Purpose: In vivo dosimetry using an electronic portal imaging device (EPID) may provide a uniquely effective means for preventing errors and may allow for real-time beam interlocks. We present graphical processor (GPU)-based fast EPID dose computation and simulate the sensitivity for detecting errors caused by patient mispositioning.

Methods: We implemented an enhanced superposition convolution algorithm to compute the EPID dose. The patient was simulated using a digital cylinder phantom ( 15 cm length and 15 cm diameter) with air and bone structure built in. Setup parameters are: SAD $100 \mathrm{~cm}, 12 \times 12-\mathrm{cm} 2$ open field, $1.5 \times 1.5 \times 1.5-\mathrm{mm} 3$ dose grid, $6-\mathrm{MV}$ photon and isocenter at the center of cylinder. 2D dose images were obtained at $1.6-\mathrm{cm}$ depth of a water slab positioned $60-\mathrm{cm}$ below the isocenter to simulate the EPID readout. To examine errors caused by mispositioning, we shifted the phantom left-and-right and up-and-down and compared dose profiles to those with no shifts. Gamma value of each pixel was calculated as an index to identify dose mismatch. Dose failure was determined as gamma $>1$ using 3-mm distance-to-agreement and 3\% dose difference criteria.

Results: Dose failures occur mainly in air-tissue and bone-tissue interfaces and in regions with rapid thickness change. Gamma is sensitive to the left-and-right shift, with a $3-\mathrm{mm}$ shift causing dose failure in $\sim 10 \%$ pixels; but is much less sensitive to the up-and-down shift, with dose failure detected only after a shift of several centimeters. Analysis with patient CT data sets is underway and will be presented.

Conclusions: In vivo EPID dosimetry enabled by GPU-based dose computation offers the potential for real-time beam interlocks. Future directions include simulation of other error scenarios, optimization of dose computation, improved EPID modeling and comparison with measured EPID profiles.

