from Koch, A., Macherel, J.M., Wirth, T., de Groot, P., Ducourant, T., Couder, D., Moy, J.P., & Calais, E. (2001). Detective quantum efficiency of an X-ray image intensifier chain as a benchmark for amorphous silicon flat panel detectors, Proc. SPIE, 4320, 115-20

## Image Intensifier

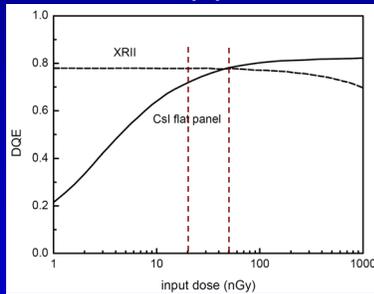


## Flat Panel



# Detector Input Dose Rates (FP)

## Detector Metrics (Fluoroscopy Doses)



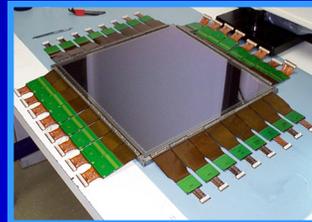
*"The minimum operating dose level is defined by the magnitude of the noise arising in the AM array and readout electronics. This typically sets the lower operating limit for detector dose at 20-50 nGy."*

Cowan AR et al., Solid-state, flat-panel, digital radiography detectors and their physical imaging characteristics, Clin Radiol (2008)

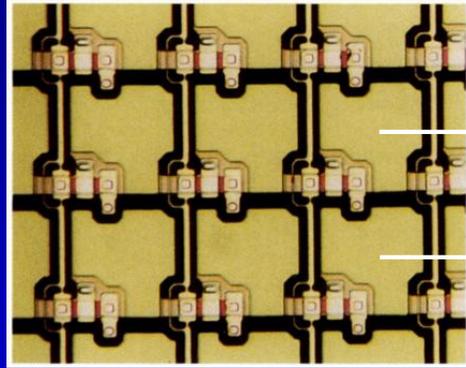
## Image Intensifier



## Flat Panel



# Pixel Pitch – Air Kerma per Pixel



Pixel Pitch

For the transition from XRII to Flat Panel, the required EERD can be estimated by determining the air kerma required for the XRII when it is operating at the same pixel pitch at that for the flat panel.

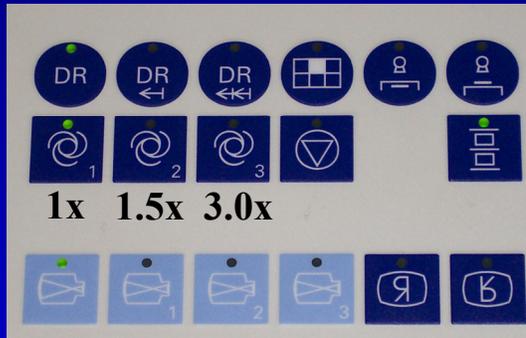
Detector	Mfg.	Pixel Pitch
Safire (a-Se, a-Si TFT)	Shimadzu	0.150
Philips, Siemens (CsI(Tl), a-Si TFT) - Angio	Trixell	0.154
Philips, Siemens (CsI(Tl), a-Si TFT) - Cardiac	Trixell	0.184
GE, Revolution (CsI(Tl), a-Si TFT)	GE	0.200

# Pixel Pitch vs Input Dose

Pixel Pitch (mm)	Equivalent XRII Diam (cm) for 1024 Pixels	Diam <sup>2</sup>	Ratio wrt 30 cm FOV	EERD (μR)	EERD (nGy)
<b>XRII</b>					
0.293	30.00	900.00	1.00	1.00*	8.76
<b>Flat Panel</b>					
0.150	15.36	235.93	3.81	3.81	33.42
0.154	15.77	248.68	3.62	3.62	31.70
0.184	18.84	355.01	2.54	2.54	22.21
0.200	20.48	419.43	2.15	2.15	18.80

\*Per Rauch's 30-30-30 rule

# Detector Input Dose Rates



What about *pulsed* fluoroscopy?

# Dose Per Pulse (<30 pps)

- For pulse rates lower than 30 pps, use Aufrichtig\* perceptual pulsed fluoroscopy scale factor to adjust dose per frame for different frame rates

$$(\text{Dose/Pulse})_2 = (\text{Dose/Pulse})_1 * \text{SQRT}[(\text{Pulse Rate})_1 / (\text{Pulse Rate})_2]$$

Example: Change from 30pps to 7.5 pps

$$\begin{aligned} (\text{Dose/Pulse})_2 &= (\text{Dose/Pulse})_1 * \text{SQRT}[30/7.5] \\ &= (\text{Dose/Pulse})_1 * 2 \end{aligned}$$

\*Perceptual comparison of pulsed and continuous fluoroscopy, Richard Aufrichtig, Med. Phys. 21 (2), February 1994

# Fluoroscopic Image Quality

Blur (Frame integration Time)

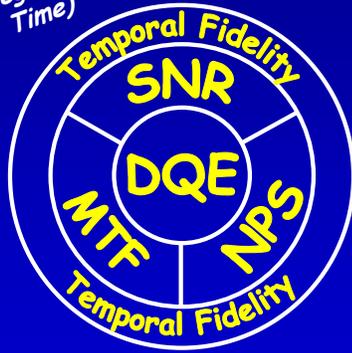
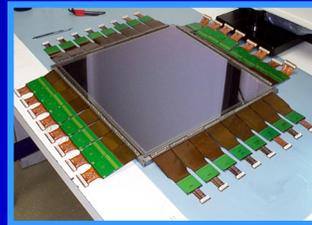


Image Intensifier

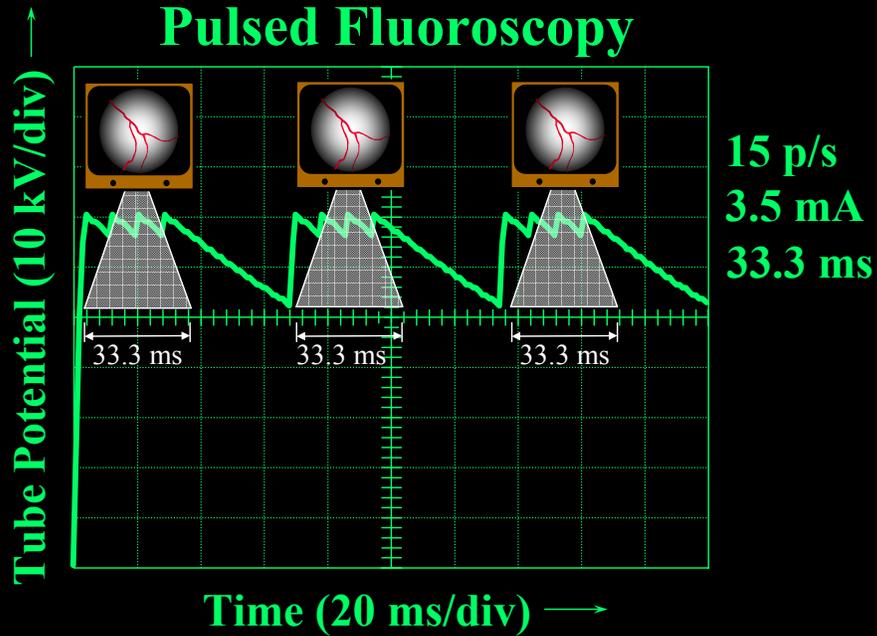


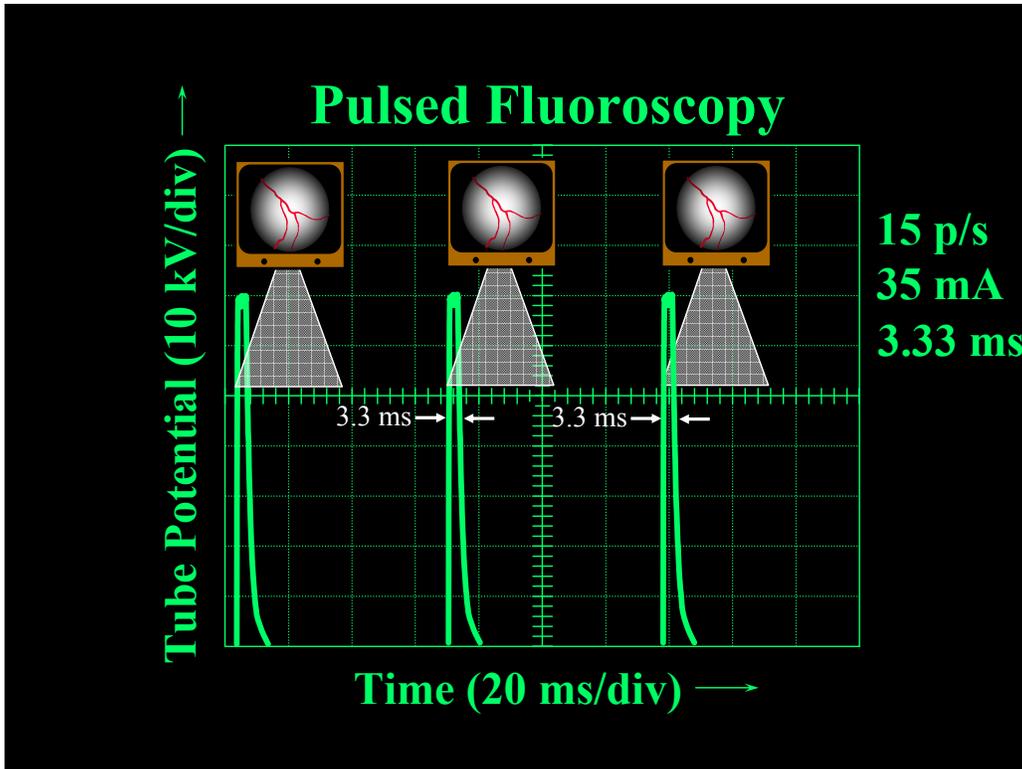
Flat Panel



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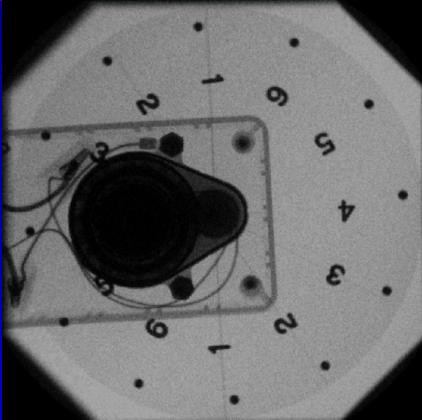
## Pulsed Fluoroscopy



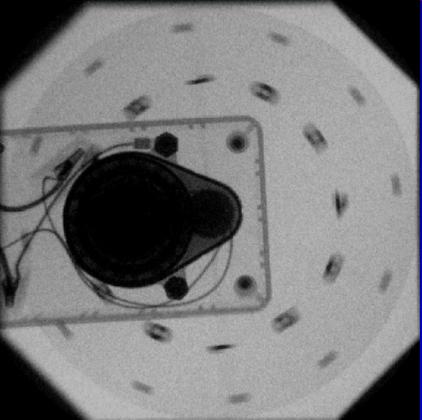


## Exposure ON-time – Pulsed vs Cont

---



**Pulsed Fluoro\***  
(30 pulses per sec)  
\*Displayed at 7.5 fps



**Continuous Fluoro\***  
(30 video frames per sec)  
\*Displayed at 7.5 fps

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# Fluoroscopic Image Quality

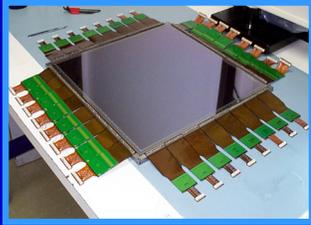
Diagram illustrating Fluoroscopic Image Quality metrics:

- Temporal Fidelity
- SNR
- DQE
- MTF
- NPS
- Temporal Fidelity
- Frame integration time
- LAG (Signal retention)

Image Intensifier

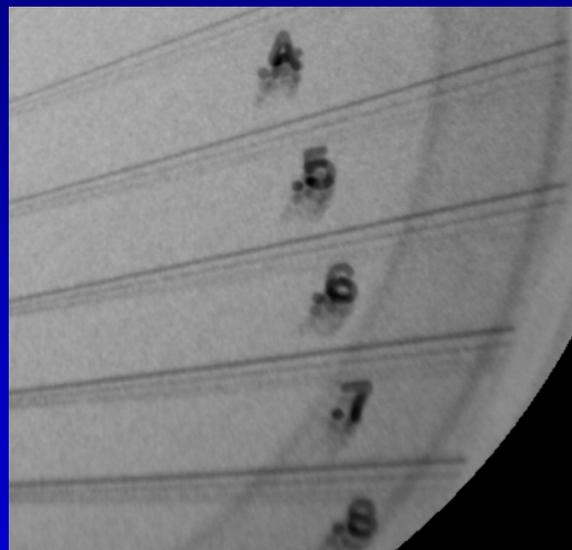


Flat Panel



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## Lag (Signal Retention)



Measured by the signal retained in the third video field following removal of the image source

# Fluoroscopic Image Quality

### Image Intensifier

### Flat Panel

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# Blur versus Recursive Filtering

IMAGE BLUR & LAG  
HIGH CONTRAST  
HLF CONTINUOUS  
NO FRAME INTEG

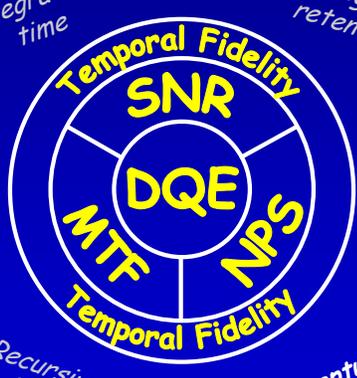
**Continuous Fluoroscropy**  
**Without Recursive Filtering**

IMAGE BLUR & LAG  
HIGH CONTRAST  
HLF 2-PPS  
NO FRAME INTEG

**Pulsed Fluoroscropy**  
**With Recursive Filtering**

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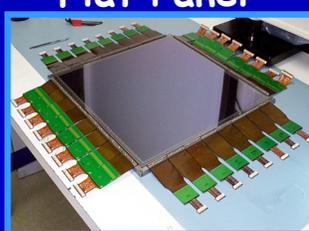
# Fluoroscopic Image Quality



**Image Intensifier**



**Flat Panel**



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# Perceptual Integration

Where are the 3's

8958425412835642102650172651270657592429  
 6576515015990176512915601765017657603141  
 6768737976671516161449120241717245670124  
 5501456576598244210542320675127688696252  
 8980949198894838482661452562949566892456

**30 Frames/sec**

# Perceptual Integration

## Where are the 3's

8958425412835642102650172651270657592429  
6576515015990176512915601765017657603141  
6768737976671516161449120241717245670124  
5501456576598244210542320675127688696252  
8980949198894838482661452562949566892456

8 Frames/sec



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# Pulsed Fluoroscopy

## Optimizing the Use of Pulsed Fluoroscopy to Reduce Radiation Exposure to Children

Mervyn D. Cohen, MB, ChB, MD

Radiologists desire to keep radiation dose as low as possible. Pulsed fluoroscopy provides an opportunity to lower radiation exposure to children undergoing fluoroscopic studies. To optimize the ability of pulsed fluoroscopy to decrease radiation dose to patients during fluoroscopic studies, radiologists need to understand how pulsed fluoroscopy operates. This report reviews the basic physics knowledge needed by radiologists to best use pulsed fluoroscopy to minimize radiation dose. It explains the paradox that the best video frame-grabbed images are obtained when using the lowest fluoroscopy pulse rate and therefore the lowest fluoroscopy radiation dose.

**Key Words:** Radiation dose, pulsed fluoroscopy, patient safety

*J Am Coll Radiol 2008;5:205-209. Copyright © 2008 American College of Radiology*

### INTRODUCTION

There have been many appropriate recent discussions regarding the need to reduce the radiation dose to pediatric patients to as low as reasonably achievable [1-3].

One method of dose reduction that has received recent attention is the use of pulsed fluoroscopy [4-9]. New grid-controlled x-ray tubes have a grid placed between the cathode and the anode [10]. This allows pulses of fluoroscopy to leave the x-ray tube at rates between 1 and 30 frames/s. Radiation no longer enters a patient continuously but in a series of short x-ray flashes [11]. Fluoroscopy at 30 frames/s has been termed continuous fluoroscopy [10,12]. Aufrecht et al [13] defined pulsed fluoroscopy as 15 frames/s or less and continuous fluoroscopy as 30 frames/s.

At my institution we have recently had experience with new pulsed fluoroscopy units from Philips and Siemens and wish to share our important learning during 12 months of experience with these units. Siemens Sireteq SD AXIOM, Siemens Medical Systems, Berlin, Ger-

many outlined in our experience should be applicable to units manufactured by other vendors. This study was approved by our institutional review board.

### DEFINITIONS

To avoid any misunderstanding, I first define 3 methods of acquiring and keeping permanent images obtained during a fluoroscopic study:

1. Recording the entire study (eg, on CD-ROM or videotape): Disadvantages of this method are that the study is cumbersome to review and cannot be sent to a picture archiving and communication system (PACS). This method is not routinely used, apart from feeding studies.
2. Exposed images: These are traditional fluoroscopically acquired images obtained by pushing an exposure button to specifically expose and acquire an image at a particular moment in time. The image can then be

Must increase the dose per pulse as the fluoroscopic pulse rate is decreased

Counters the increased perception of noise as pulse rate is reduced

Greatly improves the quality of the LIH image, often obviating the need to create a radiographic spot image

The short exposure time per frame greatly improves motion blurring

Real reduction in patient dose with improvement in image quality

More likely to use the lower frame rates due to lower perceived noise



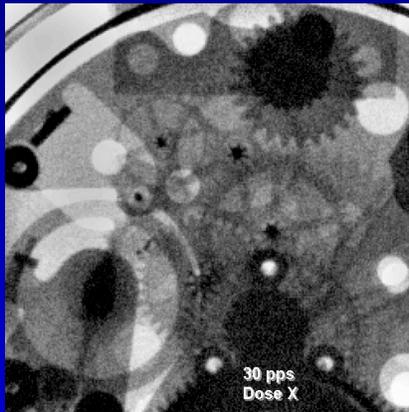
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# Dose Per Pulse



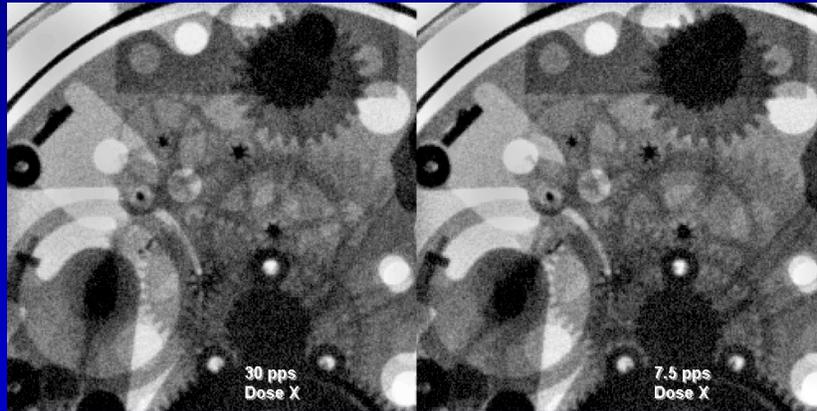
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# Dose Per Pulse



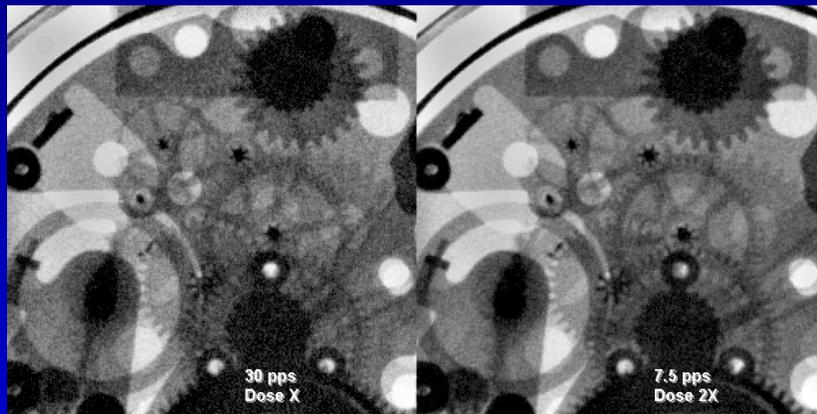
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# Dose Per Pulse



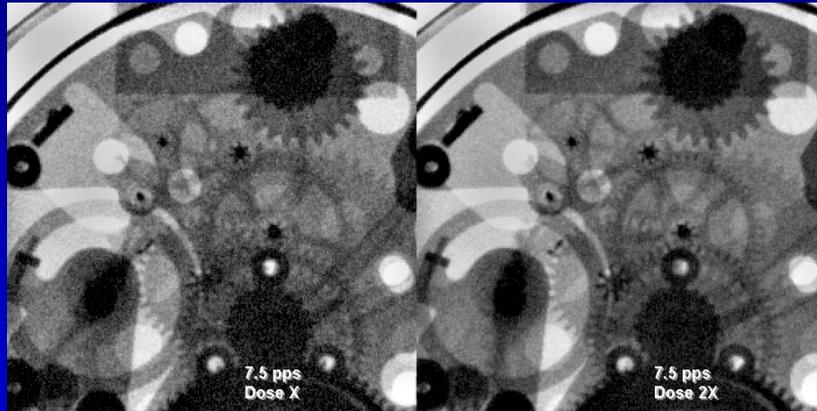
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# Dose Per Pulse



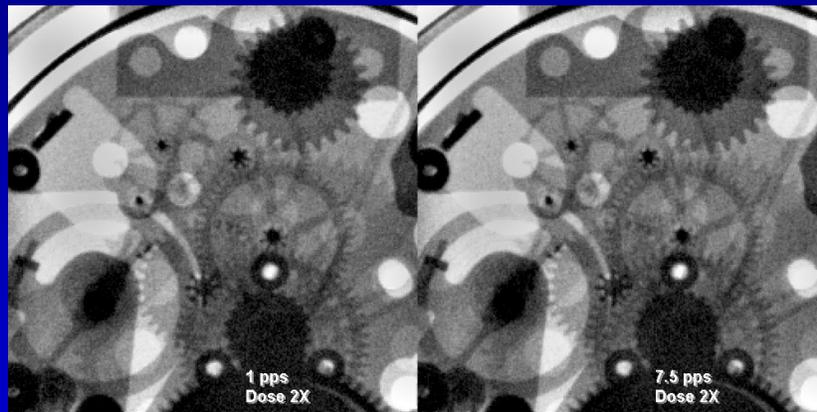
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# Dose Per Pulse



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# Dose Per Pulse



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## Subtle sources of increased dose (Re: Image Gently)

- ◆ Poor geometry

  - Short source to skin distance

  - Large gap between patient and image receptor



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## Imager Geometry



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# Imager Geometry



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## Subtle sources of increased dose (Re: Image Gently)

- ◆ Poor geometry
  - Short source to skin distance
  - Large gap between patient and image receptor
- ◆ Capacitive discharge from high tension cables during pulsed fluoroscopy

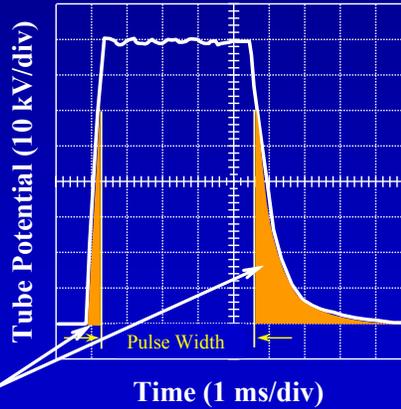


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# Exposure ON-time

X-ray ON-pulse

## Exposure Pulse

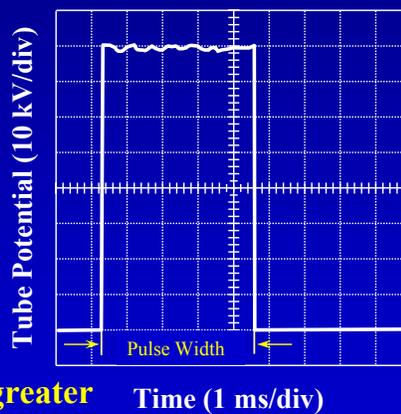


Regions of non-useful radiation production. Potential for higher skin dose

# Exposure ON-time

X-ray ON-pulse

## Exposure Pulse



**Grid-controlled pulse leads to greater control and reduced skin dose**

## Subtle sources of increased dose (Re: Image Gently)

- ◆ Poor geometry
  - Short source to skin distance
  - Large gap between patient and image receptor
- ◆ Capacitive discharge from high tension cables during pulsed fluoroscopy
- ◆ **Collimator leakage**

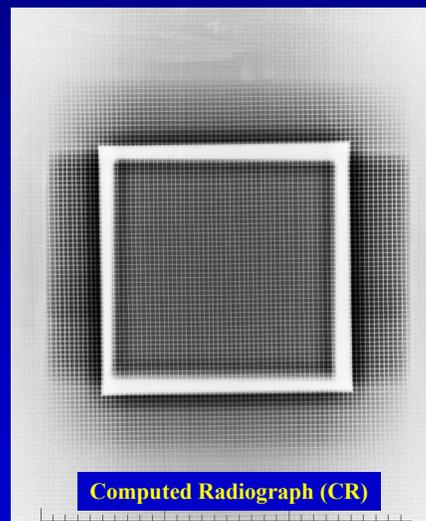
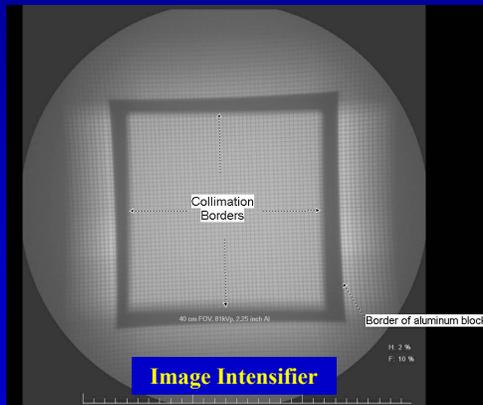


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## Collimator Leakage

All collimators leak radiation

FDA allows leakage rate to be 100 mR/Hr at 1 meter (Max kV and max continuous rate)



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# Collimator Leakage

## ◆ Not Due to Scatter



Wire screen was setting above the aluminum blocks

# Image Quality: What is it?

- ◆ “Image quality depends only on intrinsic, objective physical characteristics of an imaging system, and can be measured independently of an observer”
- ◆ “Image quality is whatever the observer says it is (i.e., it is a subjective perception of the image, ‘in the eye of the beholder’)”

*Definitions courtesy Ralph Schaezting, Agfa Corp.*

# Fluoroscopic Image Quality

The image contains two diagrams. On the left is a circular diagram with 'SNR' in the center, surrounded by 'DQE' and 'NPS'. The outer ring lists 'Contrast', 'Graininess', 'Temporal Fidelity', and 'Sharpness'. On the right is a diagram of the human visual system showing the left and right visual fields, eyes, optic chiasm, and brain structures like the pulvinar nucleus, lateral geniculate nucleus, superior colliculus, and optic radiation.

Human Visual Perception

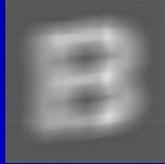
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# Human Visual Perception

- ◆ Can result in different interpretations of the same image
- ◆ Can make up for deficits in image quality

# Sharpness and HVP

- ◆ What is this?



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# Sharpness and HVP

- ◆ What is this?

Although this image is quite unsharp, that is not the underlying reason that the image is difficult to interpret....



....this task is difficult because the image is presented out of context

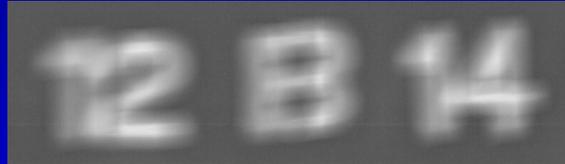


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## Sharpness and HVP

- ◆ What is this?

Image presented in context

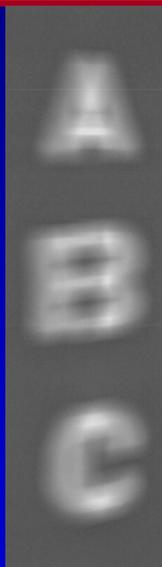


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## Sharpness and HVP

- ◆ What is this?

Same image,  
different  
context



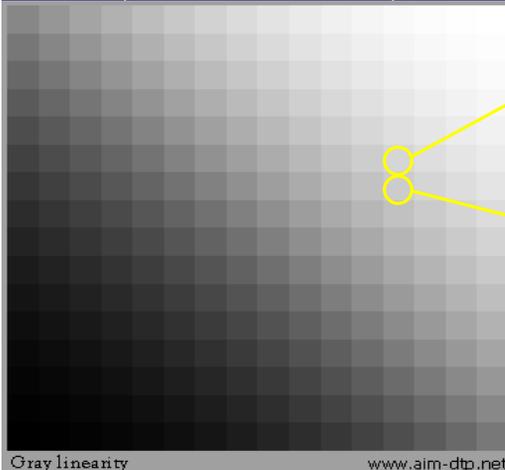
Medical imaging  
must always be  
conducted within a  
specified context



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# Contrast and HVP

256 Gray Levels  
(16 Rows x 16 Columns)



$I_1$

$I_2$

$$\text{Contrast, } (I_2 - I_1) / (I_2 + I_1)$$

Gray linearity

www.aim-dtp.net



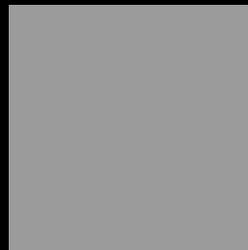
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# Contrast and HVP

Although these squares have measurably different gray levels, there is no perceptible contrast difference



Grey Level 150



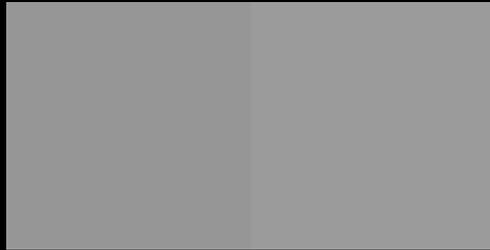
Grey Level 155



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# Contrast and HVP

## ◆ Mach Bands

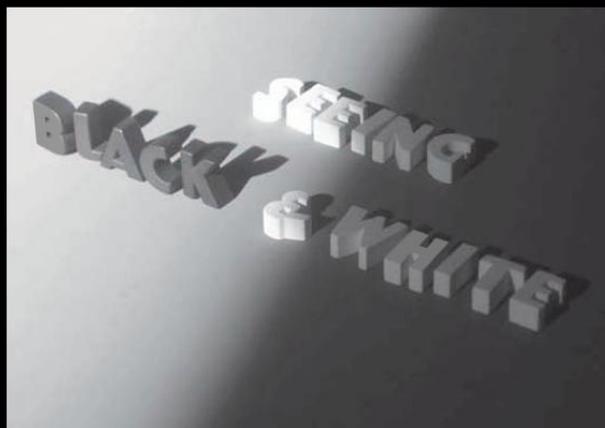


Grey Level 150

Grey Level 155



# Contrast and HVP



The letters of the word black are perceived to be of a darker shade of gray than the letters of the word white

Alan Gilchrist, "Seeing in Black & White", Scientific American Mind (2008)



# Contrast and HVP



The letter H appears to have changed its shade of gray



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# Contrast and HVP



B's are all gray level 150

H's are all gray level 119

In reality all of the H's are of the same shade of gray and are darker than the B's



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Dark → Light

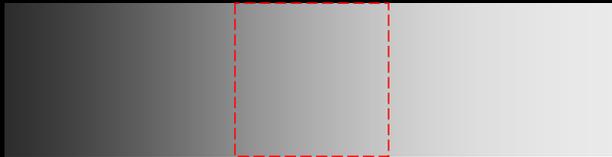


Human visual perception can result in two identical objects being perceived as having different gray levels

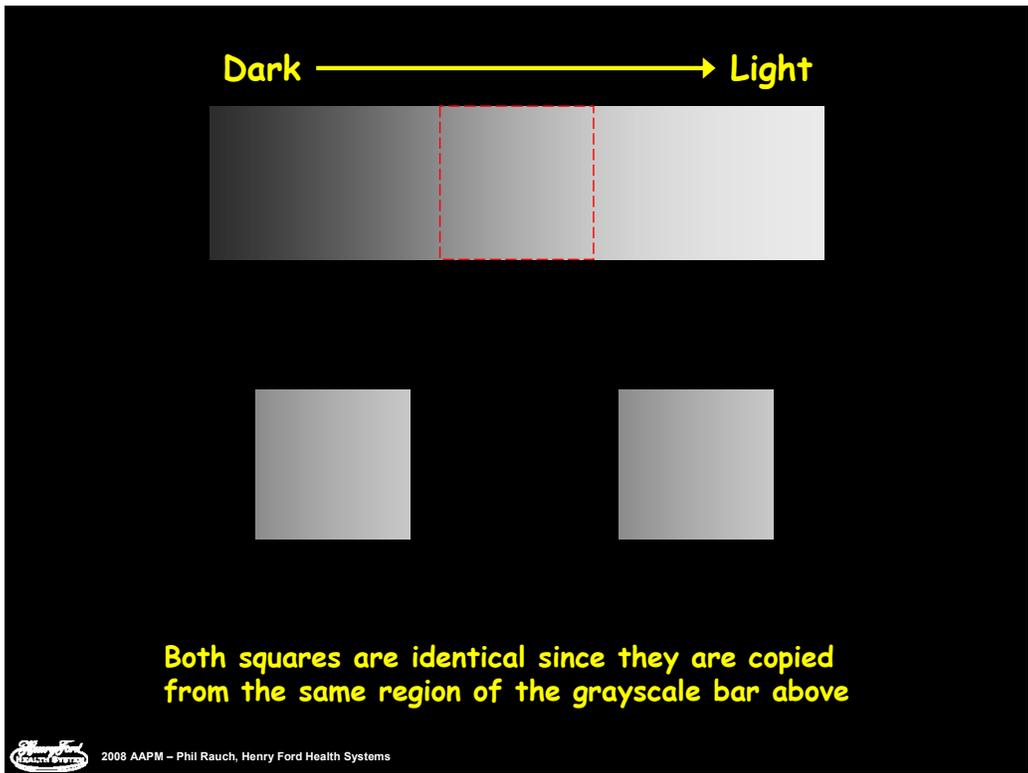
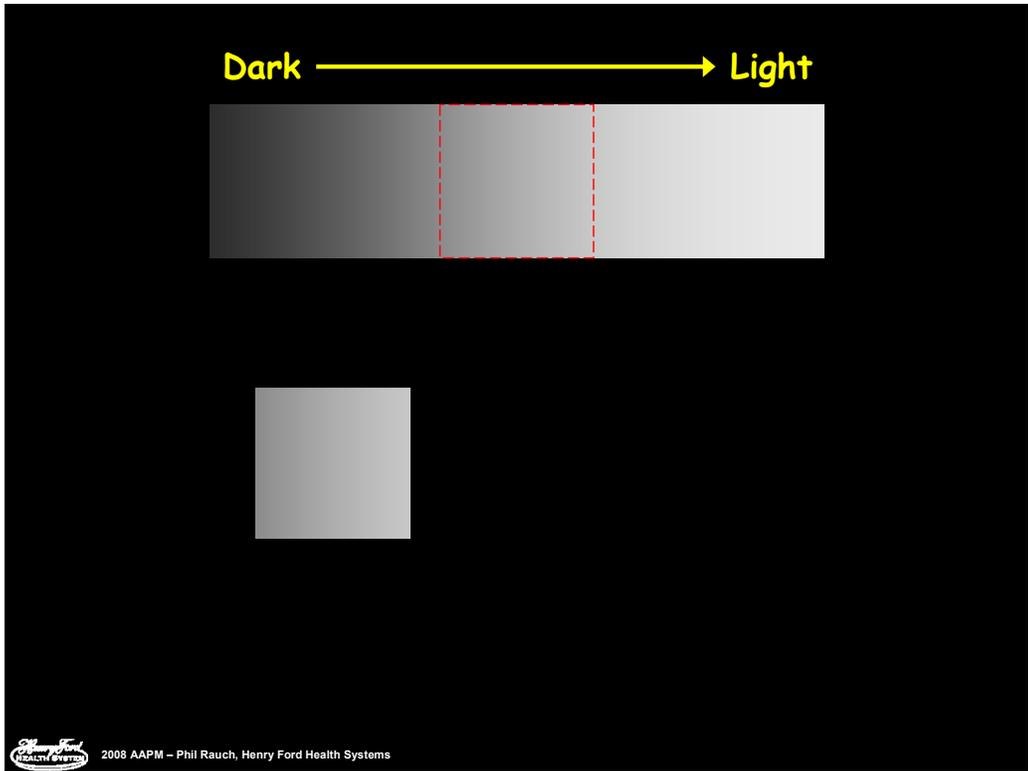


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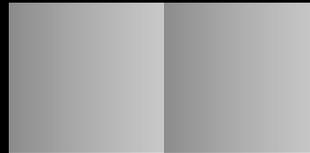
Dark → Light



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Dark → Light



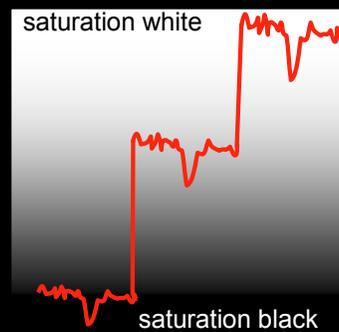
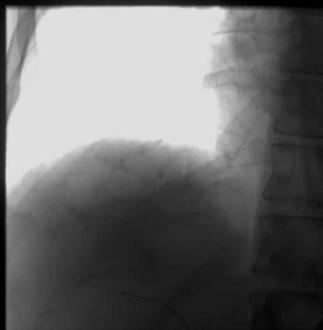
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# Contrast and HVP

## Dynamic Range Rendering

I.I. - 66 dB → 48 dB

CR - 80 dB → 48 dB



## Image Characteristics

### Dynamic Range Rendering

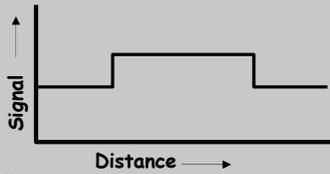


## Image Characteristics

### Dynamic Range Rendering

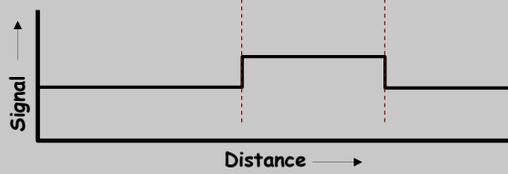
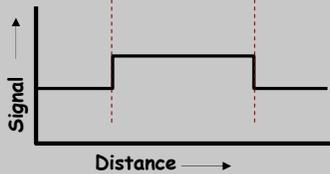


# HVS – Contrast Blindness



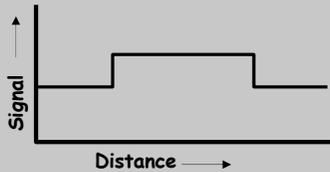
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# HVS – Contrast Blindness

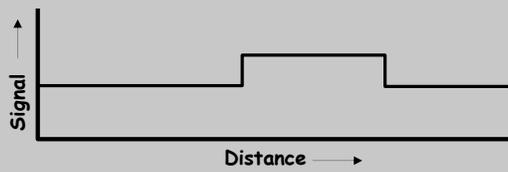


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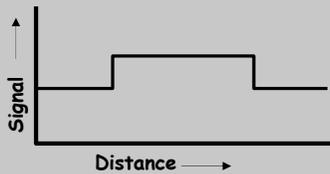
# HVS – Contrast Blindness



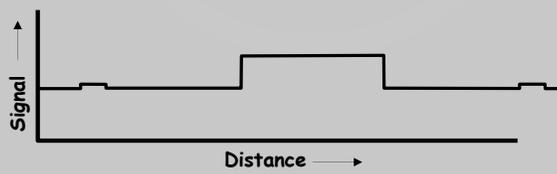
2008 AAPM – Phil Rauch, Henry Ford Health Systems



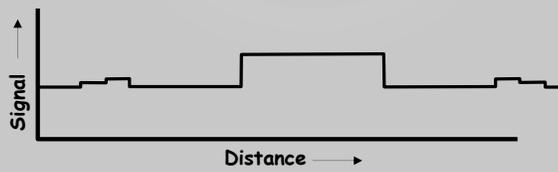
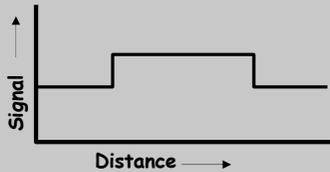
# HVS – Contrast Blindness



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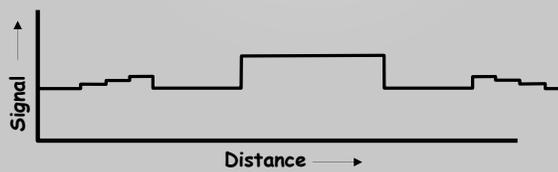
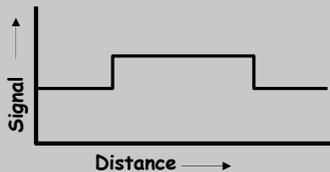


# HVS – Contrast Blindness



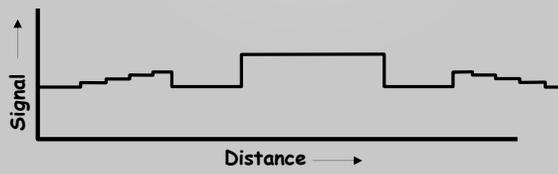
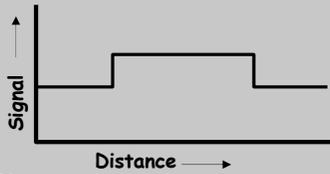
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# HVS – Contrast Blindness



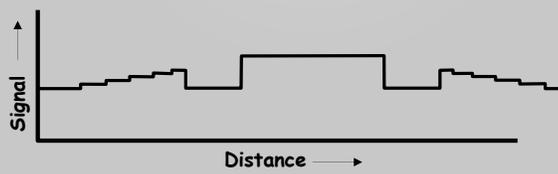
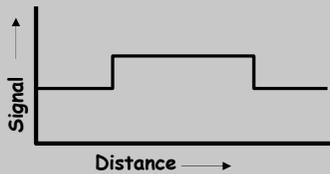
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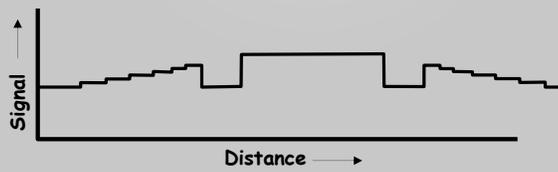
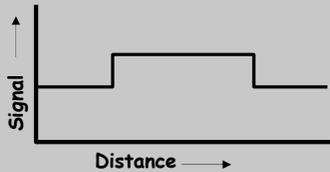
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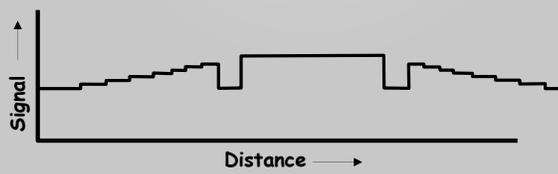
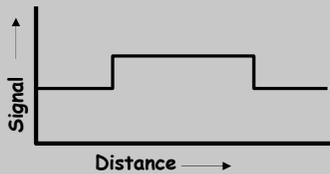
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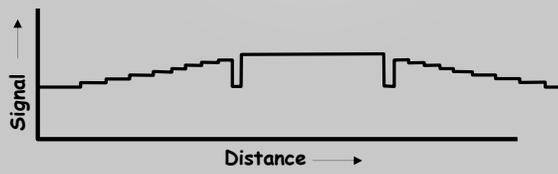
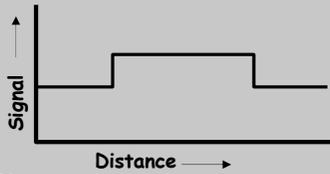
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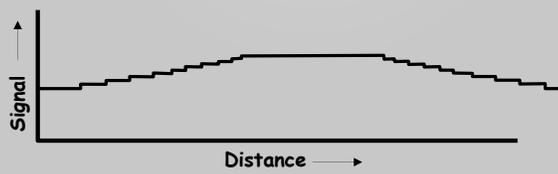
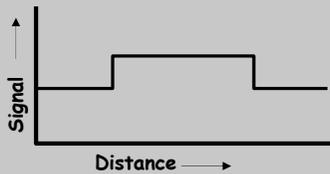
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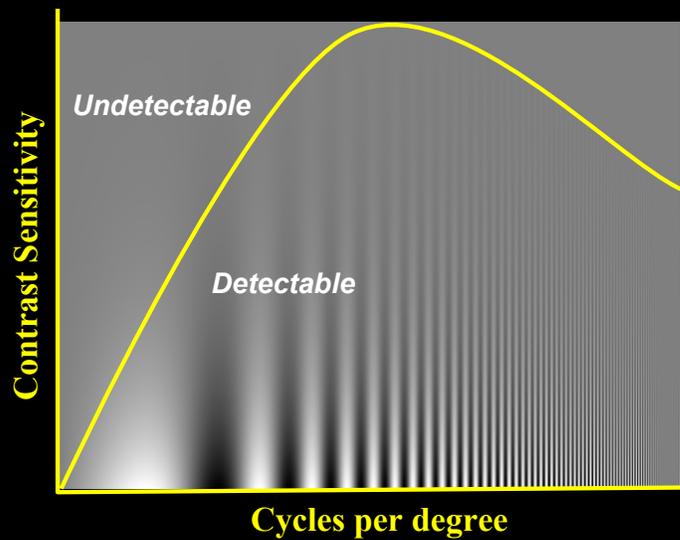
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# HVS – Contrast Blindness



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# Human Visual System

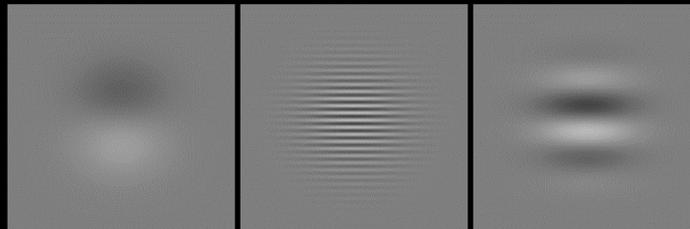


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## HVS – Contrast Perception

### GABORI ATTACK

Gabori, like the ones shown below, can sneak up slowly from anywhere.



Squash them quickly before they get you! But only click where you know you see a Gabori sneaking up through the fog. Triple click when you've had enough.

Quit

The Contrast Sensitivity Function (Peter Wenderoth)

[http://neurovision.berkeley.edu/Demonstrations/VSOC/vsoc/vsoc\\_main.html](http://neurovision.berkeley.edu/Demonstrations/VSOC/vsoc/vsoc_main.html)



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# Image Quality: What is it?

- ◆ "Image quality depends only on intrinsic, objective physical characteristics of an imaging system, and can be measured independently of an observer"
- ◆ "Image quality is whatever the observer says it is (i.e., it is a subjective perception of the image, 'in the eye of the beholder')"
- ◆ "Image quality is defined by an observer's ability to achieve an acceptable level of performance for a specified task"

*Definitions courtesy Ralph Schaetzing, Agfa Corp.*



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# Image Interpretation

Successful interpretation depends on...

- ◆ Image Attributes
- ◆ Human Observer (education, experience)
- ◆ Human Visual Perception
- ◆ Pattern Recognition
- ◆ Clarity of the imaging task
- ◆ Minimal external distractions
- ◆ Level of confidence



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## Conclusions

- ◆ Image quality is not just detector metrics
- ◆ Image quality is not just a subjective impression
- ◆ Image quality is a moving target
- ◆ Patient dose need not be linked to detector dose or kVp
- ◆ Demand and use aggressive spectral filtration



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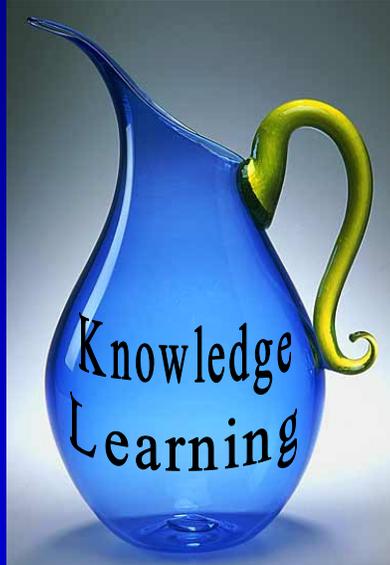
## Conclusions

- ◆ Be willing to break the *commandment* "High kV, Low mA", but only if aggressive spectral filtration is present
- ◆ Use pulsed fluoroscopy and the Aufrichtig scale to produce better images, not solely to reduce dose
- ◆ Remember that visual perception can sometimes mask the true nature of image attributes



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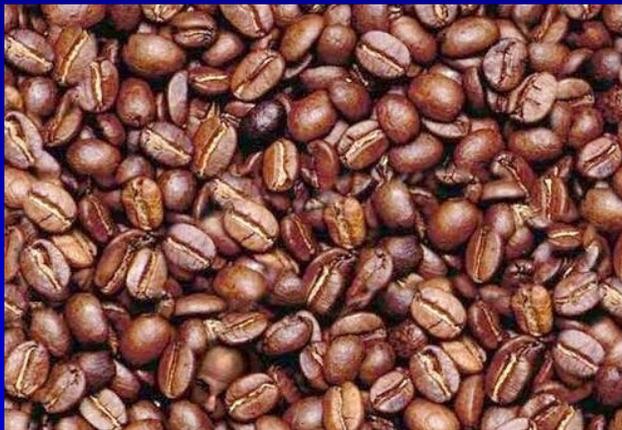
# My wish for you...



...a thirst for knowledge and learning that will last a lifetime

# Imaging Task

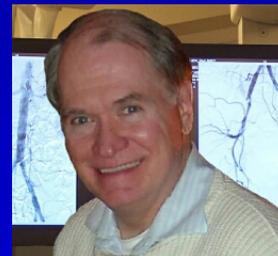
Find the human face.....



**Thank you**

Phil Rauch

philr@rad.hfh.edu



The Contrast Sensitivity Function (Peter Wenderoth)  
[http://neurovision.berkeley.edu/Demonstrations/VSOC/vsoc/vsoc\\_main.html](http://neurovision.berkeley.edu/Demonstrations/VSOC/vsoc/vsoc_main.html)