

**2014 AAPM SUMMER SCHOOL**

*University of Vermont • Burlington, VT • June 22–26, 2014*

SRS/SBRT/SABR:

Safely and Accurately Delivering  
High-Precision, Hypofractionated Treatments

# **Historical and Technical Overview of Gamma Knife Radiosurgery**

David Schlesinger, Ph.D.

University of Virginia

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## Disclosures

Research support: Elekta, AB

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## Learning Objectives

- To understand the basic characteristics of radiosurgery and how they differ from traditional external-beam techniques.
- To learn the basic operational concepts of the Gamma Knife.
- To understand the historical evolution of the Gamma Knife and possible future directions.

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## History of the Gamma Knife

Design and Physical Principles

Treatment Procedures

Acceptance/Commissioning/QA

Recent/Future Developments



## The “first” stereotactic surgery



Prehistoric female skull, San Damian, Peru, showing trephination marks.



Prehistoric female skull, Cinco Cerros, Peru, left frontal and parietal incision with no signs of healing.

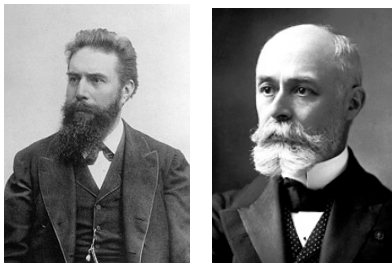
Images from the San Diego Museum of Man, San Diego, CA

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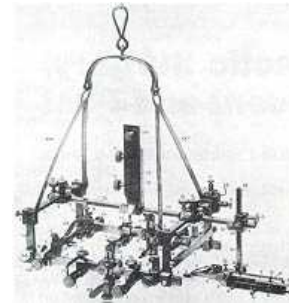
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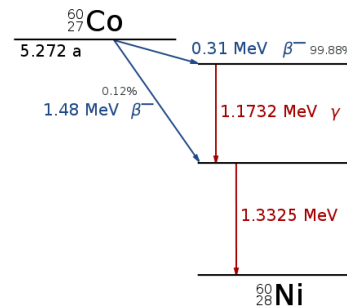
## Thousands of years later.....



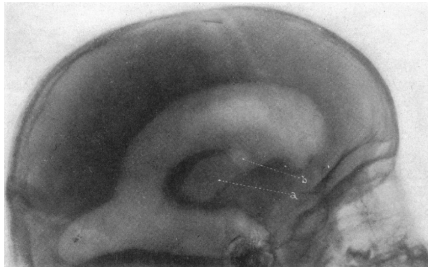
Wilhelm Röntgen  
(x-rays) 1895  
Henri Becquerel  
(spontaneous  
radioactivity) 1896



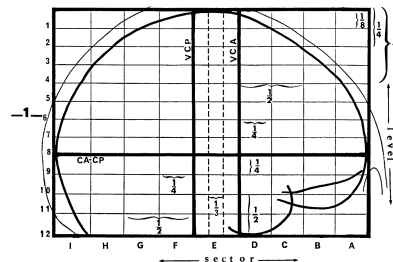
Horsley and  
Clarke apparatus  
(animals)  
1908



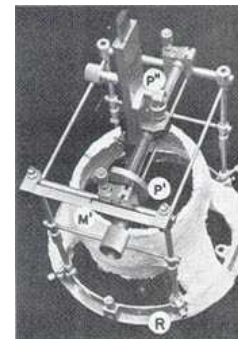
Glen Seaborg,  
John Livingood  
(Cobalt-60)  
Late 1930s



Walter Dandy  
(air  
ventriculography)  
~1919



Jean Tailarach  
(human atlas)  
1967



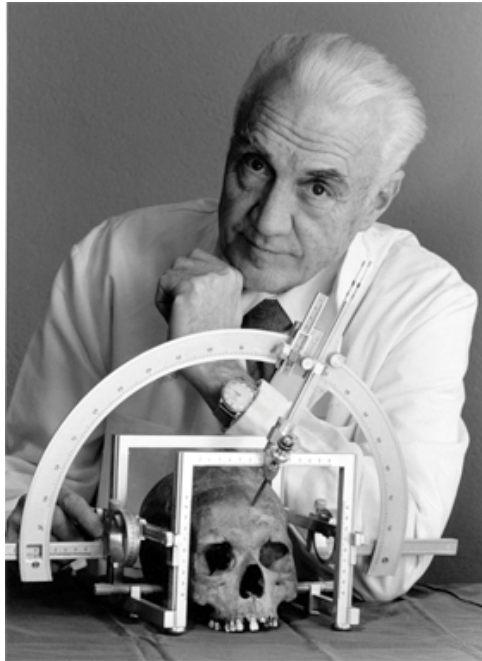
Spiegel and Wycis  
Apparatus  
(people)  
1946

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## 1951: “The Stereotactic Method and Radiosurgery of the Brain”



Lars Leksell with arc-centered stereotactic frame  
(image courtesy of Elekta, AB)



Leksell at the 185 MeV Uppsala cyclotron facility circa 1958

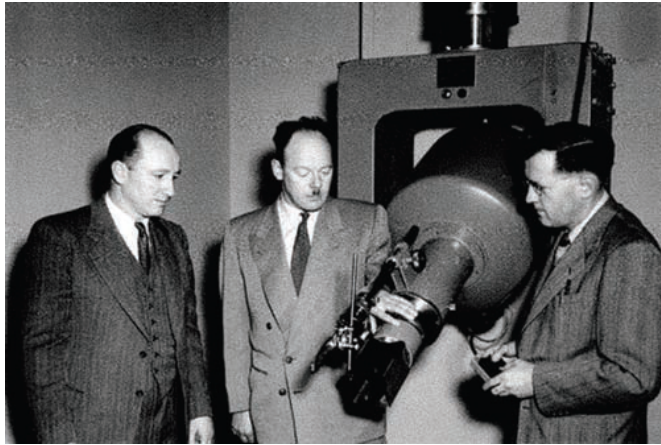
Leksell, L. 1951. The stereotactic method and radiosurgery of the brain. *Acta Chir. Scand.* 102:316–9.



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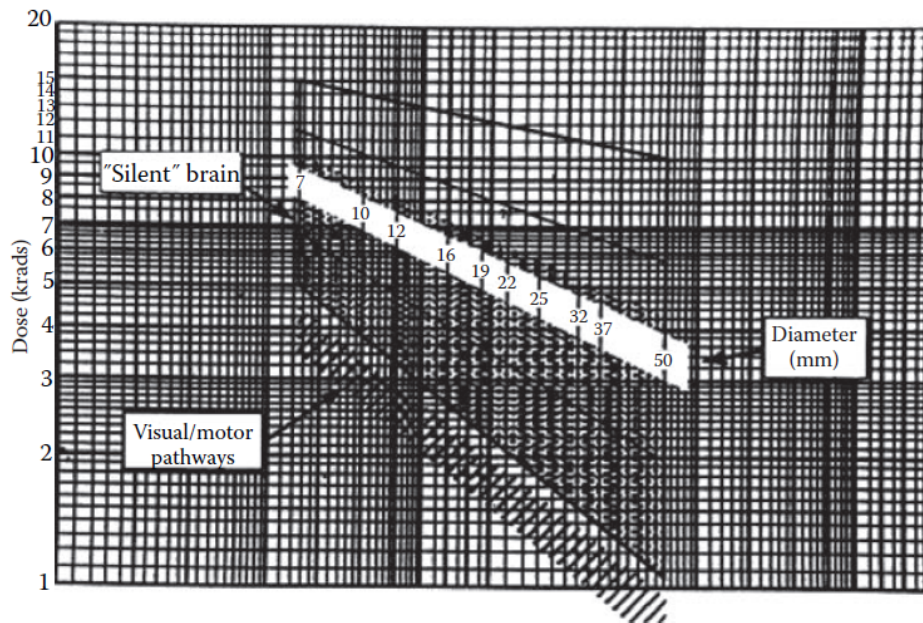
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First cobalt-60 teletherapy source at Saskatoon Cancer Centre, with Sandy Watson, John MacKay, and Harold Johns.

(image source: University of Saskatchewan)



Raymond Kjellberg dose versus total volume risk curve for proton therapy of AVM.

Kjellberg RN, Hanamura T, Davis KR, Lyons SL, Adams RD: Bragg-peak proton-beam therapy for arteriovenous malformations of the brain. **New England Journal of Medicine** 309:269-74, 1983.

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## 1967 - The first “Gamma Knife”



Lars Leksell and  
Ladislau Steiner



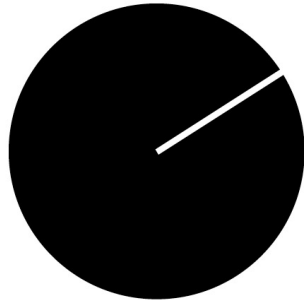
Tony DeSalles and Catherine Gilmore (the first president  
of Elekta) with original Gamma Knife at UCLA

Leksell, L. 1971. *Stereotaxis and Radiosurgery: An Operative System*.  
Springfield: Thomas Publishing.

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(1972)

E L E K T A



1988 - Model B introduced

Wu, A., et al., Physics of Gamma Knife approach on convergent beams in stereotactic radiosurgery. *IJROBP*, 18:941–9, 1990.



1987 - Model U  
201 sources, ~30 Ci each  
Circular collimators  
Beam alignment ~0.2mm



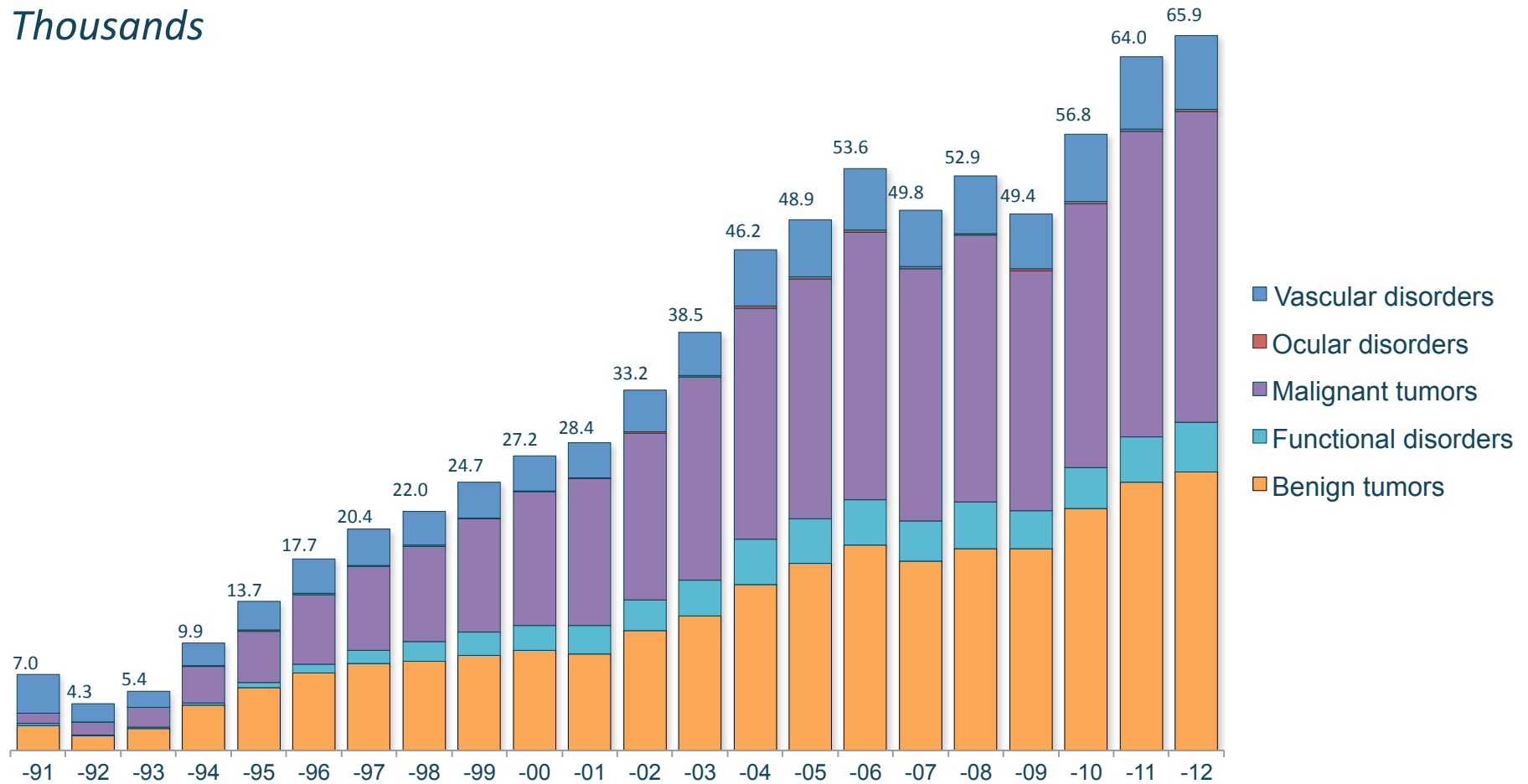
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## Annual Indications Treated, 1991-2012

Thousands



Source: Leksell Gamma Knife Society

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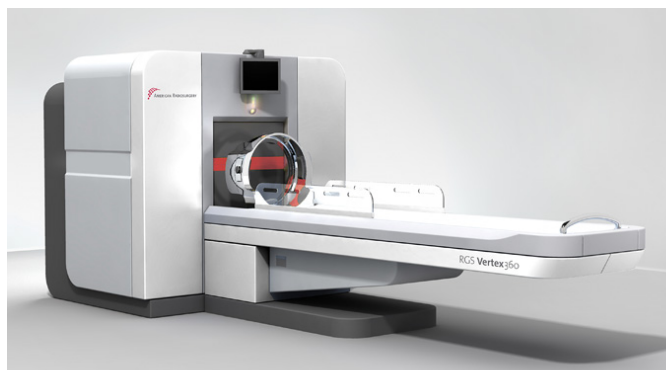
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Model C/4C (1999)      201 sources (5 annular rings)      Automatic positioning system

Model Perflexion (2006)      192 sources 8 sectors (no helmets)      Couch positioning system



OUR/American Radiosurgery (1998/2007)      30 sources (rotating, no helmets)      Automatic couch positioning



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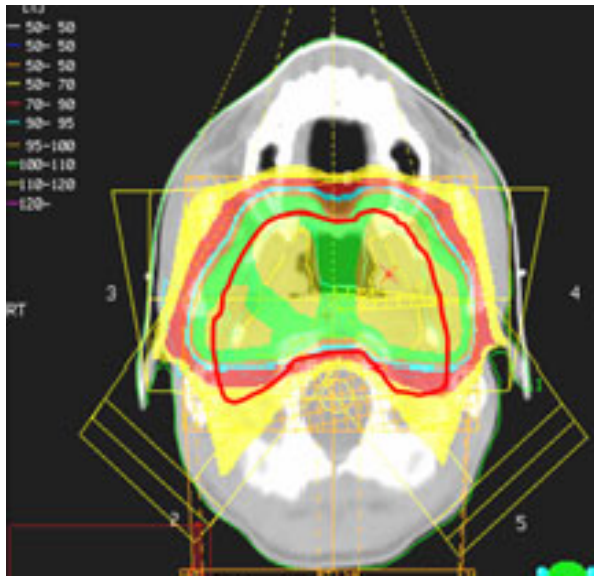
Recent/Future Developments

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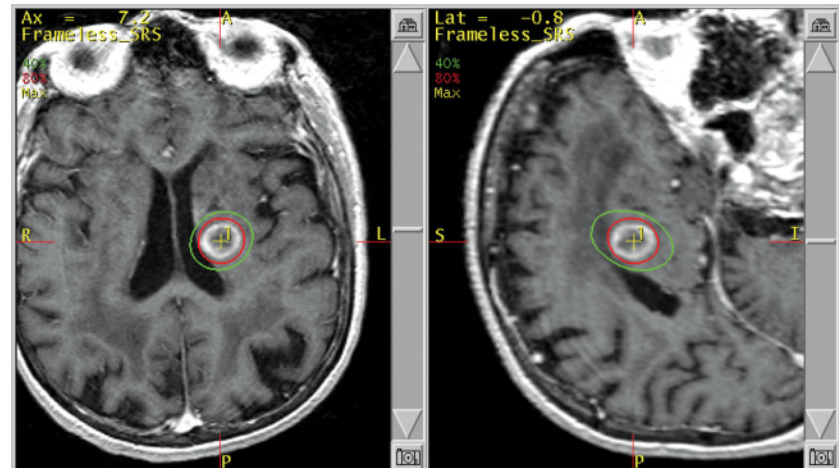
## 6-field 3D conformal plan



Cheung, Biomed Imaging Interv J 2006; 2(1):e19

- Tumor + normal tissue targeted
- Formalized treatment margins (GTV/CTV/ITV/PTV)
- Homogenous dose
- Low doses per fraction, high # fractions

## Intracranial SRS treatment plan



www.varian.com

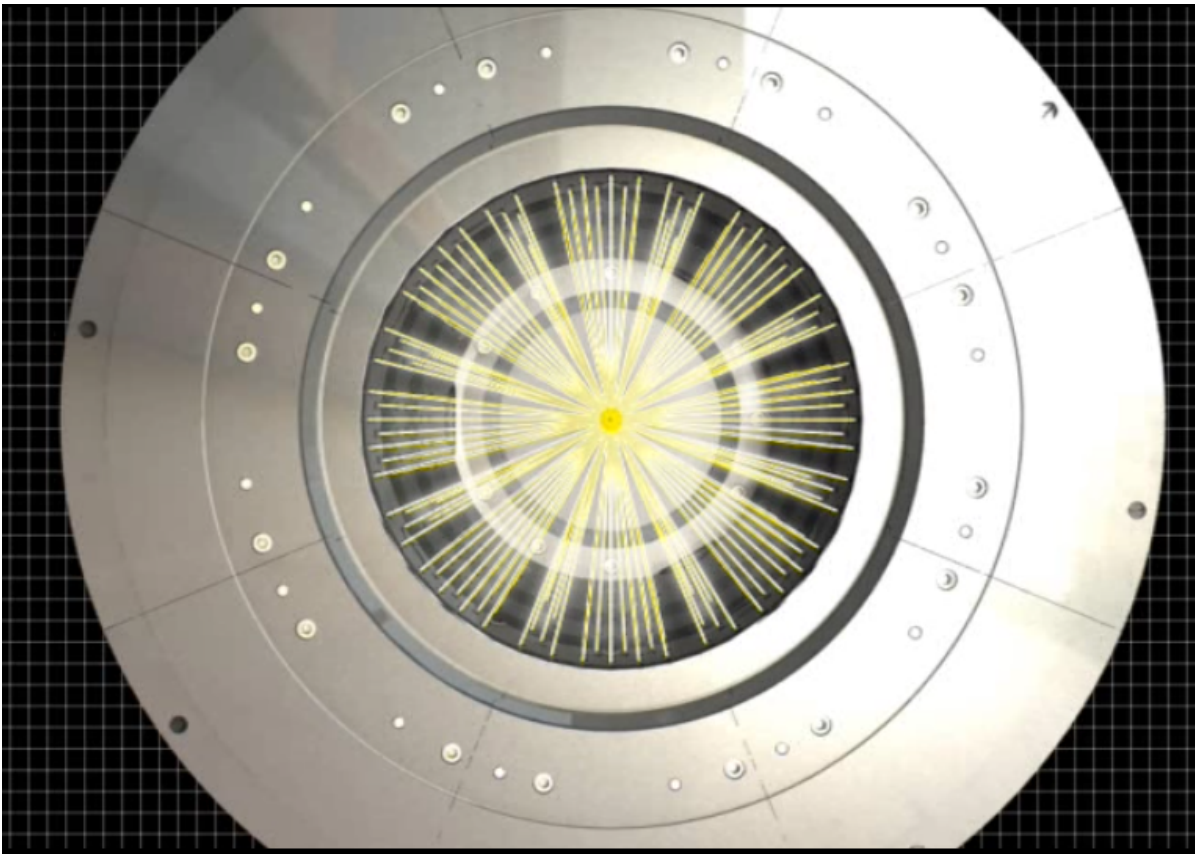
- Small fields, differential targeting
- High doses per fraction, small # fractions
- Treatment margins not as formal
- Steep dose gradients
- Inhomogeneous dose within tumor
- Extremely high requirement for accuracy!

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## Superposition of Beams

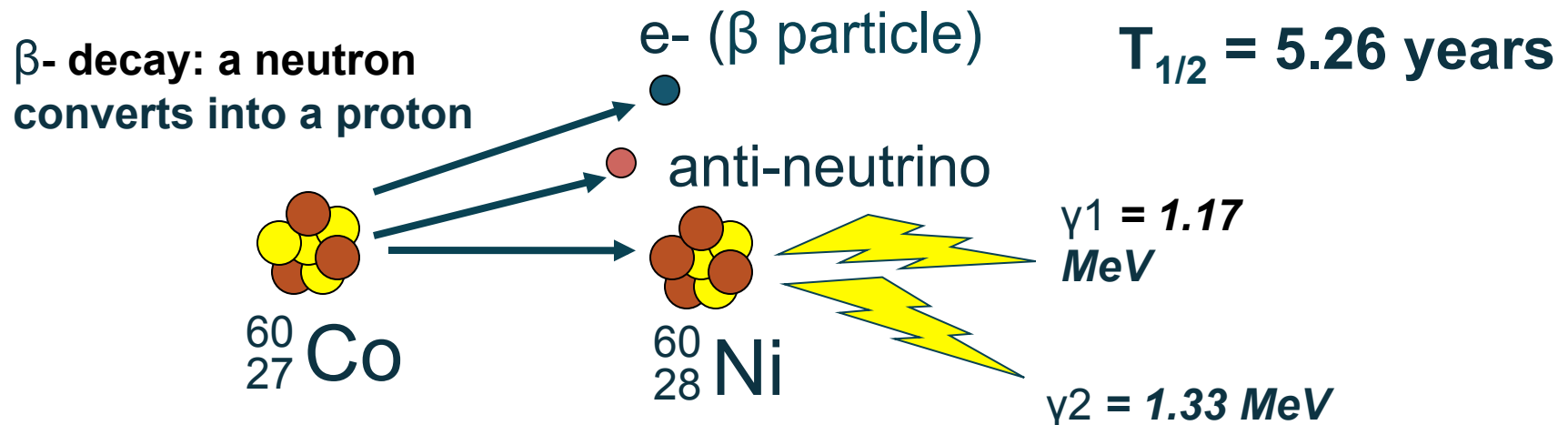


Technical ability to create many individual small beams led directly to the use of  $^{60}\text{Co}$

Spreading the energy out generates the steep dose gradients

Image courtesy of Elekta, AB

## Cobalt-60 Powered



${}^{60}\text{Co}$  decay is a very stable photon source  
Requires less technical complexity than a linac  
192/201 beams per isocenter!

## Stereotactic Targeting

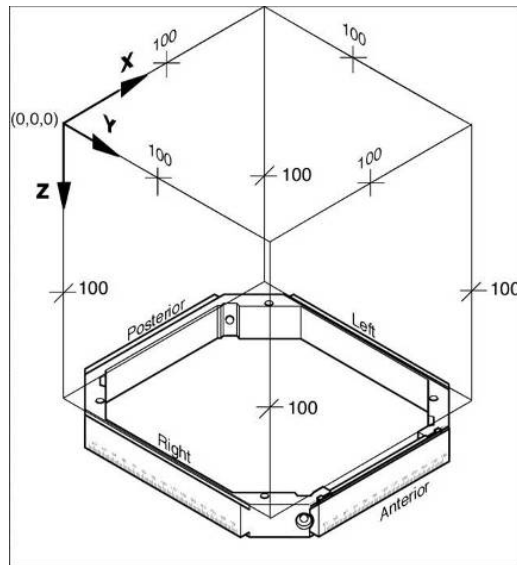


Image courtesy of Elekta



The frame defines the coordinate system

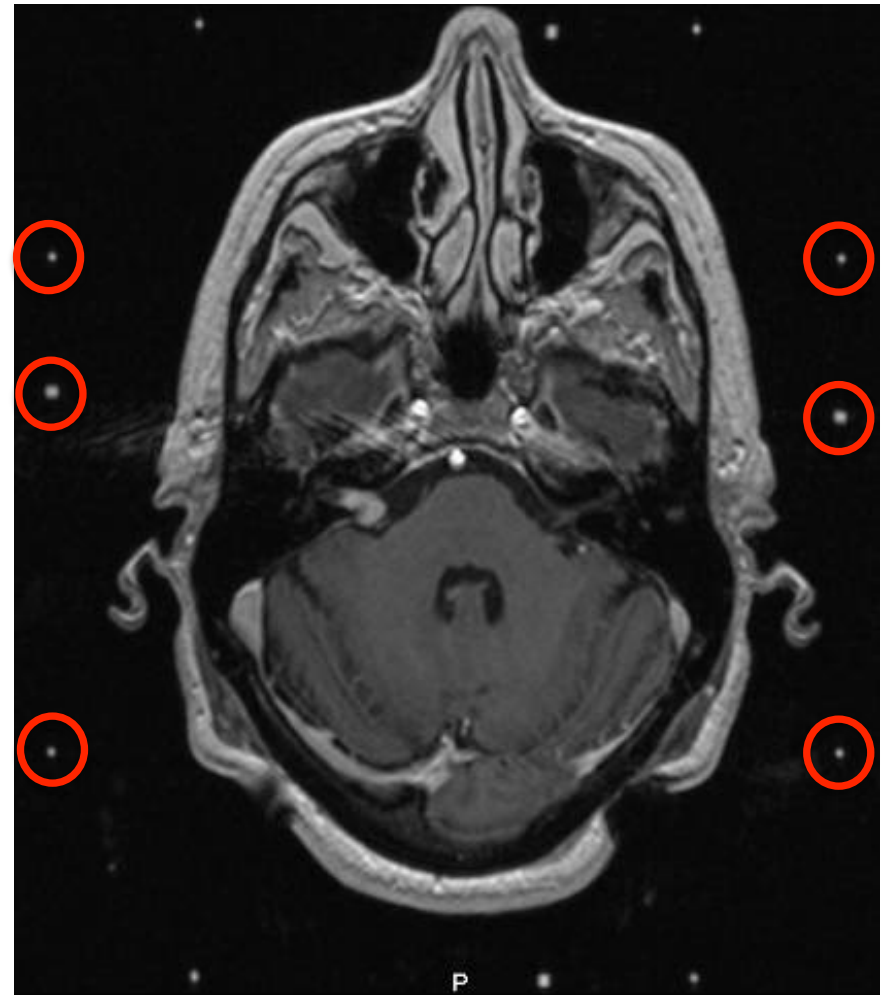
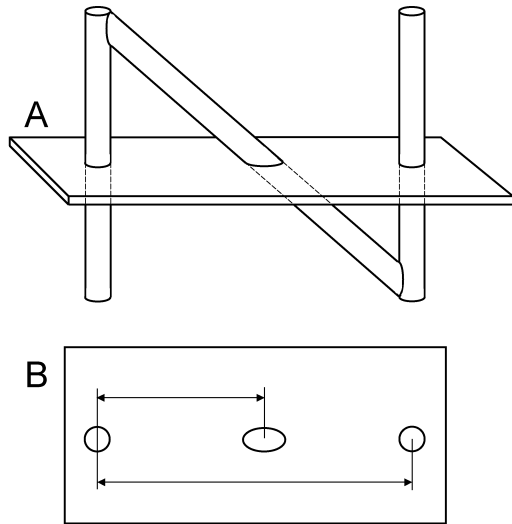
Coordinate system origin is to the right, superior, posterior of the patient's head

All coordinates are positive – no sign mistakes

Center of the system is considered to be (100, 100, 100) (mm)



# Stereotactic Fiducials



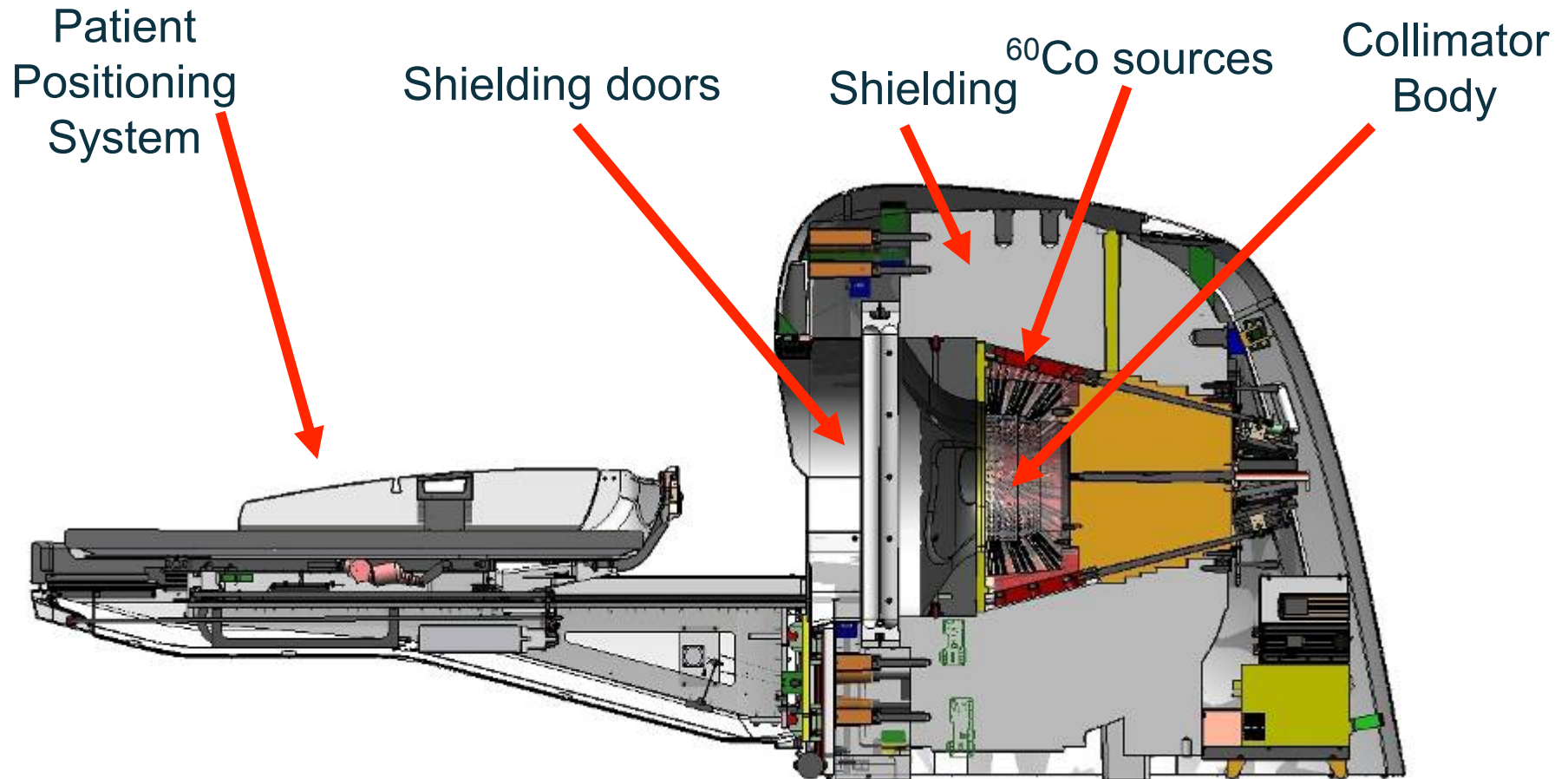
Brown R A, et al. (2013) The Origin of the N-Localizer for Stereotactic Neurosurgery. Cureus 5(9)

## Model C – Dosimetry

- Each helmet has a single-size collimator
- Each beam has an identical (400 mm) source to focus distance
- Each beam can be treated identically
- Off-axis profiles are 1D functions
- Model C has automatic (APS) and manual (trunnion) positioning methods
- Shielding is a manual operation



## Gamma Knife Perfexion



~20 metric tons to protect you from ~20 grams of  $^{60}\text{Co}$



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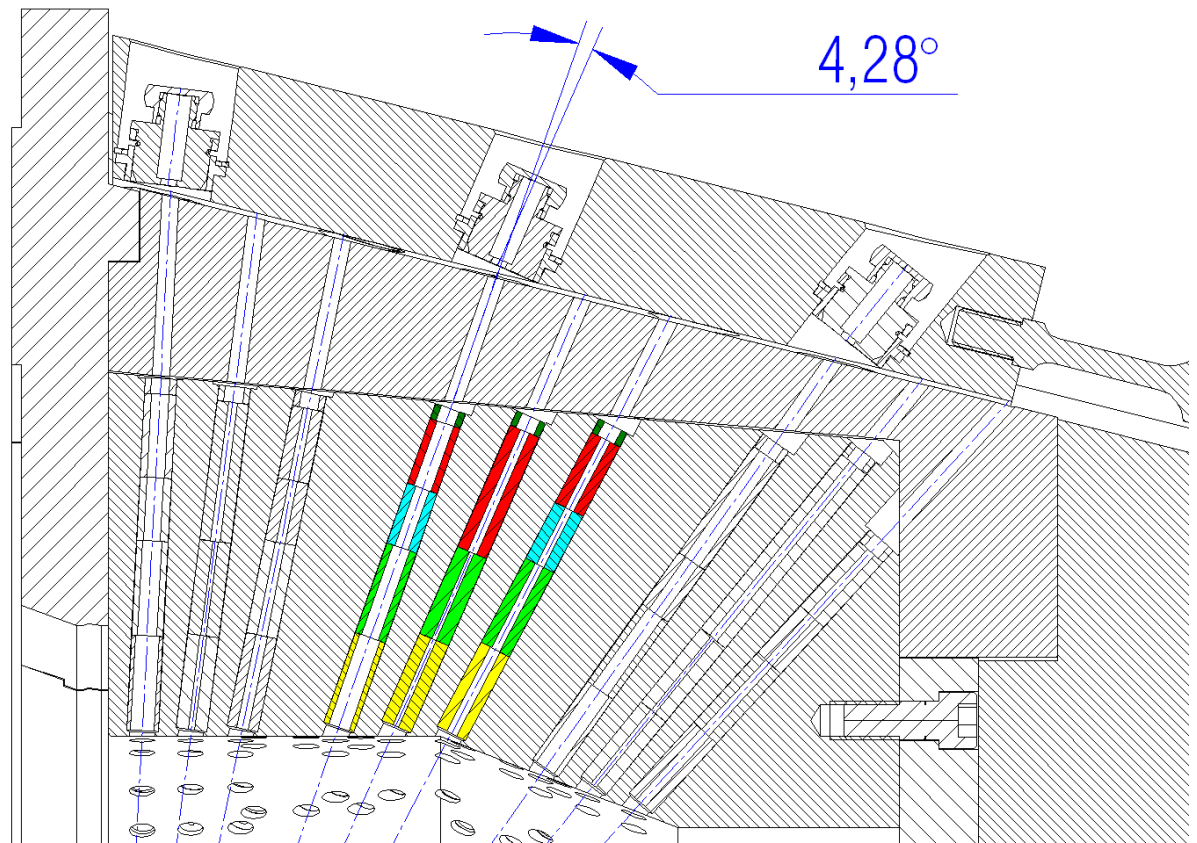
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## Perflexion Dosimetry

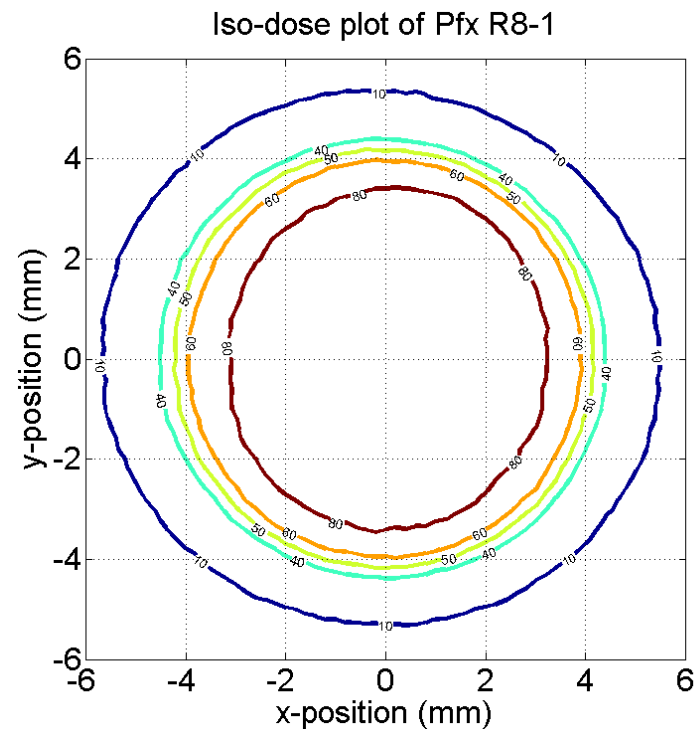
Source to focus  
distance depends on  
ring

Sources are angled  
relative to beam  
channels



## 2D Dose Profiles

Angled sources requires 2D OARs



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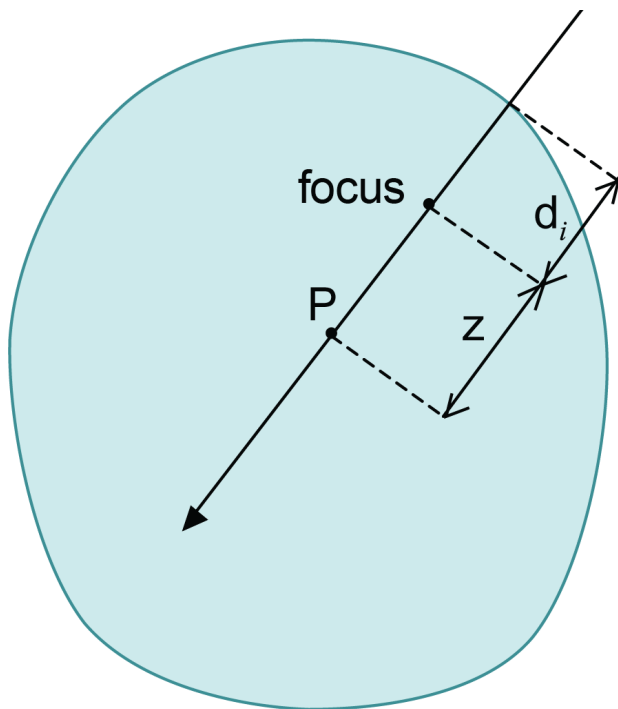
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<i>Collimator</i>	<i>Output factor</i>	<i>Attenuation constant (1/mm)</i>	<i>Scaling distances (mm)</i>	<i>Virtual source-to focus distance (mm)</i>
<i>P4_1</i>	<i>0.799</i>	<i>0.00678</i>	<i>377</i>	<i>521</i>
<i>P4_2</i>	<i>0.815</i>	<i>0.00704</i>	<i>380</i>	<i>546</i>
<i>P4_3</i>	<i>0.792</i>	<i>0.00690</i>	<i>387</i>	<i>533</i>
<i>P4_4</i>	<i>0.725</i>	<i>0.00712</i>	<i>398</i>	<i>595</i>
<i>P4_5</i>	<i>0.663</i>	<i>0.00698</i>	<i>420</i>	<i>607</i>
<i>P8_1</i>	<i>0.957</i>	<i>0.00658</i>	<i>374</i>	<i>431</i>
<i>P8_2</i>	<i>0.946</i>	<i>0.00660</i>	<i>382</i>	<i>437</i>
<i>P8_3</i>	<i>0.901</i>	<i>0.00681</i>	<i>394</i>	<i>468</i>
<i>P8_4</i>	<i>0.808</i>	<i>0.00665</i>	<i>408</i>	<i>480</i>
<i>P8_5</i>	<i>0.730</i>	<i>0.00680</i>	<i>433</i>	<i>522</i>
<i>P16_1</i>	<i>0.961</i>	<i>0.00694</i>	<i>381</i>	<i>481</i>
<i>P16_2</i>	<i>1</i>	<i>0.00685</i>	<i>379</i>	<i>459</i>
<i>P16_3</i>	<i>0.986</i>	<i>0.00675</i>	<i>383</i>	<i>455</i>
<i>P16_4</i>	<i>0.920</i>	<i>0.00690</i>	<i>389</i>	<i>488</i>
<i>P16_5</i>	<i>0.851</i>	<i>0.00694</i>	<i>409</i>	<i>519</i>

## The Basic Dose Model

$$\dot{D}_i(P) = \dot{D}_{\text{calibration},16} \times \frac{1}{192} \times of_i \times e^{-\mu_0(d_i - R_{\text{calibration}})} \times \frac{e^{-\mu_1 z}}{\left(1 + \frac{z}{R_{\text{vsf},i}}\right)^2}$$



A new TMR dose algorithm in  
Leksell GammaPlan®

The TMR 10 dose algorithm, available in Leksell GammaPlan® 10 and later, is an enhancement of the water-based dose calculation algorithm (here referred to as TMR Classic) in previous software versions. The purpose of this document is to describe the rationale for developing TMR 10, to explain the underlying physics and to review the changes in the predicted dose distributions relative to TMR Classic.

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## Stereotactic Frame Placement



UVA Gamma Knife  
(patient consented to photo use)

Takes 5-10 minutes

Usually done with local anesthesia and light sedation

Pins minimally break skin, penetrate to outer table of skull

Pin marks heal within a day or two of frame removal



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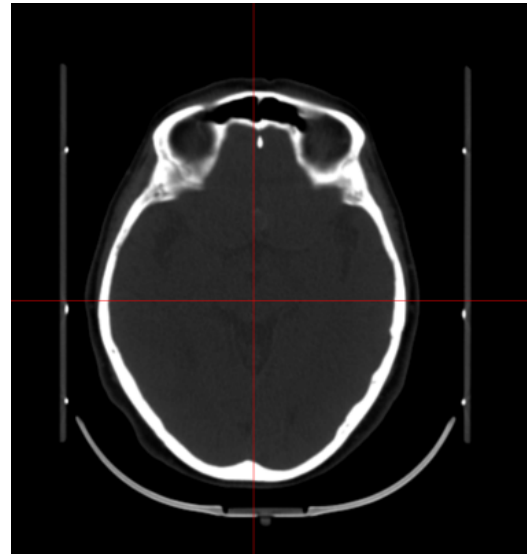
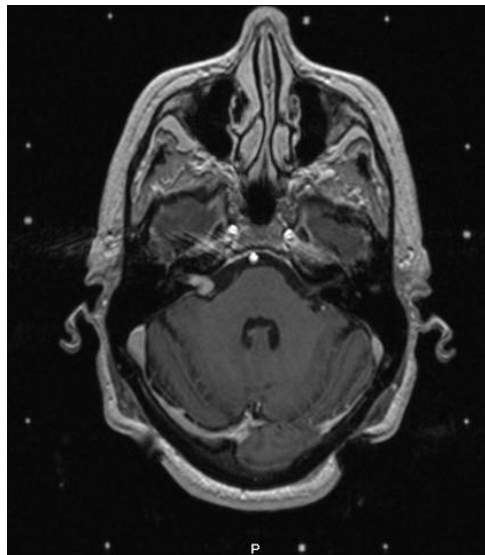
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## Treatment Planning Images

Typical imaging protocols:

Solid tumors	AVMs	Skull-base and pituitary
T1-weighted MR + contrast	Biplane DSA T1-weighted MR + contrast MRA	T1-weighted MR + contrast T2 CISS or SPACE T1-weighted + fat saturation

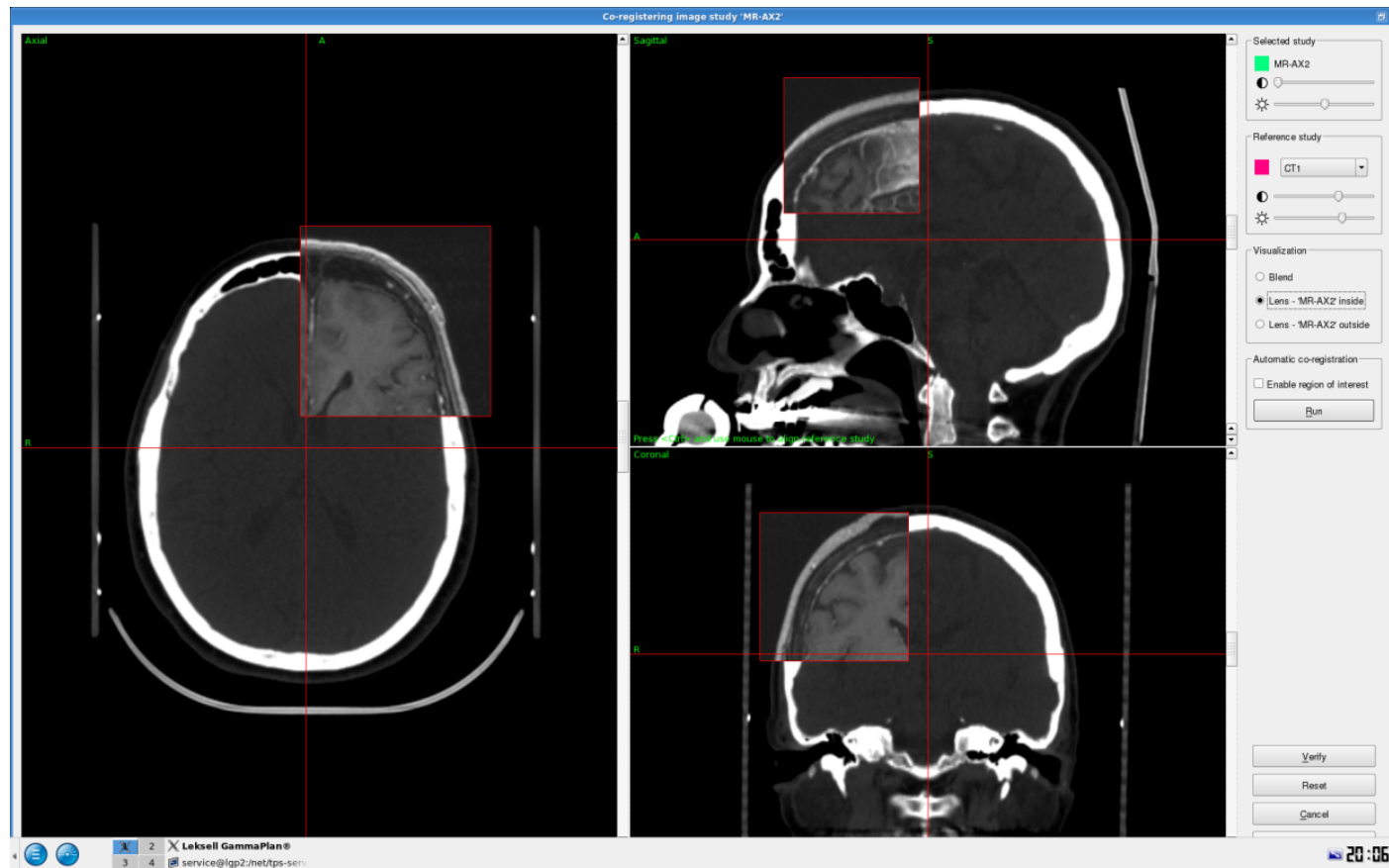


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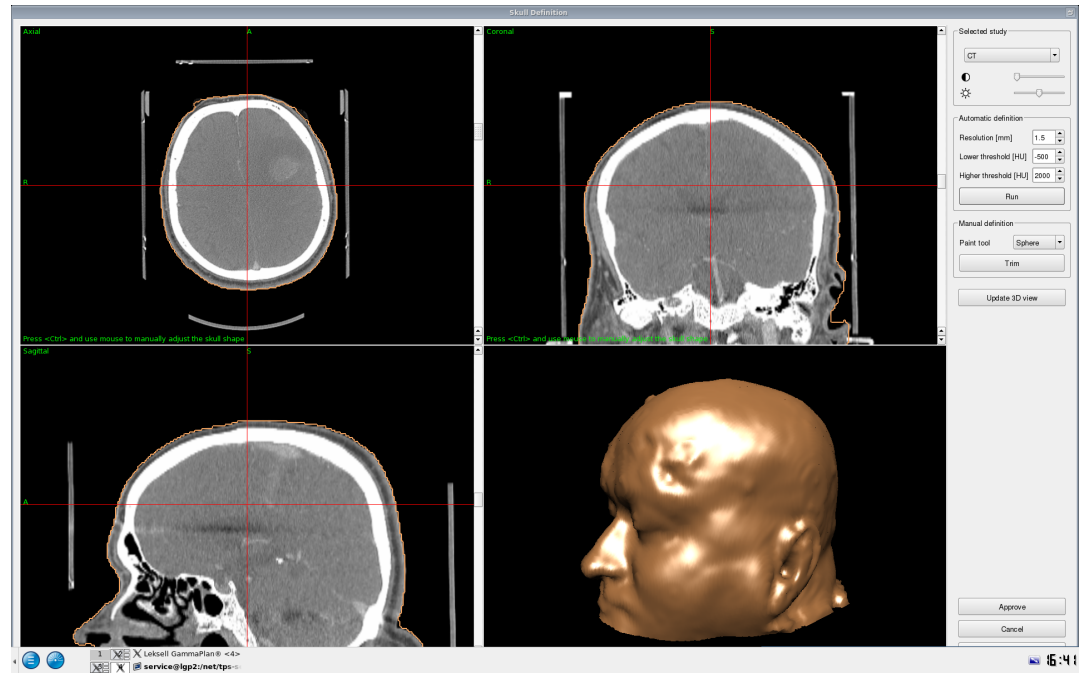
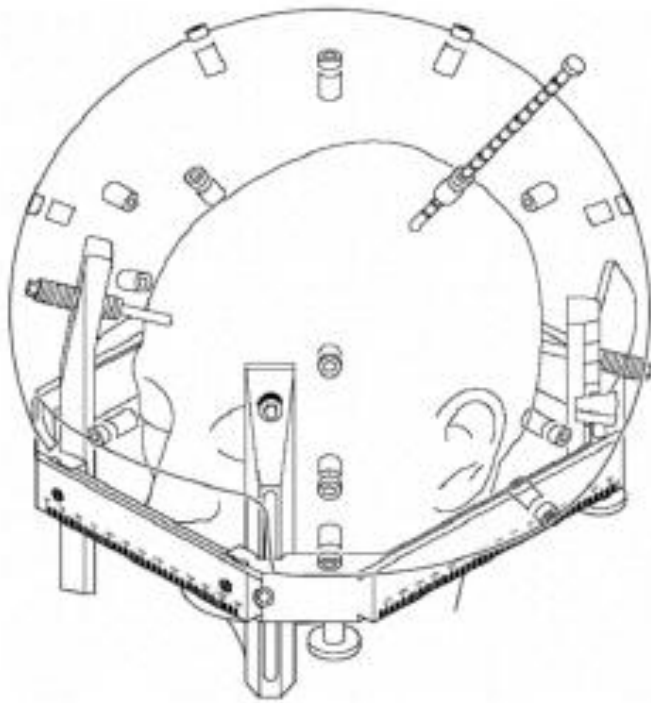
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## Co-registration of non-stereotactic imaging





## Skull Contours



Used to calculate SSD and depth of each beam

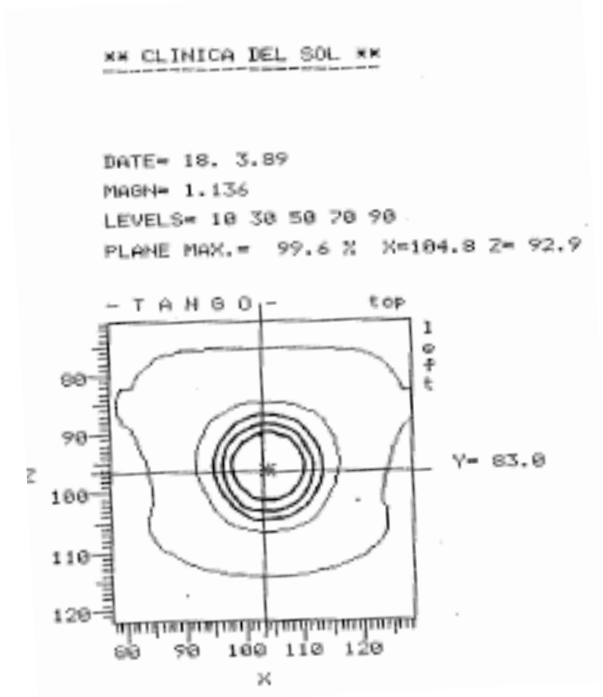
Also used to determine potential collisions between patient and helmet or side of collimator

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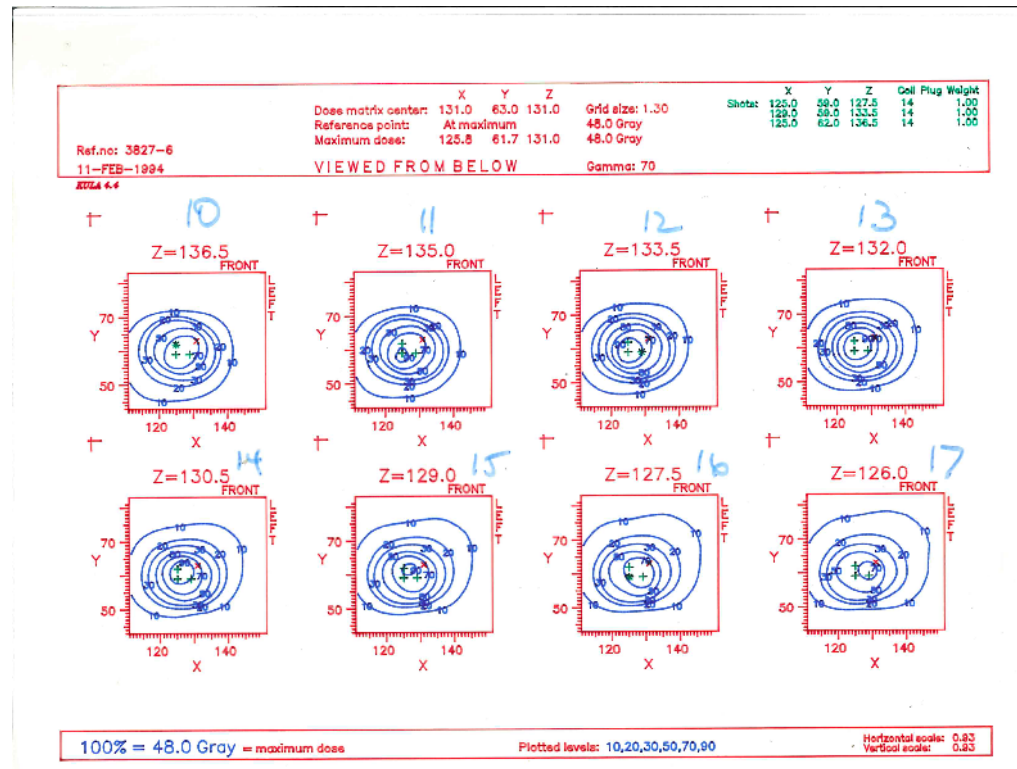
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## Evolution of Treatment Planning

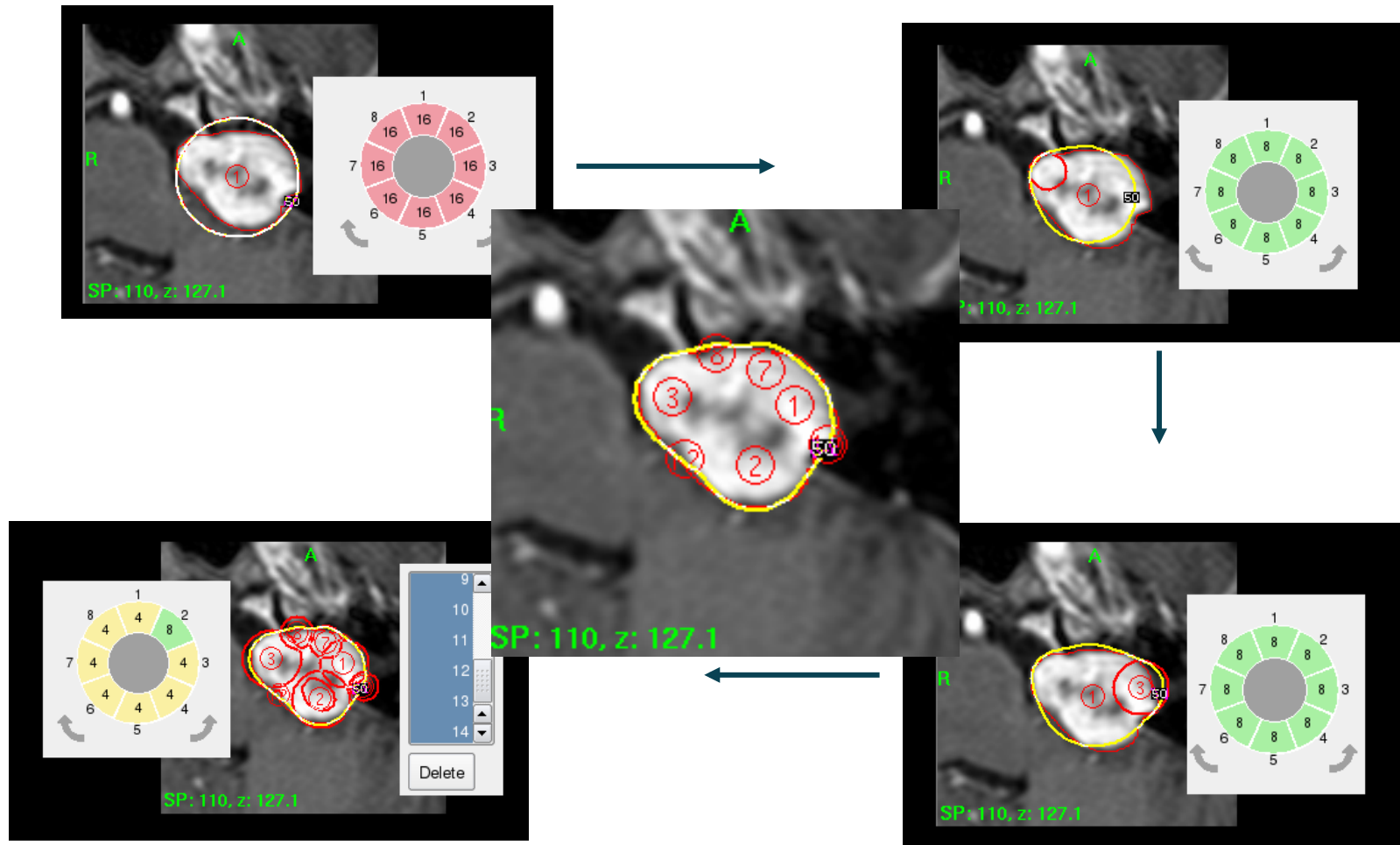


Tango treatment planning  
system  
Buenos Aires,  
plan circa 1989



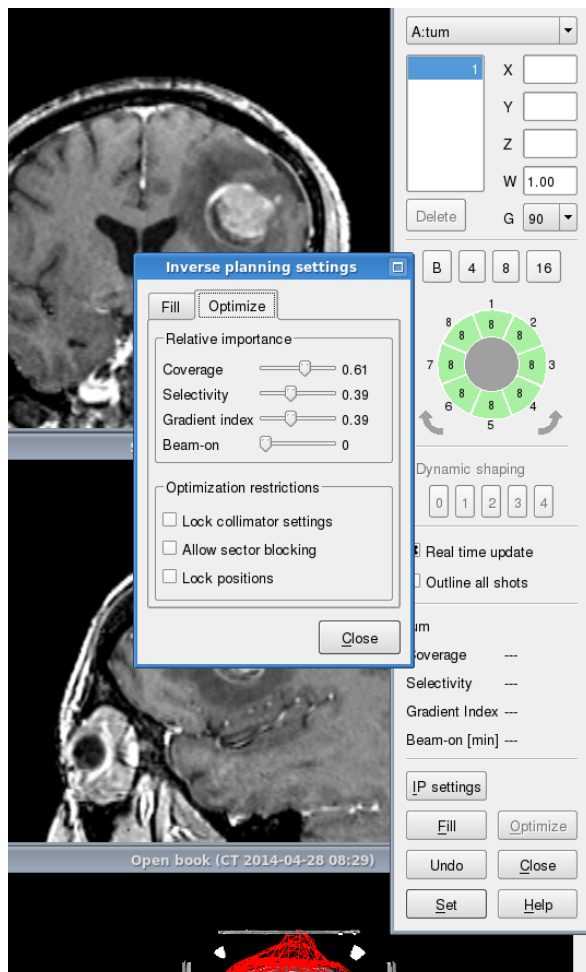
KULA treatment planning system  
Elekta, AB, plan circa 1994

## GammaPlan Treatment Planning



Doses are usually prescribed to 50% isodose line

## Gamma Knife “Inverse” Planning



Automatically fills a volume with isocenters

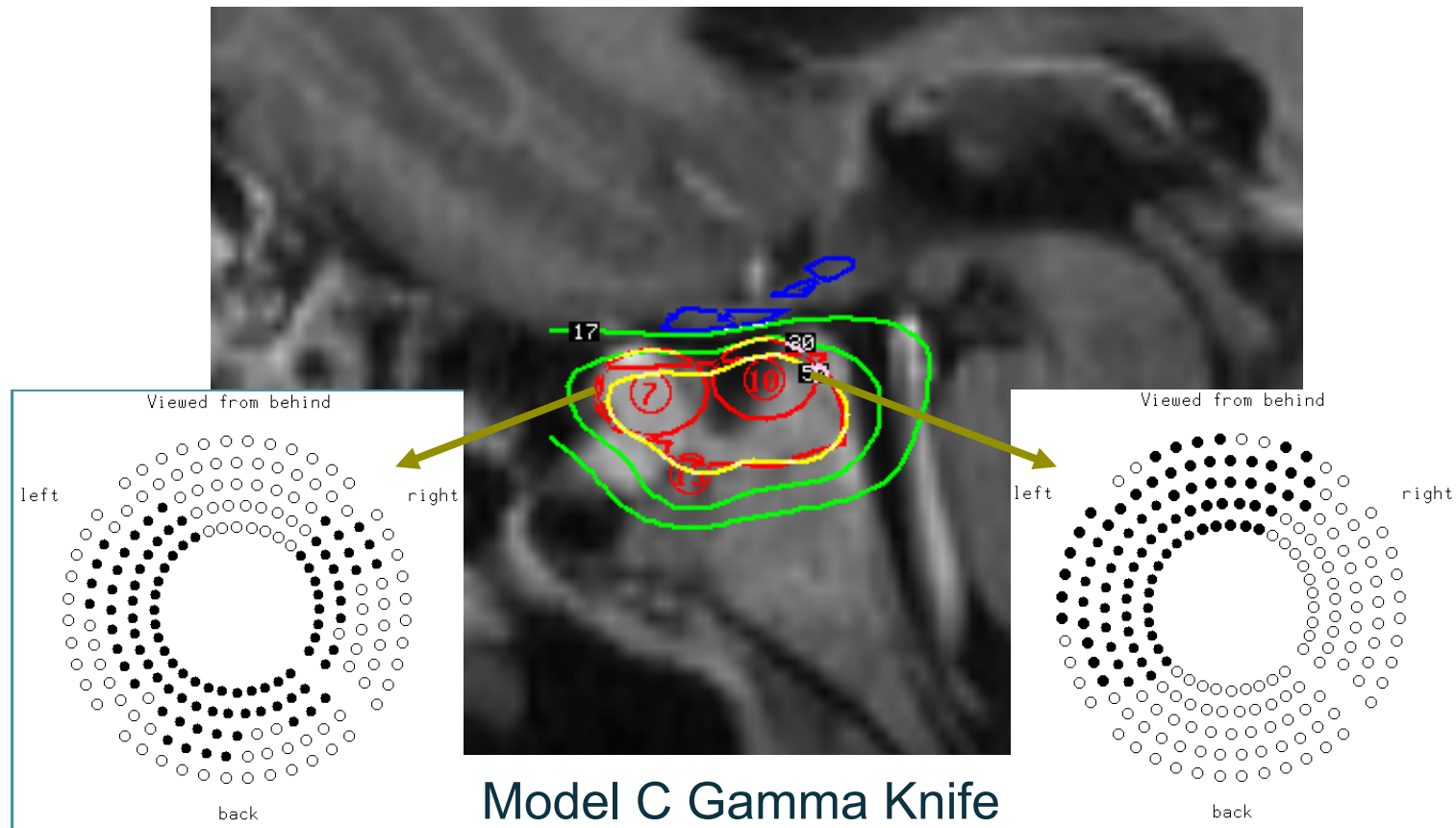
Optimizes against plan metrics such as coverage, conformity, dose falloff, and beam time

Dose NOT involve dose/volume constraints

Plan can be manually adjusted via typical forward-planning techniques

## Shielding – Protecting Critical Structures

- Combinations of plug patterns are applied to one or more isocenters
- Example: Isocenter #7 has a different optimal plug pattern than isocenter #10

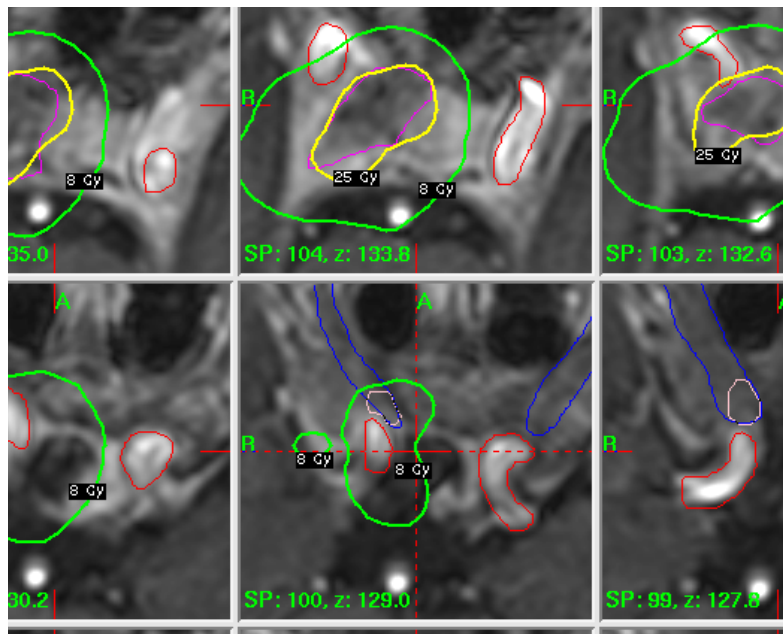




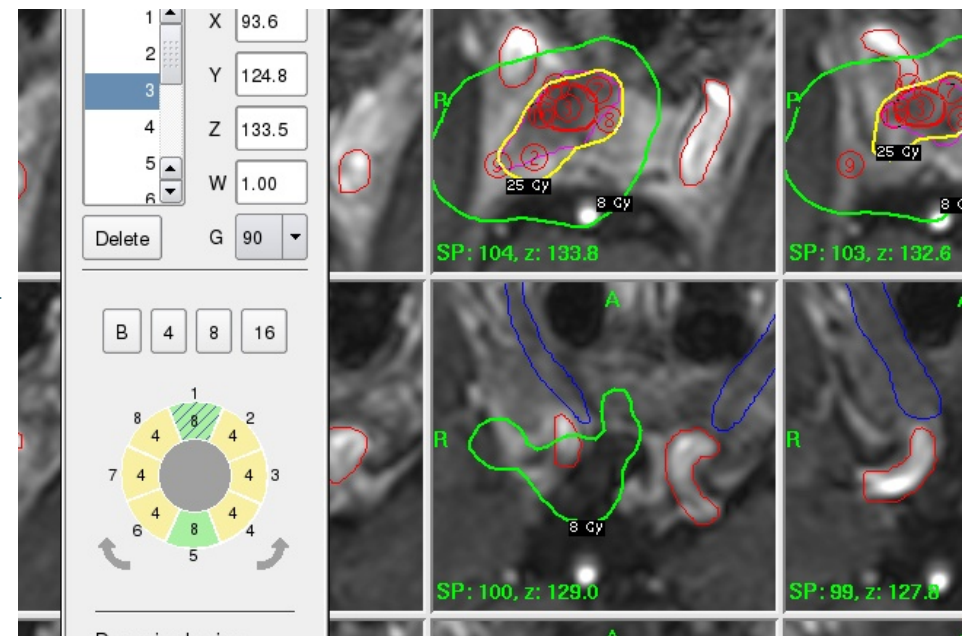
## Shielding on the Perfexion

- Shielding is an automated process.
- Effortless to use multiple shielding patterns
- However, can only shield at the level of a sector
- No annular shielding patterns

Before





After



## Evaluation – Conformity Index

$$CI = \frac{\text{Volume of target covered by PI}}{\text{Volume of PI}} \times \frac{\text{Volume of target covered by PI}}{\text{Volume of Target}}$$

 Overtreatment Ratio

 Undertreatment Ratio

CI = 1.0 represents perfect conformity

## Evaluation – Gradient Index

$$GI = \frac{\text{Volume of isodose that is } \frac{1}{2} \text{ of PI}}{\text{Volume of PI}}$$

Measures how quickly dose is dropping outside of target:

Example: If prescription isodose is at 60%, measure volume of 30% / 60%

**GI < 3.0 is “good” dose falloff**



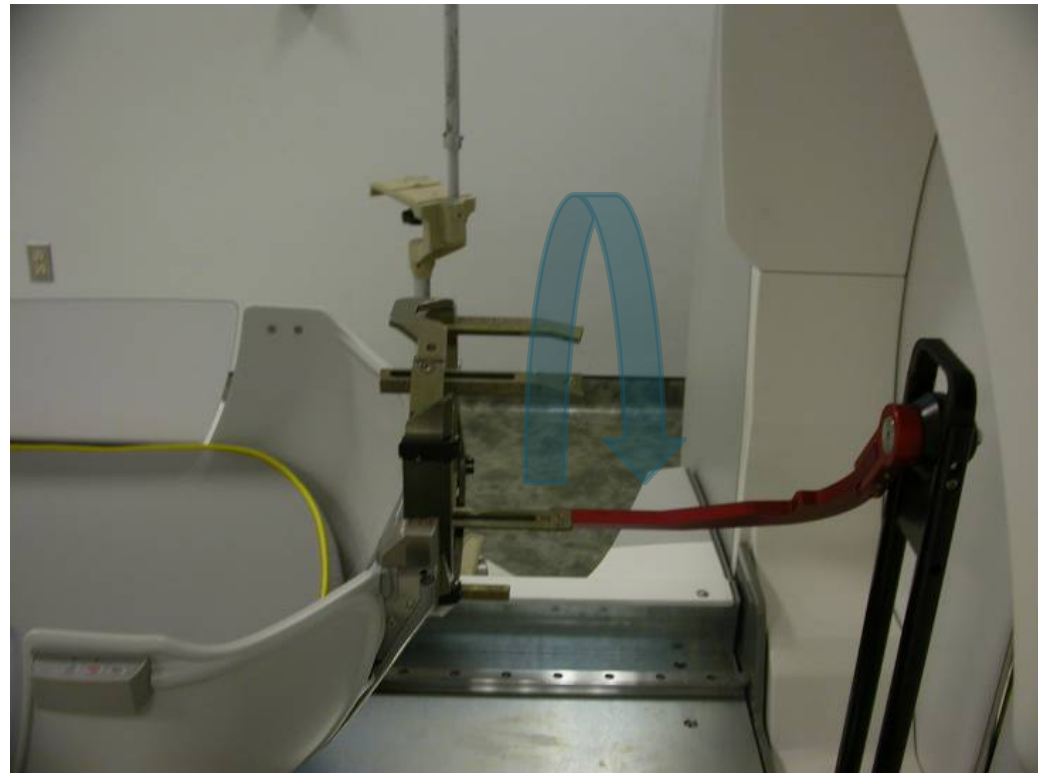
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## Preventing Collisions

Add picture  
Of space between  
helmet



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## Written Directives

UVA Gamma Knife Clinic Treatment Planning Protocol for <b>PERFECTION</b> <i>Leksell GammaPlan® 970</i>	Patient:	TEST_TLD
	Patient ID:	22233222111
	Diagnosis:	Trigeminal Neuralgia
	Plan ID:	20100715-020
	Approval Date:	2010-07-15
	Print Date:	2010-07-27
	Operator:	DJS
Gamma Knife:	AdV004 (AdV004)	

Approved for Treatment

\_\_\_\_\_ P  
 \_\_\_\_\_  
 \_\_\_\_\_ O

### Gamma Knife Data

Calibration dose	3.196 Gy/min at 2007-09-12
Days since calibration at approval date	1037
Treatment dose rate (2010-07-15)	2.198 Gy/min
Effective output factors (4, 8, 16)	0.805 0.924 1
Ring 1 output factors (4, 8, 16)	0.799, 0.957, 0.961
Ring 2 output factors (4, 8, 16)	0.815, 0.946, 1.000
Ring 3 output factors (4, 8, 16)	0.792, 0.901, 0.986
Ring 4 output factors (4, 8, 16)	0.725, 0.808, 0.920
Ring 5 output factors (4, 8, 16)	0.663, 0.730, 0.851

### Frame Configuration

Leksell® Coordinate Frame G

### Treatment Data

Target	Shots	Prescription	100% [Gy]	Max [Gy]	X [mm]	Y [mm]	Z [mm]	Grid [mm]
A: test	1	6.0 Gy @ 99%	6.1	6.1	100.0	100.0	100.0	0.9
Total number of shots: 1								
Treatment plan name: Plan1								
Beam-on time: 2.7 min								

### Run 1 (90 degrees)

Run-Step	Shot	X [mm]	Y [mm]	Z [mm]	Collimator [sectors 1-8]	Time [min]	Notes
1-1	A1	100.0	100.0	100.0	16 16 16 16 16 16 16 16	2.73	

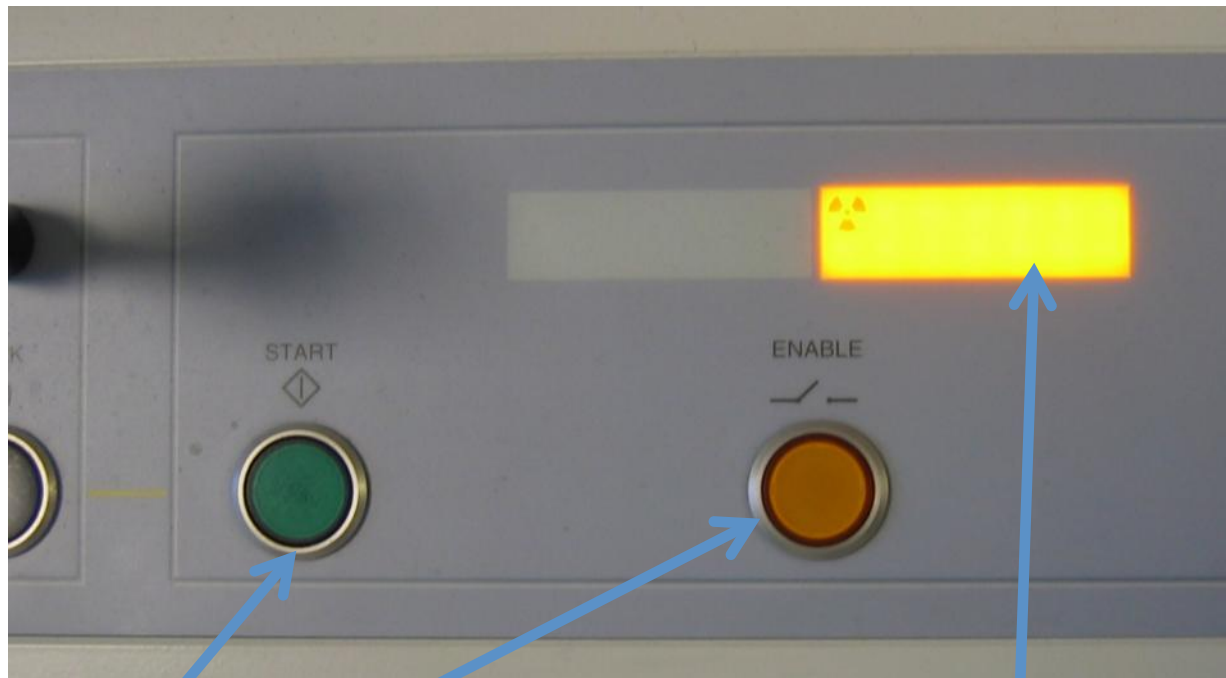
- Treatment plan serves as a “written directive”
- Official record of the prescribed treatment
- Must be signed and dated by the AU, AMP, and neurosurgeon before treatment
- AU and AMP required to be present (in normal voice range) throughout the treatment!

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## (Finally) Push “Go”



2 “Go” Buttons

Radiation light indicator comes on (or flashes) in any state where radiation may exist in room

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## Monitor Treatment

- Check off shots as they happen
- Watch to make sure each shot ends at the correct time
- Watch patient to make sure they are not in distress
- Notice that the correct side of patient's head is at isocenter



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History of the Gamma Knife  
Design and Physical Principles  
Treatment Procedures  
**Acceptance/Commissioning/QA**  
Recent/Future Developments



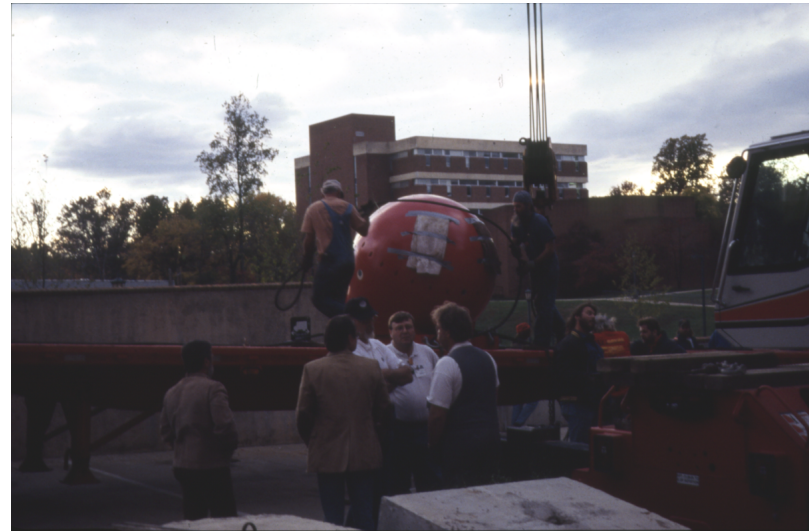
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## Loading / Reloading (the old way)



Model U unit had to be loaded  
somewhere remote using a crane.

Reloads required removing the unit  
from the building entirely!

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## The modern way is much less trouble....

- Loading performed in-room
- Loader weighs several tons
- Manipulator arms are used to assemble each source bushing





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## But...still requires detailed planning!



Still a 3-4 week  
process!

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## Acceptance

Contractual performance obligations (initial dose rate, etc.)

Tests usually performed by vendor

Signoff by receiving physicist and others

## Commissioning

Determine the baseline characteristics of the unit (output, output factors, end-effects, etc.)

Generate confidence in the safety of the unit

Performed by receiving physicist (NOT vendor)

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## ELEKTA INSTRUMENT AB

### Work Instruction

Article No 1002420	Doc No 1002420	Revision 07	Page/page(s) 23/51
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#	Action:	Expected Response:	Pass	Fail	Fault ID:
3.	Select 8 mm collimator size Diode Type Centre Note the result :	Service completed PPS precision radial within 150 microns  X: 11 Y: -28 Z: 5 Rad: 30	<input checked="" type="checkbox"/>	<input type="checkbox"/>	
4.	Select 16 mm collimator size Diode Type Centre Note the result: Disconnect the cable to the centre diode	Service completed PPS precision radial within 150 microns  X: 35 Y: -16 Z: -7 Rad: 39	<input checked="" type="checkbox"/>	<input type="checkbox"/>	
5.	Connect the cable for the long diode position. Make sure that the cable will be able to follow the movements of the PPS without risk of getting tangled.  Select 4 mm collimator size Diode Type Long Note the result: Disconnect the cable to the long diode	Service completed PPS precision radial within 300 microns Each axis within 200 microns  X: -25 Y: 21 Z: 51 Rad: 60	<input checked="" type="checkbox"/>	<input type="checkbox"/>	
6.	Connect the cable for the short diode position. Make sure that the cable will be able to follow the movements of the PPS without risk of getting tangled.		<input checked="" type="checkbox"/>	<input type="checkbox"/>	

All of the checks on this page performed:	Initials: 20	Date: 4/10-11
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# Acceptance

- Source inventory
- Dose rate verification
- Isocenter verification
- Positioning accuracy
- Communications / networking
- TPS configuration
- Field size verification
- Sector position measurements

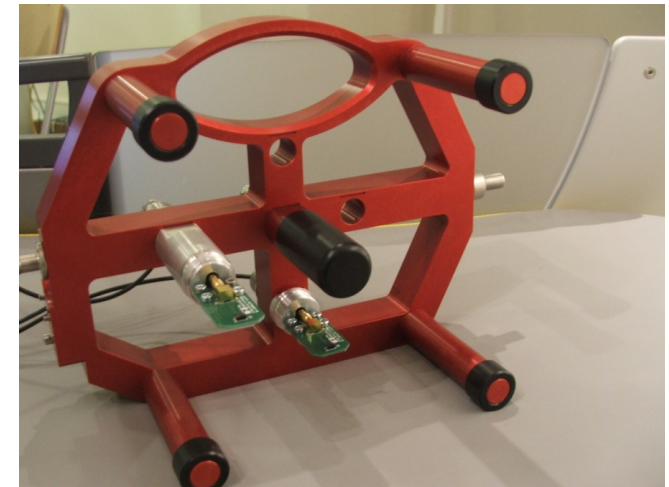
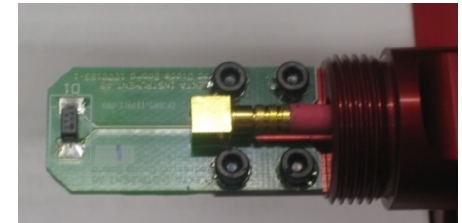
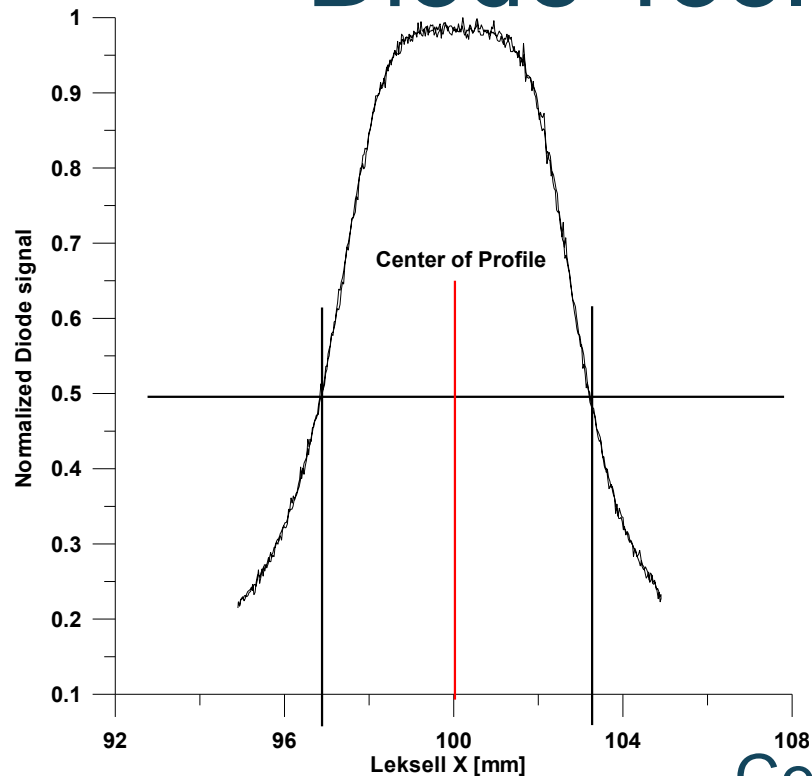


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## Installation (master) Diode Tool



Calibrated at “reference” unit  
at Timone Hospital, Marseille

Center diode < 0.08 mm repeatability  
at installation

## Site-specific diode tool



QA specification:  
 $\leq 0.5$  mm radial  
repeatability

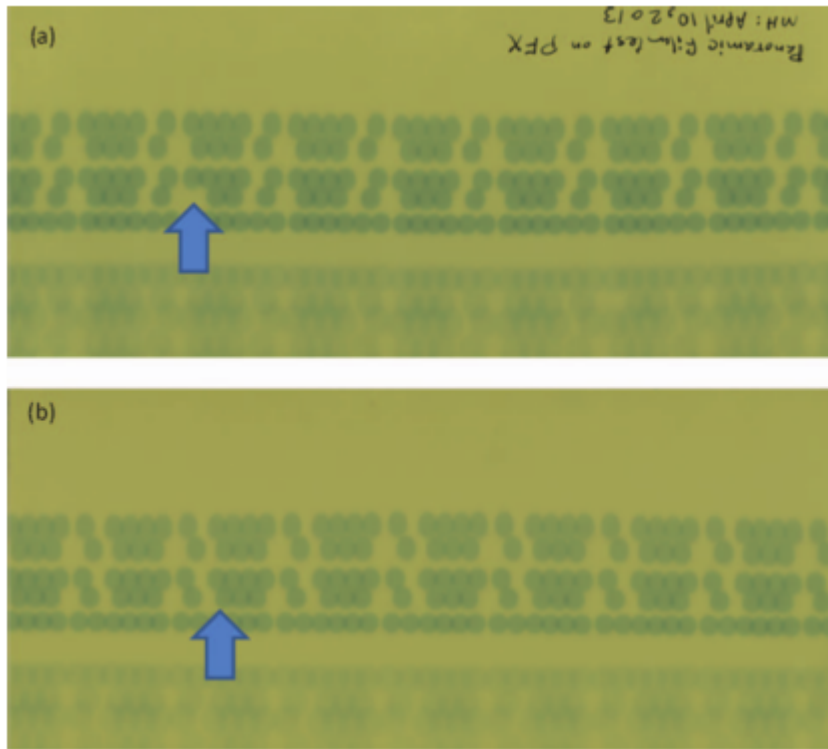
Has a calibrated offset from “master” diode tool  
Run at least 1 time per month by client site

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## Commissioning



Make sure you have all of your sources!  
Also, don't forget staff training!

Y. Chao, et al., Med Phys 40(9), 2013

- Radiation surveys
- Dose rate verification / calibration
- Output factor validation
- Beam alignment precision
- Beam accuracy
- Mechanical checks
- TPS accuracy
- Interlock tests
- Sector position measurements
- Updated OP notes / documentation

<http://www.nrc.gov/materials/miau/med-use-toolkit/perflexion-guidance.pdf>

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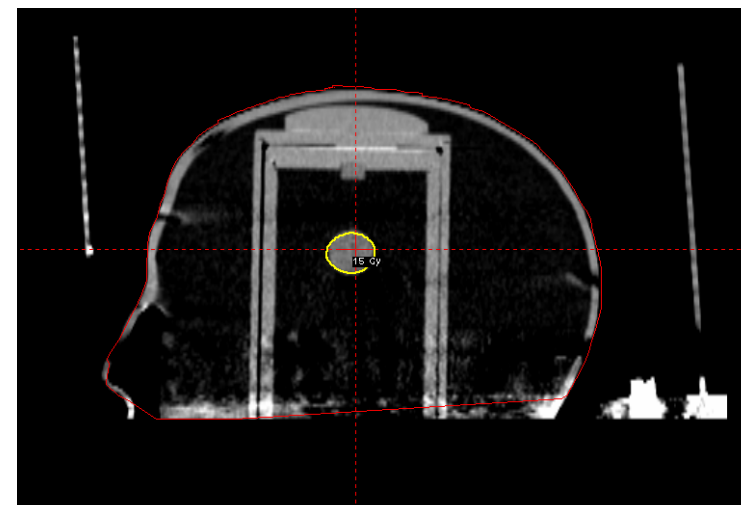
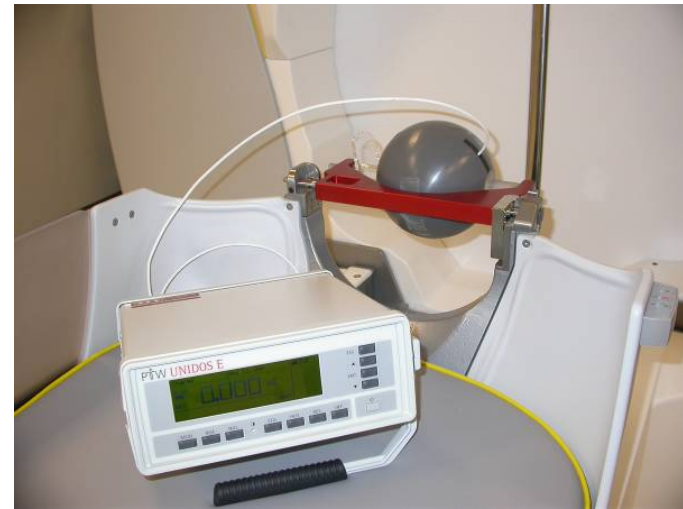
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## Output dose rate

- Only time you don't know the Gamma Knife dose rate is at initial commissioning and reload
- Probably the most important measurement you take
- There is no single standard for GK output calibration (TG-21, TG-51, IAEA TRS398, etc.)
- Use multiple methods and compare
- Watch for report of TG 178

**BE CAREFUL!!!!**



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## Quality Assurance (Perfexion)

Daily	Monthly	(Semi) Annually
-Radiation monitors	-Output check	-Surveys
-Survey meters	-Timer check	-Wipe tests
-NRC postings	-Linearity check	-Film tests
-Alarms	-Diode checks	-Other
-Interlocks	-Power supply	mechanical
-Basic morning QA test	-Clearance check tool	checks
		-TPS checks



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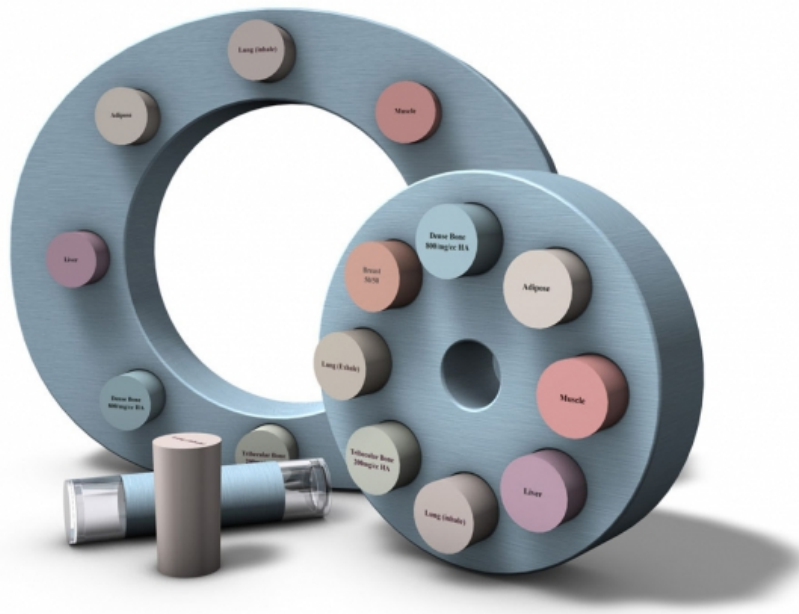
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## New: Convolution algorithm

$$\text{Dose}(\mathbf{r}) = \iiint \text{TERMA}(\rho - \mathbf{r}') \text{Kernel}(\rho \cdot (\mathbf{r} - \mathbf{r}')) d^3(\mathbf{r}')$$

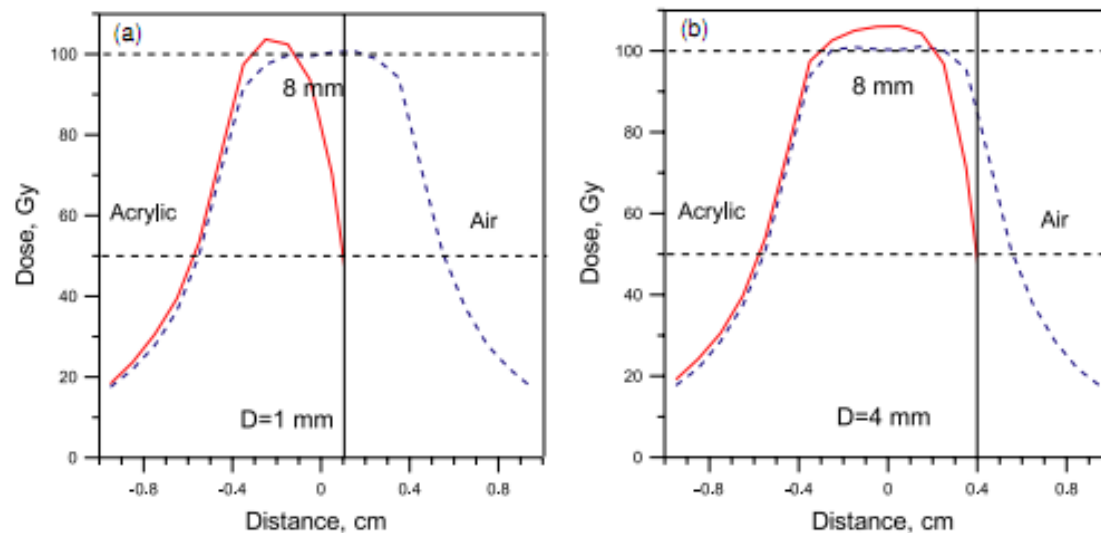


- Allows correction for tissue inhomogeneity
- Requires a calibrated CT scan

CIRS Model 062 electron density phantom

<http://www.cirsinc.com/products?show=modality&id=24>

## Why consider convolution?



**Figure 6.** Dose profiles in the direction perpendicular to the air-tissue interface for homogeneous (dashed lines) and heterogeneous (solid lines) phantoms. A collimator of 8 mm is used for computations. The positions of the isocentre were selected at 1 mm (a) and 4 mm (b) from the interface. In the case of area 2 (see figure 1), the isocentre is marked as 'A' in figure 2. *D* indicates the distance from isocentre to the interface.

- ~7% underdose of regions adjacent to air interface
- Dose away from cavity is under-attenuated, so overdose regions further from cavity

Moskvin, et al., Monte Carlo simulation of the Leksell Gamma Knife: II. Effects of heterogeneous versus homogeneous media for stereotactic radiosurgery, *Phys Med Bio* 49(21), 2004.

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Fractionated stereotactic radiotherapy with the Leksell Gamma Knife:  
feasibility study.

G. Simonová, et. al., Radiother Oncol, 37(2), 1995.

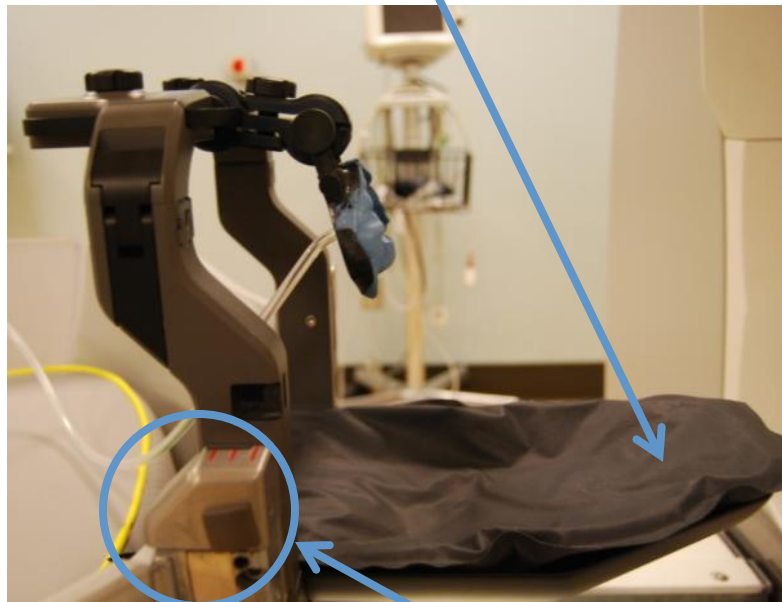


- 48 patients in series
- Frames kept on 2-6 days
- 1 fraction / day

UVA Gamma Knife (patient consented to photo use)

# Extend frame system

Vac-loc  
headrest



Interface to  
bed/positioning  
system

Patient-  
specific  
frame

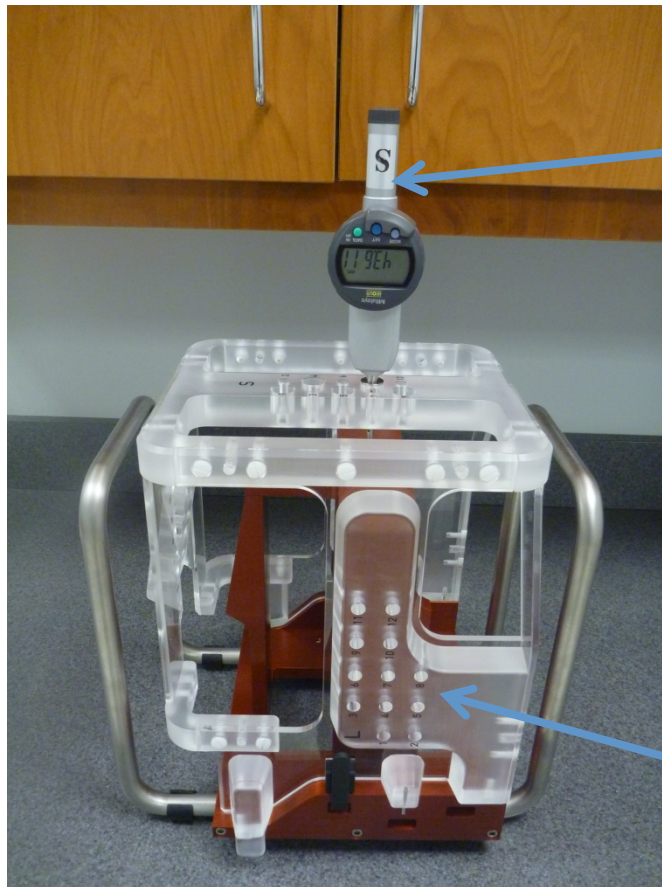


Vacuum  
tube (to  
pump)

Mouthpiece



## Reposition Check Tool (RCT)

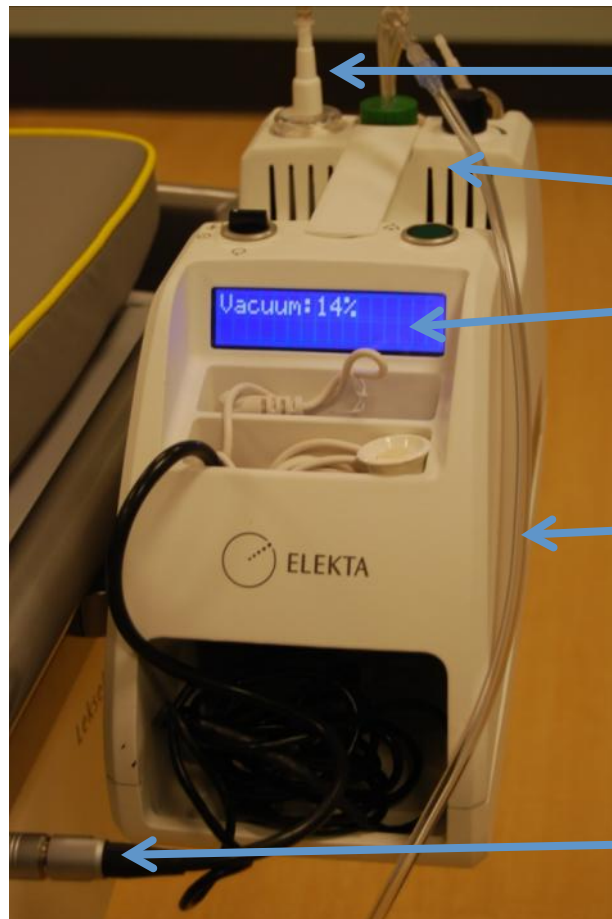


C150XB

- Mitutoyo Corporation
- Resolution: 0.001 mm
- Accuracy: < 0.006 mm
- Repeatability: < 0.002 mm
- We found 0.006-0.06 mm

Reposition check  
tool (RCT)

## Patient Control Unit (PCU)



Saliva guard and  
bacterial filter

Display and  
controls

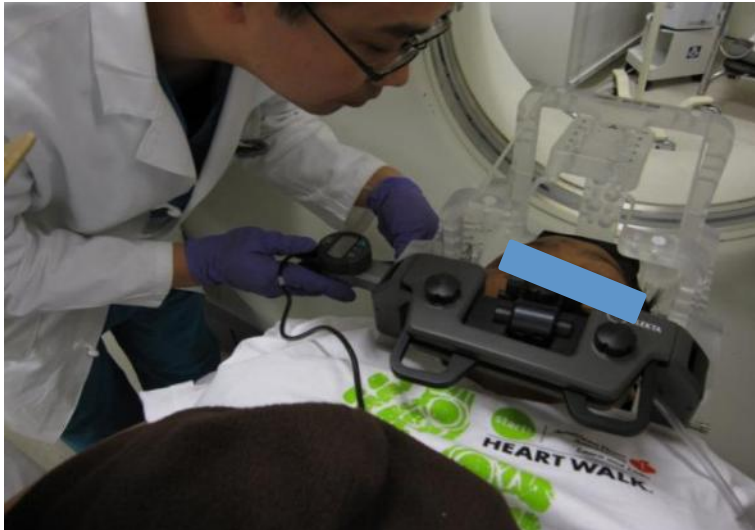
Vacuum tube  
(from  
mouthpiece)

Interface to  
Gamma Knife

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Reference  
← measurements taken at  
time of CT imaging

Patient position measured at GK  
before each fraction. Patient →  
repositioned to match reference  
measurements.



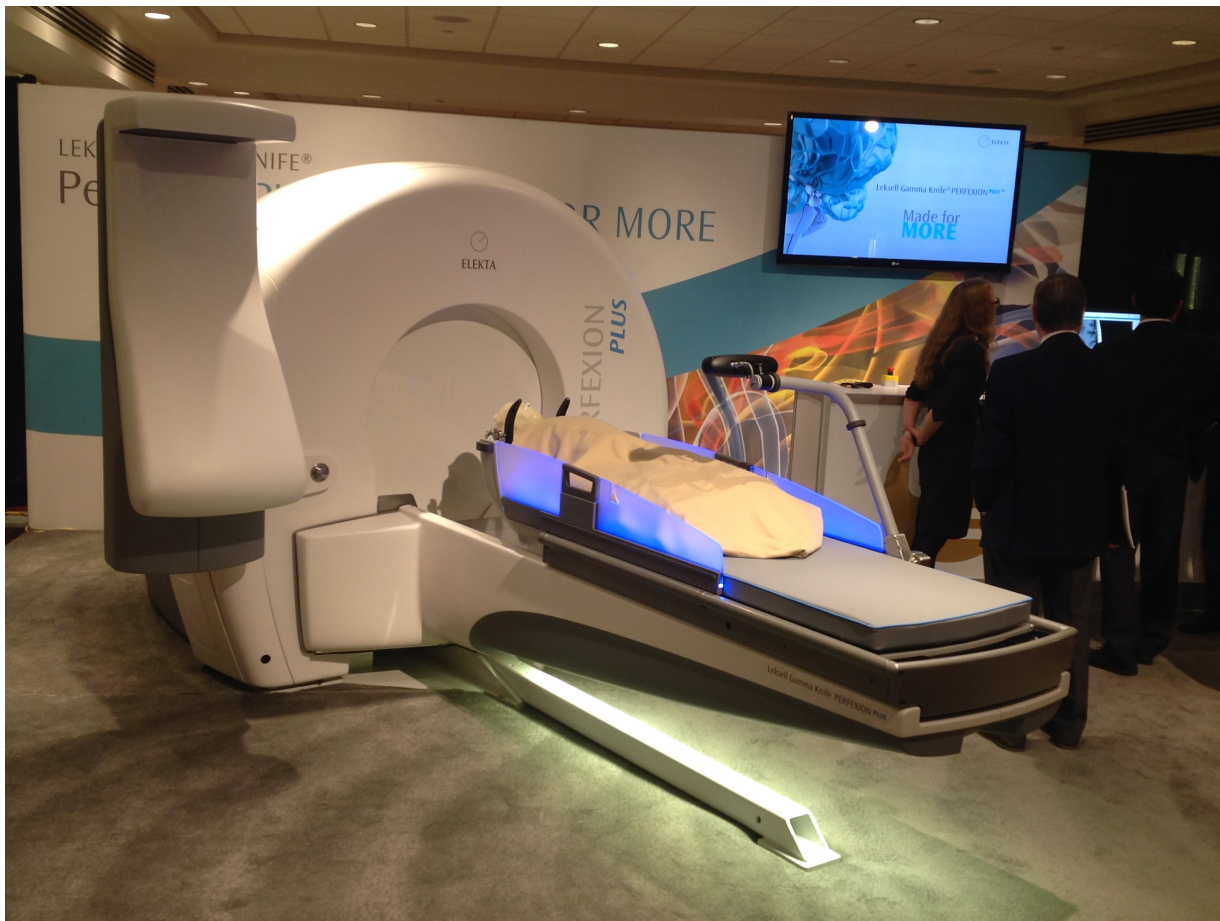


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## Gamma Knife Perfexion *Plus*



CBCT image guidance

Optical motion tracking  
and gating

Compatible with G-  
frame, Extend Frame,  
or thermoplastic mask

Expected release in  
2015

## Summary | Conclusions

The design of the Gamma Knife was in direct response to specific requirements of intracranial radiosurgery.

After almost 50 years of development, it remains an elegant solution to the problem.

Future developments will further decrease treatment uncertainty and add treatment flexibility.



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### Historical

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Stereotactic Radiosurgery and Stereotactic Body Radiation Therapy, S. Benedict, D, Schlesinger, S. Goetsch, B. Kavanagh, editors, CRC Press, Jul 2014.

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<http://www.nrc.gov/materials/miau/med-use-toolkit/perfexion-guidance.pdf>

M. Ruschin et. al., “Performance of a novel repositioning head frame for gamma knife perfexion and image-guided linac-based intracranial stereotactic radiotherapy”, *IJROBP* 78(1), 2010.

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## Acknowledgements

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Thomas Jefferson's Rotunda at the University of Virginia