

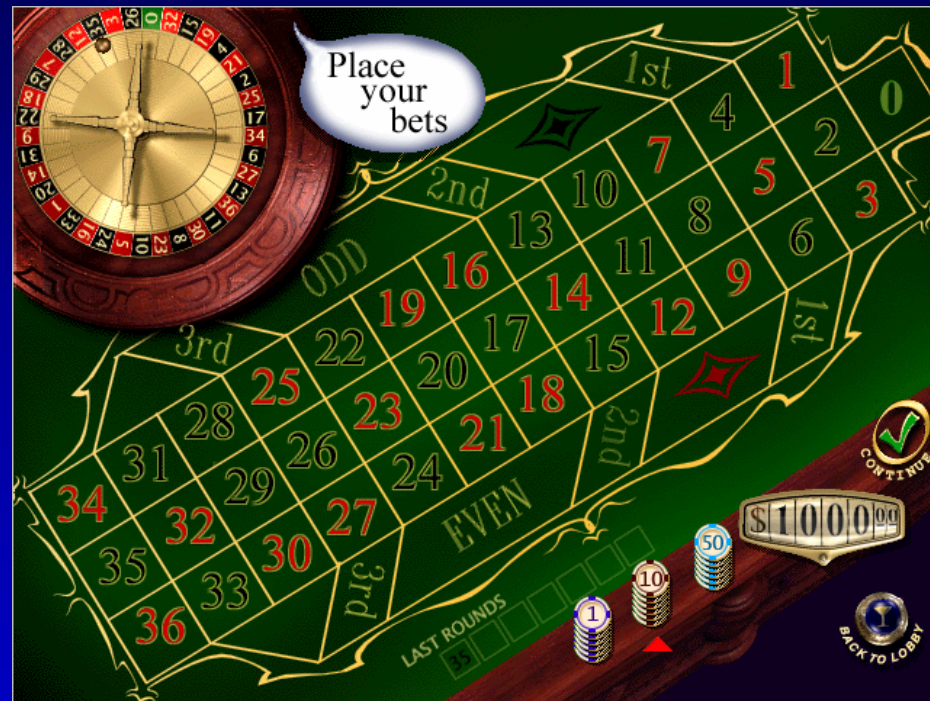
Clinical Monte Carlo: Photon Beams

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Philadelphia, PA 19111

What is Monte Carlo?



A mathematical method using random sampling

What is Monte Carlo ?

- The originators : Neumann and Ulam 1949
- The method : Random sampling from pdf's to construct solutions to problems.



John Von Neumann
(1903-1957)

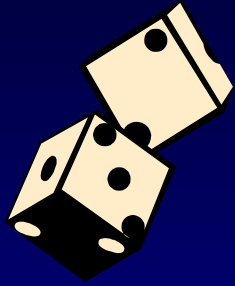


Stanislaw M. Ulam
(1909-1984)

Why call it Monte Carlo?



After the city in the Monaco principality ...



What is Monte Carlo Radiation Transport?

- Random sampling of particle interactions
 - a good supply of random numbers
 - probability distributions governing the physics processes
- Information obtained by simulating large number of histories

Why Use Monte Carlo for Radiotherapy Treatment Planning

An accuracy of about 5% in dose delivery is required to effectively treat certain types of cancers and to reduce complications.

ICRU Reports 24 (1976) and 42 (1988)

The Accuracy Requirement for Treatment Planning Dose Calculation

$$\sigma^2 = \sigma_{\text{calib}}^2 + \sigma_{\text{dose}}^2 + \sigma_{\text{setup}}^2 + \sigma_{\text{motion}}^2 + \dots$$

and

$$\sigma \geq 2\sigma_{\text{dose}} = 5\%$$

then

$$\sigma_{\text{dose}} = 2.5\%$$



CPU time required

1 Gy => 1 billion electrons (1cmx1cm field)

1% uncertainty for 0.3 cm cubes requires a few million electrons (hours on a PC)

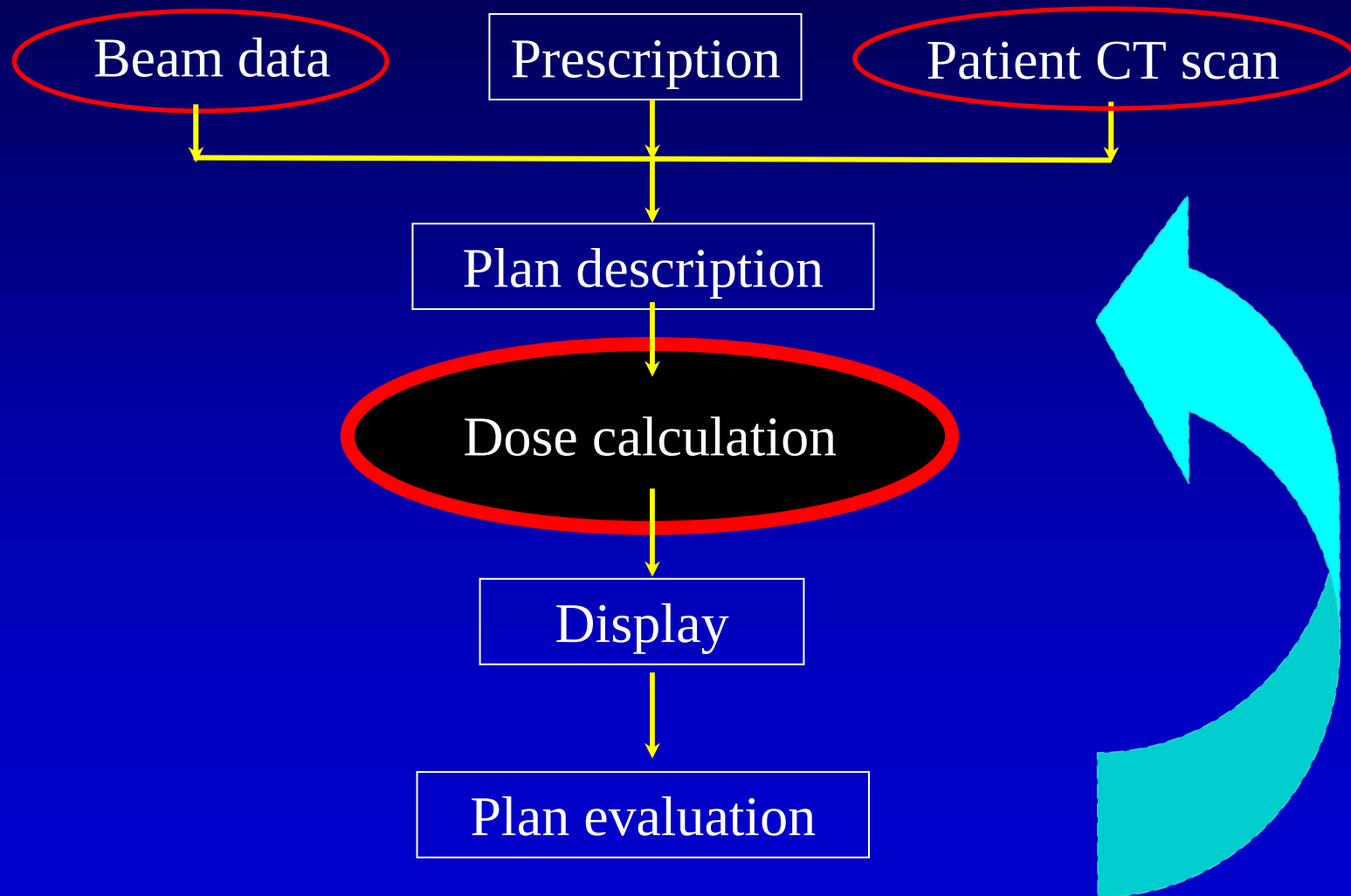
1 Gy => 1000 billion photons (1cmx1cm field)

1% uncertainty for 0.3 cm cubes requires up to a few billion photons (days on a PC)

Applications of M-C in radiotherapy

- Fluence and spectrum calculations
- Dosimetric parameters (stopping powers, etc.)
- Correction factors (BSF, HS, PS, P/S ratio...)
- Dosimeter response simulations
- Treatment head simulations
- Treatment planning dose calculations

Radiotherapy treatment planning



Dose algorithms for RTP

- Photon beams

Clarkson

FFT, FSPB, superposition convolution

super MC, XVMC

Monte Carlo

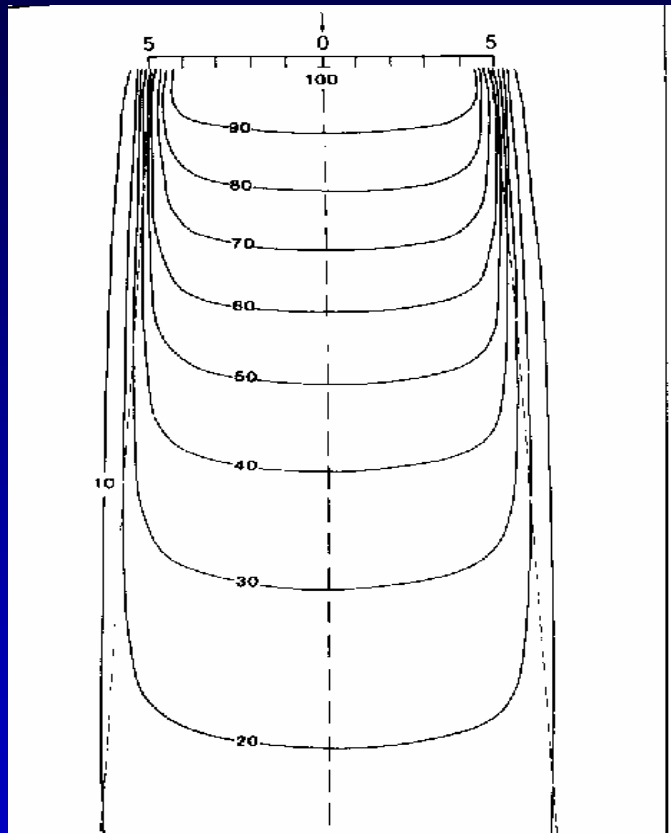
- Electron beams

3D pencil beam

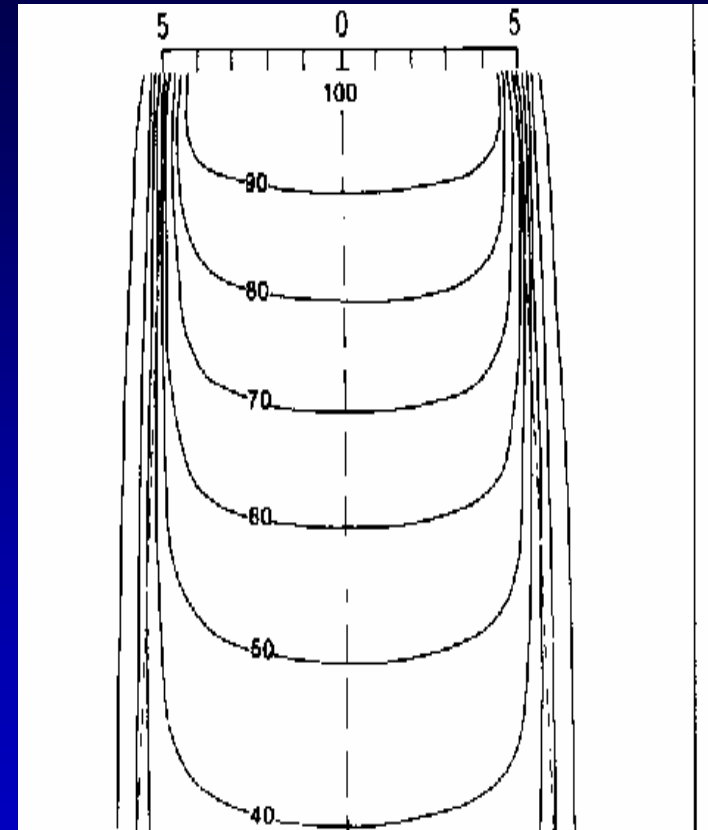
MMC, super MC, VMC

Monte Carlo

Equivalent Pathlength Correction

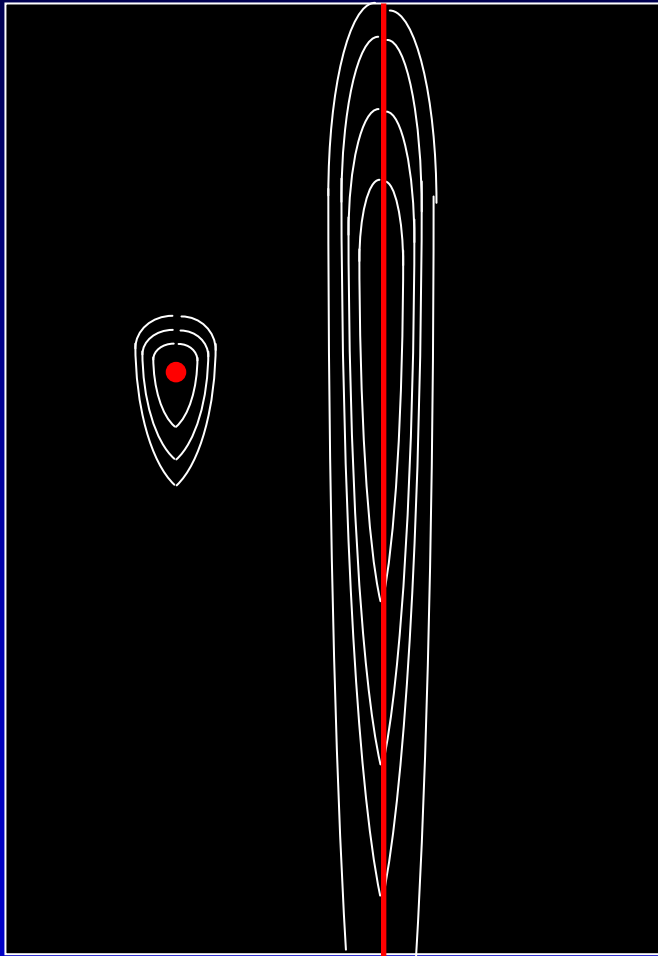


High-density medium

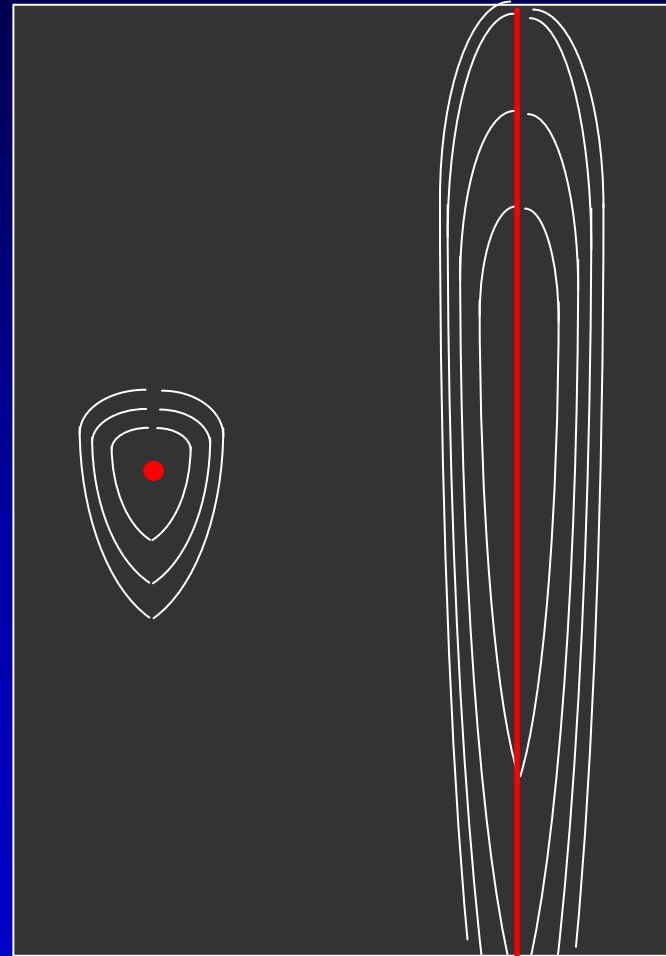


Low-density medium

Variation of Dose Kernels with Density

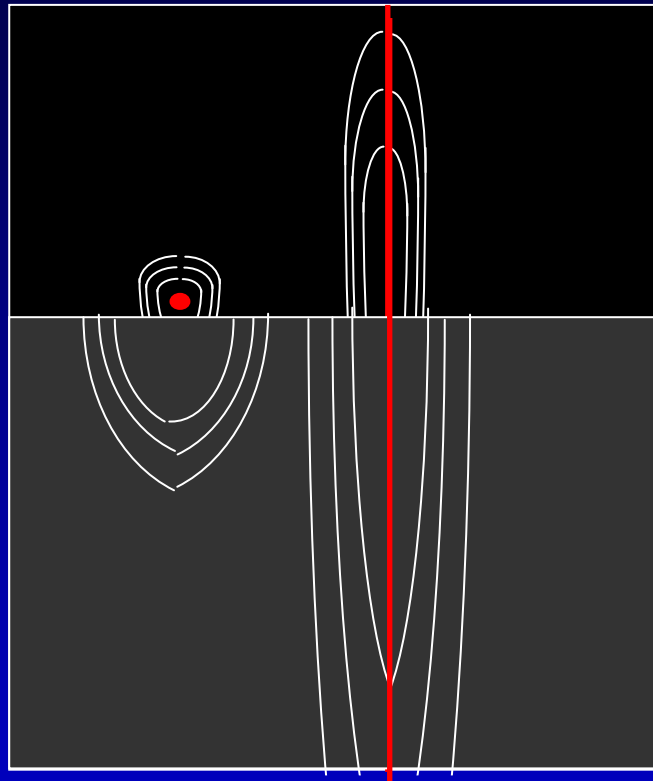


High-density medium



Low-density medium

Variation of Dose Kernels with Density

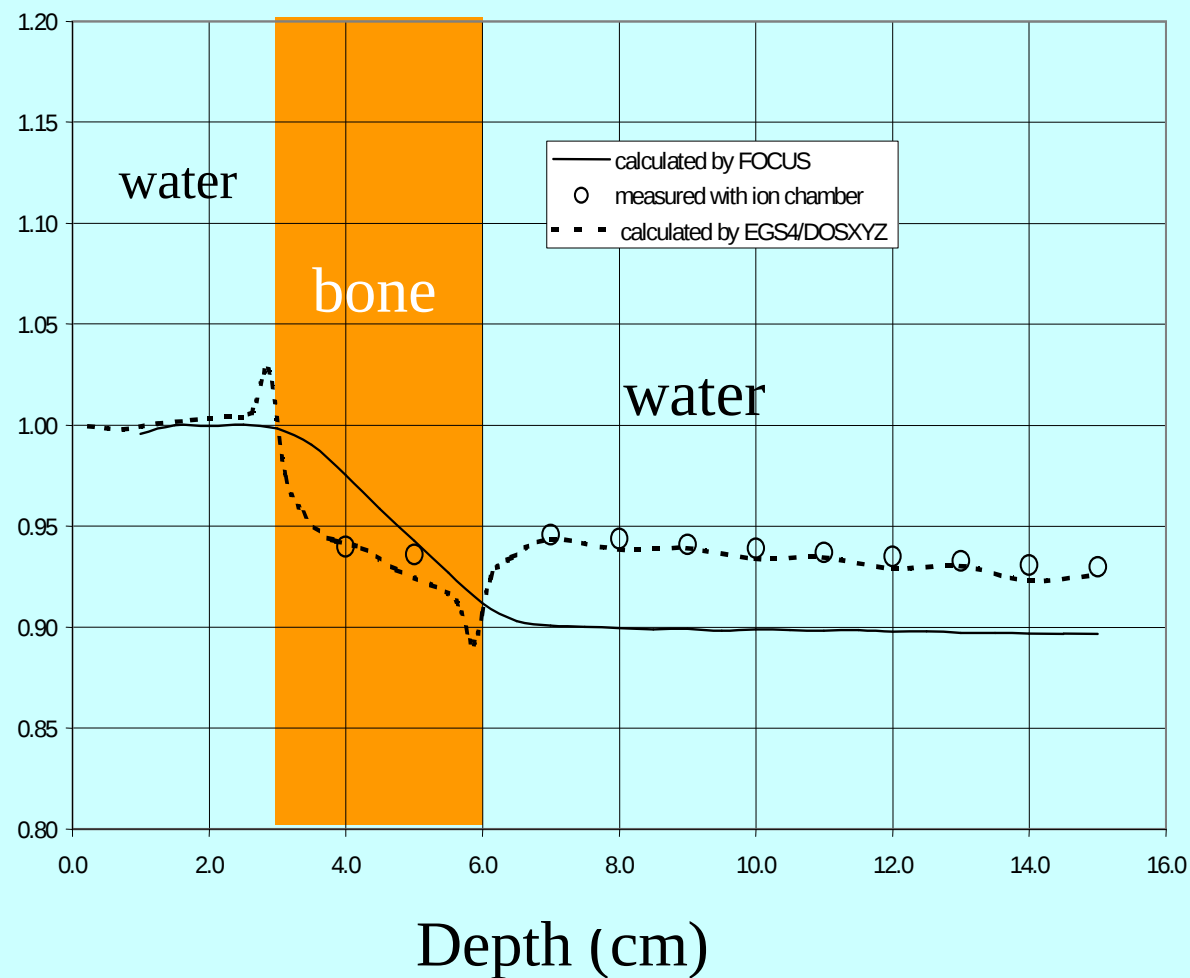


High-density medium

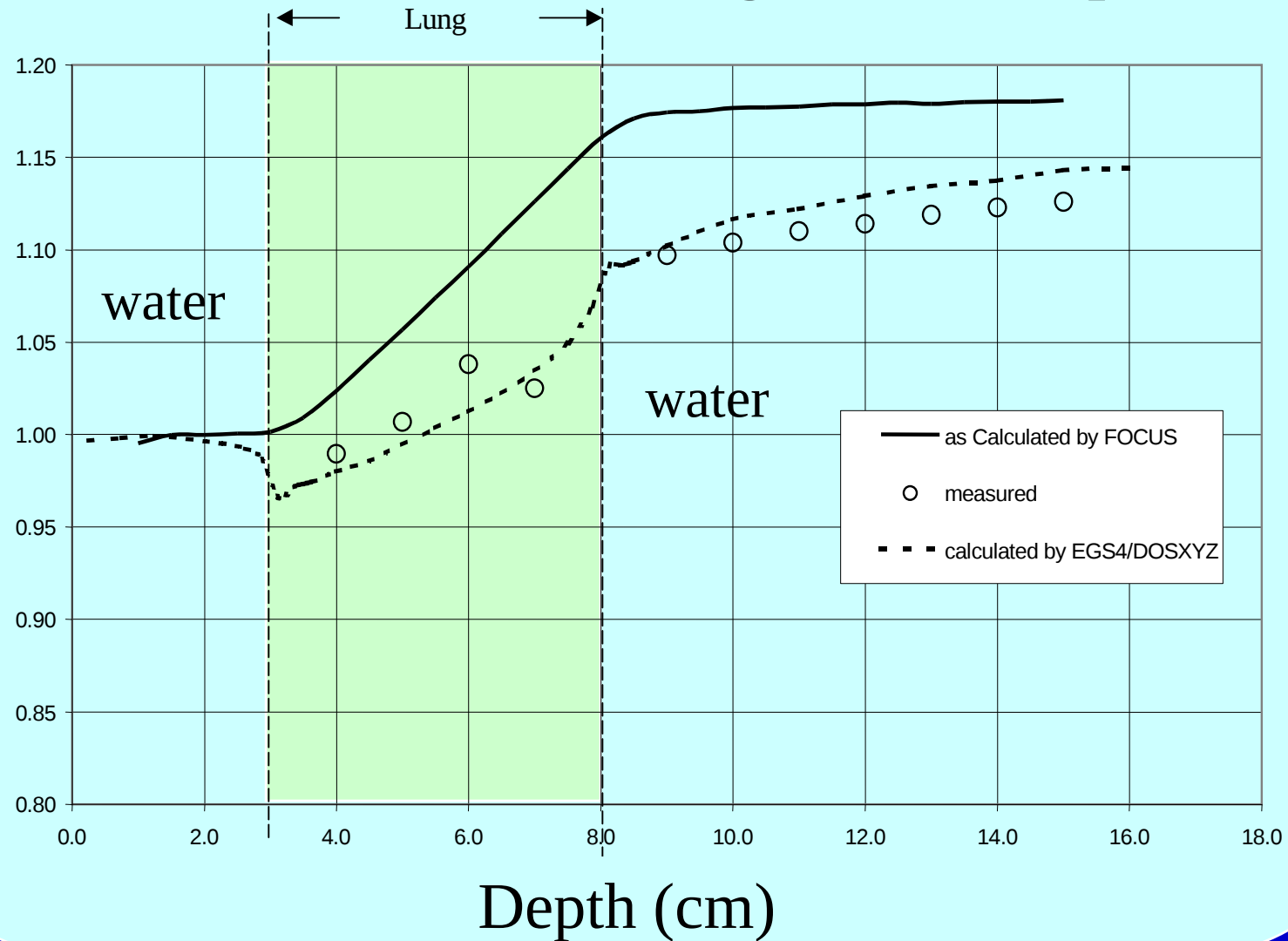
Low-density medium

The accuracy depends on how it is implemented.

Correction factor for bone for 6 MV photons

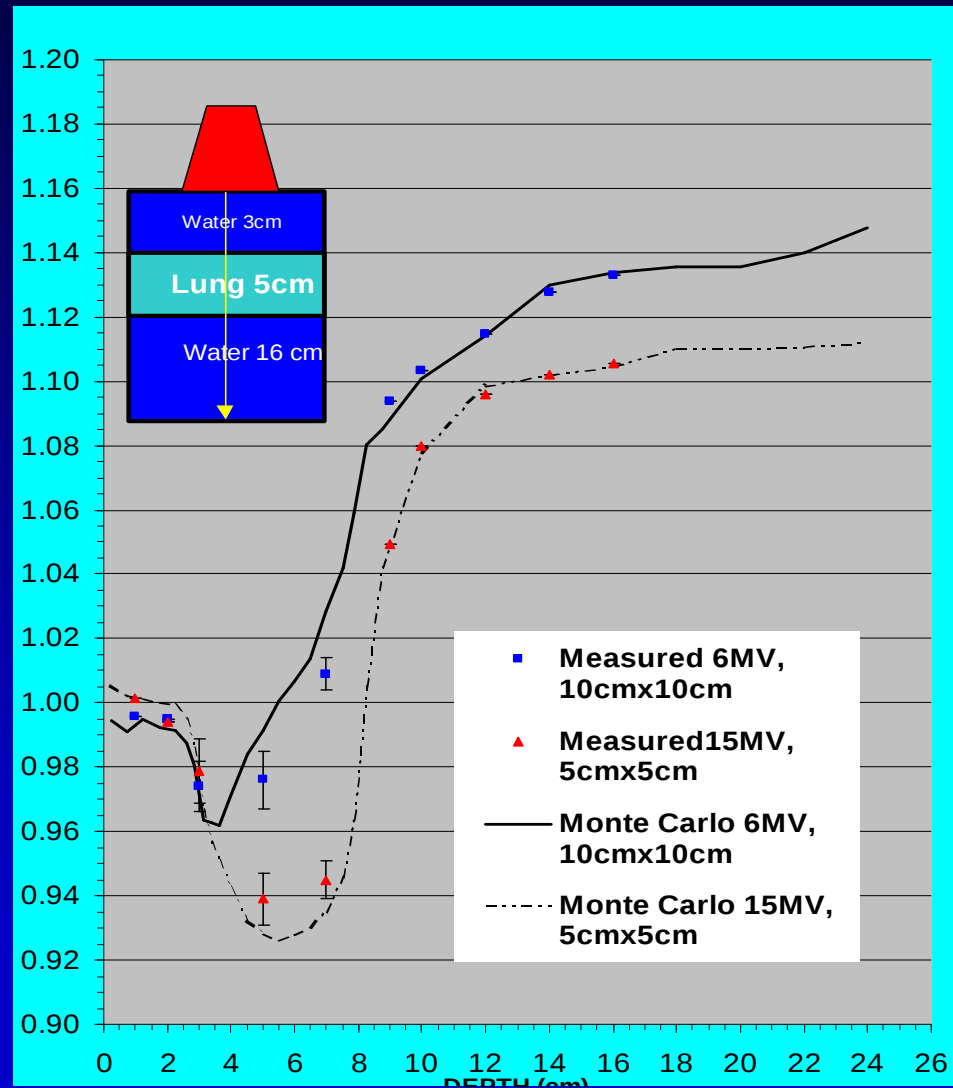


Correction factor for lung for 6 MV photons



Layered Lung Phantom

Heterogeneity Correction Factor



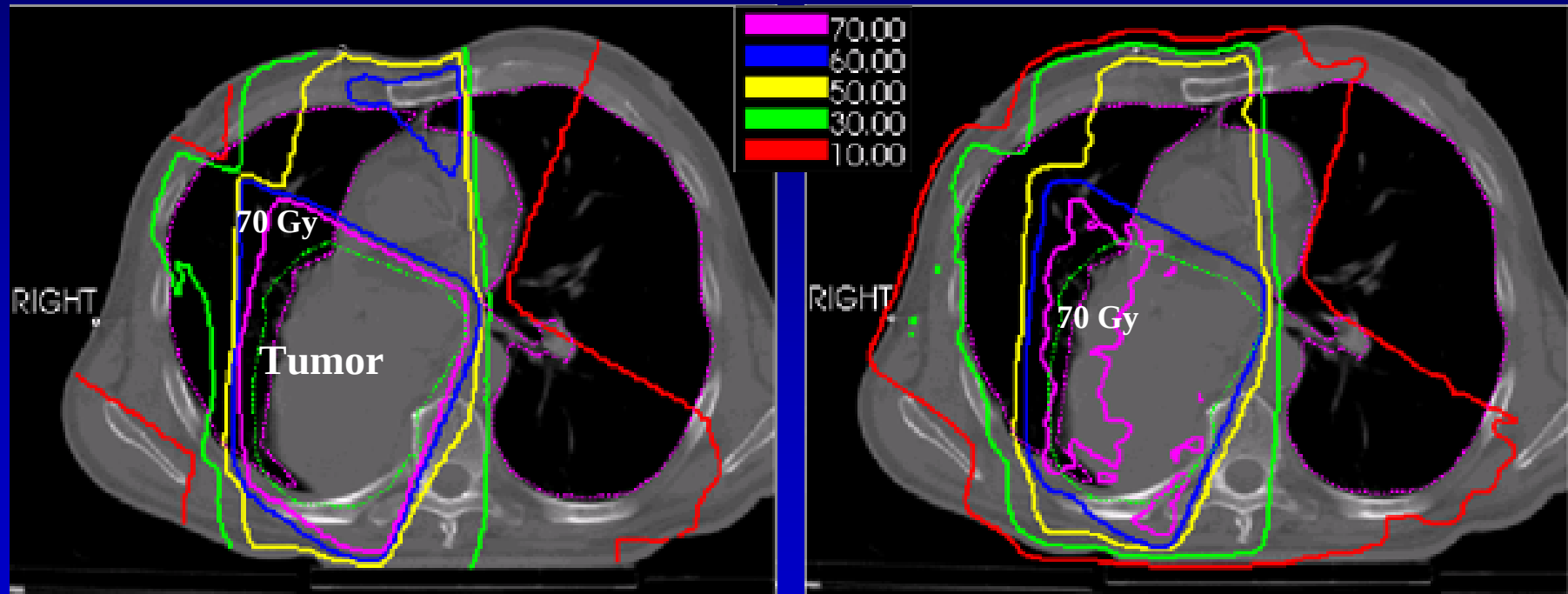
Depth (cm)

Comparisons of Pencil Beam and Monte Carlo

Mohan et al (1997)

Conventional Method (Pencil Beam)

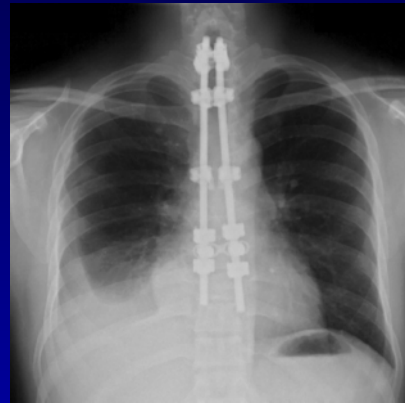
PEREGRINE



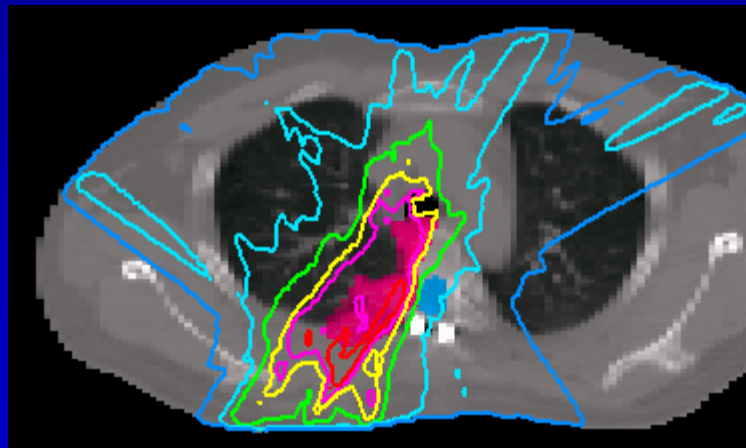
Dose Verification for IMRT

(Pawlicki et al 2000)

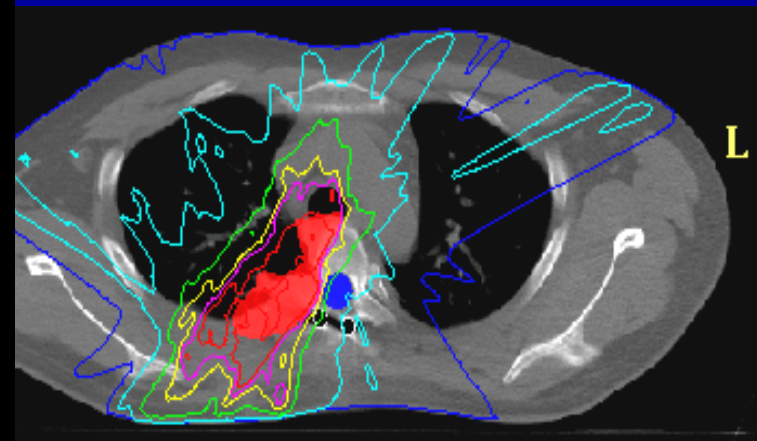
Monte Carlo



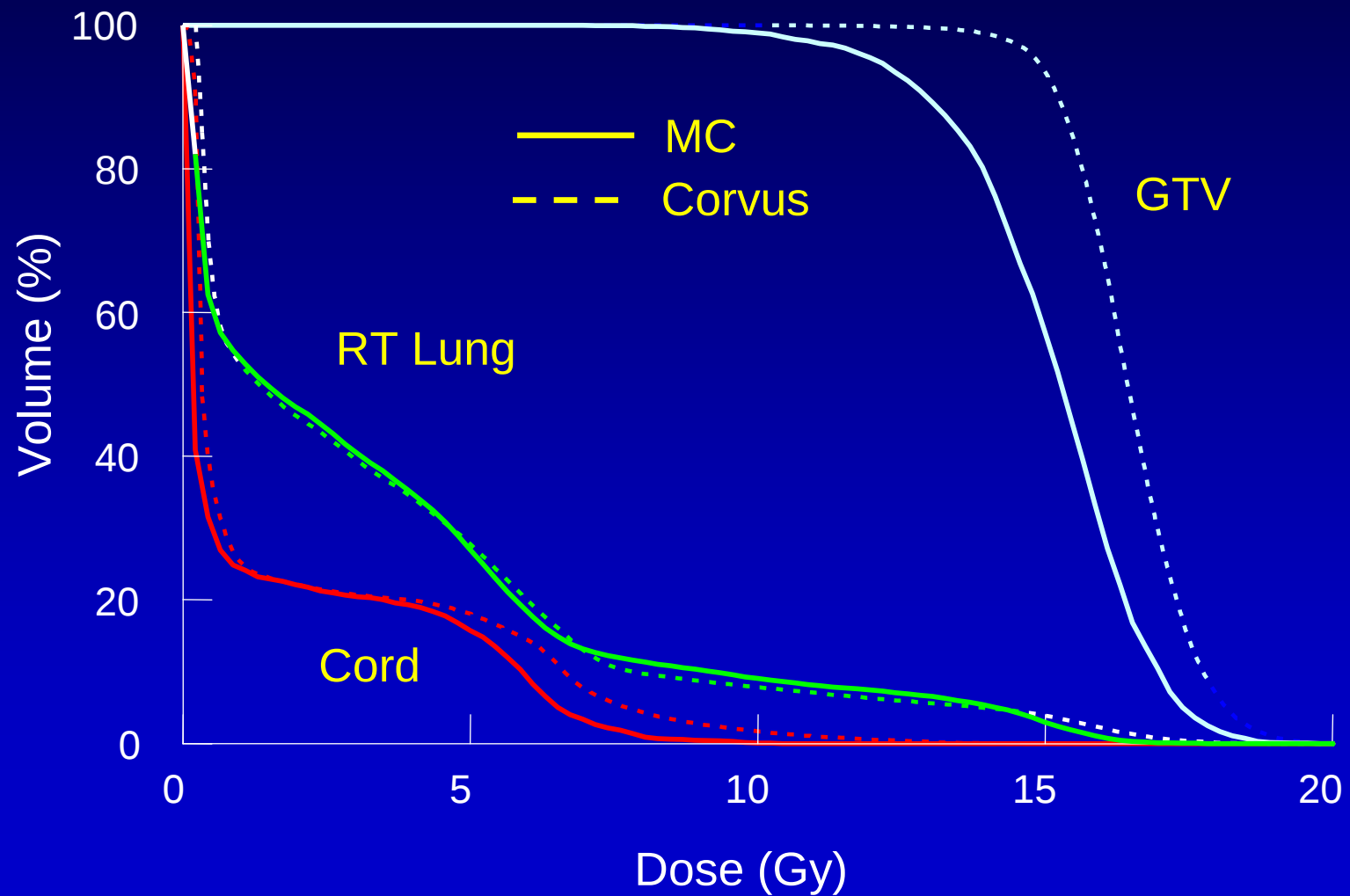
Corvus



Gy
16.2
14.4
12.6
9.0
5.4
1.8



DVH Comparison



Monte Carlo Algorithms

- Electron beams reported

VMC

DOSXYZ

MCDOSE/MCSIM

PENELOPE

MCRTTP

DPM

- Photon beams reported

XVMC

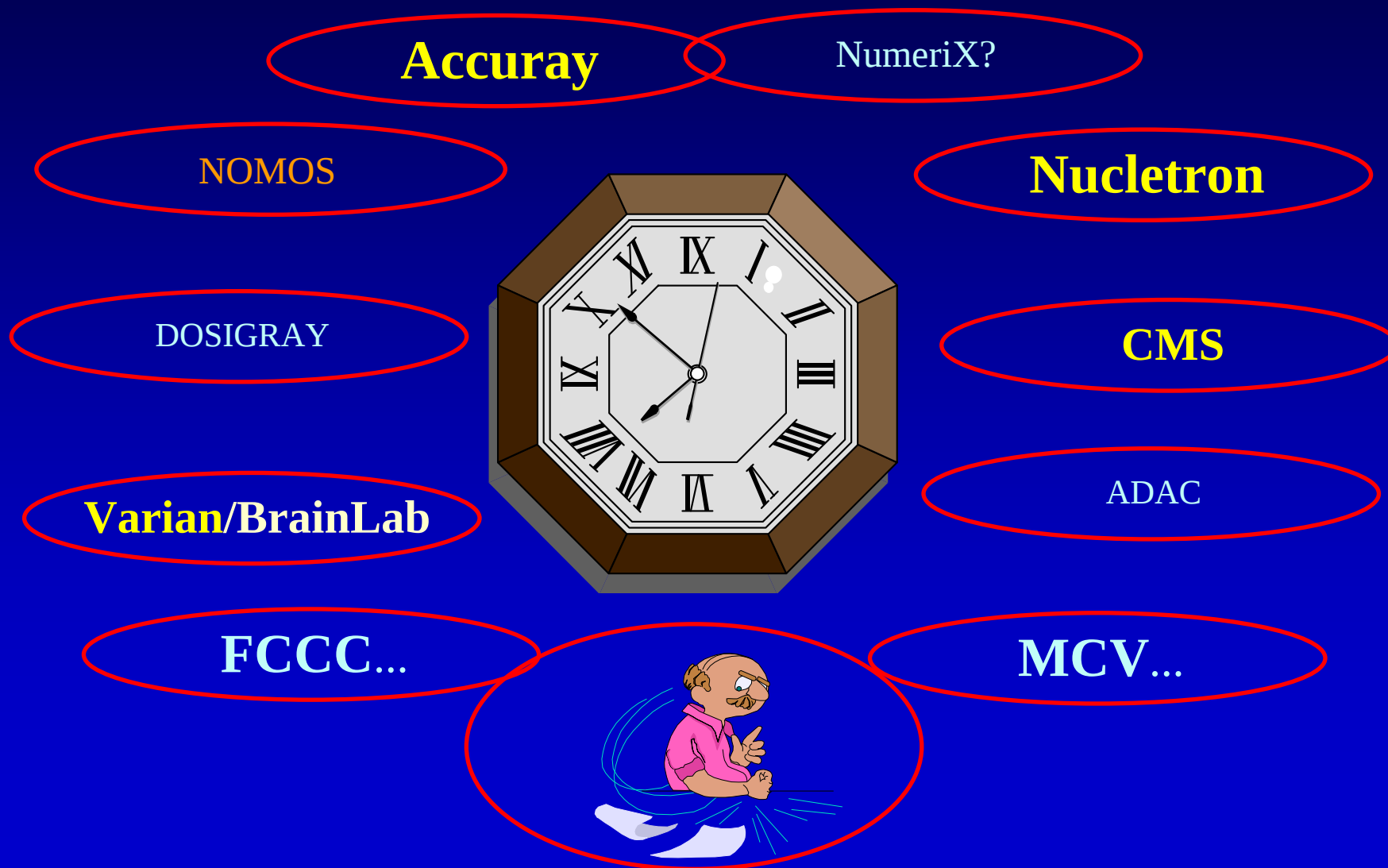
PEREGRINE

MCNP

DOSXYZ

MCDOSE/MCSIM/MCRS

Current Status of MCTP

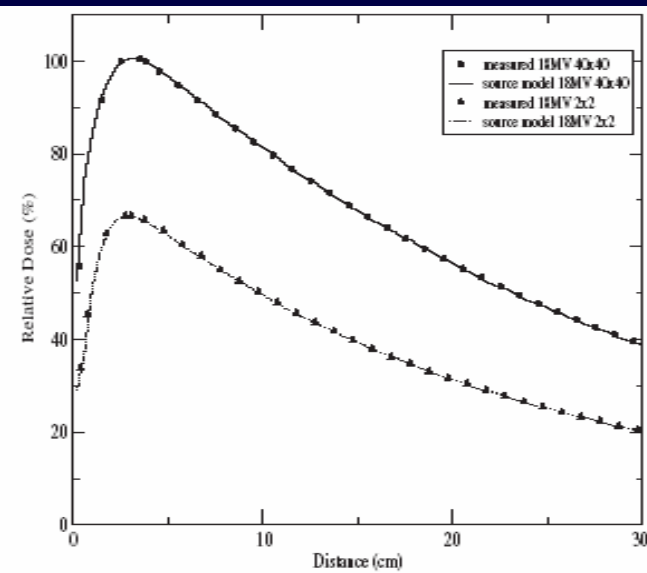
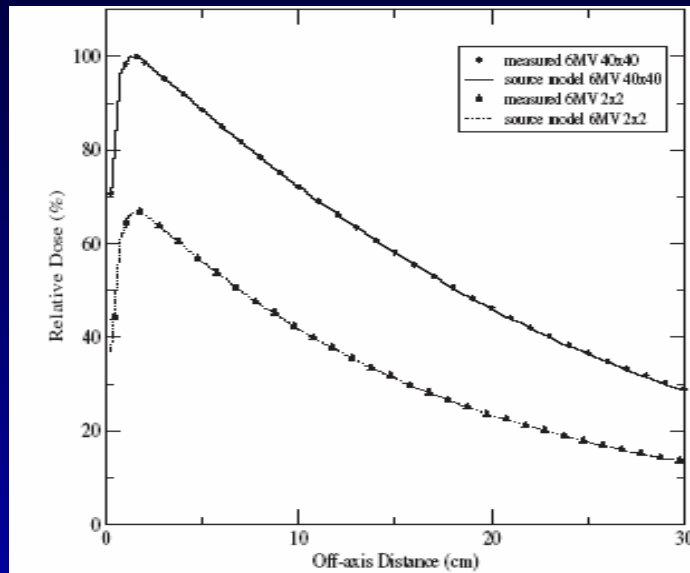


Implementation of MCTP

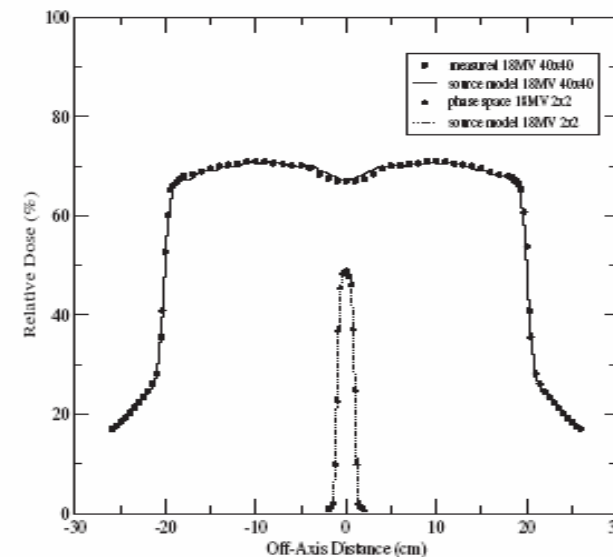
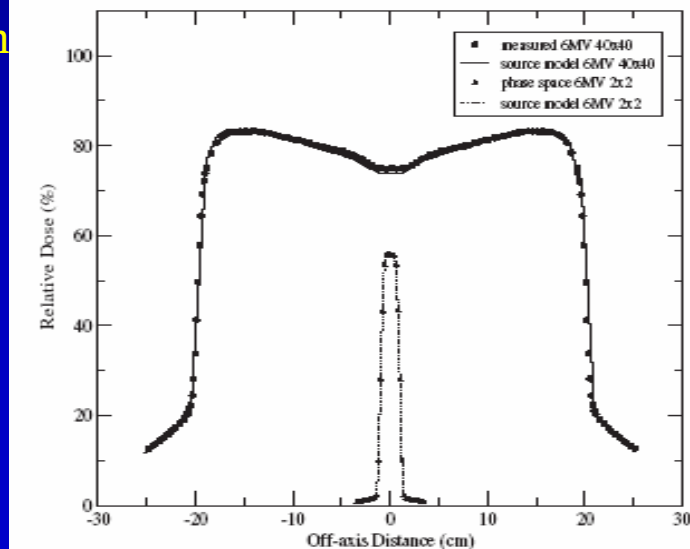
- Accelerator simulation
- Source modeling
- Beam commissioning
- CT data conversion and phantom setup
- Dose calculation algorithms
- Data processing and plan evaluation
- Plan optimization

Measured vs MC Reconstructed Dose Distributions

6 MV
40cmx40cm



18 MV
40cmx40cm



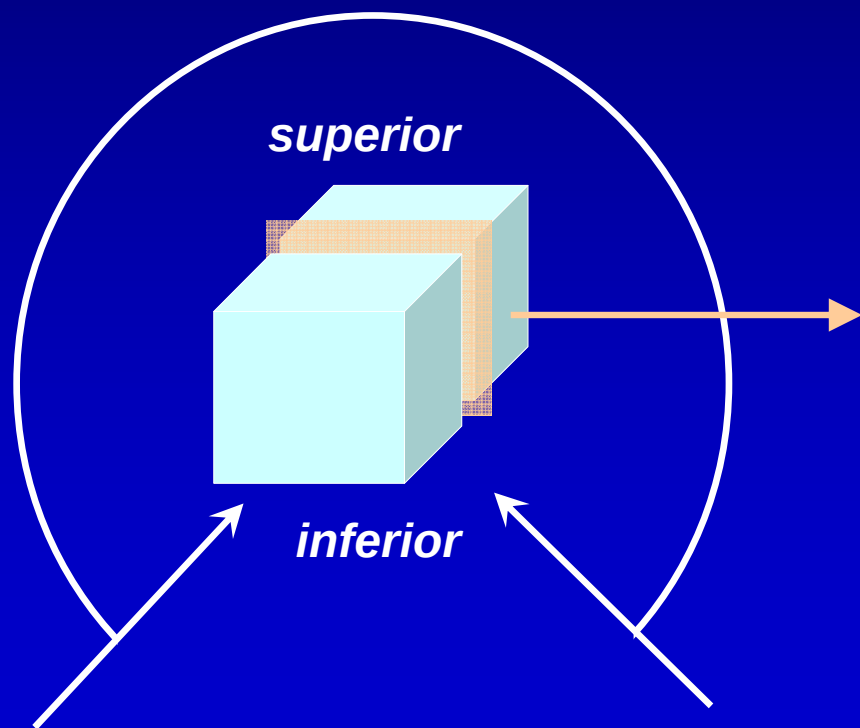
Yang et al, *Phys Med Biol* (2004) 49: 2657-73

Combined Dose Distribution: Film vs Monte Carlo

Patient plan (Corvus)

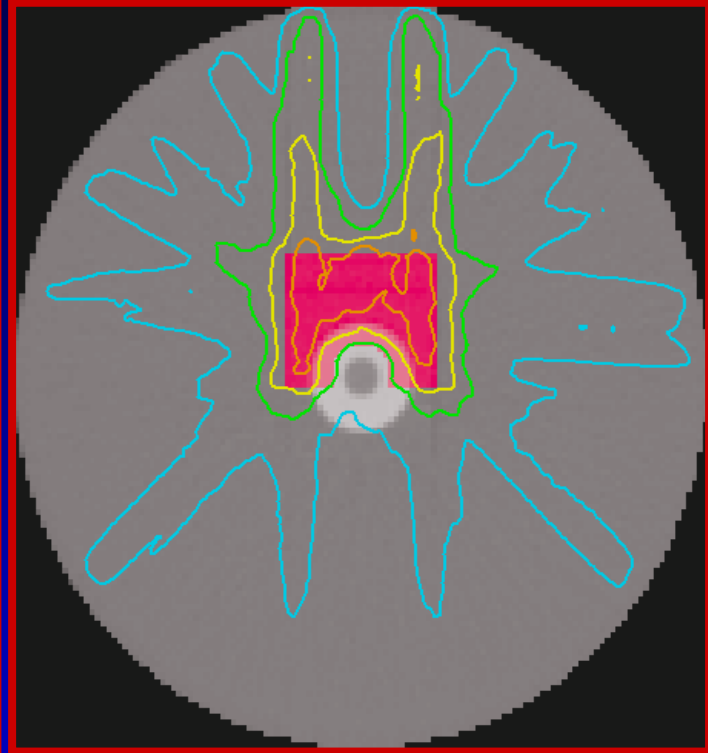
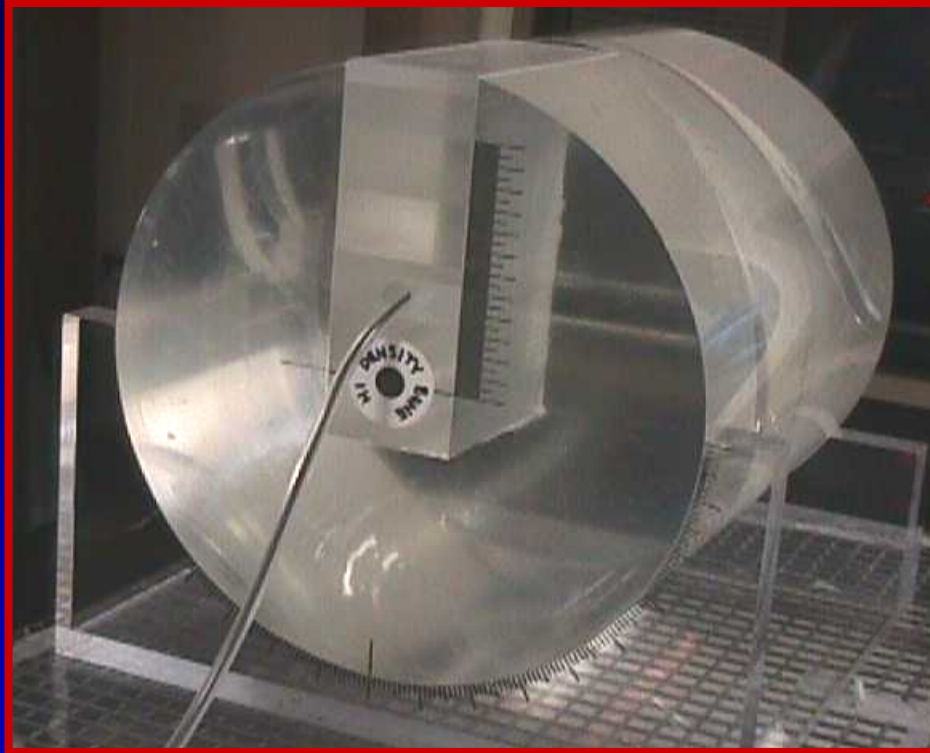
Delivery in film phantom

Monte Carlo dose calculation



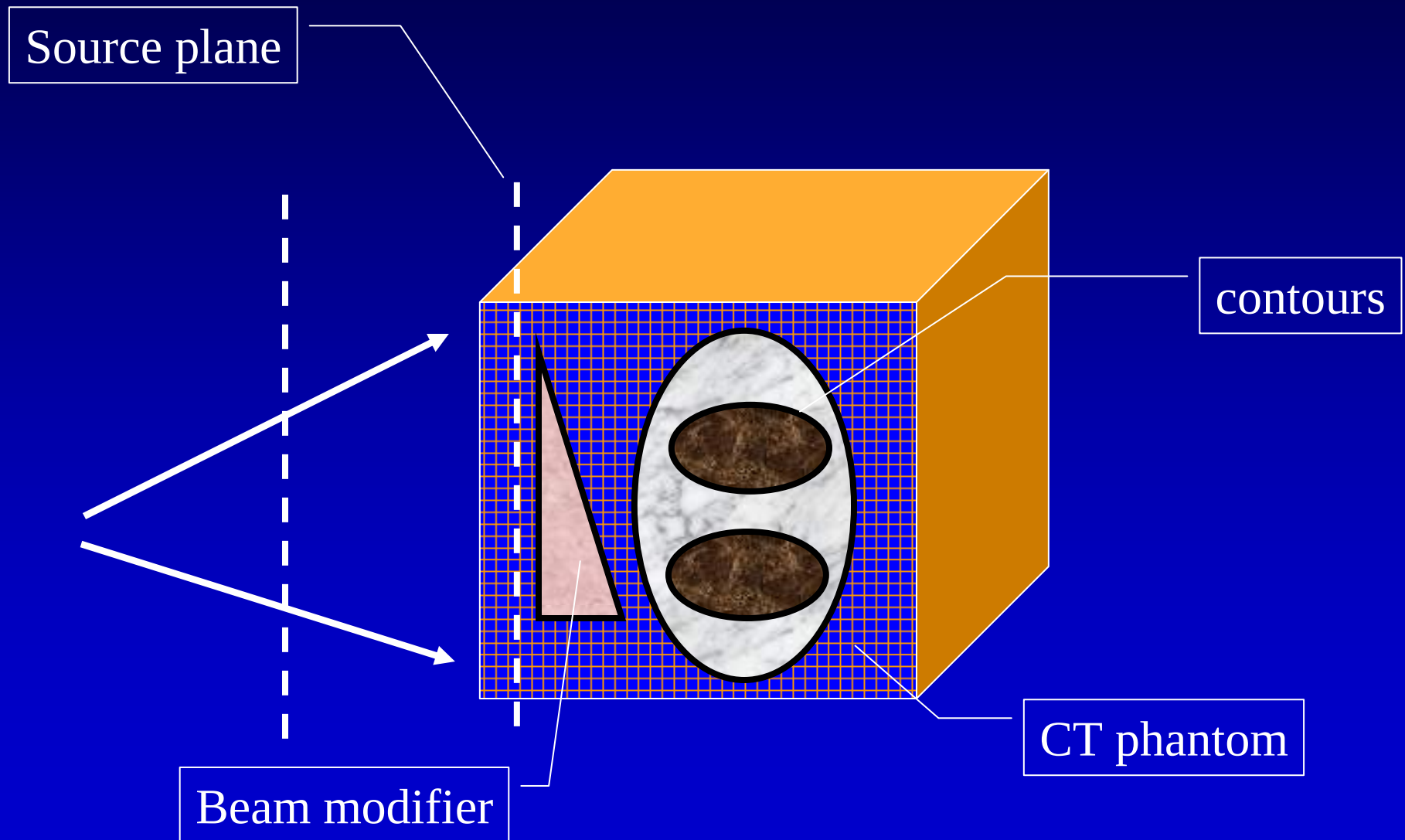
3 cm from isocenter

Calculations vs. Measurements



Energy	M-C	Meas	CORVUS
4 MV	2.177 Gy	2.177 Gy	2.201 Gy
15 MV	2.146 Gy	2.161 Gy	2.276 Gy

M-C Simulation Geometry



CT Number to Medium Conversion

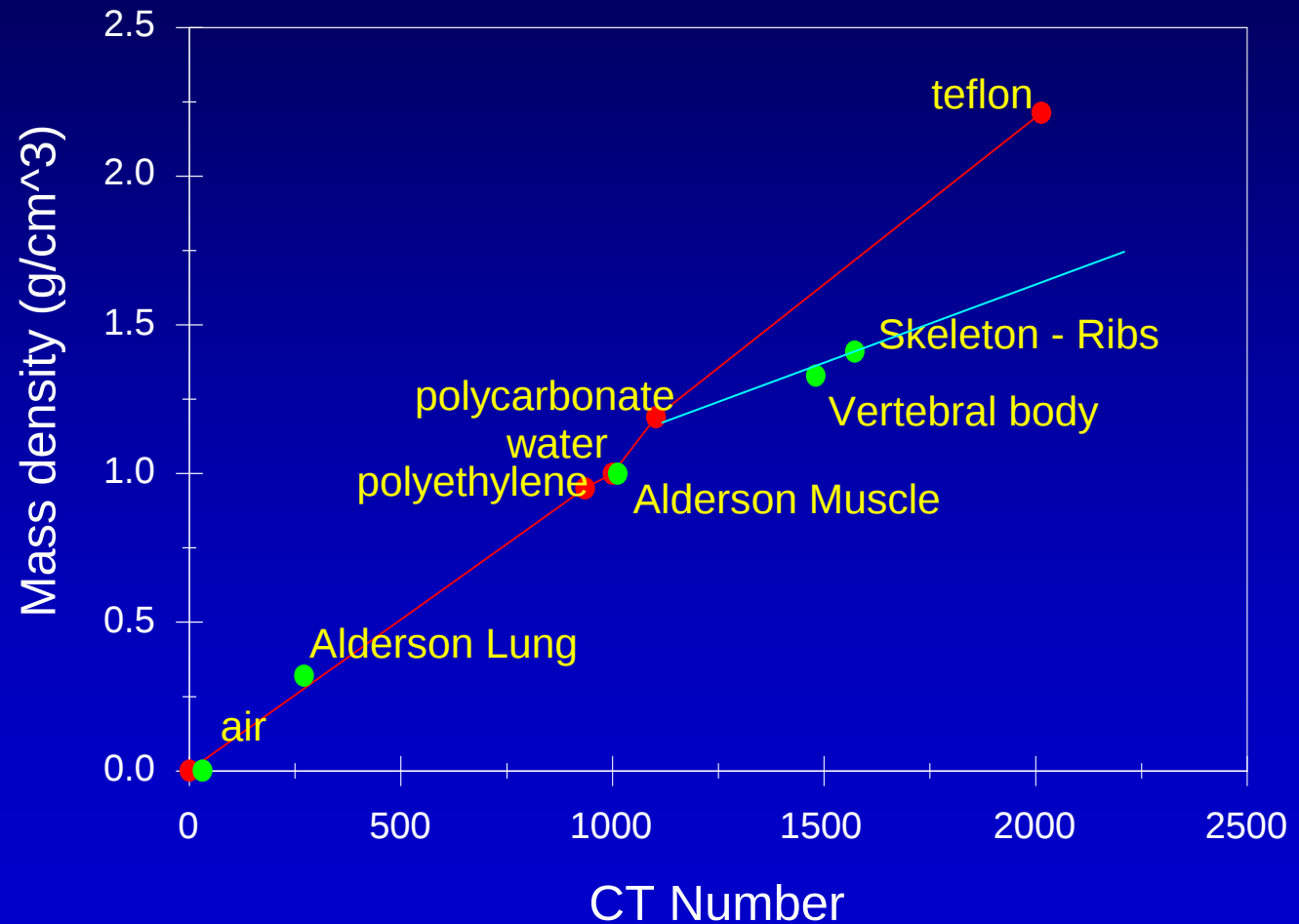
2000~2.088g/cm³

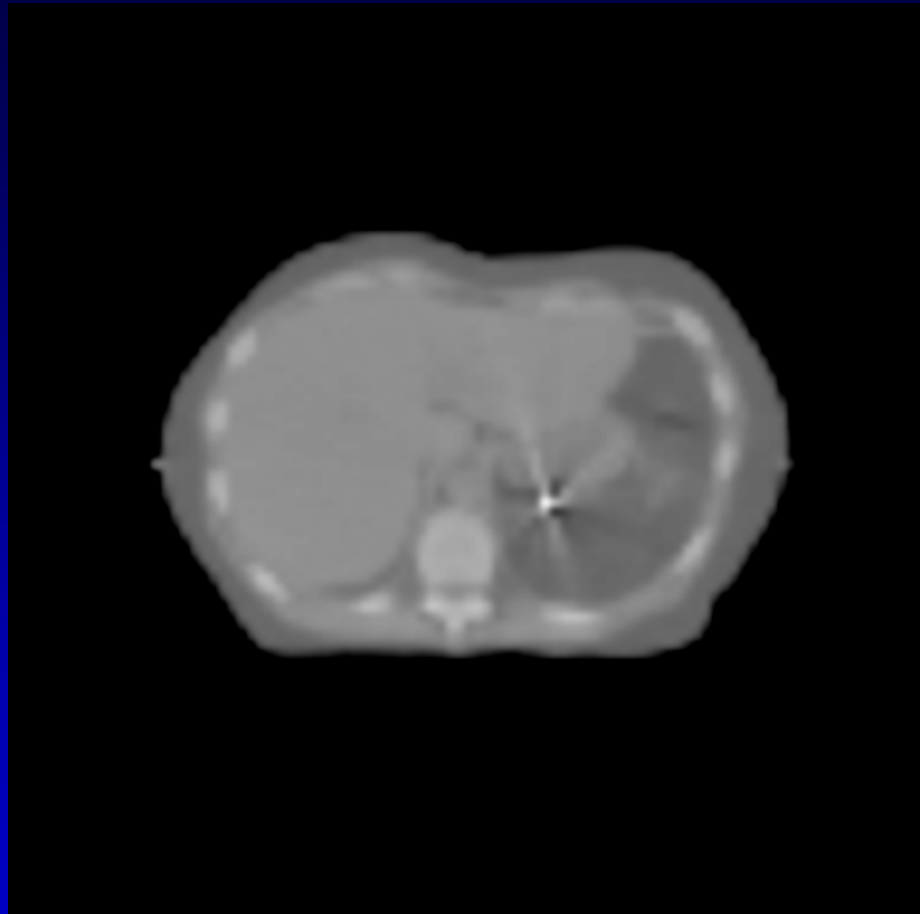
125~1.101g/cm³

-700~0.302g/cm³

-950~0.044g/cm³

-1000~0.001g/cm³





Density map

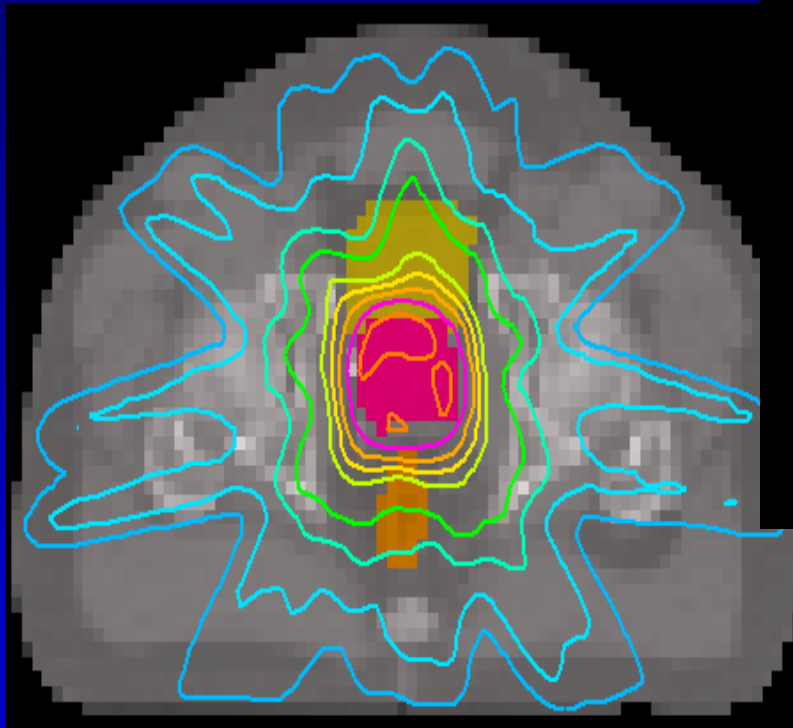


Medium map

Treatment Plan Comparison

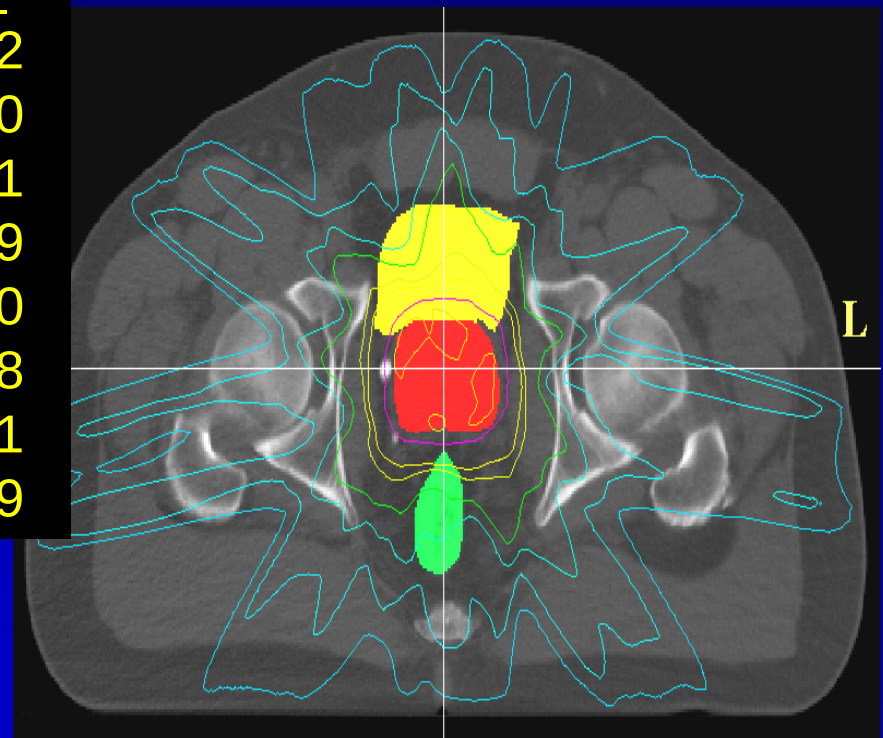
Prostate

Monte Carlo

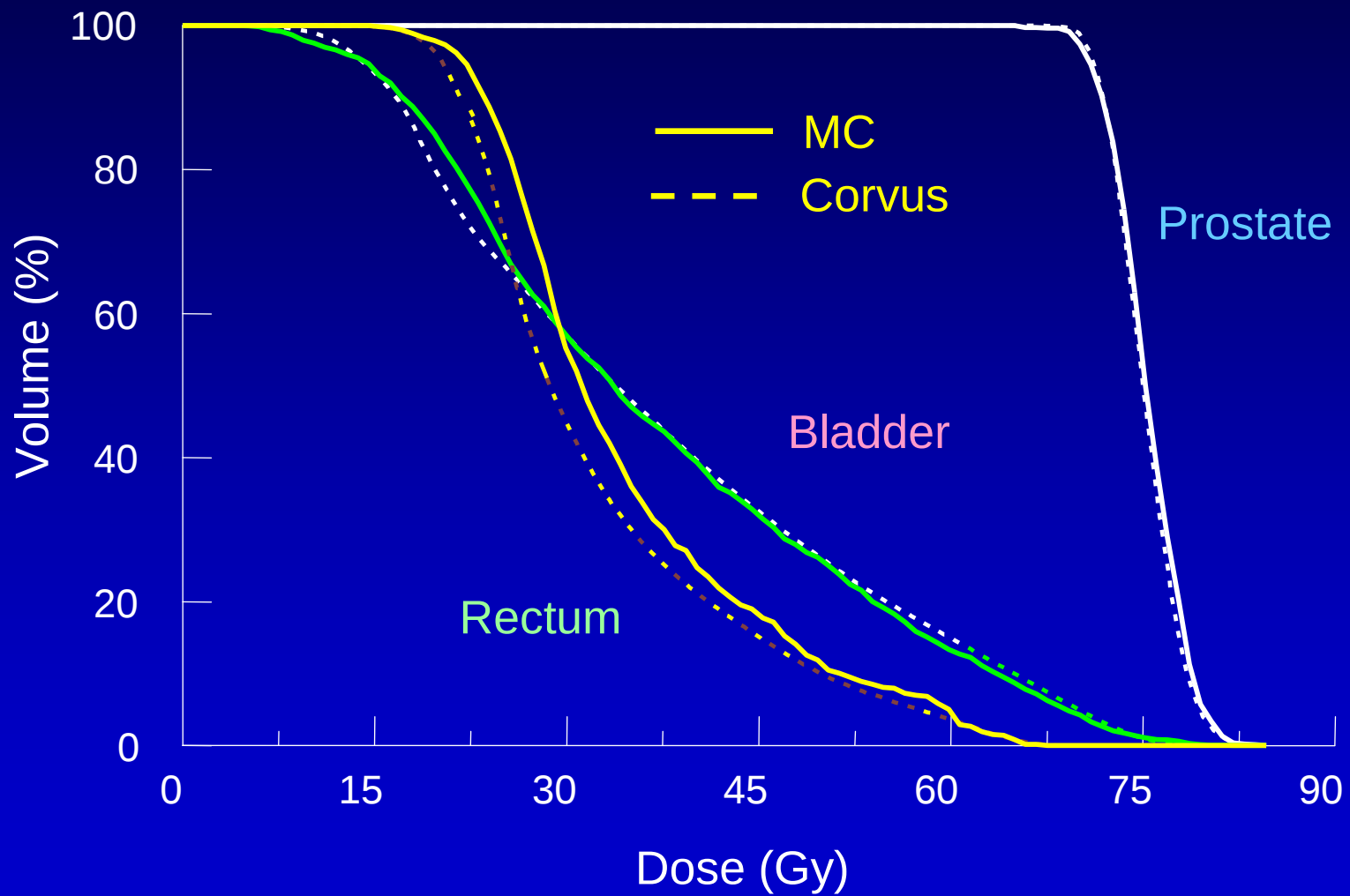


Gy
77.2
70.0
56.1
48.9
35.0
27.8
21.1
13.9

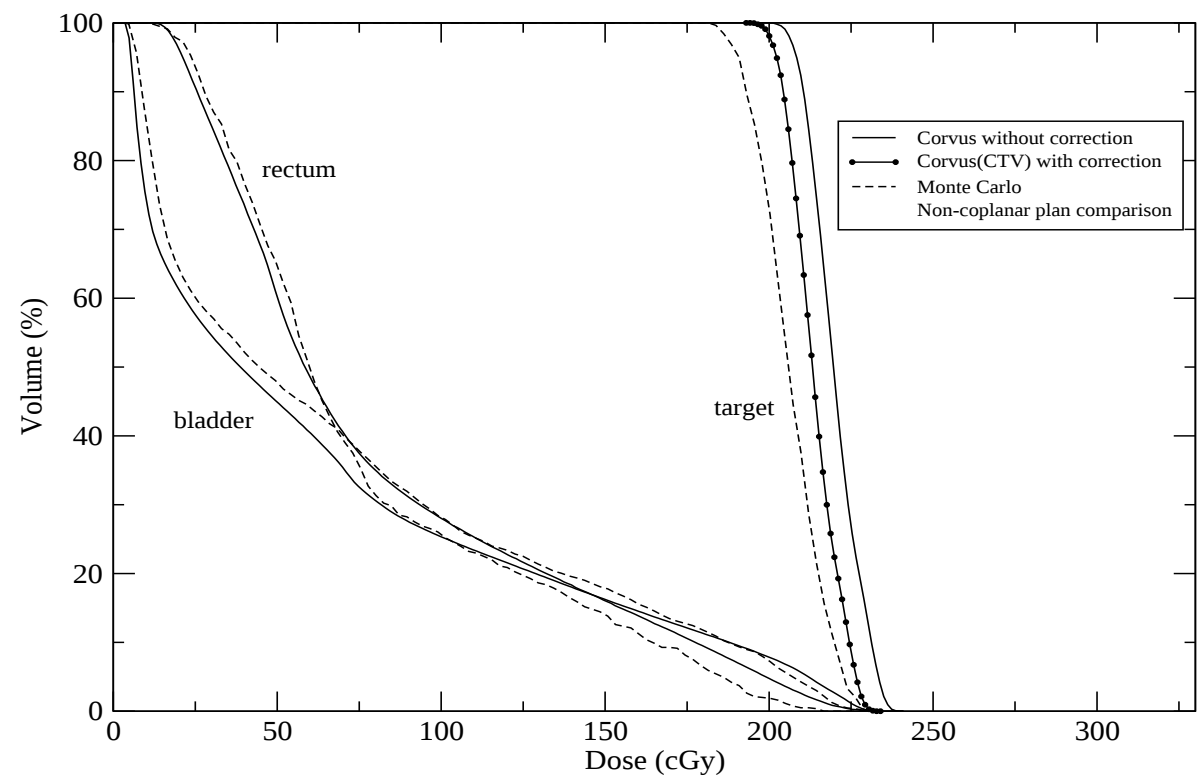
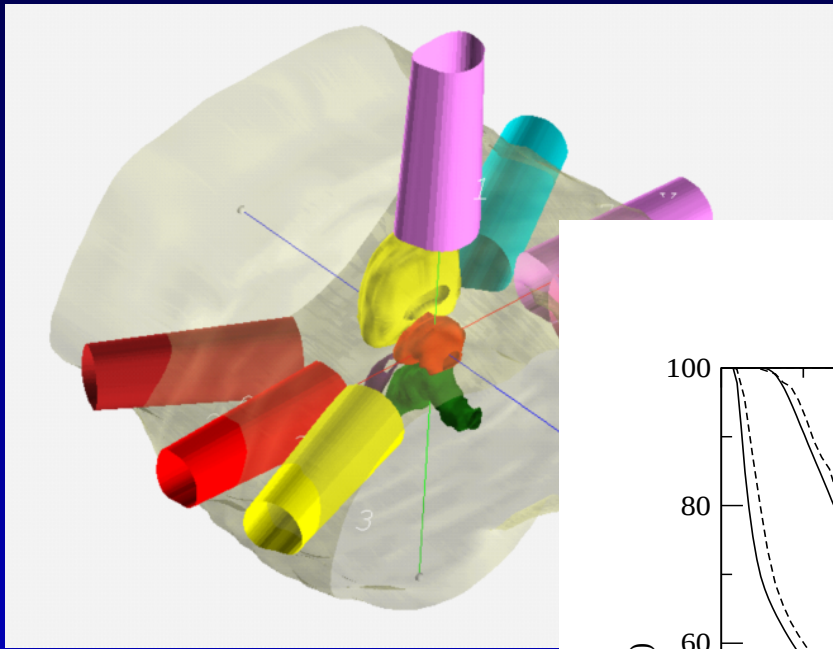
Corvus



Prostate

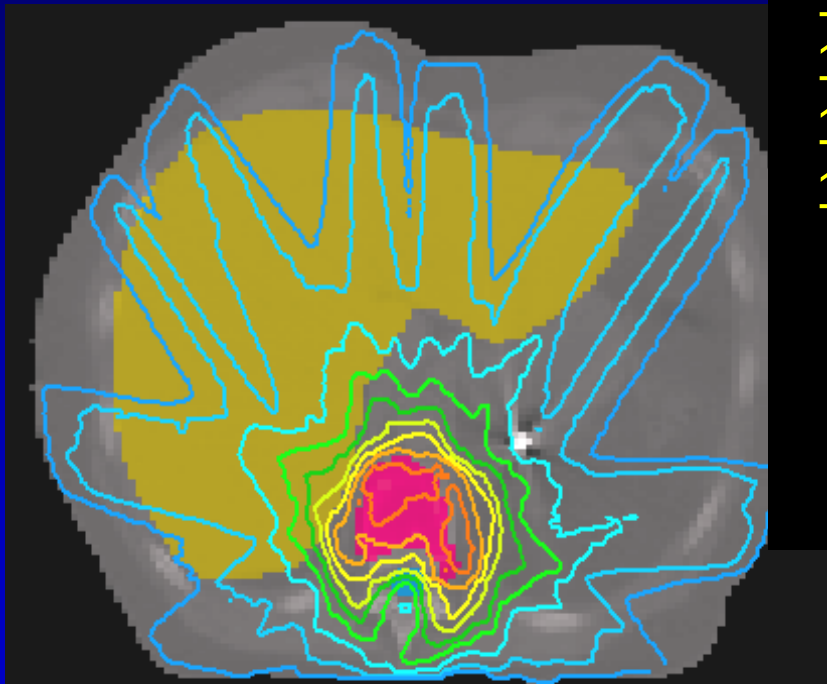


Dose Verification for Non-coplanar Prostate IMRT



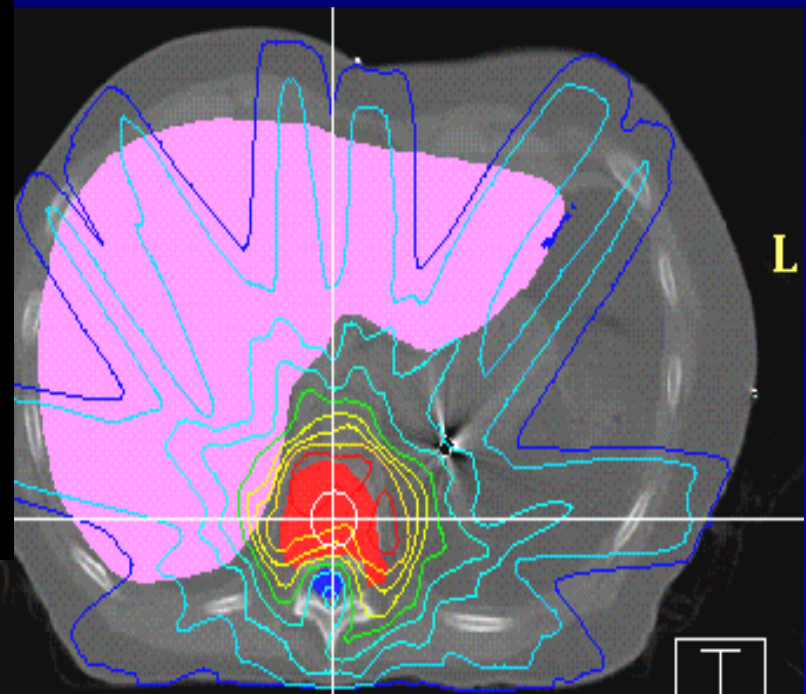
T11-L1 Vertebra

Monte Carlo

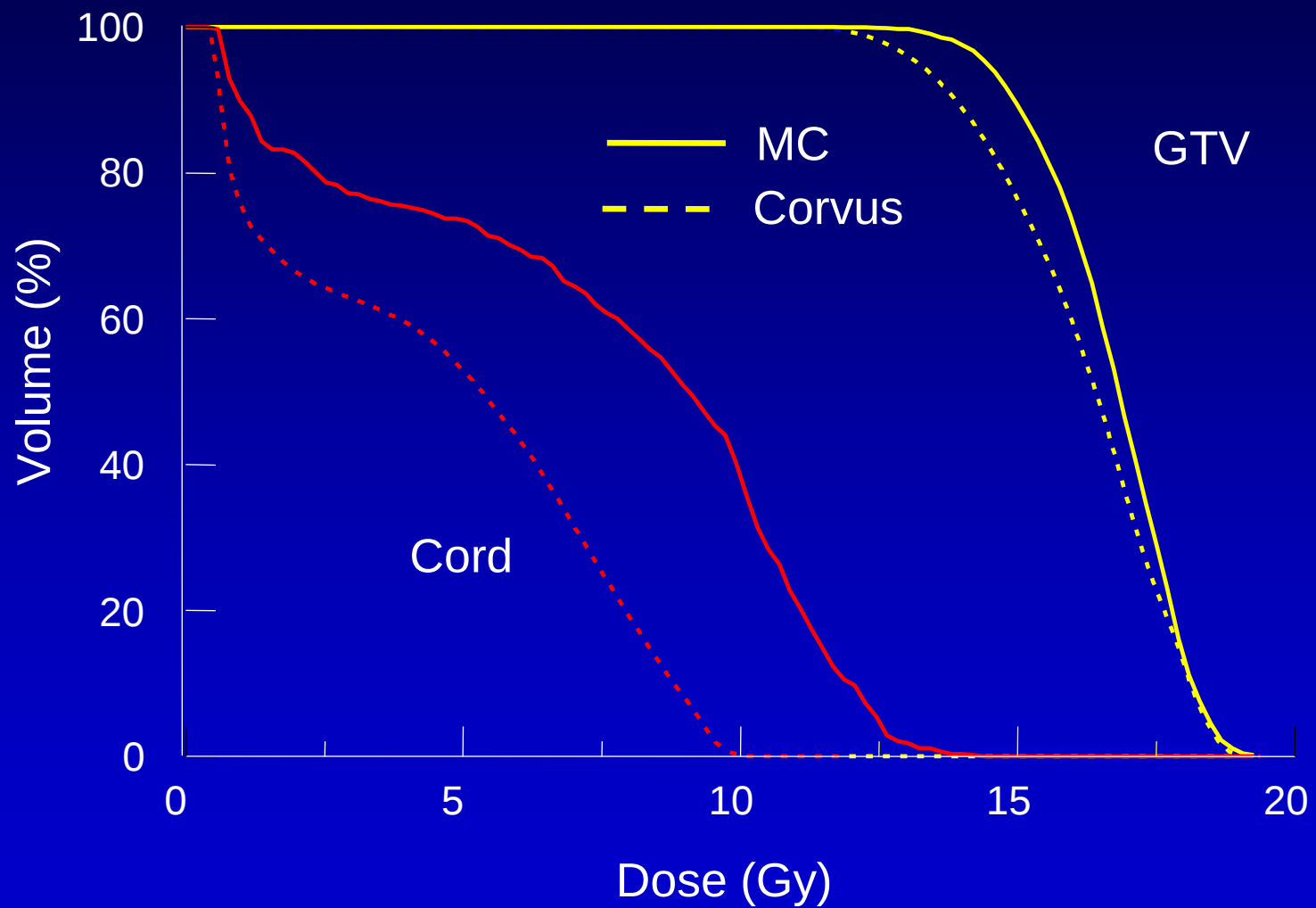


Gy
17.6
15.6
13.7
11.7
9.8
7.8
5.9
3.9
2.0

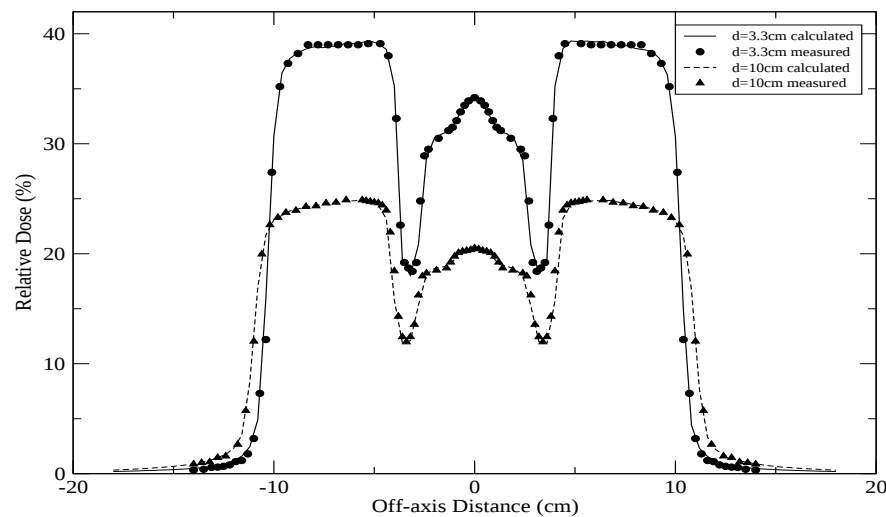
Corvus



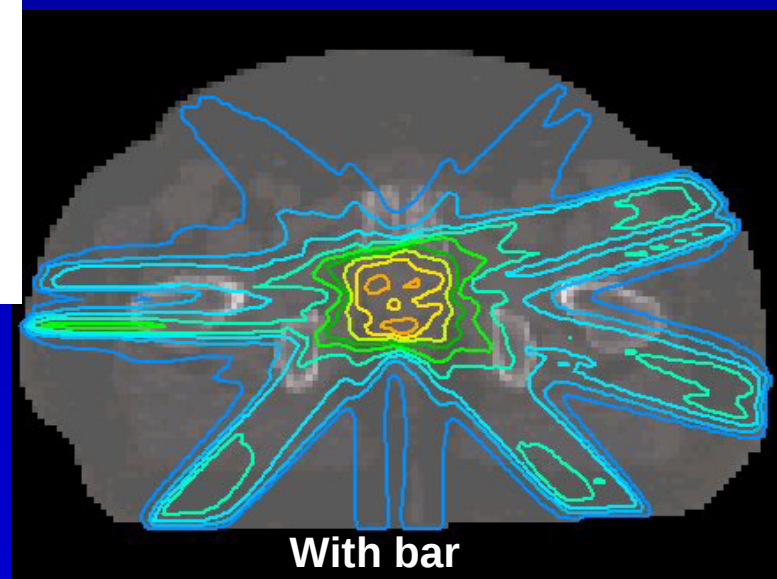
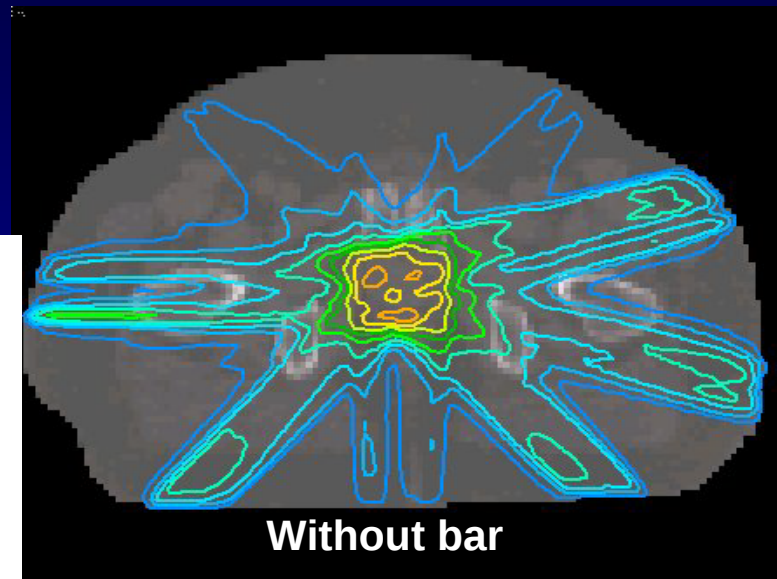
T11-L1 Vertebra



Effect of Couch Bar on IMRT Dose Distribution



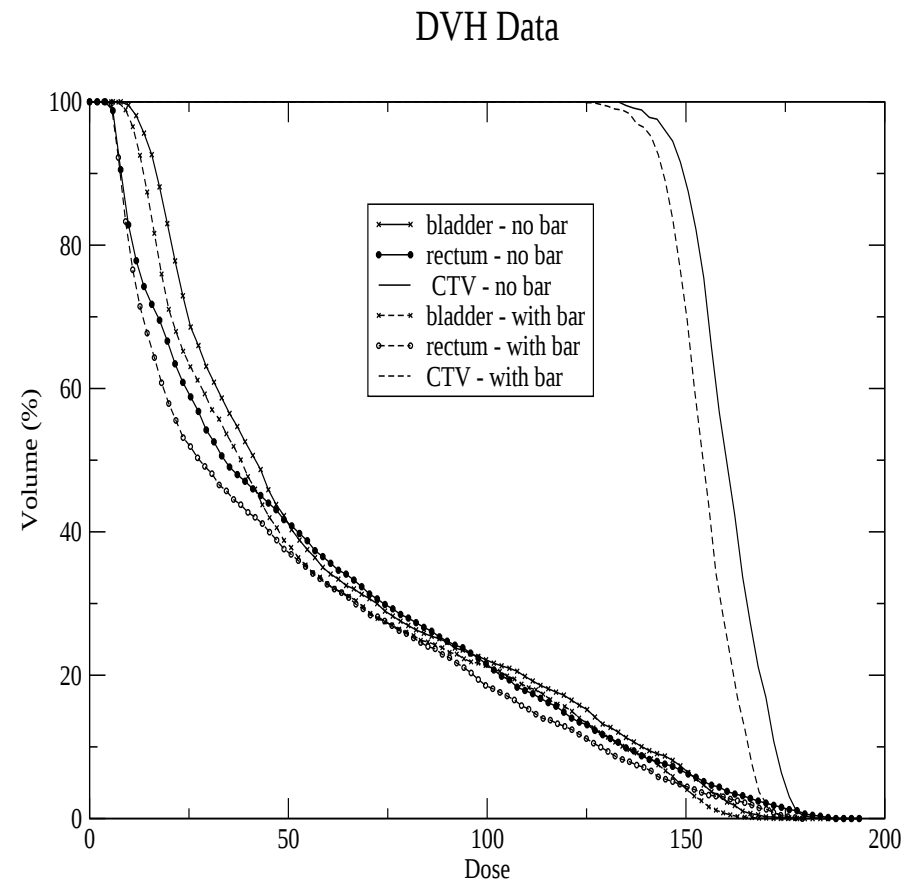
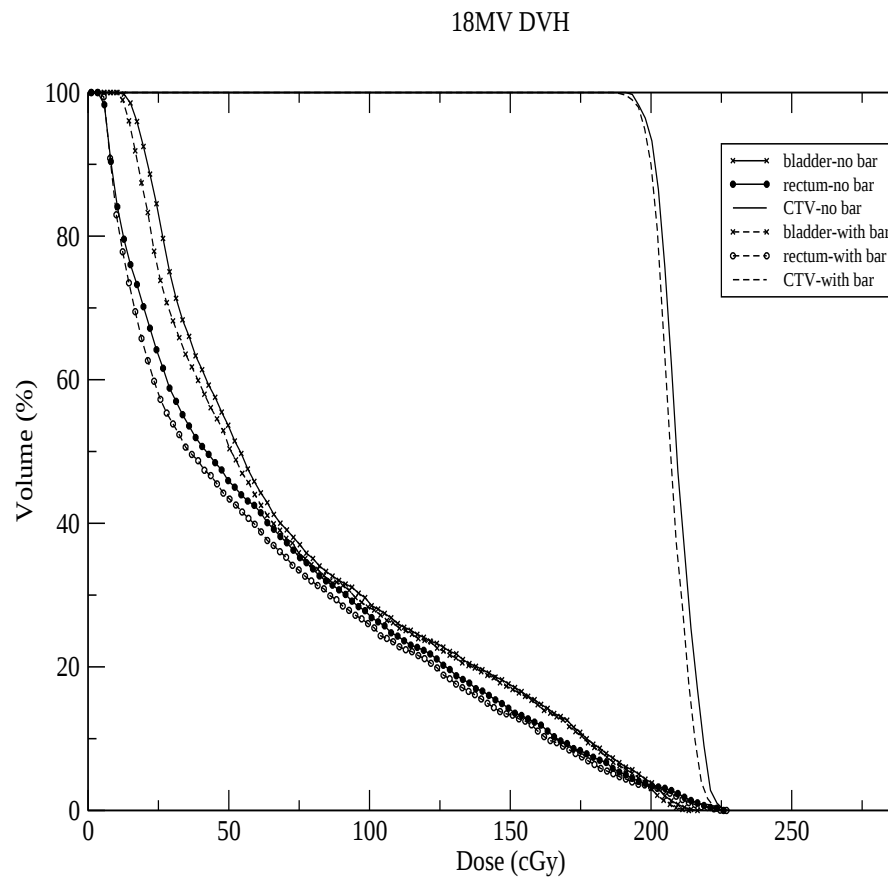
MC vs film measurement



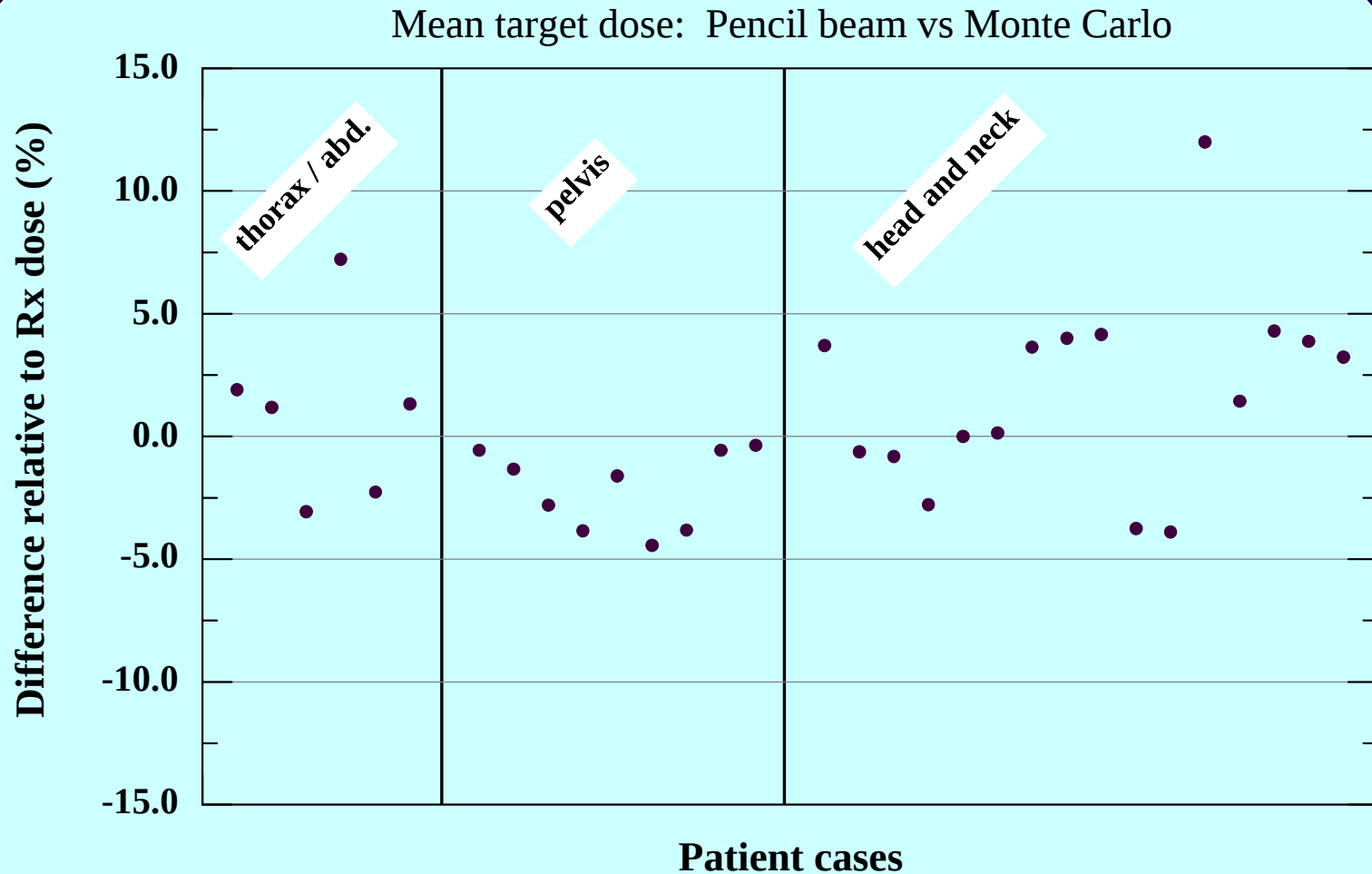
Effect of Couch Bar on IMRT Dose Distribution

IMRT using 18 MV photons

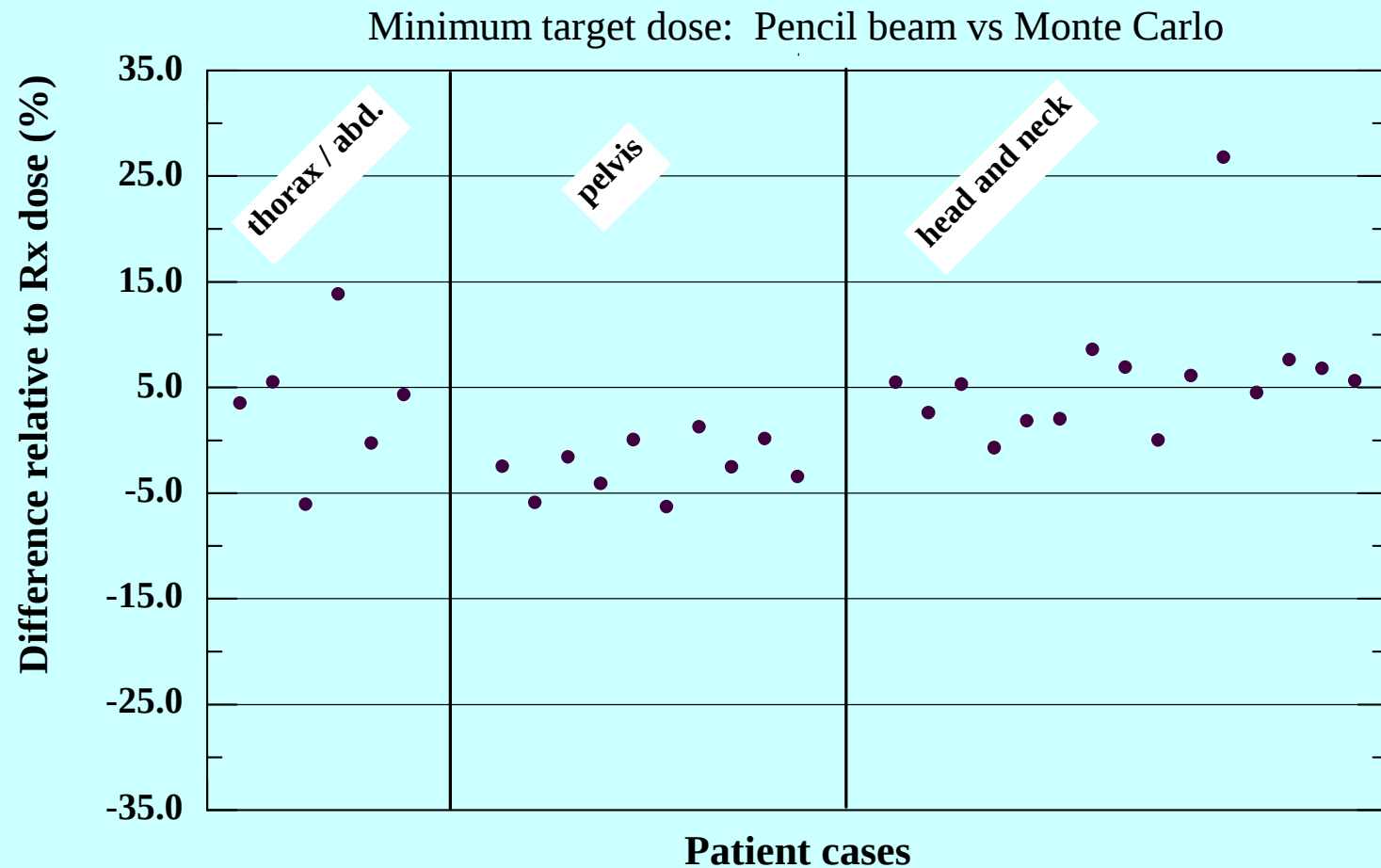
IMRT using 6 MV photons



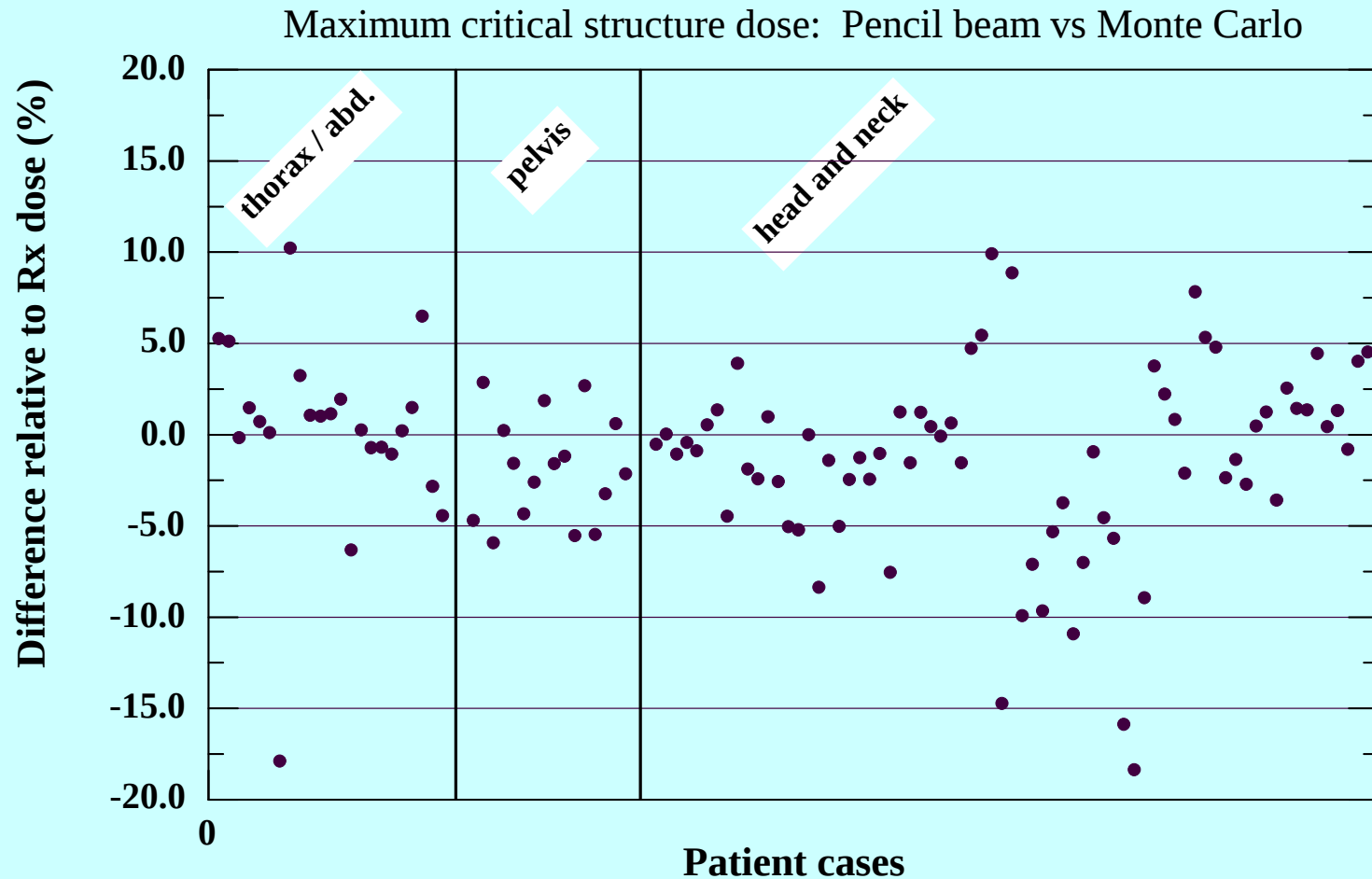
Mean Target Dose (BP vs MC)



Minimum Target Dose (BP vs MC)

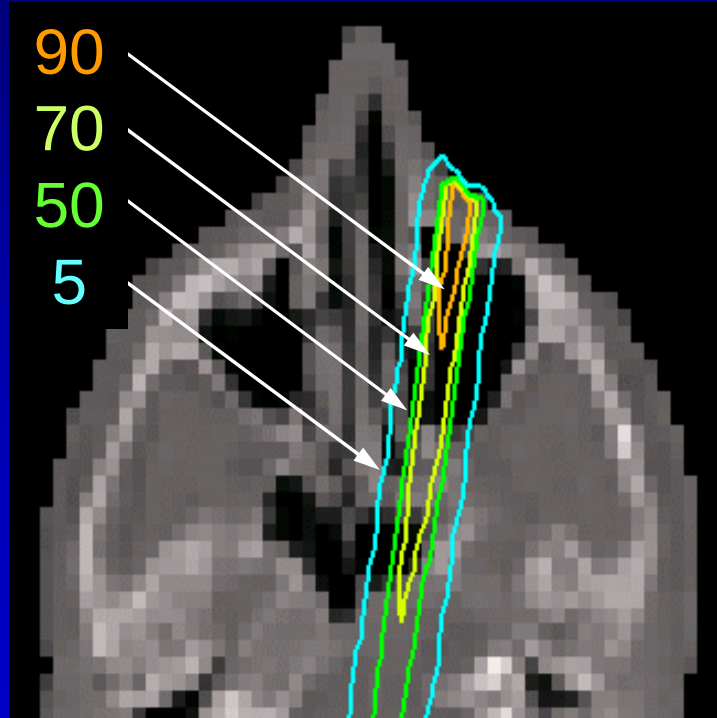


Max. Critical Structure Dose (BP vs MC)

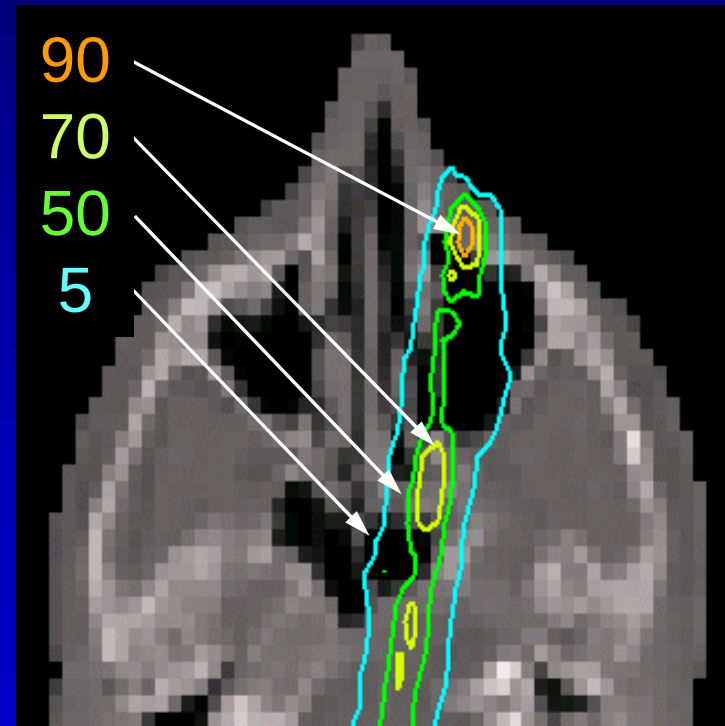


Beamlet Dose Distributions

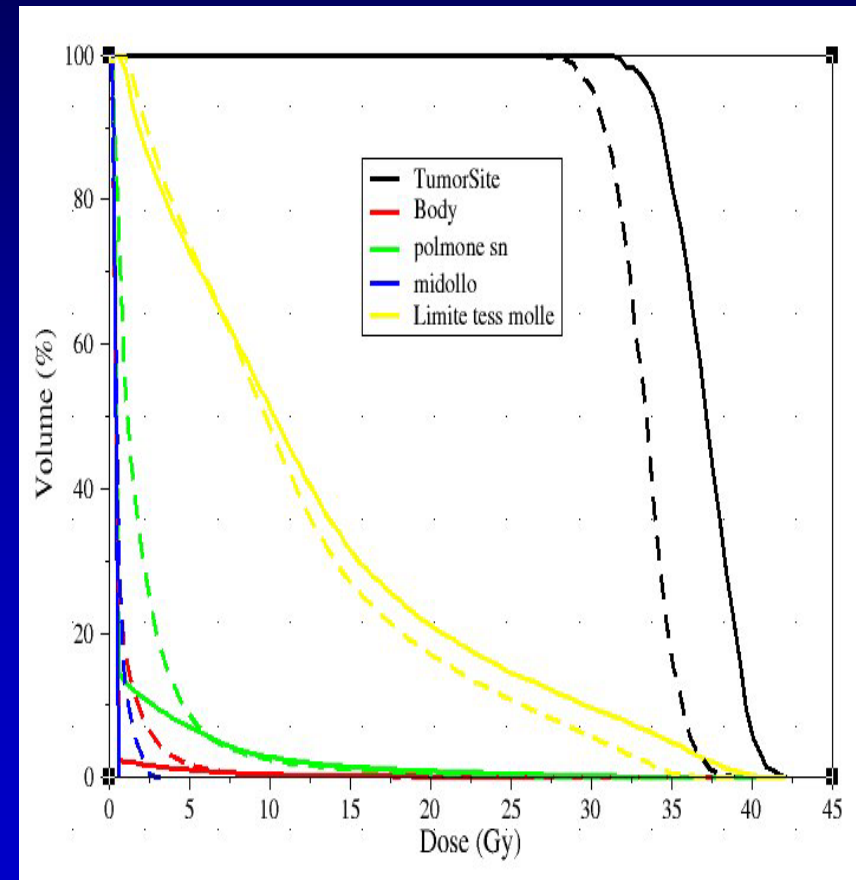
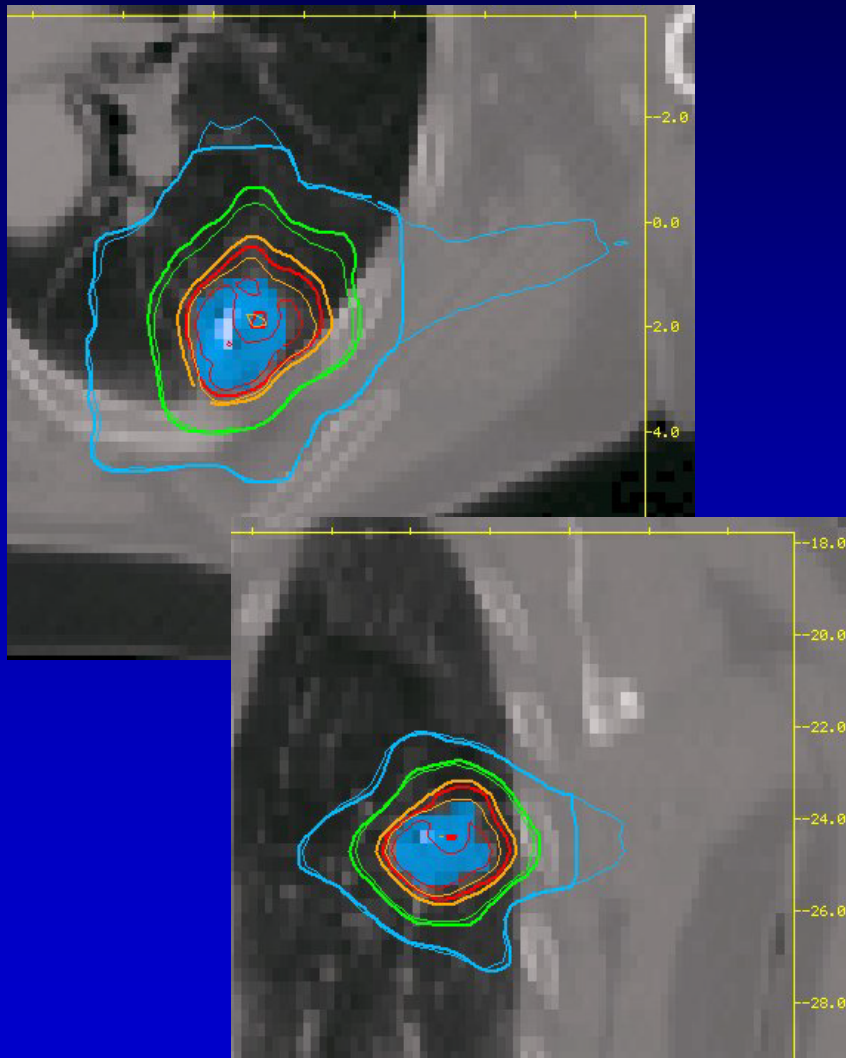
FSPB



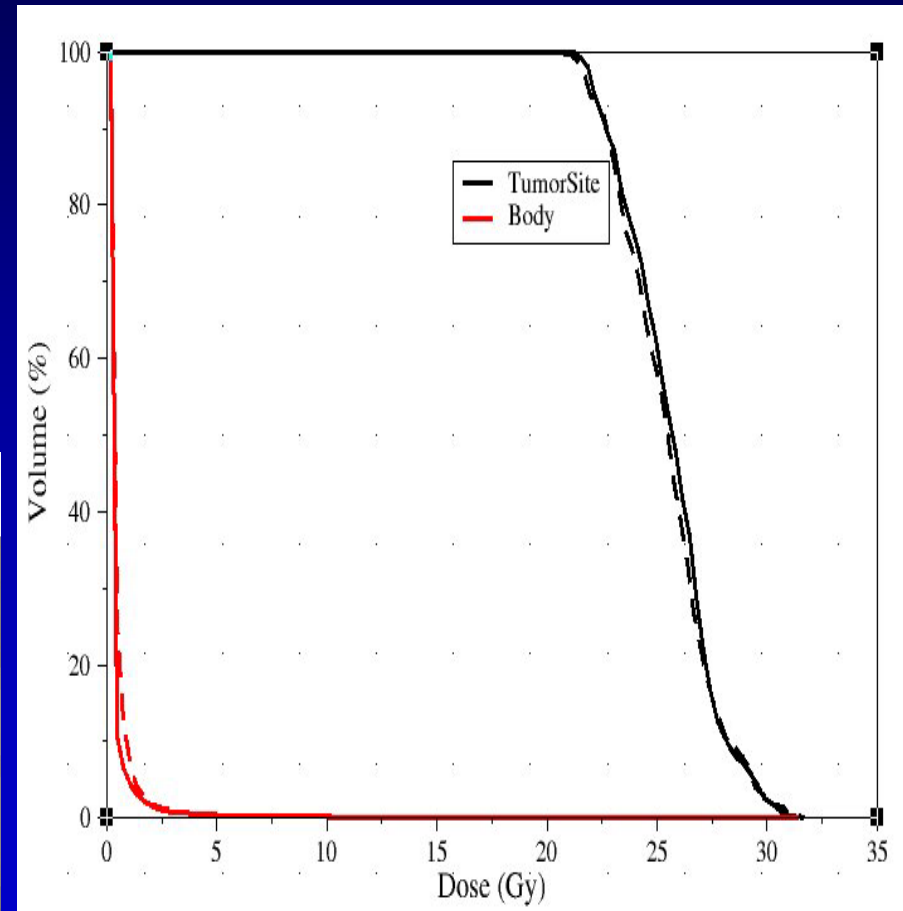
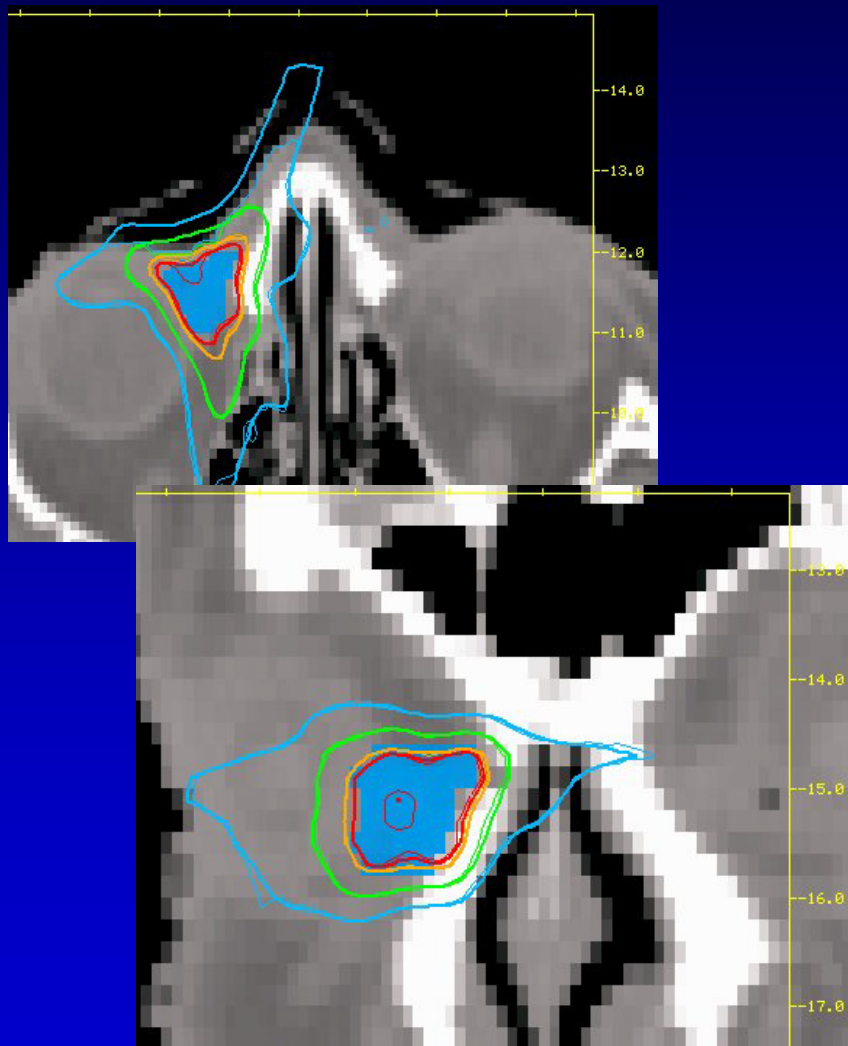
Monte Carlo



CyberKnife Monte Carlo



CyberKnife Monte Carlo



Summary

- MC dose calculation is becoming a practical tool for advanced radiotherapy treatments
- The accuracy of MC dose calculation depends on the implementation
- The potential of MC dose calculation remains to be explored

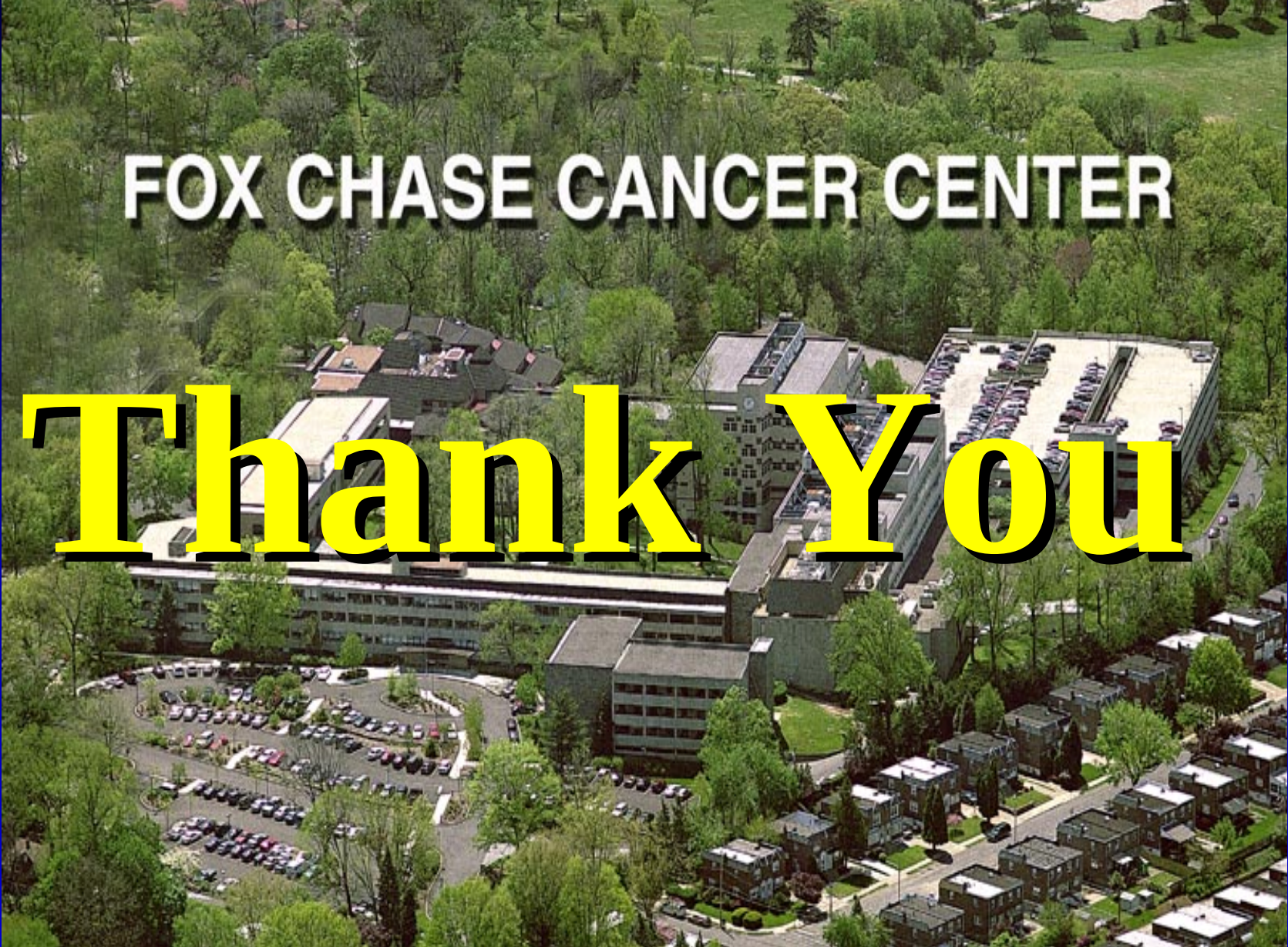
Acknowledgments

The FCCC/Stanford Monte Carlo Team



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Jay Chen
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Lihong Qin
Meisong Ding
Omar Chibani
Grisel Mora
Thai Bing Nguyen
William Xiong
Antonio Leal
Freek Du Plessis

An aerial photograph of the Fox Chase Cancer Center, showing several large, modern buildings with flat roofs and extensive parking lots filled with cars. The center is surrounded by lush green trees and a residential neighborhood with smaller houses is visible in the lower right corner.

FOX CHASE CANCER CENTER

Thank You

FCCC Monte Carlo courses, April 2010