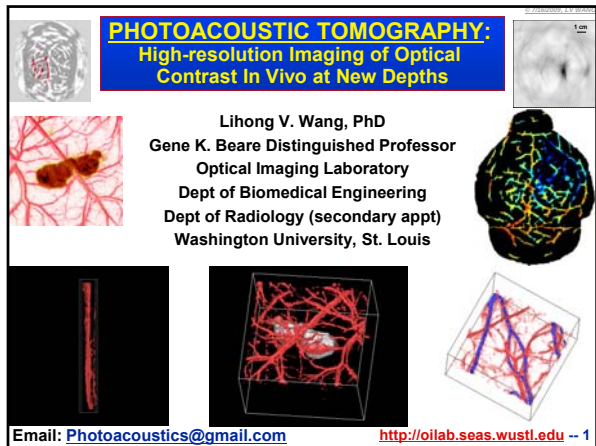


PHOTOACOUSTIC TOMOGRAPHY:
High-resolution Imaging of Optical Contrast In Vivo at New Depths

Lihong V. Wang, PhD
Gene K. Beare Distinguished Professor
Optical Imaging Laboratory
Dept of Biomedical Engineering
Dept of Radiology (secondary appt)
Washington University, St. Louis

Email: Photoacoustics@gmail.com <http://oilab.seas.wustl.edu> -- 1



Credits to Lab Members

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• X. Cai	• J. Ai, PhD	• X. Xie, MS
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• C. Favazza	• D. Feng, MS	• Y. Xu, PhD
• A. Garcia-Urbe	• J. Hollmann	• X. Yang, PhD
• Z. Guo	• S. Jiao, PhD	• G. Yao, PhD
• S. Hu	• X. Jin, PhD	• W. Yu, MS
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• B. Rao	• M. Sivaramakrishnan, MS	
• L. Song	• E. Smith, MS	
• V. Tsytarev	• K. Song, PhD	
• Y. Wang	• E. Stein, PhD	
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• J. M. Yang	• M. Todorovic, PhD	
• J. J. Yao	• X. Wang, PhD	
	• Y. Wang, MS	

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Motivation for Optical Imaging

- Safety — Non-ionizing radiation: photon energy is ~2 eV
- Physics — Related to molecular conformation of tissue
- Optics — High intrinsic contrast:
 - Absorption: oxy- & deoxy-hemoglobin, melanin, water
 - Scattering: cell nuclei and mitochondria
 - Polarization: Collagen and muscle fibers
- Physiology — Functional imaging (endogenous contrast):
 - Concentration of hemoglobin (angiogenesis)
 - Oxygen saturation of hemoglobin (hyper-metabolism)
 - Blood flow (Doppler)
 - Enlargement of cell nuclei
 - Orientation and denaturation of collagen
- Physiology — Molecular imaging (exogenous contrast):
 - Integrin, VEGF (vascular endothelial growth factor).
 - Reporter genes
-

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Major Challenge in Optical Tomography: High Resolution Beyond the Quasiballistic (~1-mm Depth) Regime

1 mm

Soft limit* ~ l_t'

Hard limit ~ 10 δ ~ 5-7 cm (20,000X or 43 dB one-way attenuation)

Laser

CFM & 2PM

OCT

DOT, PAT

CFM: Confocal microscopy
2PM: Two-photon microscopy
OCT: Optical coherence tomography
DOT: Diffuse optical tomography
PAT: Photoacoustic tomography
 l_t' : Optical transport mean free path ~ 1 mm (mean free path ~ 0.1 mm)
 δ : Effective penetration depth

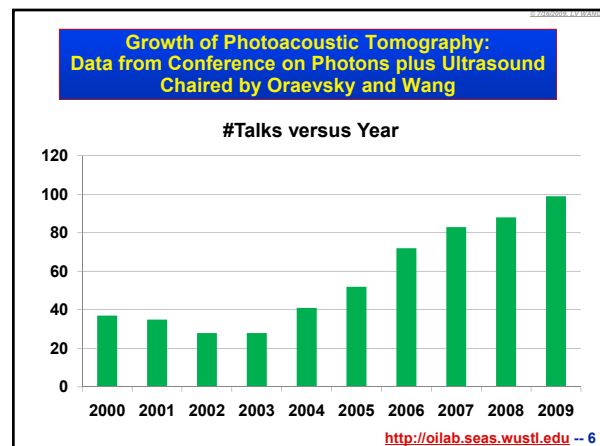
* Applied Optics 38, 4951 (1999).
Simulation software MCML available on the web

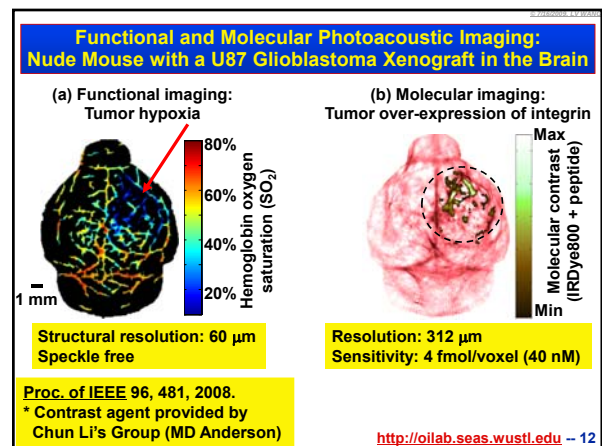
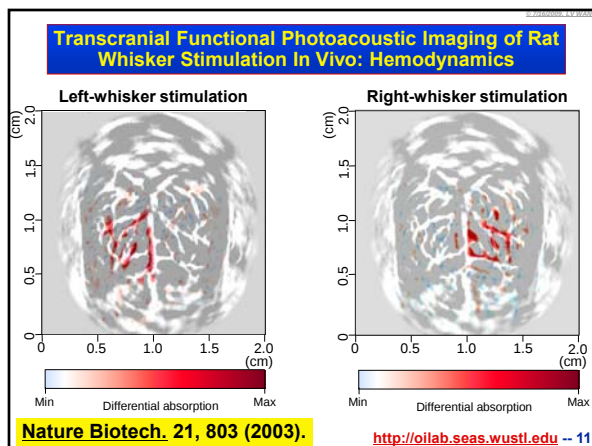
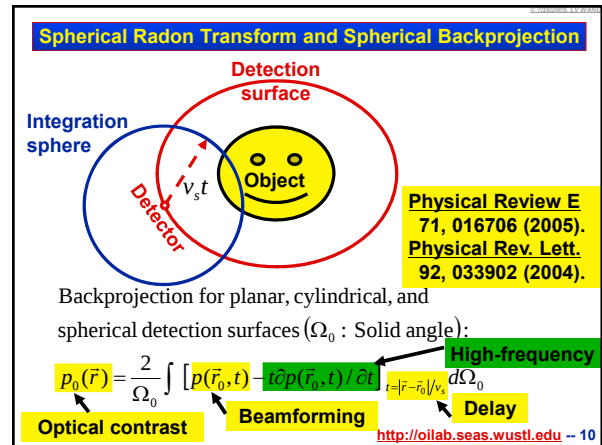
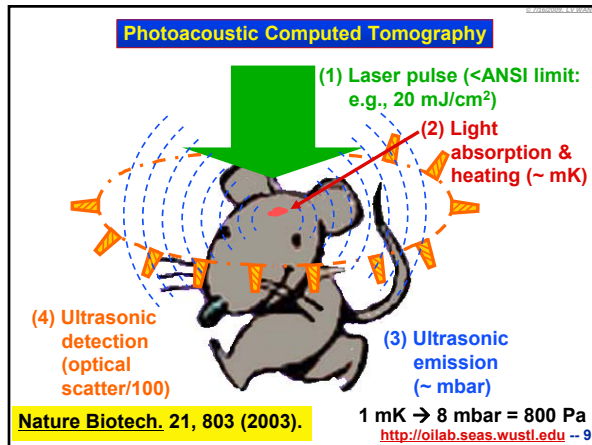
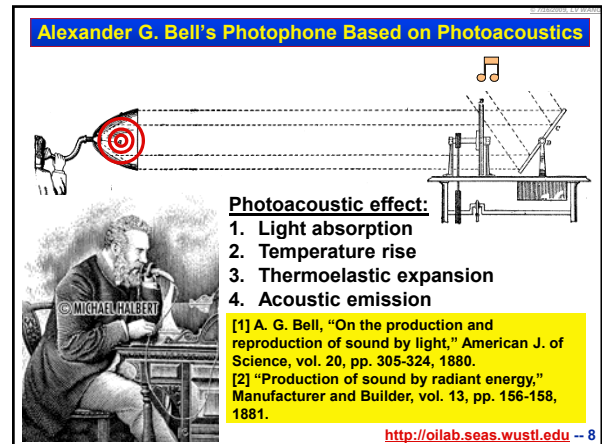
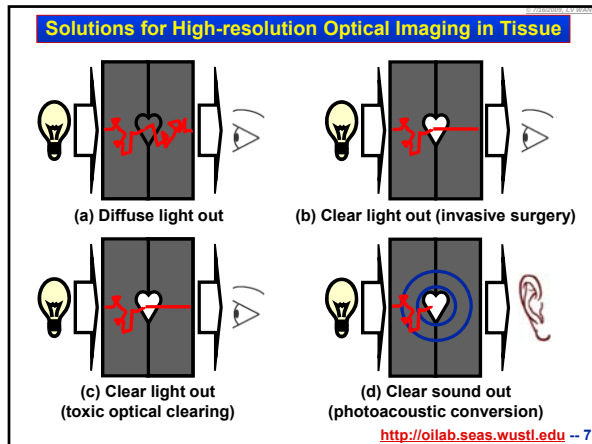
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Optical Diffraction versus Diffusion

- Diffraction limits the spatial resolution of ballistic imaging
- Breaking the diffraction limit leads to super-resolution imaging
- Diffusion limits the penetration of ballistic imaging
- Breaking the diffusion limit leads to super-depth imaging

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5-MHz Ring Ultrasonic Array

- Transducers:**
 - Elements: 512-elements.
 - Center frequency: 5 MHz.
 - Bandwidth: 80% of center freq.
- Geometry:**
 - Shape: Ring with 50 mm diam.
 - Pitch: 0.308 mm. Kerf: 0.1 mm.
 - Elevation height: 10 mm.
 - Elevation focal length: 19 mm.
- Data acquisition:**
 - Channels: 64 channels A/D (8:1 MUX)
 - Sampling rate: 40 MHz.
 - Sampling dynamic range: 12 bits.
 - Frame rate: 0.9 Hz with a 7-Hz laser pulse repetition.
- Resolution:**
 - In plane: ~200 μm .
 - Elevation: ~1.9 mm.

J. Biomed. Optics 13, 024007, 2008.
Optics Express, submitted, 2009.
* Detection system by Q. Zhu's Group (UConn).

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Noninvasive Photoacoustic Image of a Mouse Brain: 360° View, 0.9 Hz Frame Rate and Gel Coupling

Photoacoustic Image
Field of view: 10 mm x 14 mm

Photograph

C. Li et al., unpublished.

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Reflection-mode Photoacoustic Microscopy: Illustration

Surface

Target

B-scan

A-scan

Photoacoustic signal

Time of arrival or depth

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Reflection-mode Dark-field Confocal Photoacoustic Microscopy: System

Tunable laser Nd:YAG pump laser

Photodiode

Motor driver

Translation stages

Conical lens

Sample holder

Base

Amplifier

AD

Computer

Heater & temperature controller

Optical illumination

Ultrasonic transducer

Mirror

Dual foci

Sample

Annular illumination with a dark center

Optics Letters 30, 625 (2005).
Nature Biotech. 24, 848 (2006).
Nature Protocols 2, 797 (2007).

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Photoacoustic Imaging Depth and Resolution: 50 MHz System (High Ultrasonic Frequency)

B-scan of a double-stranded cotton thread embedded in a rat

Surface

Thread

3 mm

1 mm

- Imaging depth: ~3 mm
- Axial resolution: ~15 microns
- Depth/resolution: ~200 pixels
- Lateral resolution: ~45 microns
- Acquisition time: 2 μs /A-scan
- Signal averaging: None

Super-depths for high-resolution optical imaging (beyond the quasiballistic regime)

Optics Letters 30, 625 (2005).

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Volumetric Imaging of Rat Microvasculature In Vivo

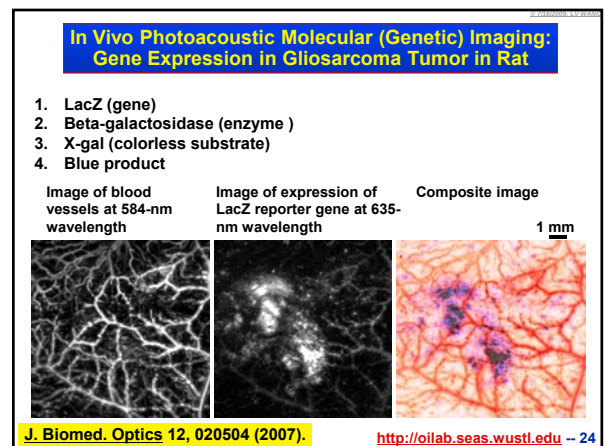
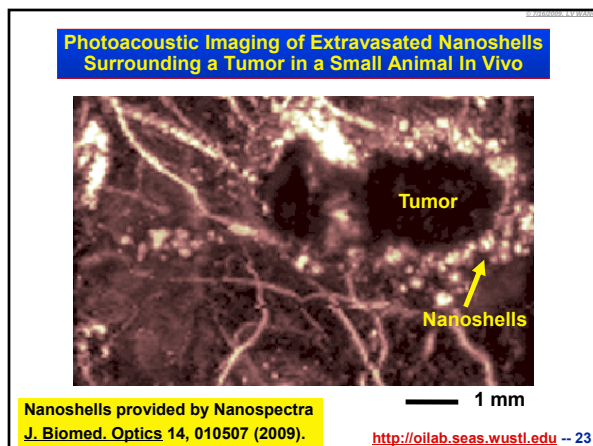
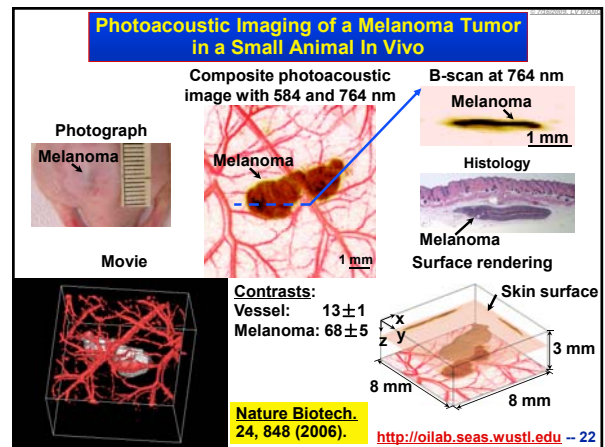
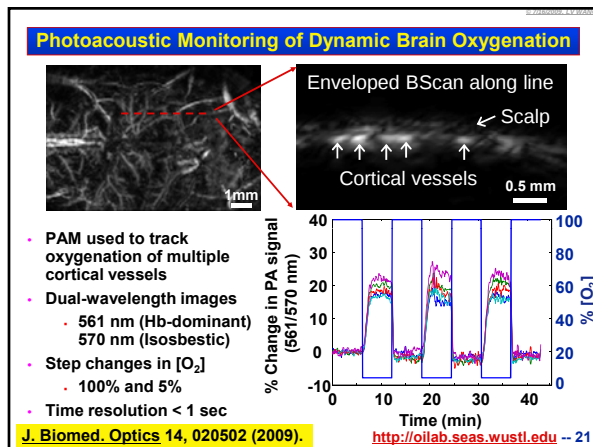
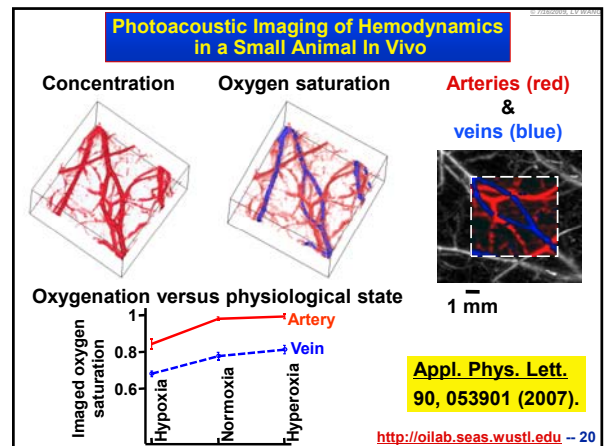
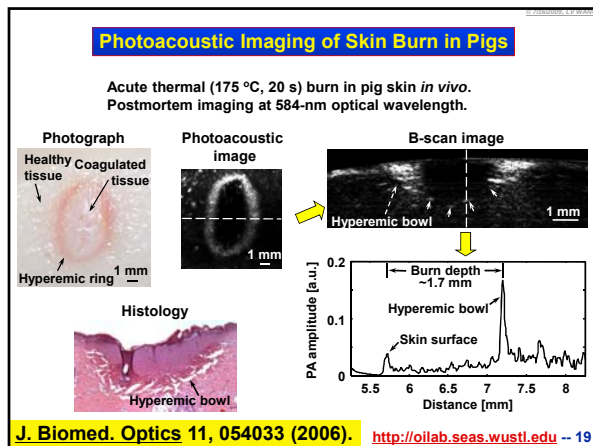
Maximum amplitude projection onto the skin

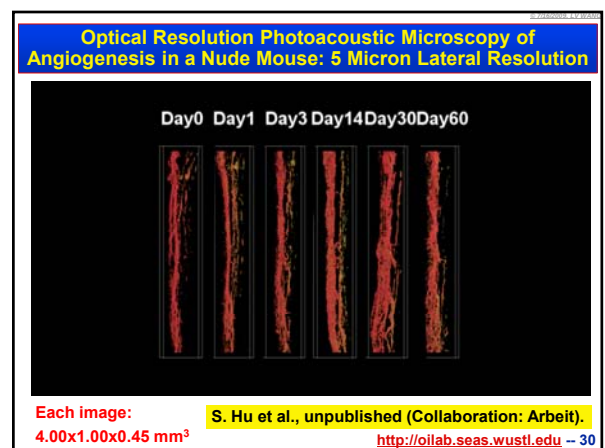
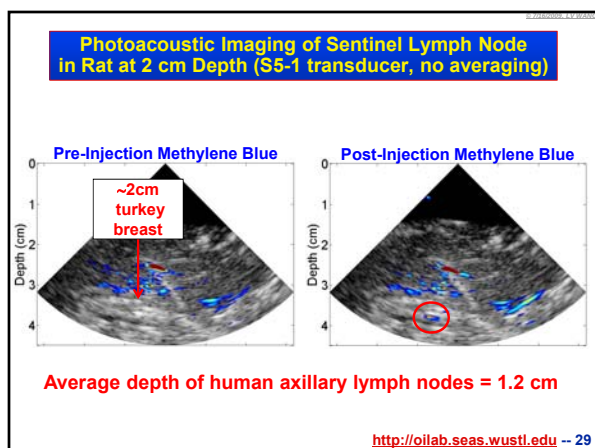
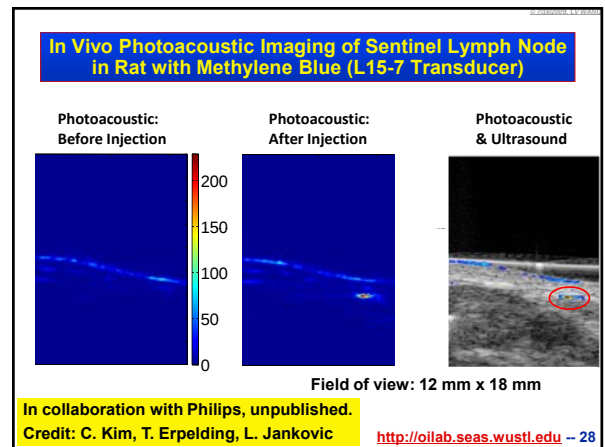
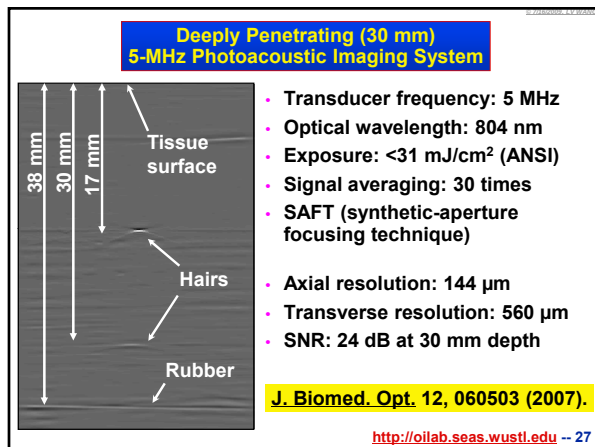
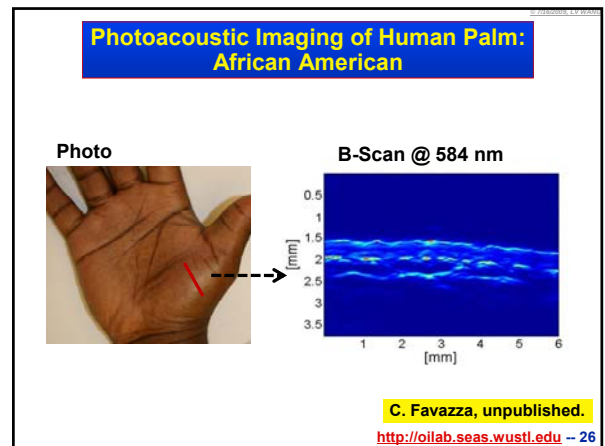
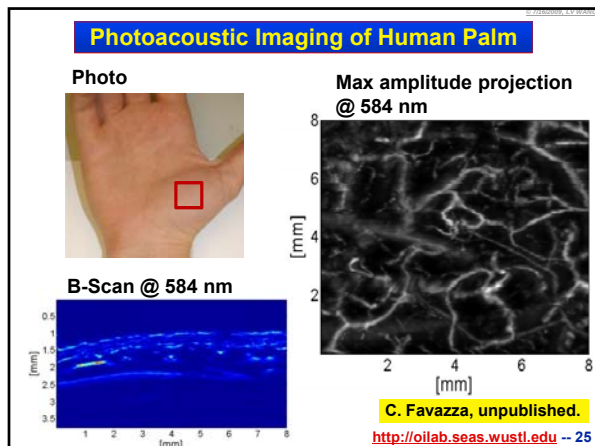
1 mm

Volume: 10 mm x 8 mm x 3 mm

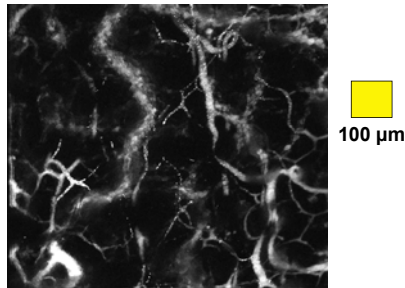
Optics Express 14, 9317 (2006).

<http://oilab.seas.wustl.edu> -- 18





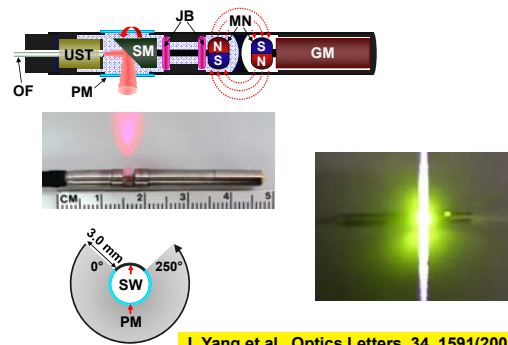
Optical Resolution Photoacoustic Microscopy of Single Red Blood Cells In Situ: 2 Micron Lateral Resolution



G. Ku et al., unpublished.

<http://oilab.seas.wustl.edu> -- 31

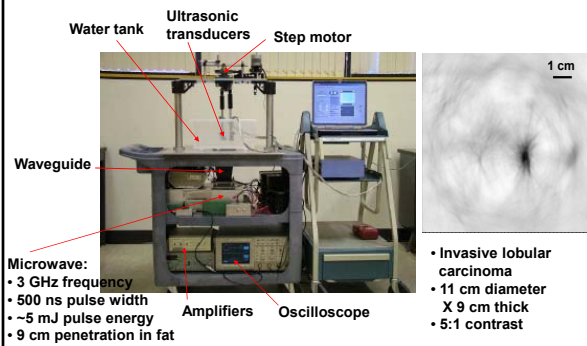
Photoacoustic Endoscopy



J. Yang et al., Optics Letters, 34, 1591(2009).

<http://oilab.seas.wustl.edu> -- 32

Microwave-Induced Thermoacoustic Tomography (TAT): Experimental System and Image of Mastectomy Specimen



Microwave:
• 3 GHz frequency
• 500 ns pulse width
• ~5 mJ pulse energy
• 9 cm penetration in fat

• Invasive lobular carcinoma
• 11 cm diameter
• X 9 cm thick
• 5:1 contrast

Tech. in Cancer Res. & Treat. 4, 559 (2005).

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Summary

- **Photoacoustic tomography** achieved by optical excitation and ultrasonic detection: Physically integrated single modality.
- **Depths** beyond optical transport mean free path imaged
 - Absorption of both unscattered and scattered photons used
 - “Soft limit” (~1 mm in skin) broken (i.e., superdepths achieved)
 - “Hard limit” (~5 cm) reached
- **Spatial resolution** at superdepths determined ultrasonically
 - Number of resolvable pixels enhanced: Depth/resolution > 200
 - Depth and resolution scaled: Scalable multiscale imaging
 - 15 micron axial resolution at 3 mm depth shown
 - 150 micron axial resolution at 30 mm depth shown
- **Spatial resolution** within “soft limit” determined both optically and ultrasonically
 - 2-5 micron transverse resolution demonstrated
 - Single capillaries (smallest blood vessels) resolved
 - Single red blood cells imaged

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Summary (Continued)

- **Contrast** provided by optical absorption properties
 - Ultrasonic or fluorescent contrasts complemented
 - Sensitivity to specific absorption (mJ/cc) shown to be 100%
 - High specificity attributed to high intrinsic contrast: Blood:bg>10:1
 - Multiple chromophores detected spectrally: Oxy- and deoxy-Hb
 - Functional imaging allowed by endogenous chromophores: sO₂
 - Molecular biomarker imaging enabled by targeted contrast agents: Organic IRDye800 bound to integrin
 - Molecular gene-expression imaging derived from reporter genes: Blue product from lacZ gene
- **Frame rate** limited theoretically by range/sound speed: 0.1 ms → 15 cm
 - 50 frames/second (Hz) achieved thus far
 - Limited practically by the number of ultrasonic transducers
 - Limited practically by the pulse repetition rate of the laser

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Summary (Continued)

- **Thermoacoustic tomography** achieved by microwave/RF excitation and ultrasonic detection.
 - Optical “hard limit” broken
 - Water or ion contrasts imaged
 - Deep-penetrating nonionizing molecular imaging possible
- **Speckle** in optical coherence tomography or ultrasonography avoided
- **Non-ionizing** radiation used
- **Costs** estimated comparable to those of ultrasound imaging systems

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[Source codes](#)

Biomedical Optics
Principles and Imaging



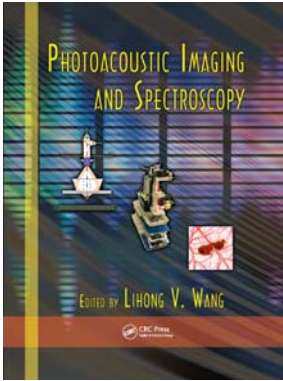
LIHONG V. WANG
HSIN-I WU

Chapters

1. Introduction to biomedical optics
2. Single scattering: Rayleigh theory and Mie theory
3. Monte Carlo modeling of photon transport
4. Convolution for broad-beam responses
5. Radiative transfer equation and diffusion theory
6. Hybrid model of Monte Carlo method and diffusion theory
7. Sensing of optical properties and spectroscopy
8. Ballistic imaging and microscopy
9. Optical coherence tomography
10. Mueller optical coherence tomography
11. Diffuse optical tomography
12. **Photoacoustic tomography**
13. Ultrasound-modulated optical tomography

Homework solutions provided for instructors

Taped tech presentations available on our web <http://oilab.seas.wustl.edu> -- 37



Edited by LIHONG V. WANG

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